Developments in AI model: 2D and 3D

14/03/25

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Sommario

Fase 2D

- Risultati finali
 - Modello, addestramento, gamma-analisi
- DEMO InTrEPID-2D system
- Paper per Radiotherapy & Oncology

Fase 3D

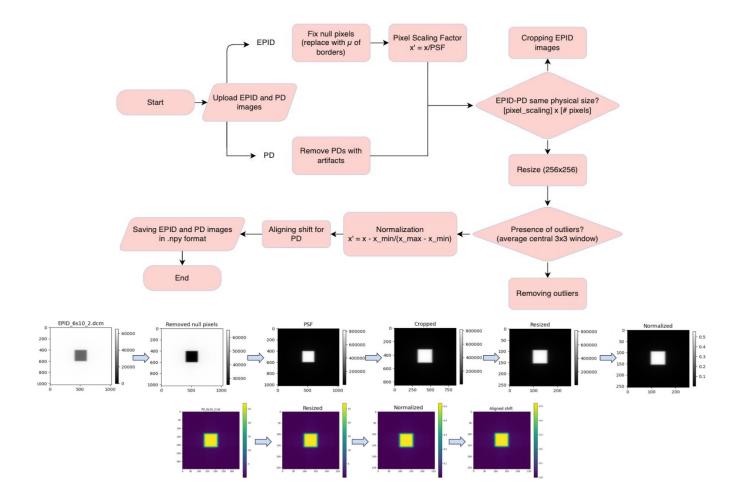
- Data exploration
- Coregistrazione CT-RTDOSE
- Qualche idea...

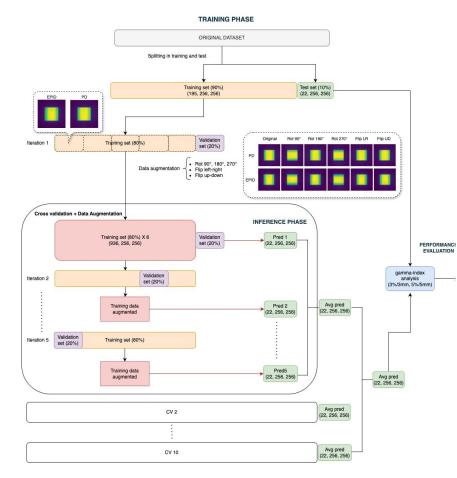
Fase 2D

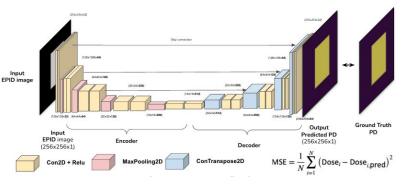
TEST SET

Area [cm ²]	OMG	CIRS	SLAB	MP	Tot
2×2	14	8	7		29
5×5	12	9	7	12	40
10×10	16	7	7	8	38
20×20	14	-	7	-	21
2×10	13	8	7	8	36
10×2	13	8	2	-	10
15×1	4	8	-	8	16
1×15	-	8	-	-	8
4×20	-		7	10	7
Ellipses	-	-	-	8	8

		QU	ADRATI		RETTANGOLI					CERCHI/ELLISSI
Phantoms	2x2 cm^2	5x5 cm^2	10x10 cm^2	20x20 cm^2	2x10 cm^2	10x2 cm^2	15x1 cm^2	1x15 cm^2	4x20 cm^2	
Omogeneus	6s10b3_1	6s30b1_2	6s10b2_3	6s20_4	6s10b2_6				SLABBone _5	
CIRS		_	CIRS_Ogradi _ISOlesione _3		CIRS_270gra di_ISOcentro _6					
SLAB	SLABinho mAir2_1	SLAB_Bo neb2_2sl ab_2	SLABBone_ 3	SLAB_Bone _2slab_4	SLABinhomA ir2_6					
Multi_Plug		Multiplug _90g_5c m_ARIA_ 2	Multiplug_P MMA_90g_ 3		Multiplug_P MMA_180g_ 6		Multiplug_ Ti_90g_8			Multiplug_Ti_t ondo_1E0g
# images	3	4	4	2	4	1	2	1	1	1







Hyperparameter Optimization

A **GS** approach was implemented to find out the best hyperparameter configurations: # filters: [8, 16], learning rate: [0.01, 0.001, 0.0001], batch size: [4, 8, 16, 32] \rightarrow 24 different configuration!

Cross-Validation Strategy

To improve generalization and reduce overfitting, **10 CV** schemes were applied. Each training: **150 epochs** per model, **5-fold CV** per training

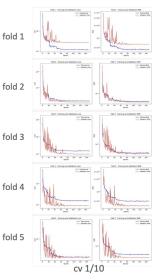
Ensemble Learning

An EL approach was adopted <u>by averaging the</u> <u>predictions of the best models from each</u> <u>training run</u>.

Hardware

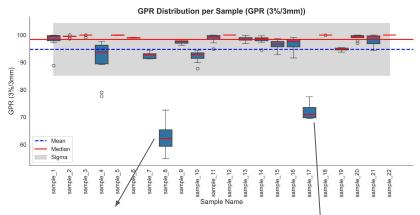
The training process was conducted using the <u>NVIDIA V100 Tensor Core GPU</u> of the **Computing Center of the INFN - Pisa division**.

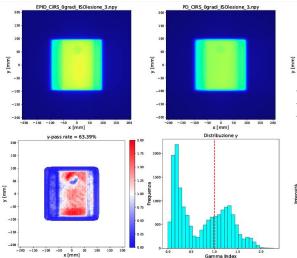
f16, lr0.001, bs8



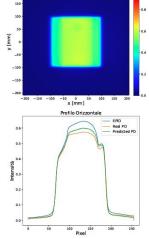
100 R 90 0 0 GPR (3%/3mm) f16 lr0.001 bs8 80 Median μ σ 00 95,02245 9,16085 cv 1 98,13686 cv_10 94,50223 97,91041 9,44479 CV 2 95,04624 98,51857 9,49802 95.59046 98,45063 8,04998 CV_3 70 cv_4 94,6782 98,75133 10,43327 CV_5 94,89045 98,84238 9,48046 93,95543 97,81283 10,10313 CV 6 CV 7 93,99619 98,39791 10,21614 CV 8 94,72434 98,09562 8,98636 Mean 60 cv 9 95,00334 98,36919 9,14435 Median σμ u Sigma 94,740933 0,1569932785 sample_3 sample_13 sample_2 sample_4 sample_5 sample_6 sample_7 sample_8 sample_9 sample_10 sample_11 sample_12 sample_14 sample_15 sample_16 sample_17 sample_18 sample_19 sample_20 sample_21 sample_22 sample_ Sample Name

GPR Distribution per Sample (GPR (3%/3mm))

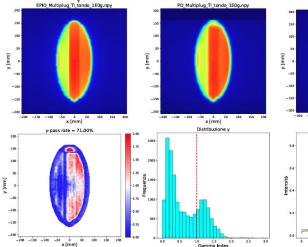


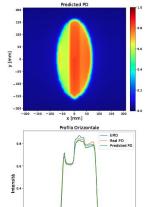


0.0 0.5 1.0 1 Gamma Index 1.5 2.0



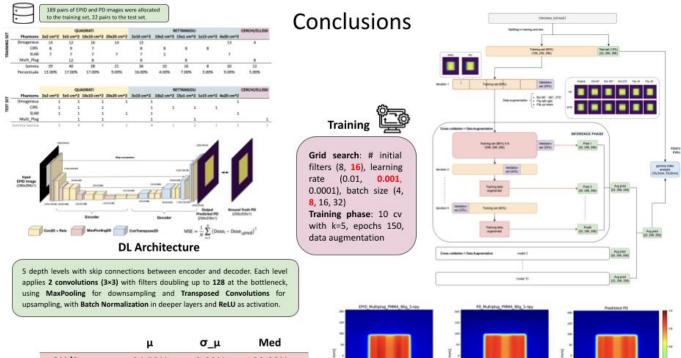
Predicted PD

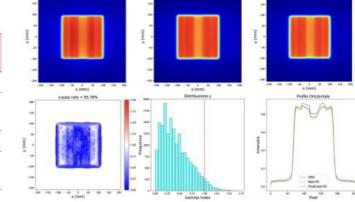




100 150

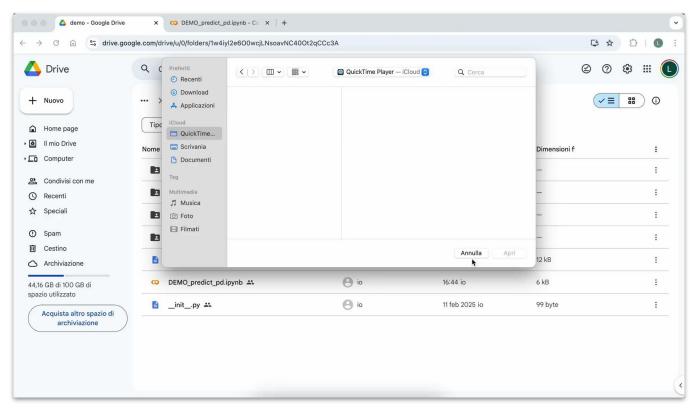
Pixel





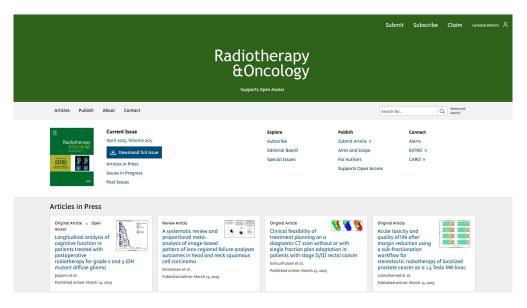
		μ	σ_μ	Med	
	3%/3mm	94,53%	2,08%	98,00%	
a)	5%/5mm	99,55%	0,25%	100,00%	
		μ	σ_μ	Med	
,	3%/3mm	92,45%	2,42%	98,00%	
)	5%/5mm	99,27%	0,48%	100,00%	
-		μ	σ_μ	Med	
,	3%/3mm	92,21%	2,59%	98,00%	
c)	5%/5mm	98,44%	1,33%	100,00%	

DEMO 2D-InTrEPID system



https://drive.google.com/drive/folders/1w4iyl2e6O0wcjLNsoavNC40Ot2qCCc3A?ths=true

Paper



Link alla rivista: https://www.thegreenjournal.com/

Link a overleaf: https://www.overleaf.com/project/67c18a3d64c68a9c0a426c58

Per essere aggiunti, chiedere ad @Alessandra

6 pagine, 6 figure. Manca qualche autore??

Deep learning methods for transit dosimetry with EPID images

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"University of Pias, Department of Computer Science, Pian, Italy "Initian Washington & Takisa Nactions (INIX), Pian Davision, No., Italy "Centre & Referience Densinging (RDR) & Aviens, Forence, Italy "Department of Experimental and China's Biomedical Science Monisory of Florence, Pineteee, Italy "Initiane Nacional et al. Takisa Nucleary (INFN), Section of Florence, Florence, Italy "Initiane Nacional et al. Takisa Nucleary (INFN), Section of Florence, Italy "Agende Organismo", Italy (INFN), Section of Thomas, Italy "Agende Organismo", Italy (INFN), Section of Thomas, Italy

Abstract

Background and Purpose: The complexity of external beam photon radiotherapy has significantly increased, leading to a higher risk of errors that require advanced systems for dose verification. Electronic Portal Imaging Devices (EPIDs), originally designed for patient positioning, have become essential tools for in-vivo dosimetry (IVD) and pre-treatment dose verification. Traditional dose reconstruction methods, such as physical models and Monte Carlo simulations, face limitations in complexity, computational power, and time-efficiency, hindering routine clinical use. Materials and methods: This study introduces a deep learning (DL) framework for 2D dose reconstruction using real EPID images acquired during treatment. A 2D U-Net model maps EPID images to water-equivalent portal dose images (PDIs), leveraging a database of 211 EPID-PD pairs obtained from phantoms with diverse material densities. The performance was evaluated through mean absolute error (MAE) metrics and 2D -analysis with a 3mm/3% and 5mm/5% criterion. Results: 2D framework achieved a predictive mean -passing rate of (94.53 ± 2.08)% and (99.55 ± 0.25)% for the 3mm/3% and 5mm/5% criteria, respectively. The median -passing rates across all test cases were 98.03% and 100.00%, demonstrating the model's robustness across different scenarios. The dose predictions completed within 1 second, significantly faster than TPS calculations (=20-30 minutes). Conclusions: Deep learning enables real-time, accurate dose reconstruction from EPID images, demonstrating its potential for in-vivo treatment verification. This work highlights the performance of the 2D model, emphasizing their clinical potentiality in radiotherapy.

Keywords: EPID, Transit dosimetry, Radiotherapy, Deep Learning, U-Net

1. Introduction w [4, 5, 6]. EPIDs measure X-ray fluence on an amor-17 phous silicon flat-panel detector, producing 2D digital · images containing dose information (the so-called Por-2 In the last decades, the complexity of external beam n tal Dose, PD). Therefore, a dose reconstruction is then 3 photon radiotherapy treatments has increased significantly [1]. However, due to the advancement in techniical models and Monte Carlo simulations. Nonetheless, cal complexity, the risk of errors has grown too requir-21 s ing sophisticated systems to ensure correct dose admin- 22 these methods have several limitations, due the comistration and verification [2]. Errors caused by equip- n plexity of the dose reconstruction algorithms, the com-24 puting power and the significant time-consuming, limitment malfunctioning, patient positioning or anatomiing their routine clinical use. 25 + cal changes must be promptly detected to prevent aca cidents and comply with the stringent EU dose verifica- 28 In this scenario, Artificial Intelligence, in particular tion guidelines [3]. 17 Deep Learning (DL), offers a promising alternative for Electronic Portal Imaging Devices (EPIDs), initially = IVD in radiotherapy [7, 8, 9]. By bypassing the tradia designed for real-time monitoring patient position- as tional physical models, DL can achieve Monte Carloing, have become the preferred tools for both in-vivo 20 level accuracy while maintaining the speed of a trained a dosimetry (IVD) and for pre-treatment dose verification a model. Most existing studies are mainly based on simu-Preprint submitted to Nuclear Physics B March 14 2021

Struttura del paper

1. Introduction

2. Materials and methods

- a. Experimental setup and data collection
- b. Preprocessing
- c. Deep learning model and training phase
- *d. Grid search, repeated k-fold cross-validation and ensemble learning*
- *e. Evaluation of the performance*

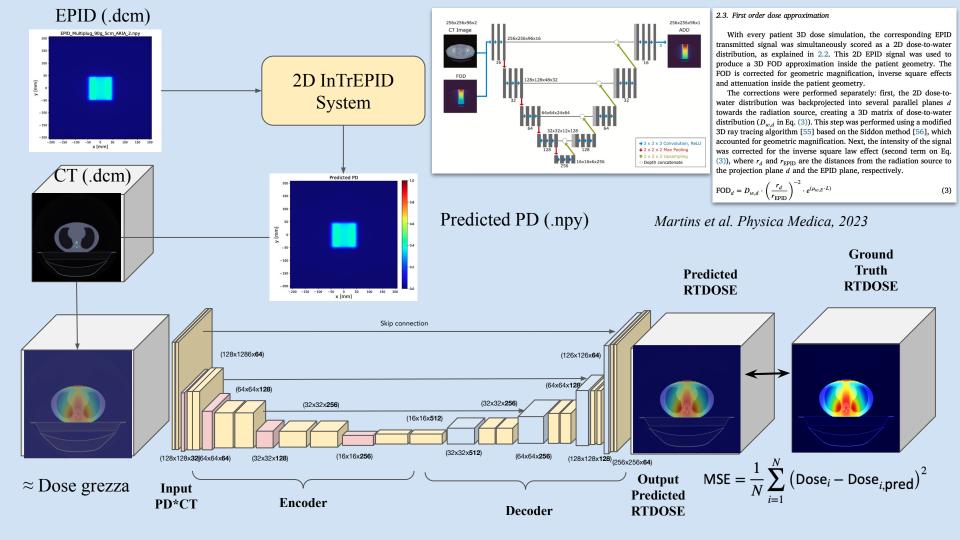
3. Results

- a. Dataset quality
- b. Model performance
- 4. Discussion
- 5. Credit authorship contribution statement
- 6. Declaration of competing interest
- 7. Acknowledgements
- 8. References

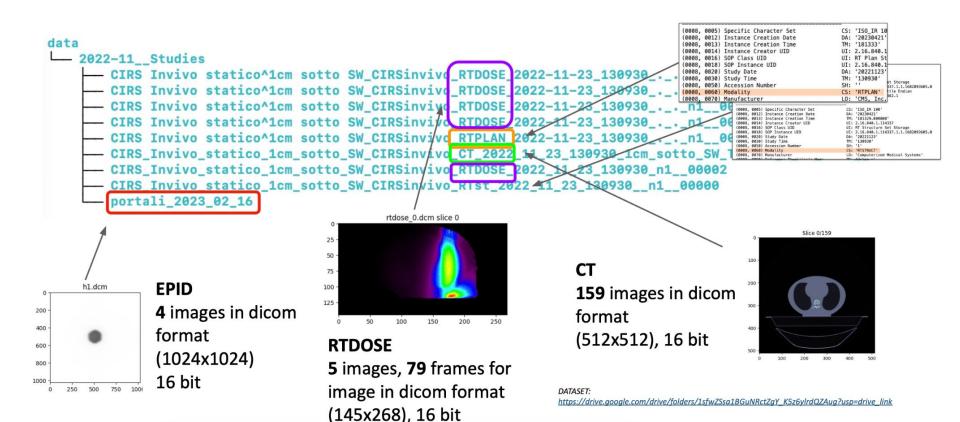
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244 ing phantoms with higher density gradients, where the 222
                                                                          [9] Li, Y., Xiao, F., Liu, B., Oi, M., Lu, X., Cai, J., Zhou, L., Song,
                                                                               T. Deep learning-based 3D in-vivo dose reconstruction with an
245 y-passing rate dropped below ???%. This suggests that 220
                                                                               electronic portal imaging device for magnetic resonance-linear
246 the model may struggle with more complex dose dis-
                                                                               accelerators: a proof of concept study. Physics in Medicine and
247 tributions, where important scatter effects or significant 248
                                                                               Biology, 66(23), 2021.
240 heterogeneities are present.
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                                                                               Networks for Biomedical Image Segmentation. Lecture Notes
                                                                               in Computer Science, vol. 9351, Springer, 2015.
                                                                         [11] Ioffe, S., Szegedy, C. Batch Normalization: Accelerating Deep
240 5. Credit authorship contribution statement
                                                                               Network Training by Reducing Internal Covariate Shift. arXiv
                                                                               preprint, arXiv:1502.03167, 2015.
        Lorenzo Marini:, Carlotta Mozzi:, Aafke C. Kraan:
                                                                    303 [12] Low, D. A., Harms, W. B., Mutic, S., Purdy, J. A. A technique
     , Michele. Avanzo: , Francesca Lizzi: , Alessandra 104
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Retico: , Icro Meattini: , Livia Marrazzo: , Cinzia Tala-
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                                                                               vestigation of parameters with a surface-based distance method
                                                                               Medical Physics, 38, 6730-6741, 2011.
        Declaration of competing interest
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                                                                         [14] Khan, F. M., Gibbons, J. P. Khan's The Physics of Radiation
                                                                               Therapy, Lippincott Williams Wilkins, 2014.
        The authors declare that they have no known com- 312
                                                                              Santos, T., Ventura, T., do Carmo Lopes, M. A review on ra-
    peting financial interests or personal relationships that 313
                                                                               diochromic film dosimetry for dose verification in high energy
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                                                                               EBT3 films for patient specific IMRT QA using a multichannel
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220 7. Acknowledgements
                                                                               approach. Physica Medica, 31(8), 1035-1042, 2015.
                                                                    310
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                                                                               Gargiulo, L., Azario, L., Piermattei, A. Correlation functions
        This research was partly funded by the In-
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                                                                               for Elekta aSi EPIDs used as transit dosimeter for open fields.
TrEPID project (MUR PRIN 2022CWXR8K - CUP 522
                                                                               Journal of Applied Clinical Medical Physics, 12(1), 218-233,
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          imaging for radiotherapy dosimetry. Radiotherapy and Oncol-
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          lation and deep learning-based modeling of EPID detector re-
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          Chan, M. F., Witztum, A., Valdes, G. Integration of AI and Ma-
          chine Learning in Radiotherapy QA. Frontiers in Artificial In-
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telligence, 3, 2020.

Fase 3D



Data exploration 3D



Coregistrazione

How does 3D Slicer overlay the RTDOSE and Image data in the correct position?

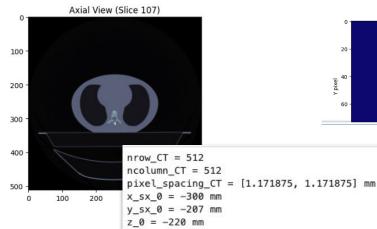
Support python dicom extensions-manager registration slicerrt

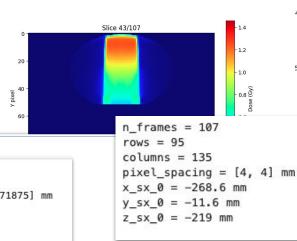


I'm currently an MS student in Medical Physics and I have a great need to be able to overlay an isodose distribution from an RTDOSE file onto a CT image from a .dcm file set.

I've managed to extract the image and the dose pixel arrays myself using pydicom and dicom_numpy, but the two arrays are not the same size! So, if I overlay the two together, the dose will not be in the correct position based on what the Elekta Gamma Plan software exported it as.

I've played around with slicerrt and it obviously is able to do this even though the arrays are not the same size. However, I think I cannot export the numerical data when using slicert...I can only scroll through and view it as an image. What section of the code has the algorithm for overlaying the RTDOSE to an image?





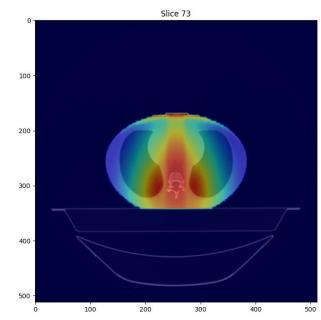
Oct 2019

Sep 2023

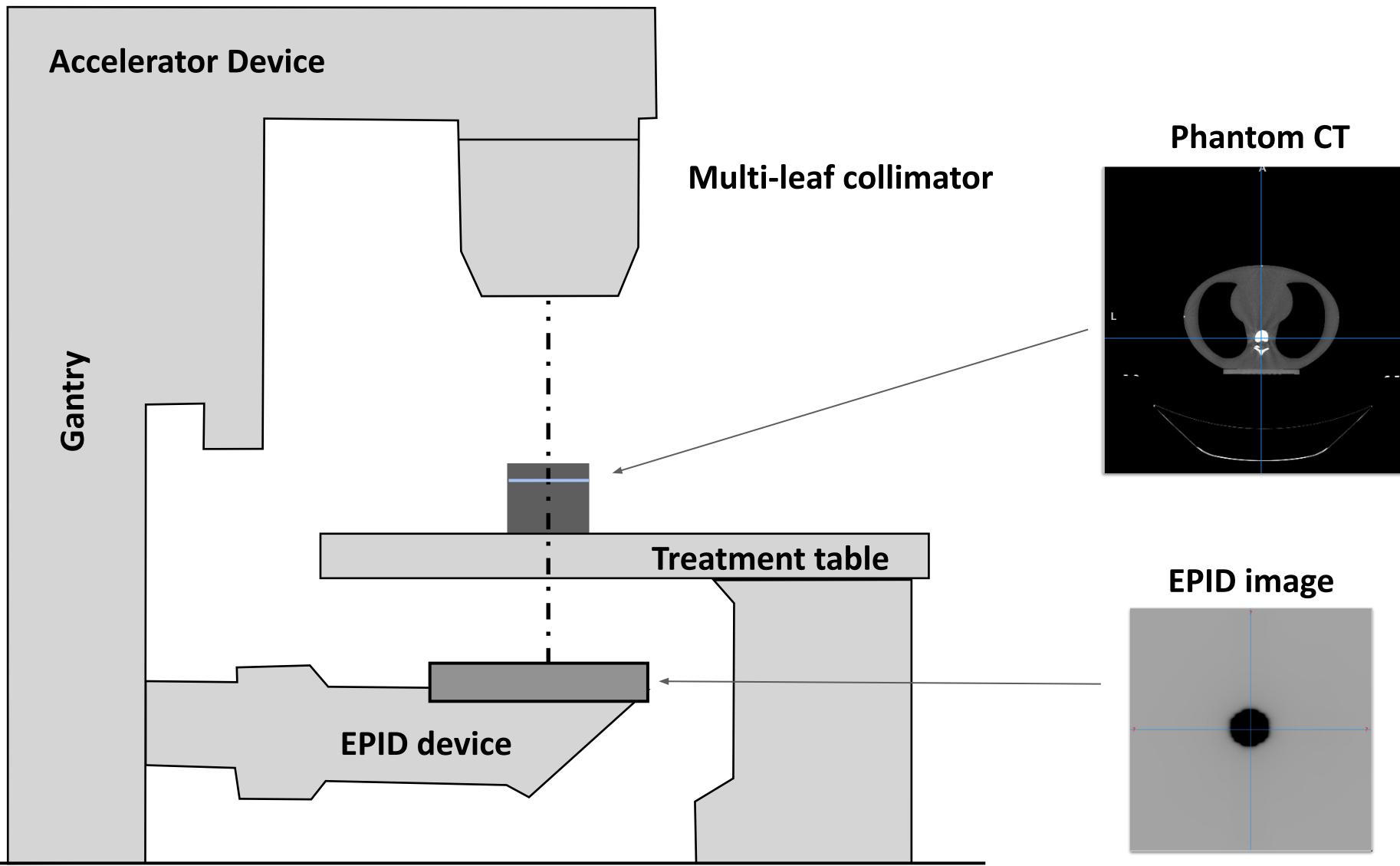
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Oct 2019

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Experimental setup





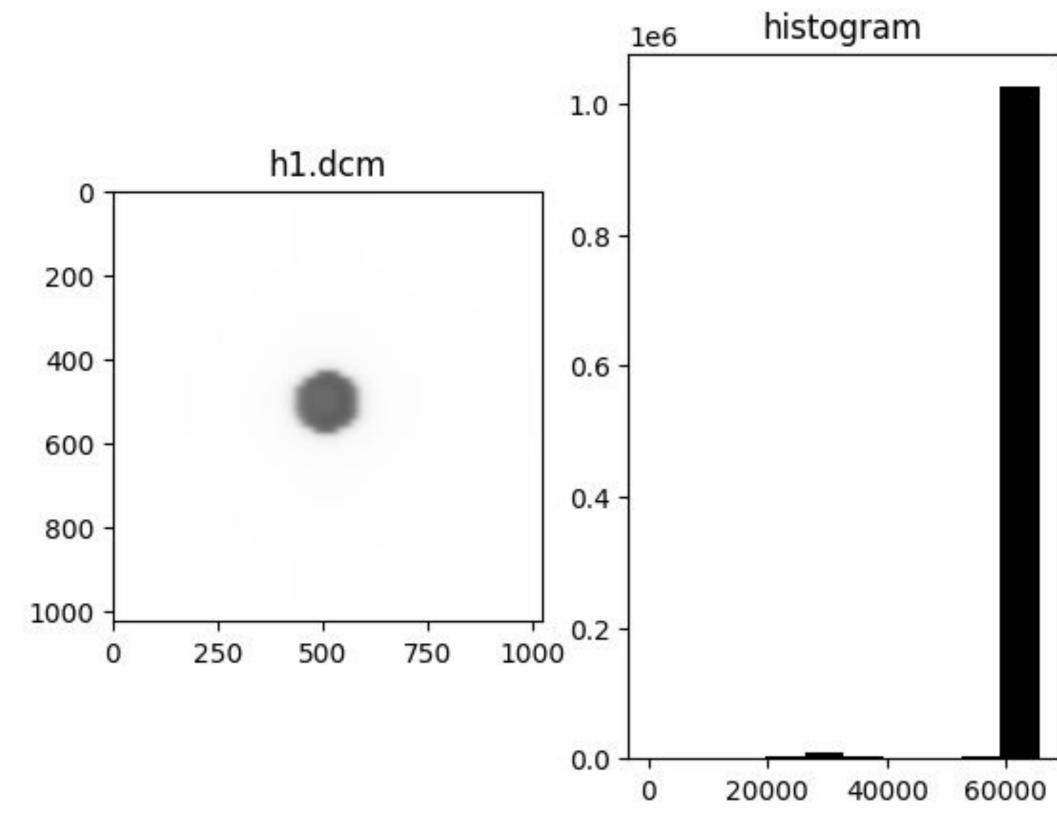




table]	EPID image
		,

(0020,	0011)	Series Number	IS:	'10517'
(0020,	0013)	Instance Number	IS:	'10521'
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(0020,	1002)	Images in Acquisition	IS:	'1'
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(0021,	1002)	Private tag data	DS:	'0.0937319'
(0028,	0002)	Samples per Pixel	US:	1
(0028,	0004)	Photometric Interpretation	CS:	'MONOCHROME2'
(0028,	0010)	Rows	US:	1024
(0028,	0011)	Columns	US:	1024
(0028,	0100)	Bits Allocated	US:	16
(0028,	0101)	Bits Stored	US:	16
(0028,	0102)	High Bit	US:	15
(0028,	0103)	Pixel Representation	US:	0
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(0028,	1051)	Window Width	DS:	'22555.1'
(3002,	0002)	RT Image Label	SH:	'iViewPortalImage'
(3002,	000a)	Reported Values Origin	CS:	'OPERATOR'
(3002,	000c)	RT Image Plane	CS:	'NORMAL'
(3002,	000e)	X-Ray Image Receptor Angle	DS:	'0.0'
(3002,	0011)	Image Plane Pixel Spacing	DS:	[0.405, 0.405]
(3002,	0012)	RT Image Position	DS:	None
(3002,	0020)	Radiation Machine Name	SH:	11
(3002,	0022)	Radiation Machine SAD	DS:	'1000.0'
(3002,	0024)	Radiation Machine SSD	DS:	'0.0'
		RT Image SID	DS:	'1600.0'
(300a,	00b3)	Primary Dosimeter Unit	CS:	
(300a,	011e)	Gantry Angle	DS:	'-0.1'
(7fe0,	0010)	Pixel Data	OW:	Array of 2097152 elemen

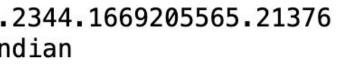
See: DICOM Standard Browser



nents

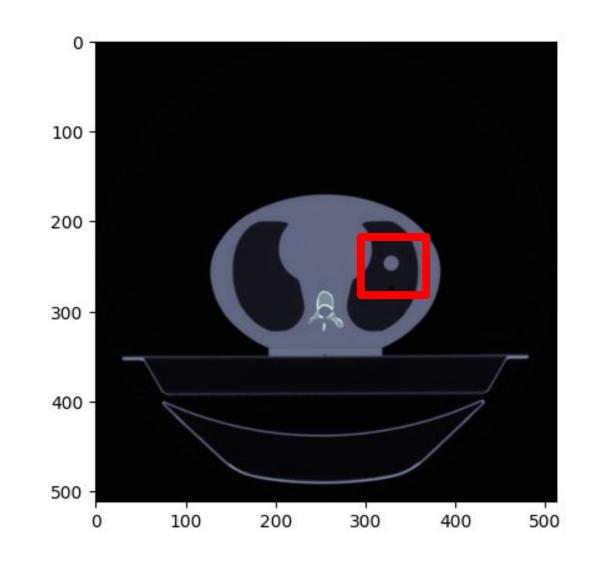


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(0002,	0003)	Media Storage SOP Instance UID	UI:	1.2.840.113704.1.111.23
(0002,	0010)	Transfer Syntax UID	UI:	Explicit VR Little Endi
(0002,	0012)	Implementation Class UID	UI:	2.16.840.1.114362.1
(0002,	0013)	Implementation Version Name	SH:	'MIM723M31402'
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(0008,	0023)	Content Date	DA:	'20221123'
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(0008,	0030)	Study Time	TM:	'130930'
(0008,	0032)	Acquisition Time	TM:	'131232'
(0008,	0033)	Content Time	TM:	'131233.985001'
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(0008,	0081)	Institution Address	ST:	'FIRENZE'
(0008,	0090)	Referring Physician's Name	PN:	11
(0008,	1010)	Station Name	SH:	'H0ST-7424'
(0008,	1030)	Study Description	L0:	'1cm sotto SW'
(0008,	103e)	Series Description	L0:	'TORACE 5 MM'
(0008,	1040)	Institutional Department Name	L0:	'Radioterapia DEAS_1'
(0008,	1070)	Operators' Name	PN:	11
(0008,	1090)	Manufacturer's Model Name	L0:	'Brilliance Big Bore'
(0008,	1140)	Referenced Image Sequence 1 item	(s) —	



/', 'AXIAL', 'HELIX']

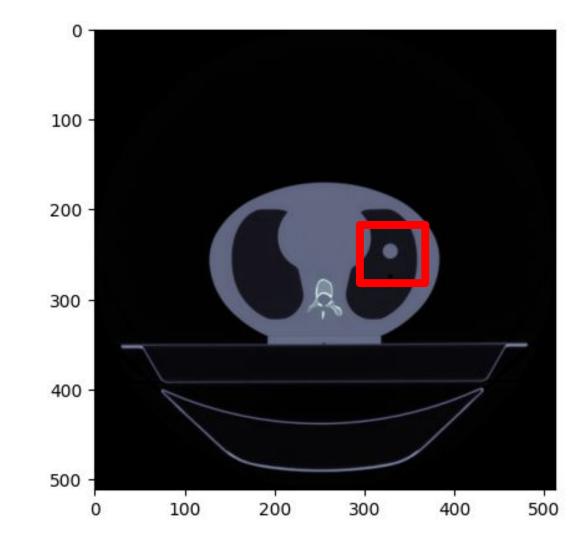
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(0010, 1010) Patient's Age	AS: '020Y'
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(0018, 0050) Slice Thickness	DS: '2.0'
(0018, 0060) KVP	DS: '120.0'
(0018, 0088) Spacing Between Slices	DS: '1.0'
(0018, 0090) Data Collection Diameter	DS: '600.0'
(0018, 1020) Software Versions	LO: '2.3.5'
(0018, 1030) Protocol Name	LO: 'TORACE 5mm/OncoBody'
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(0018, 1120) Gantry/Detector Tilt	DS: '0.0'
(0018, 1130) Table Height	DS: '173.0'
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(0018, 1152) Exposure	IS: '390'
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(0018, 1210) Convolution Kernel	SH: 'C'
(0018, 5100) Patient Position	CS: 'HFS'
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(0018, 9323) Exposure Modulation Type	CS: 'ZDOM'
(0018, 9324) Estimated Dose Saving	FD: 0.0
(0018, 9328) Exposure Time in ms	FD: 1.2302839116719242
(0018, 9330) X-Ray Tube Current in mA	FD: 317.0
(0018, 9332) Exposure in mAs	FD: 390.0
(0018, 9345) CTDIvol	FD: 20.6





.1669205515.21357

on (JPEG p14), Selection Value =

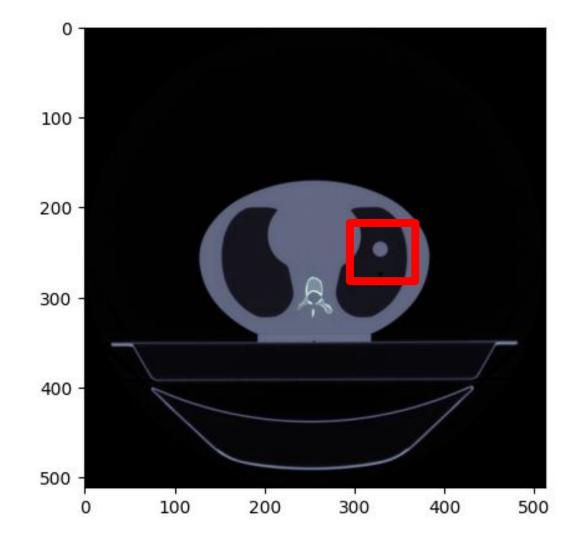
to SW'





(0018,	9323)	Exposure Modulation Type	CS:	'ZDOM'
		Estimated Dose Saving	FD:	0.0
		CTDIvol	FD:	20.6
(0020,	000d)	Study Instance UID	UI:	1.2.840.113704.1.111.3464.166
(0020,	000e)	Series Instance UID	UI:	1.2.840.113704.1.111.6596.166
(0020,	0010)	Study ID	SH:	'56000'
(0020,	0011)	Series Number	IS:	'2'
(0020,	0012)	Acquisition Number	IS:	None
(0020,	0013)	Instance Number	IS:	'19'
19		Image Position (Patient)	DS:	[-300, -218, -658]
		Image Orientation (Patient)	DS:	[1, 0, 0, 0, 1, 0]
		Frame of Reference UID	UI:	1.2.840.113704.1.111.6596.166
(0020,	0060)	Laterality	CS:	
(0020,	1040)	Position Reference Indicator	L0:	
		Slice Location		'-658.0'
		Image Comments	LT:	'TORACE 5 MM'
		Samples per Pixel	US:	1
		Photometric Interpretation		'MONOCHROME2'
(0028,				512
		Columns	1990 N. 1990 N. 1991	512
		Pixel Spacing		[1.171875, 1.171875]
		Bits Allocated	US:	the stranged of the stranged o
		Bits Stored	US:	
		High Bit		11
		Pixel Representation	US:	
12	1000 mm	Window Center		[00050, 00050]
		Window Width		[00350, 00350]
		Rescale Intercept		'-1024.0'
-	-	Rescale Slope		'1.0'
2		Requested Contrast Agent	L0:	
이는 이번 방법에서 지하는 것이 같아.		Pre-Medication	L0:	
		Performed Procedure Step ID		5600096
		Private Creator		'ELSCINT1'
Constant and the second		[Data Dictionary Version]	US:	
		[Presentation Relative Center]		[00000, 00000]
		[Presentation Relative Part]		[00001, 00001]
	_	[Image Label]		'TORACE 5 MM'
(00e1,	1042)	[Unknown]	LU:	'453567–129831'





669205363.54 669205536.6

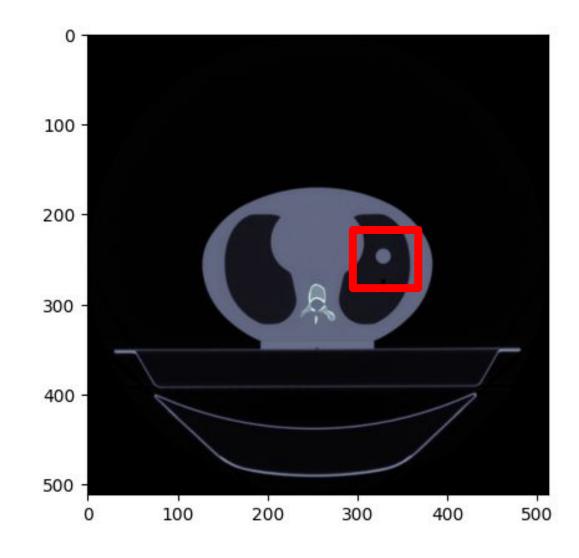
669205471.3

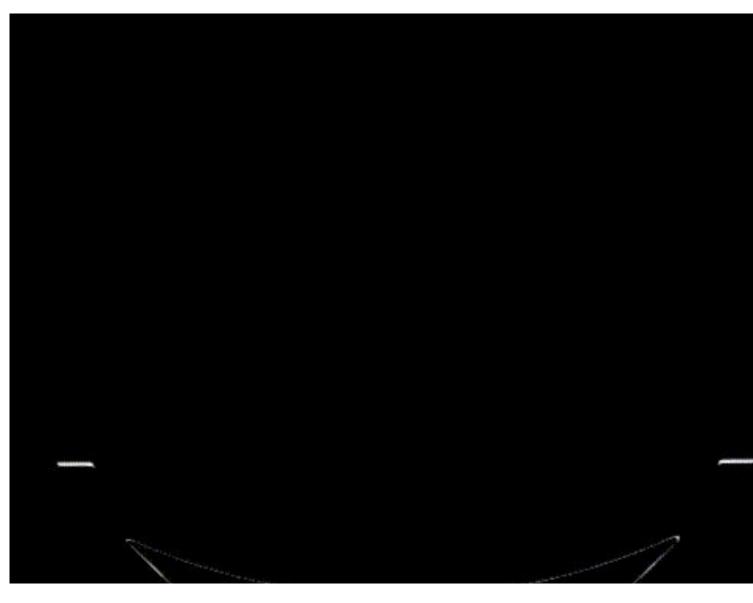




	-			
		[Acquisition Duration]		'10.219'
		[Protocol File Name]		'OncoBody_Multi_1063_usr.proc'
	_	[Patient Language]		'ITALIAN'
Construction of the second		Private Creator		'ELSCINT1'
		Private tag data		Array of 128 elements
		Private Creator		'ELSCINT1'
		[Acquisition Type]		'SPIRAL'
		[Unknown]		'STANDARD'
		[Concurrent Slices Generation]		'E'
		[Angular Sampling Density]		'NORMAL'
		[Reconstruction Arc]		'180.0'
Second and second second second		[Table Velocity]		'19.5'
		[Acquisition Length]	DS:	'160.0'
(01f1,	100a)	<pre>[Edge Enhancement Weight]</pre>	US:	
		[Scanner Relative Center]	DS:	[0, 0]
(01f1,	100d)	[Rotation Angle]	DS:	'0.0'
(01f1,	100e)	[Unknown]	FL:	0.0
(01f1,	1026)	[Pitch]	DS:	'0.813'
		[Rotation Time]	DS:	'1.0'
(01f1,	1032)	[Image View Convention]	CS:	'RIGHT_ON_LEFT'
		[Unknown]		'No'
(01f1,	1044)	[Unknown]	OW:	Array of 644 elements
(01f1,	1046)	[Unknown]	FL:	1.5
(01f1,	1047)	[Unknown]	SH:	'3D'
(01f1,	1049)	[Unknown]	DS:	'390.0'
(01f1,	104a)	[Unknown]	SH:	'DOM'
(01f1,	104b)	[Unknown]	SH:	'16x1.5'
(01f1,	104c)	[Unknown]	SH:	'NO '
(01f1,	104d)	[Unknown]	SH:	'YES'
(01f1,	104e)	[Unknown]	L0:	'Body'
(01f7,	0010)	Private Creator	L0:	'ELSCINT1'
(01f7,	1010)	[Unknown]	0B:	None
(01f7,	1011)	[Unknown]	OW:	Array of 552 elements
(01f7,	1013)	[Unknown]	OW:	Array of 136 elements
(01f7,	1014)	[Unknown]	OW:	Array of 108 elements
(01f7,	1015)	[Unknown]	OW:	Array of 188 elements
(01f7,	1016)	[Unknown]		Array of 40 elements
		[Unknown]		b'\x00\x00\x00\x00\x00\x00\x00\x00\
		[Unknown]		Array of 228 elements







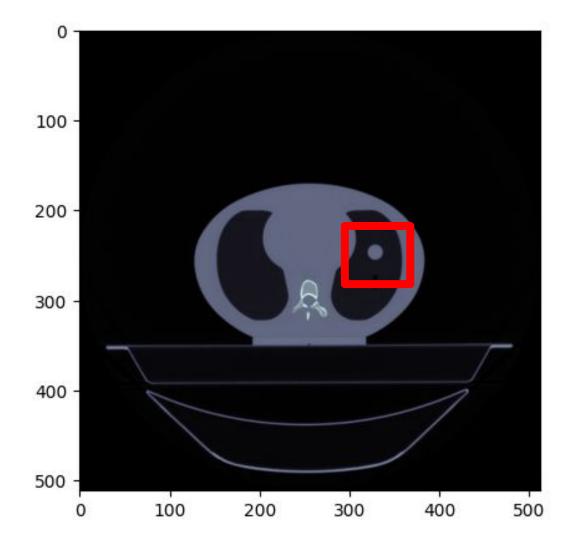


- (01f7, 1019) [Unknown] (01f7, 101a) [Unknown] (01f7, 101b) [Unknown] (01f7, 101c) [Unknown] (01f7, 101e) [Unknown] (01f7, 101f) [Unknown] (01f7, 1022) [Unknown] (01f7, 1023) [Unknown] (01f7, 1025) [Unknown] (01f7, 1026) [Unknown] (01f7, 1027) [Unknown] (01f7, 1029) [Unknown] (01f7, 102b) [Unknown] (01f7, 102c) [Unknown] (01f7, 102d) [Unknown] (01f7, 1030) [Unknown] \x00' (01f7, 1031) [Unknown] (01f7, 1070) [Unknown] (01f7, 1074) [Unknown] (01f7, 1075) [Unknown] (01f7, 107f) Private tag data (07a1, 0010) Private Creator (07a1, 1010) [Tamar Software Version] (7fdf, 0010) Private Creator (7fdf, 10f0) [Unknown] (7fdf, 10ff) [Unknown]
- (7fe0, 0010) Pixel Data

OW: Array of 2160 elements OW: Array of 28 elements OW: Array of 1744 elements OW: Array of 116 elements OW: Array of 364 elements OW: Array of 148 elements UI: 1.2.840.113704.1.111.6596.1669205536.5.1.1111111111111111111111 OW: b'.\x00\x00\x00' OW: b'\x01\x00\x00\x00\x00\x00\x00\x00\x00\x12\x12\x00' OW: Array of 10764 elements OW: Array of 36 elements OW: Array of 440 elements OW: Array of 36 elements OW: Array of 656 elements OW: b'\x00\x00\x00\x00\x00\x00\x00\x00 OW: Array of 124 elements OW: Array of 1312 elements OW: Array of 288 elements OW: Array of 136 elements UN: Array of 1312 elements LO: 'ELSCINT1' LO: '3.5' LO: 'ELSCINT1' **OB:** None SH: ''

OW: Array of 524288 elements

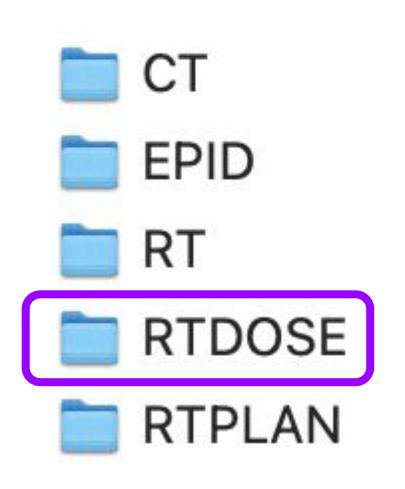




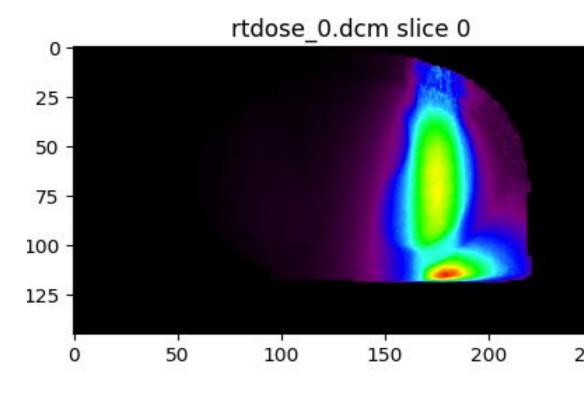


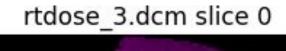


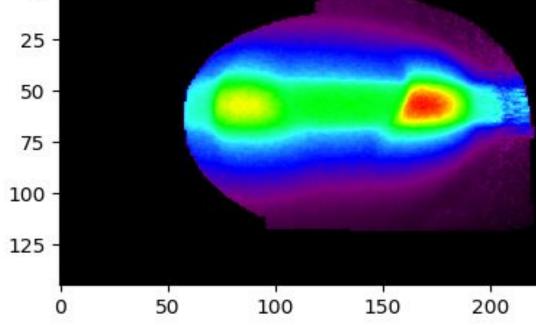
RT dose data



Multi-frame dose images \rightarrow the dose distribution is encoded as a multi-frame image (79 frames)

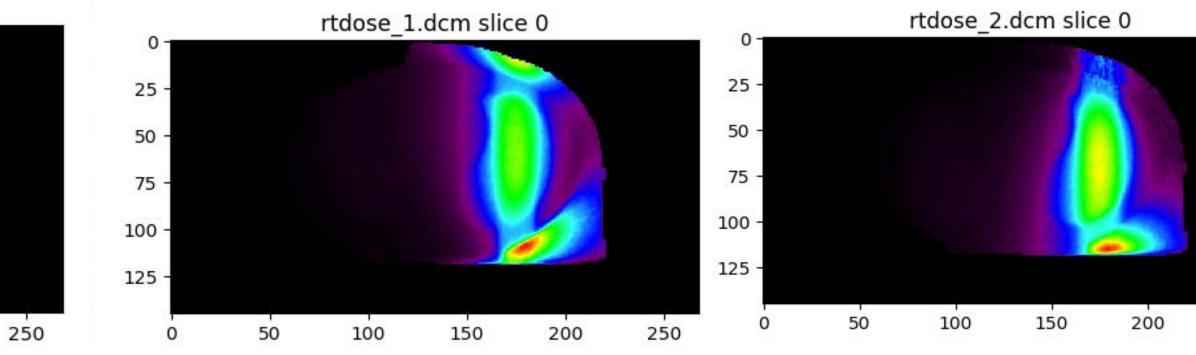


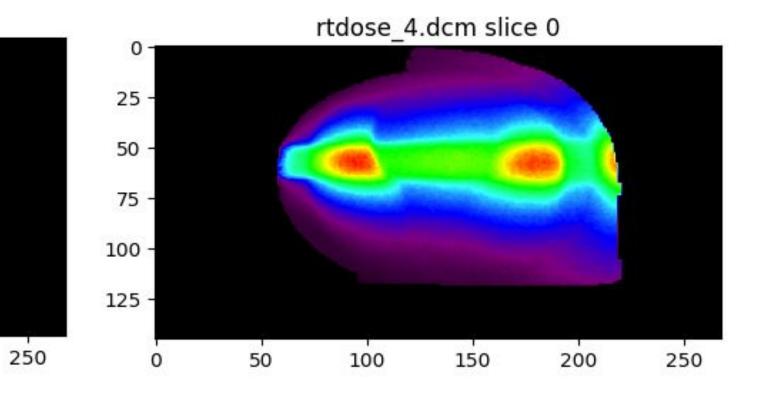




0 -











RT dose file: tags & attributes

Dataset.file_meta		(0028, 0008) Number of Frames	TS: '79'
(0002, 0000) File Meta Information Group Length		(0028, 0009) Frame Increment Pointer	AT: (3004, 000c)
(0002, 0001) File Meta Information Version	0B: b'\x00\x01'	(0028, 0010) Rows	US: 145
(0002, 0002) Media Storage SOP Class UID	UI: RT Dose Storage	(0028, 0011) Columns	US: 268
(0002, 0003) Media Storage SOP Instance UID	UI: 2.16.840.1.114337.1.1.1682093615.0	(0028, 0030) Pixel Spacing	DS: [2, 2]
(0002, 0010) Transfer Syntax UID	UI: Implicit VR Little Endian		
(0002, 0012) Implementation Class UID	UI: 2.16.840.1.114362.1	(0028, 0100) Bits Allocated	US: 16
(0002, 0013) Implementation Version Name	SH: 'MIM723M31402'	(0028, 0101) Bits Stored	US: 16
		(0028, 0102) High Bit	US: 15
(0008, 0005) Specific Character Set	CS: 'ISO_IR 100'	(0028, 0103) Pixel Representation	US: 0
(0008, 0016) SOP Class UID	UI: RT Dose Storage	(0028, 0106) Smallest Image Pixel Value	US: 0
(0008, 0018) SOP Instance UID	UI: 2.16.840.1.114337.1.1.1682093615.0	(0028, 0107) Largest Image Pixel Value	US: 65535
(0008, 0020) Study Date	DA: '20221123'	(3004, 0002) Dose Units	CS: 'GY'
(0008, 0030) Study Time (0008, 0050) Accession Number	TM: '130930' SH: ''	(3004, 0004) Dose Type	CS: 'PHYSICAL'
(0008, 0050) Accession Number	CS: 'RTDOSE'	(3004, 000a) Dose Summation Type	CS: 'BEAM'
(0008, 0060) Modality (0008, 0070) Manufacturer	LO: 'CMS, Inc.'	(3004, 000c) Grid Frame Offset Vector	DS: Array of 79 elements
(0008, 0090) Referring Physician's Name	PN: ''	(3004, 000e) Dose Grid Scaling	DS: '9.53212e-06'
(0008, 1090) Manufacturer's Model Name	LO: 'Monaco'	(3004, 0014) Tissue Heterogeneity Correction	CS: 'ROI_OVERRIDE'
(0010, 0010) Patient's Name	PN: 'CIRS Invivo statico^1cm sotto SW'	(300c, 0002) Referenced RT Plan Sequence 1 i	
(0010, 0020) Patient ID	LO: 'CIRSinvivo'	(0008, 1150) Referenced SOP Class UID	
(0010, 0030) Patient's Birth Date	DA: '20021122'	(0008, 1155) Referenced SOP Instance UID	UI: 2.16.840.1.114337.1.1.16820
(0010, 0040) Patient's Sex	CS: '0'	(300c, 0020) Referenced Fraction Group Sec	
(0018, 0050) Slice Thickness	DS: None		
(0018, 1020) Software Versions	LO: '5.51.10'	(300c, 0004) Referenced Beam Sequence	and a second sec
(0020, 000d) Study Instance UID	UI: 1.2.840.113704.1.111.3464.1669205363.54	(300c, 0006) Referenced Beam Number	IS: '2'
(0020, 000e) Series Instance UID	UI: 2.16.840.1.114337.1.1.1682093613.0.1.3		
(0020, 0010) Study ID	SH: '56000_6'	(300c, 0022) Referenced Fraction Group N	lumber IS: '1'
(0020, 0011) Series Number	IS: None		
(0020, 0013) Instance Number	IS: '1'	·	
(0020, 0032) Image Position (Patient)	DS: [-265.3, -41.9, -675]	(300c, 0060) Referenced Structure Set Sequence	ce 1 item(s)
(0020, 0037) Image Orientation (Patient)	DS: $[1, 0, 0, 0, 1, 0]$	(0008, 1150) Referenced SOP Class UID	UI: RT Structure Set Storage
(0020, 0052) Frame of Reference UID (0020, 1040) Position Reference Indicator	UI: 1.2.840.113704.1.111.6596.1669205471.3	(0008, 1155) Referenced SOP Instance UID	UI: 2.16.840.1.114337.1.1.16820
(0028, 0002) Samples per Pixel	US: 1	······································	
(0028, 0004) Photometric Interpretation	CS: 'MONOCHROME2'	(7fe0, 0010) Pixel Data	OW: Array of 6139880 elements







82093613.0

32093605.0

RT dose file: tags & attributes

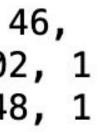
Selection of specific tags

PatientName: CIRS Invivo statico^1cm sotto SW PatientID: CIRSinvivo StudyDate: 20221123 Modality: RTDOSE SliceThickness: None Image Position: [-265.3, -41.9, -675] Image Orientation: [1, 0, 0, 0, 1, 0] NumberOfFrame: 79 Rows: 145 Columns: 268 PixelSpacing: [2, 2] BitsAllocated: 16 BitsStored: 16 Dose Units: GY Dose Type: PHYSICAL DoseSummationType: BEAM GridFrameOffsetVector: [0, 2, 4, 6, 8, 10, 12, 14, 16, 18, 20, 22, 24, 26, 28, 30, 32, 34, 36, 38, 40, 42, 44, 46, 48, 50, 52, 54, 56, 58, 60, 62, 64, 66, 68, 70, 72, 74, 76, 78, 80, 82, 84, 86, 88, 90, 92, 94, 96, 98, 100, 102, 1 04, 106, 108, 110, 112, 114, 116, 118, 120, 122, 124, 126, 128, 130, 132, 134, 136, 138, 140, 142, 144, 146, 148, 1 50, 152, 154, 156] DoseGridScaling: 9.53212e-006









Meaning of the tags

(0008, 0060) Modality: Type of equipment that originally acquired the data used to create the images in this Series.

(0018, 0050) Slice Thickness: Nominal slice thickness, in mm.

(0020, 0032) Image Position (Patient): The x, y, and z coordinates of the upper left hand corner (center of the first voxel transmitted) of the image, in mm.

(0020, 0037) Image Orientation (Patient): The direction cosines of the first row and the first column with respect to the patient. See https://dicom.innolitics.com/ciods/rt-dose/image-plane/00200037

(0020, 0052) Frame of Reference UID: Uniquely identifies the Frame of Reference for a Series. See https://dicom.innolitics.com/ciods/rt-plan/frame-of-reference/00200052

(0028, 0008) Number of Frames: Number of frames in a Multi-frame Image. A Multi-frame Image is defined as a Image whose pixel data consists of a sequential set of individual Image Pixel frames. A Multi-frame Image is transmitted as a single contiguous stream of pixels. Frame headers do not exist within the data stream.

(0028, 0010) Rows: Number of rows in the image.

(0028, 0011) Columns: Number of columns in the image.

(0028, 0030) Pixel Spacing: Physical distance in the patient between the center of each pixel, specified by a numeric pair - adjacent row spacing (delimiter) adjacent column spacing in mm.

(0028, 0100) Bits Allocated: Number of bits allocated for each pixel sample.

(0028, 0101) Bits Stored: Number of bits stored for each pixel sample.

(3004, 0002) Dose Units: Dose axis units.

(3004, 0004) Dose Type: Type of dose. Defined Terms:

- PHYSICAL: physical dose
- **EFFECTIVE**: physical dose after correction for biological effect using user-defined modeling technique
- **ERROR**: difference between desired and planned dose

(3004, 000a) Dose Summation Type: Type of dose summation. Defined Terms:

- **PLAN**: dose calculated for entire delivery of all fraction groups of RT Plan
- **MULTI_PLAN**: dose calculated for entire delivery of 2 or more RT Plans
- **FRACTION**: dose calculated for entire delivery of a single Fraction Group within RT Plan
- **BEAM**: dose calculated for entire delivery of one or more Beams within RT Plan
- **BRACHY**: dose calculated for entire delivery of one or more Brachy Application Setups within RT Plan
- **FRACTION_SESSION**: dose calculated for a single session ("fraction") of a single Fraction Group within RT Plan
- **BEAM_SESSION**: dose calculated for a single session ("fraction") of one or more Beams within RT Plan
- **BRACHY_SESSION**: dose calculated for a single session ("fraction") of one or more Brachy Application Setups within RT Plan
- **CONTROL_POINT**: dose calculated for one or more Control Points within a Beam for a single fraction
- RECORD: dose calculated for RT Beams Treatment Record

(3004, 000c) Grid Frame Offset Vector: An array that contains the dose image plane offsets (in mm) of the dose image frames in a multi-frame dose. Required if multi-frame pixel data are present and Frame Increment Pointer (0028,0009) points to Grid Frame Offset Vector (3004,000C).

(3004, 000e) Dose Grid Scaling: Scaling factor that when multiplied by the dose grid data found in Pixel Data (7FE0,0010) Attribute of the Image Pixel Module, yields grid doses in the dose units as specified by Dose Units (3004,0002).

Grid Frame Offset Vector

Grid Frame Offset Vector Attribute

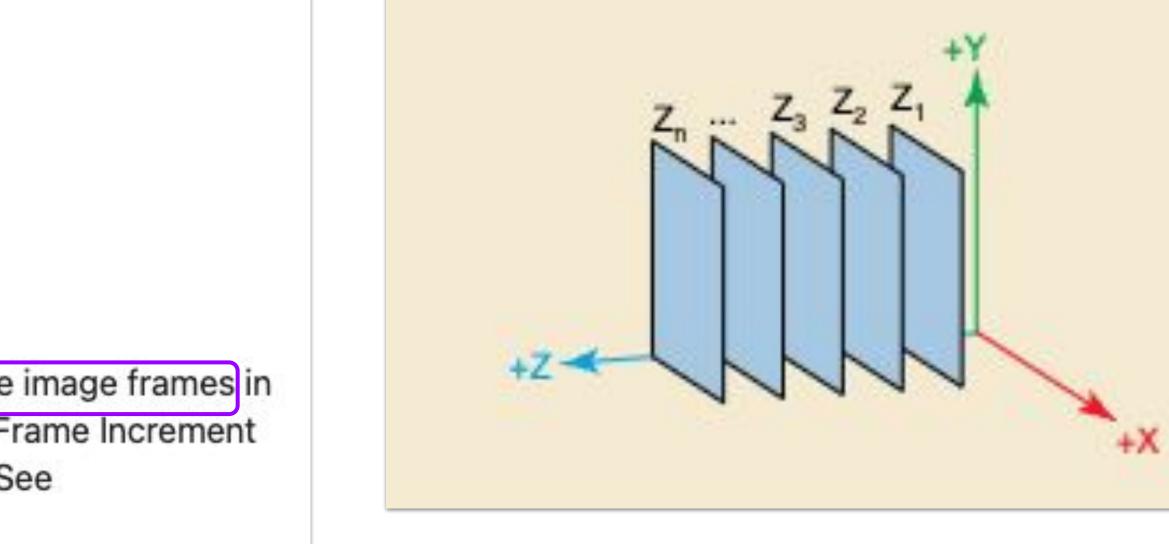
Tag	(3004,000C)
Туре	Conditionally Required (1C)
Keyword	GridFrameOffsetVector
Value Multiplicity	2-n
Value Representation	Decimal String (DS)

An array that contains the dose image plane offsets (in mm) of the dose image frames in a multi-frame dose. Required if multi-frame pixel data are present and Frame Increment Pointer (0028,0009) points to Grid Frame Offset Vector (3004,000C). See Section C.8.8.3.2.

https://dicom.innolitics.com/ciods/rt-dose/rt-dose/3004000c

```
Dose Units: GY
Dose Type: PHYSICAL
DoseSummationType: BEAM
GridFrameOffsetVector: [0, 2, 4, 6, 8, 10, 12, 14, 16, 18, 20, 22, 24, 26, 28, 30, 32, 34, 36, 38, 40, 42, 44, 46,
48, 50, 52, 54, 56, 58, 60, 62, 64, 66, 68, 70, 72, 74, 76, 78, 80, 82, 84, 86, 88, 90, 92, 94, 96, 98, 100, 102, 1
04, 106, 108, 110, 112, 114, 116, 118, 120, 122, 124, 126, 128, 130, 132, 134, 136, 138, 140, 142, 144, 146, 148, 1
50, 152, 154, 156]
DoseGridScaling: 9.53212e-006
```





Dose Grid Frame example



Grid Frame Offset Vector

Section C.8.8.3.2

C.8.8.3.2 Grid Frame Offset Vector

Grid Frame Offset Vector (3004,000C) shall be provided if a dose distribution is encoded as a multi-frame image. Values of the Grid Frame Offset Vector (3004,000C) shall vary monotonically and are to be interpreted as follows:

- a. If Grid Frame Offset Vector (3004,000C) is present and its first element is zero, this Attribute contains an array of n elements indicating the plane location of the data in the right-handed image coordinate system, relative to the position of the first dose plane transmitted, i.e., the point at which Image Position (patient) (0020,0032) is defined, with positive offsets in the direction of the cross product of the row and column directions.
- b. If Grid Frame Offset Vector (3004,000C) is present, its first element is equal to the third element of Image Position (patient) (0020,0032), and Image Orientation (patient) (0020,0037) has the value (1,0,0,0,1,0), then Grid Frame Offset Vector contains an array of n elements indicating the plane location (patient z coordinate) of the data in the Patient-Based Coordinate System.

In future implementations, use of option a) is strongly recommended.

This Attribute is conditional since the RT Dose Module may be included even if pixel doses are not being transmitted, or the image may be a single-frame image. If the Multiframe Module is present, Frame Increment Pointer (0028,0009) shall have the Enumerated Value of 3004000C (Grid Frame Offset Vector).

Note

Option (a) can represent a rectangular-parallelepiped dose grid with any orientation with respect to the patient, while option (b) can only represent a rectangular-parallelepiped dose grid whose planes are in the transverse patient dimension and whose x- and y-axes are parallel to the patient x- and y-axes.

https://dicom.innolitics.com/ciods/rt-dose/rt-dose/3004000c



GridFrameOffsetVector: [0, 2, 4, 6, 8, 10, 12, 14, 16, 18, 20, 22, 24, 26, 28, 30, 32, 34, 36, 38, 40, 42, 44, 46, 48, 50, 52, 54, 56, 58, 60, 62, 64, 66, 68, 70, 72, 74, 76, 78, 80, 82, 84, 86, 88, 90, 92, 94, 96, 98, 100, 102, 104, 106, 108, 110, 112, 114, 116, 118, 120, 122, 124, 126, 128, 130, 132, 134, 136, 138, 140, 142, 144, 146, 148, 150, 152, 154, 156]

RT dose

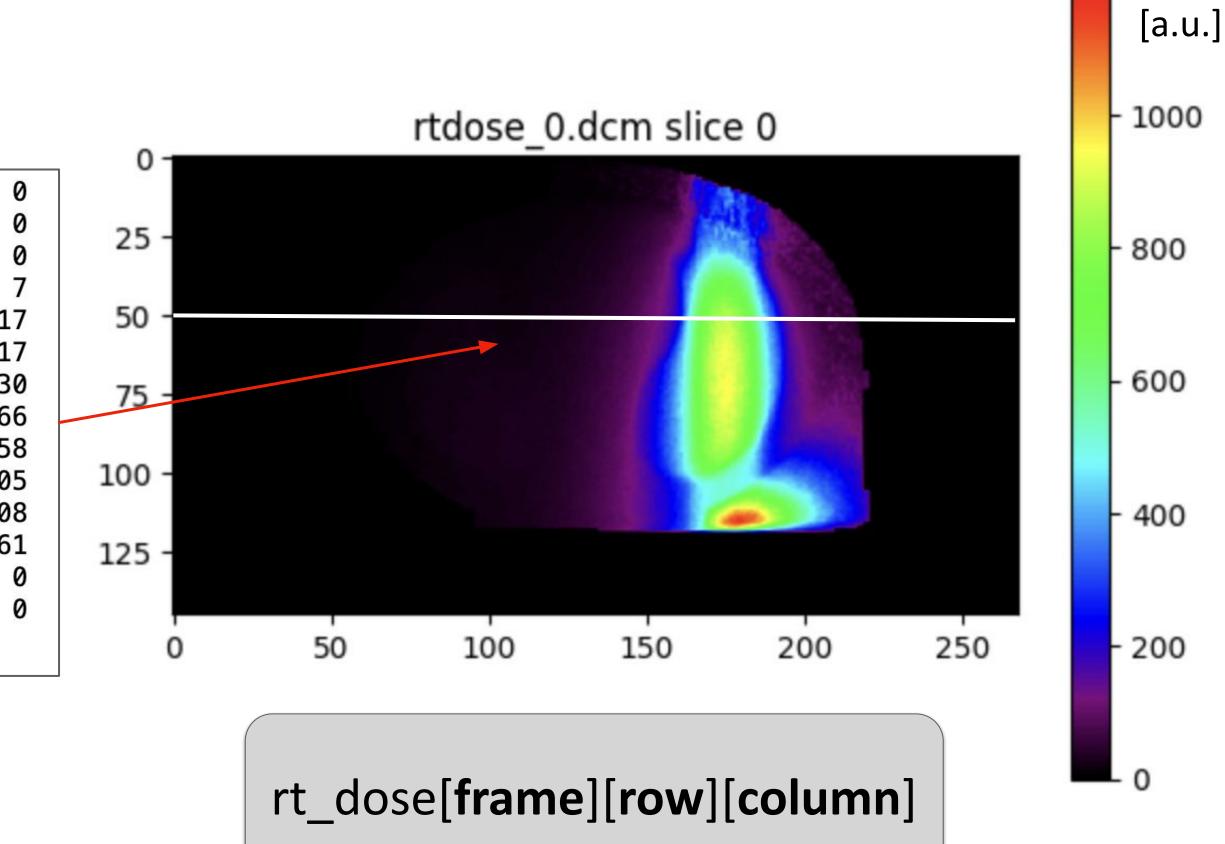
rt_dose[**0**][**50**][:]

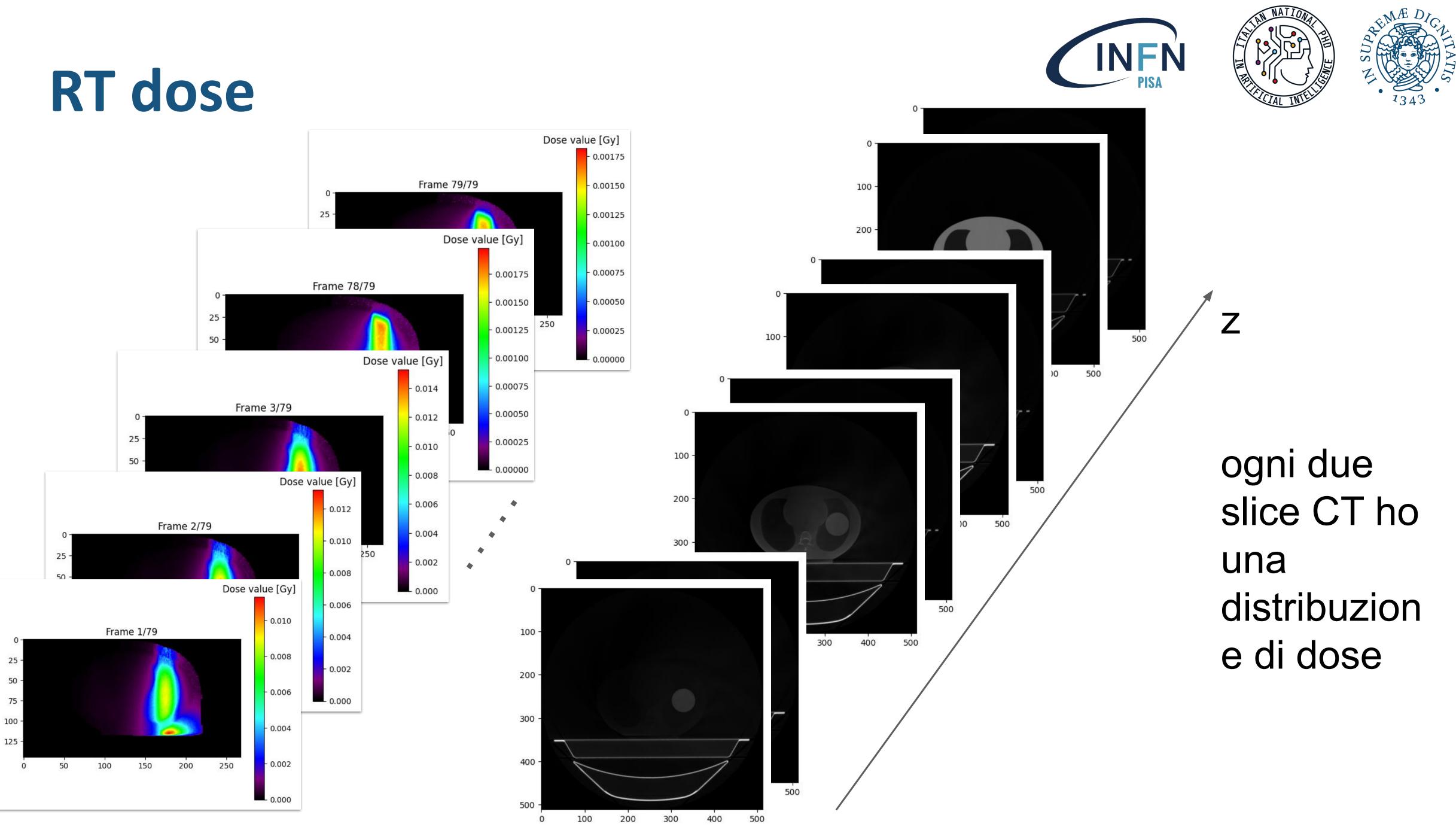
[0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	(
	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	(
	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	(
	0	0	0	0	0	3	4	4	4	6	6	6	6	6	6	6	7	Ţ
	7	9	9	10	10	13	13	13	13	15	15	15	15	15	17	17	17	17
	17	17	18	18	18	18	18	19	19	20	18	18	18	17	15	15	18	17
	15	17	19	18	19	19	20	20	21	21	21	23	24	24	25	26	26	30
	32	30	35	35	34	36	38	40	40	44	49	49	53	54	57	60	66	6
	72	74	81	85	93	95	99	108	108	112	122	129	143	160	177	189	219	258
	336	439	507	581	653	691	728	757	771	821	834	830	830	844	850	845	797	80!
	774	744	720	663	627	553	487	467	402	346	320	267	217	173	151	137	126	108
	104	98	88	85	89	75	63	57	55	69	78	53	100	60	49	57	49	63
	57	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	(
	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	(
	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0]	







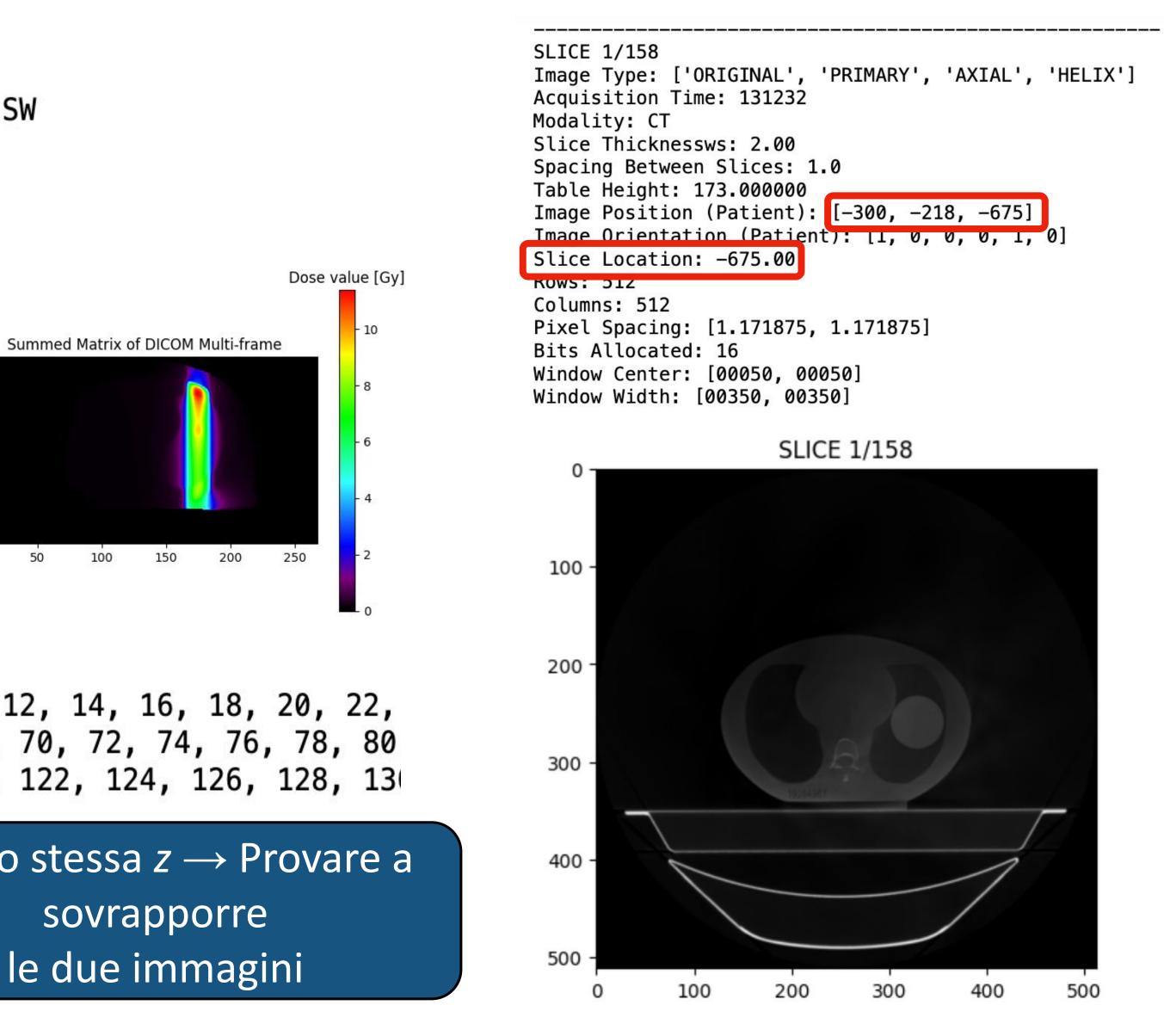




RT dose & CT

PatientName: CIRS Invivo statico^1cm sotto SW PatientID: CIRSinvivo StudyDate: 20221123 Modality: RTDOSE SliceThickness: None Image Position: [-265.3, -41.9, -675] Image Urientation: [1, 0, 0, 0, 1, 0] Summed Matrix of DICOM Multi-frame NumberOfFrame: 79 25 -Rows: 145 50 -Columns: 268 75 -PixelSpacing: [2, 2] 100 -BitsAllocated: 16 125 -BitsStored: 16 0 50 100 150 200 Dose Units: GY Dose Type: PHYSICAL DoseSummationType: BEAM GridFrameOffsetVector: [0, 2, 4, 6, 8, 10, 12, 14, 16, 18, 20, 22, 48, 50, 52, 54, 56, 58, 60, 62, 64, 66, 68, 70, 72, 74, 76, 78, 80 04, 106, 108, 110, 112, 114, 116, 118, 120, 122, 124, 126, 128, 130 50, 152, 154, 156] DoseGridScaling: 9.53212e-006 Hanno stessa $z \rightarrow$ Provare a







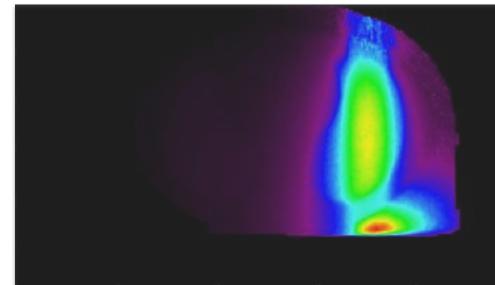
How to overlay the RTDOSE and Image data in the correct position?

	Image Position (Patient) [mm]	Pixel
СТ	[-300, -218, -675]	[1.17]
RTDOSE	[-265.3, -41.9, -675]	





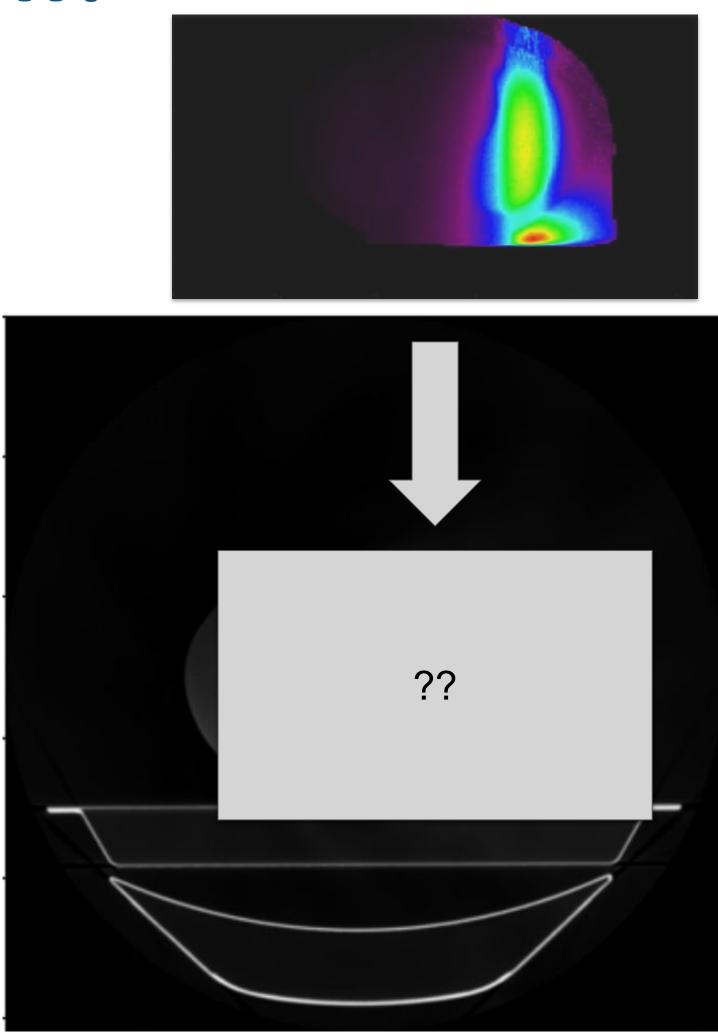


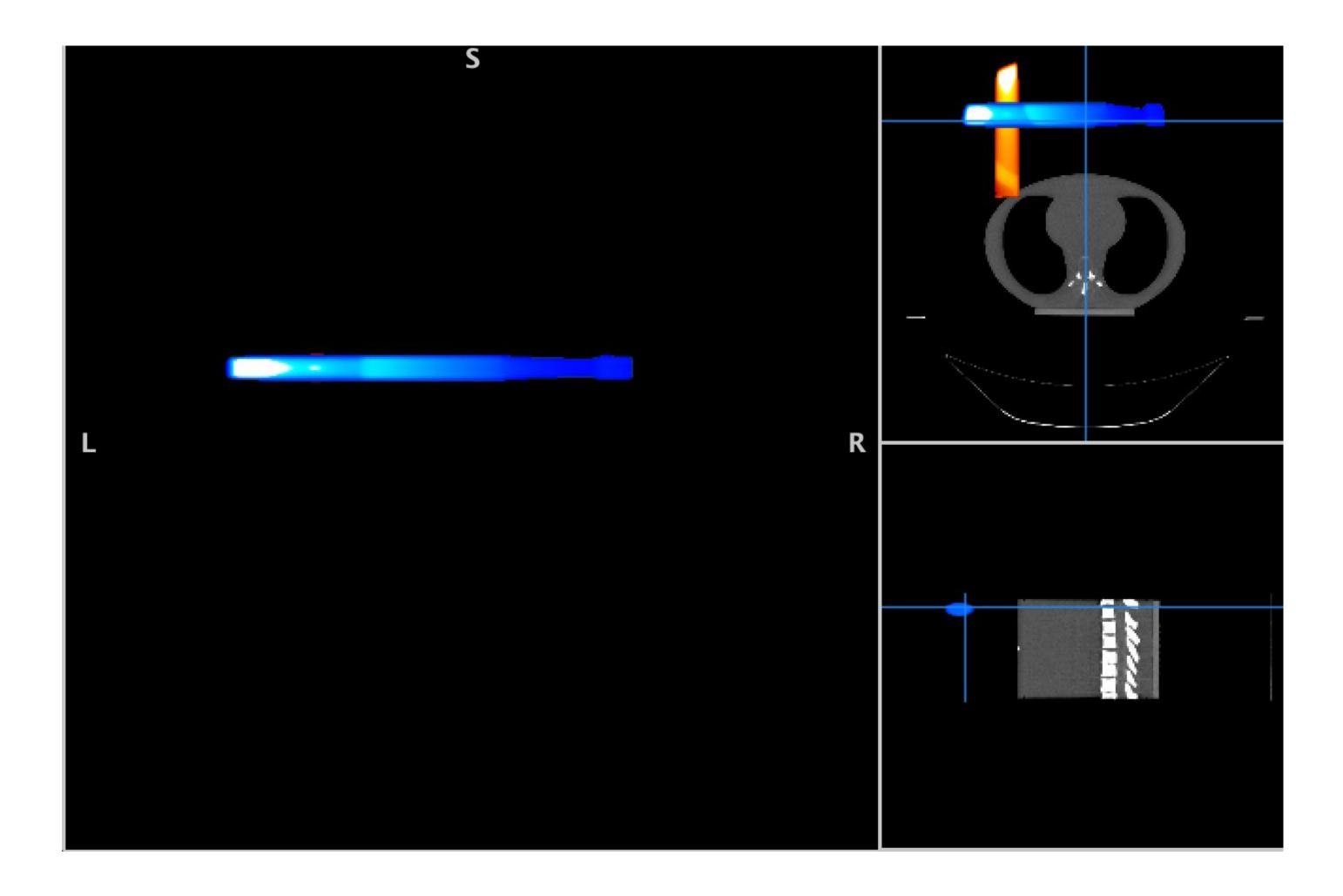


Spacing [mm]

1875, 1.171875]

[2, 2]











Overview	Forum	Mango	iMango Papaya		aya	Multi-image Analysi		
Features	Downloads	Video Tutorials	Using Ma	ango	Publications	Online Web Viewer		

Mango – short for Multi-image Analysis GUI – is a viewer for medical research images. It provides analysis tools and a user interface to navigate image volumes.

Versions

There are three versions of Mango, each geared for a different platform:

- Mango Desktop Mac OS X, Windows, and Linux
- Papaya Browser Firefox, Chrome, Safari and IE
- iMango Mobile Apple iPad

Features

- Support for Analyze, DICOM, NEMA-DES, MINC, NIFTI and NIFTI2 image formats
- Support for VTK (legacy), GIFTI (.surf.gii) and BrainVisa surface formats
- Partial support for TIFF, Concorde microPET, AFNI (legacy), Stimulate, and CTI ECAT
- Development: Supports both Java Plugin API and Python Script API development
- Customizable: Create custom filters, color tables, file formats, and atlases
- Command-line integration: open and process images from the command-line
- Web: Custom protocol and Papaya JavaScript viewer
- ROI Editing: Threshold and component-based tools for painting and tracing ROIs
- Surface Rendering: Interactive surface models supporting cut planes and overlays
- Image Registration: Semi-automatic image coregistration and manual transform editing
- Image Stacking: Threshold and transparency-based image overlay stacking
- Analysis: Histogram, cross-section, time-series analysis, image and ROI statistics
- Processing: Kernel and rank filtering, arithmetic/logic image and ROI calculators

Credits

Designed and developed by:

- Mohamad Habes, Ph.D.
- · Jack L. Lancaster, Ph.D.
- Michael J. Martinez.

Publications

 Lancaster JL, Cykowski MD, McKay DR, Kochunov PV, Fox PT, Rogers W, Toga AW, Zilles K, Amunts K, Mazziotta J (2010). Anatomical Global Spatial Normalization. Neuroinformatics, 8:171–182. [PDF]

- Lancaster JL, Laird AR, Eickhoff SB, Martinez MJ, Fox PM, Fox, PT (2012). Automated
 regional behavioral analysis for human brain images. Frontiers in Neuroinformatics, 6, 23. [PDF]
- Lancaster JL, McKay DR, Cykowski MD, Martinez MJ, Tan X, Valaparla S, Zhang Y, Fox PT (2011). Automated analysis of fundamental features of brain structures. Neuroinformatics, 9(4):371-80. [PDF]

https://mangoviewer.com/





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3D Slicer image computing platform

📥 Download	Documentation	Developers				
😁 Training	Forum	🎔 Twitter				

3D Slicer is a free, open source software for visualization, processing, segmentation, registration, and analysis of medical, biomedical, and other 3D images and meshes; and planning and navigating image-guided procedures.

What is **3D Slicer**?

Desktop software to solve advanced image computing challenges with a focus on clinical and biomedical applications. Development platform to quickly build and deploy custom solutions for research and commercial products, using free, open source software. **Community** of knowledgeable users and developers working together to improve medical computing.

https://www.slicer.org/

https://slicer.readthedocs.io/en/latest/ https://pypi.org/project/pynrrd/

https://www.slicer.org/w/index.php/Documentation/Nightly/Extensions/SlicerRT#Tutorials

https://discourse.slicer.org/t/how-does-3d-slicer-overlay-the-rtdose-and-image-data-in-the-correct-position/8924







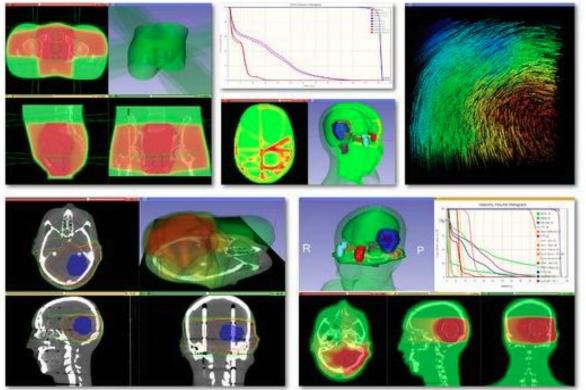
SlicerRT is a radiation therapy toolkit for 3D Slicer, containing generic RT features for import/export, analysis, visualization, aiming to make 3D Slicer a powerful radiotherapy research platform. SlicerRT development is currently funded by CANARIE.

SlicerRT was originally created via funding by Cancer Care Ontario and the Ontario Consortium for Adaptive Interventions in Radiation Oncology (OCAIRO) to provide free, open-source toolset for radiotherapy and related image-guided interventions.

- The SlicerRT extension incorporates Plastimatch modules and algorithms.
- Additional information for users can be found on the User's Guide page

Modules

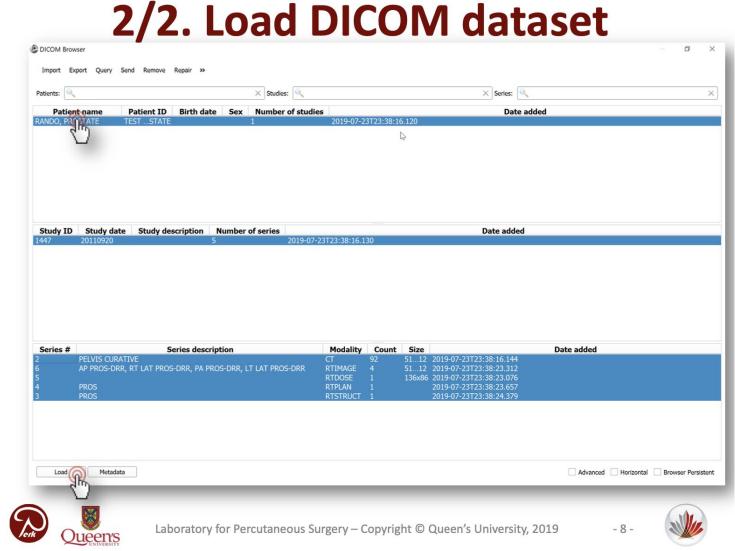
- External Beam Planning (Treatment planning)
- Dose analysis
 - Dose volume histogram
 - Dose accumulation
 - Dose comparison (Gamma dose similarity index)
 - Isodose line and surface display
- Contour analysis
- Segment comparison (Dice Similarity Coefficient, Hausdorff distances)
- Segment morphology (Add/remove margin, Unify, Intersect, etc.)
- I/O
 - DICOM-RT import, export d (handles datasets of types) RT Structure Set, RT Dose, RT Plan, RT Image)
 - DICOM-SRO import/export (handles DICOM Spatial) Registration object, both rigid and deformable)
- Batch processing scripts I (currently only one is available for command-line conversion of RTSS to volume nodes)
- Modules from Plastimatch
 - Plastimatch Automatic deformable image registration
 - Plastimatch LANDWARP Landmark





2/1. Import DICOM dataset

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3/1. Switch to Dose Volume Histogram module

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	Diffusion	•	(Segment Morphology
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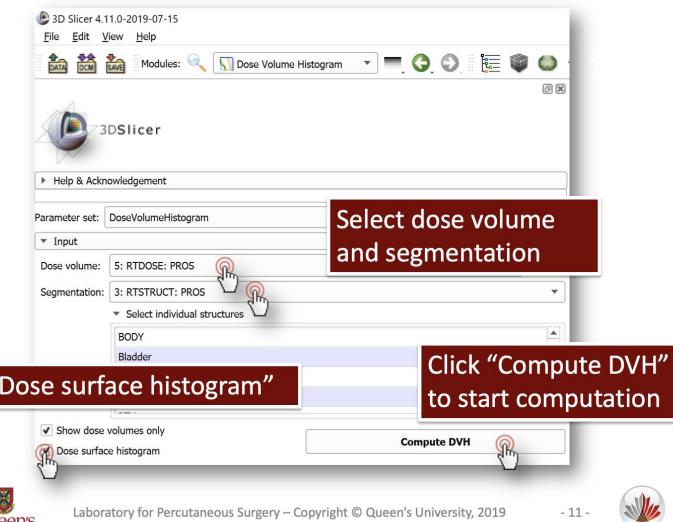


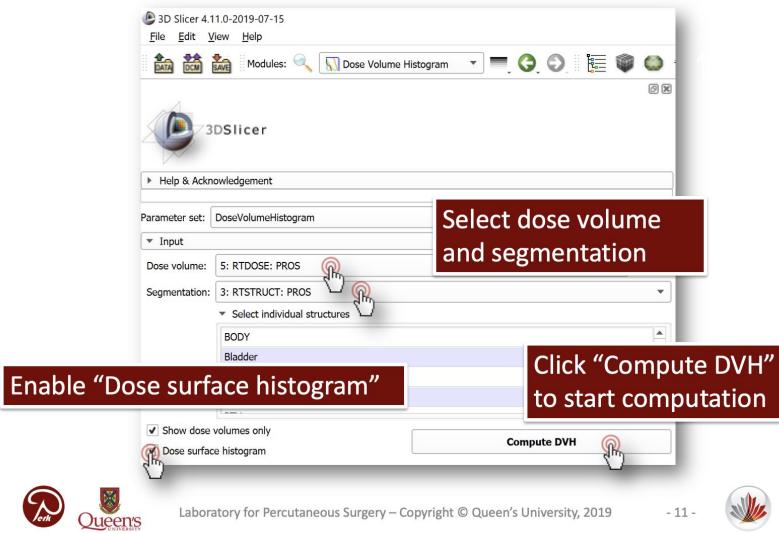
Laboratory for Percutaneous Surgery – Copyright © Queen's University, 2019

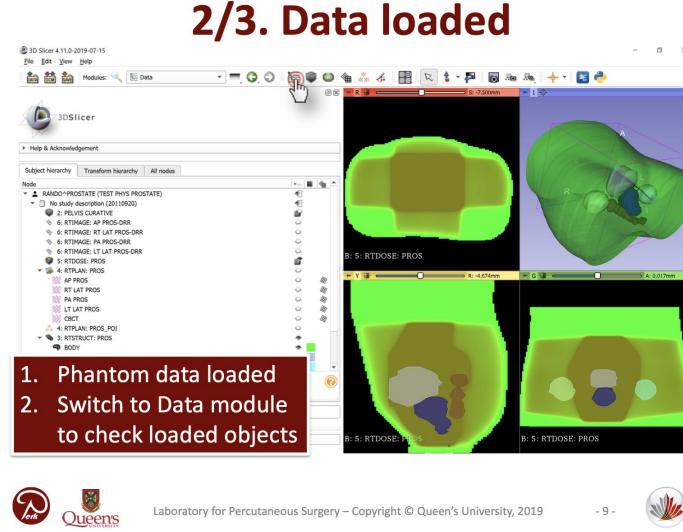


Port

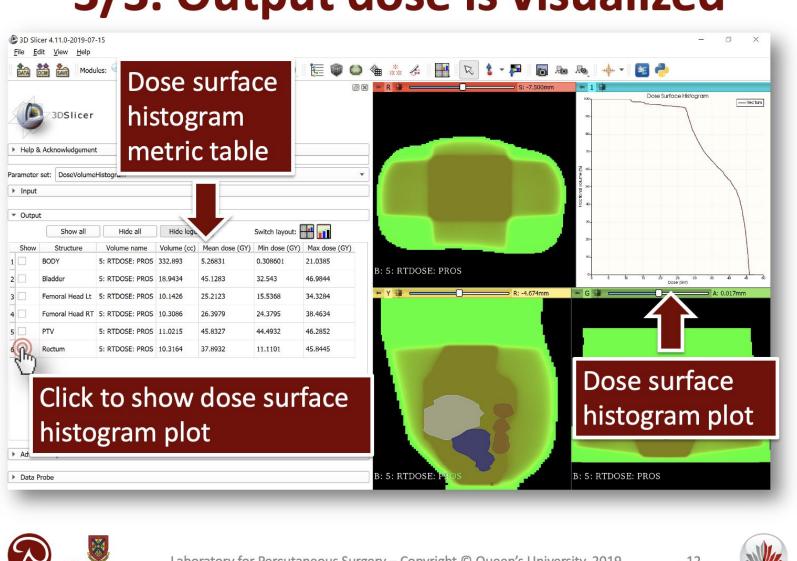
3/2. Set inputs and compute







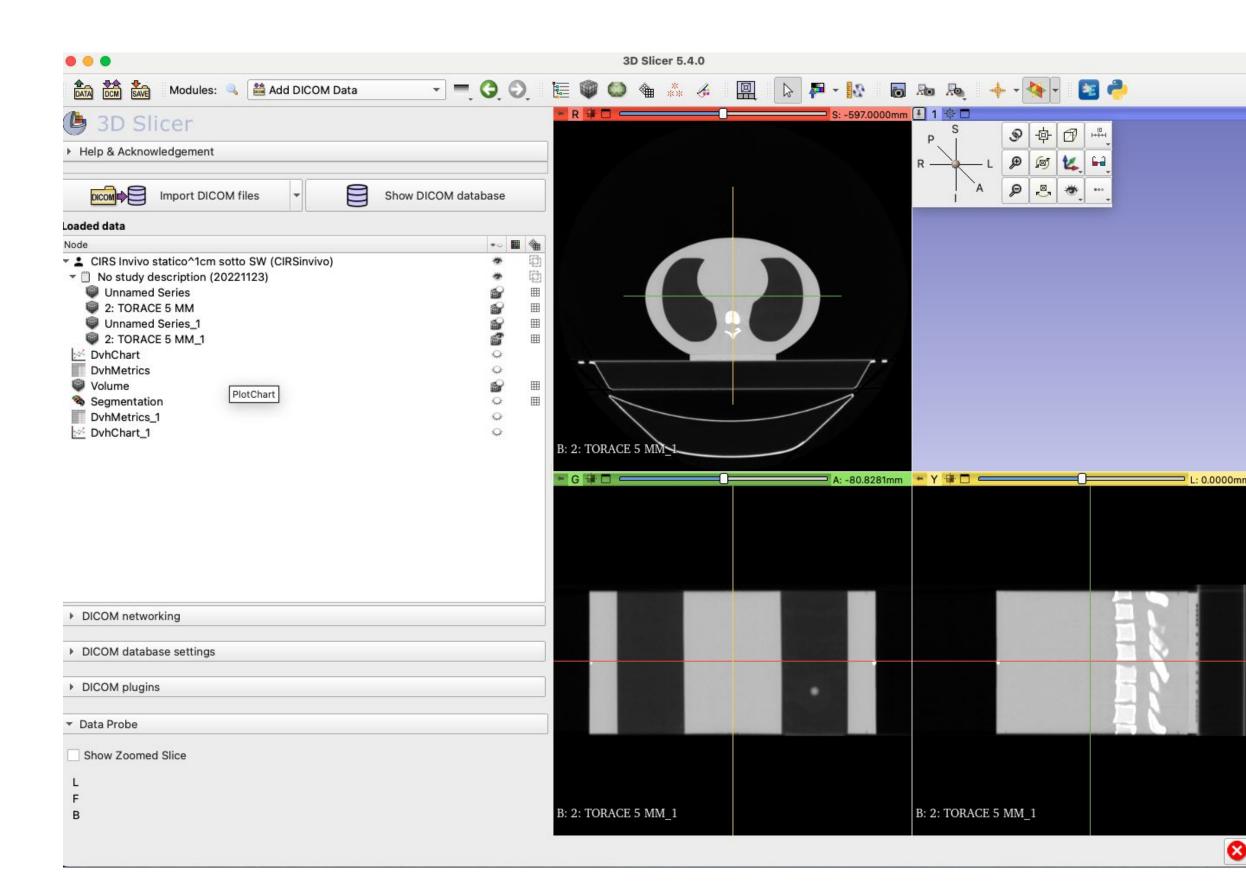
3/3. Output dose is visualized







How to overlay the RTDOSE and Image data in the correct position?

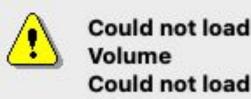








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Could not load: Unnamed Series as a Scalar Could not load: 1: Unnamed Series as a Scalar Volume

OK



How to overlay the RTDOSE and Image data in the correct position?

When I click on "Load selection to Slicer" I get an error message "Could not load ... as a scalar volume"

A common cause of loading failure is corruption of the DICOM files by incorrect anonymization. Patient name, patient ID, and series instance UID fields should not be empty or missing (the anonymizer should replace them by other valid strings). Try to load the original, non-anonymized sequence and/or change your anonymization procedure.

If none of the above helps then check the Slicer error logs and report the error on the Slicer forum. If you share the data (e.g., upload it to Dropbox and add the link to the error report) then Slicer developers can reproduce and fix the problem faster.

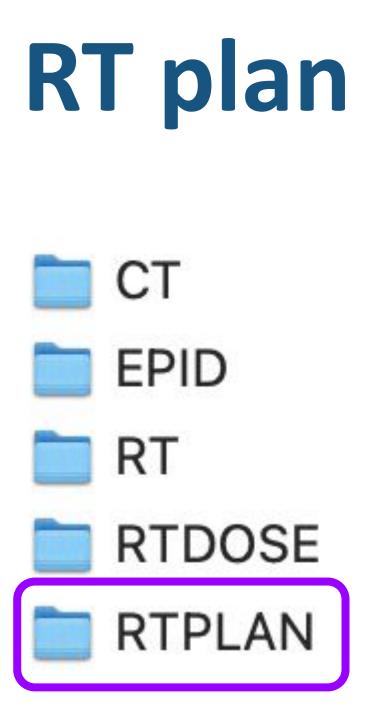
https://slicer.readthedocs.io/en/latest/user_guide/modules/dicom.html#when-i-click-on-load-selection-to-slicer-i-get-an-error-message-could-not-load-as-a-scalar-volume

···· \$#	 Series description 	Modality	Size	Count	Date added
		RTDOSE	268x145	4	20233.675
		RTDOSE	268x145	1	20233.678
	STRCTRNAME	RTSTRUCT		1	20235.829
	4beams	RTPLAN		1	20230.583
	TORACE 5 MM	СТ	512x512	159	20233.329









RT Plan

The focus for this Radiotherapy Plan IOD (RT Plan IOD) is to address the **requirements for transfer of treatment plans generated by** manual entry, a virtual simulation system, or a **treatment planning system** before or during a course of treatment. Such plans may **contain fractionation information**, and **define external beams** and/or brachytherapy application setups. Out[63]:





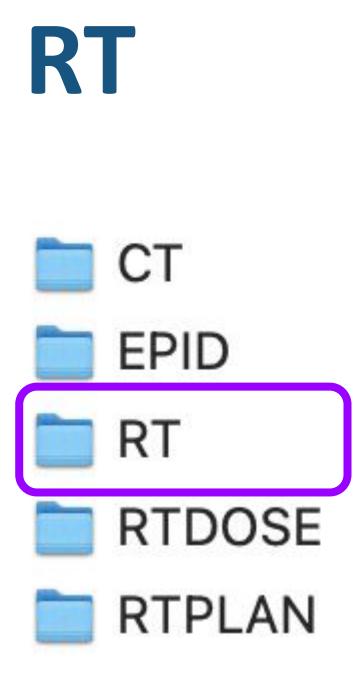


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(0002,	0003)	Media Storage SOP Instance UID	UI:	2.16.840.1.114337.1.1.168209361
(0002,	0010)	Transfer Syntax UID	UI:	Implicit VR Little Endian
(0002,	0012)	Implementation Class UID	UI:	2.16.840.1.114362.1
(0002,	0013)	Implementation Version Name	SH:	'MIM723M31402'
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(0008,	0005)	Specific Character Set	CS:	'ISO_IR 100'
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(0008,	0060)	Modality	CS:	'RTPLAN'
		Manufacturer	L0:	'CMS, Inc.'
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(0008,	1070)	Operators' Name	PN:	11
(0008,	1090)	Manufacturer's Model Name	L0:	'Monaco'
(0010,	0010)	Patient's Name	PN:	'CIRS Invivo statico^1cm sotto
(0010,	0020)	Patient ID	L0:	'CIRSinvivo'









RT Structure Set CIOD

The focus for this Radiotherapy Structure Set IOD (RT Structure Set IOD) is to address the **requirements for transfer of Patient structures and related data defined on CT scanners**, virtual simulation workstations, treatment planning systems and similar devices. Datas (0002 (0002 (0002 (0002 (0002 (0002 (0002 ____ (0008 (0008 (0008 (0008 (0008 (0008 (0008 (0008 (0008 (0008 (0008 (0008 (0008 (0008 (0010 (0010 (0010







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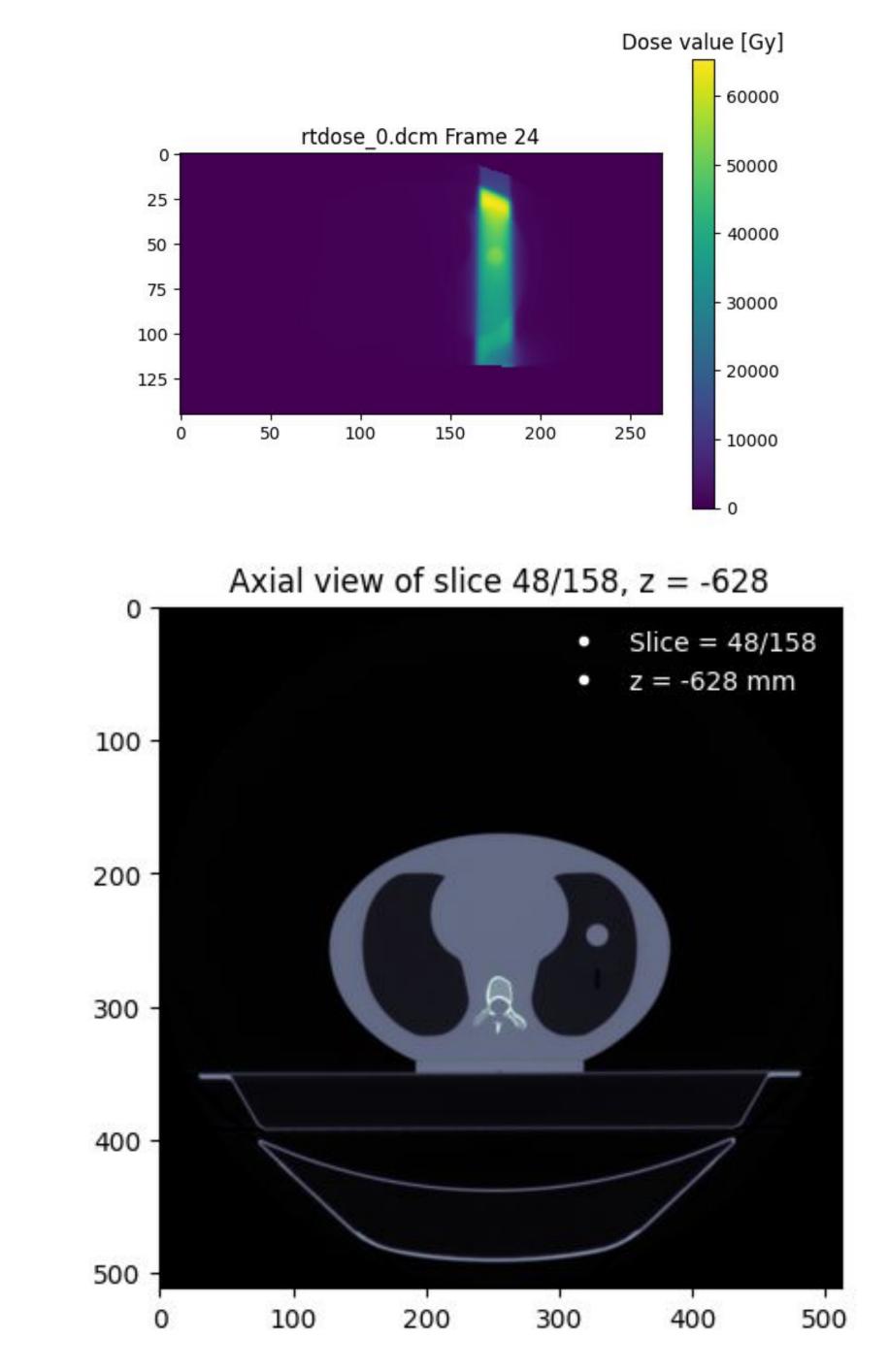






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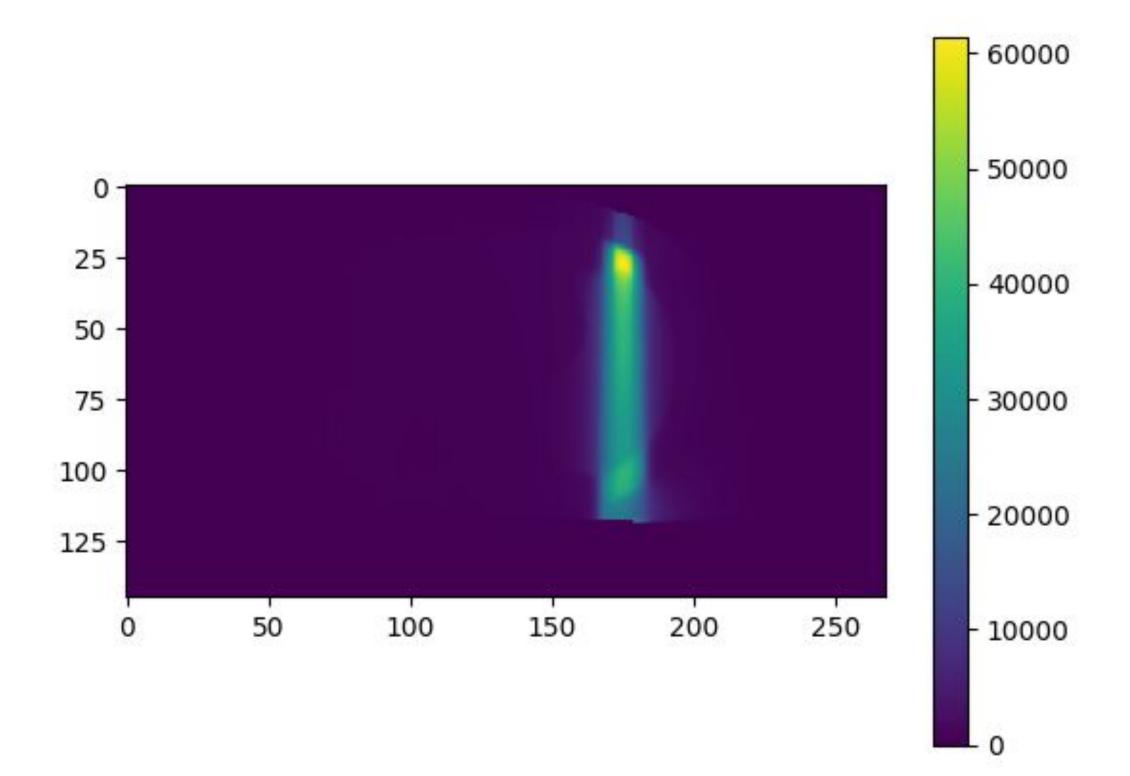
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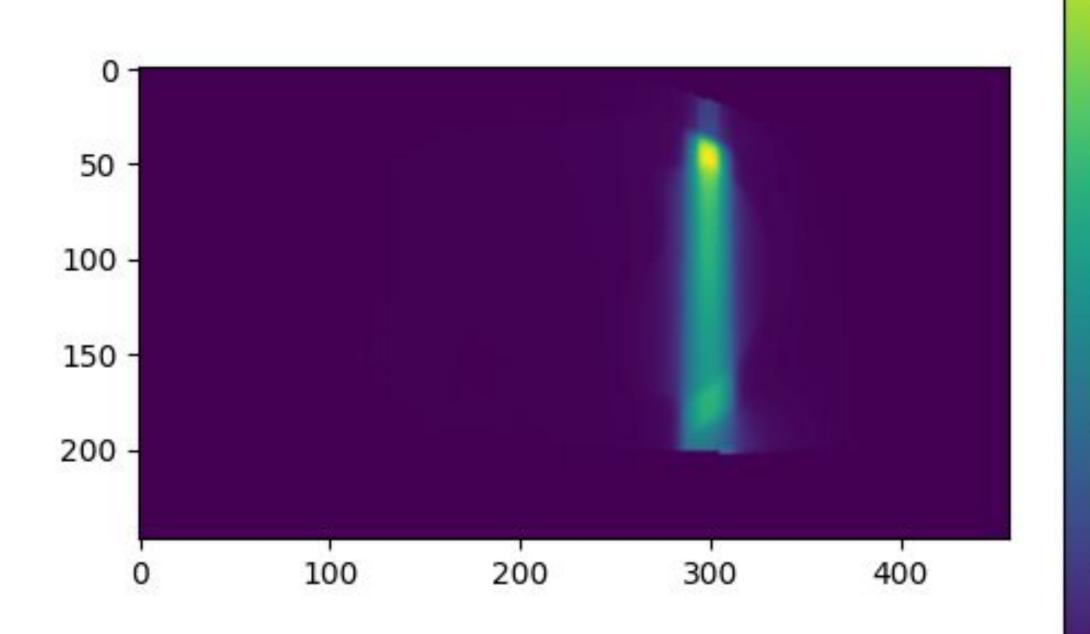


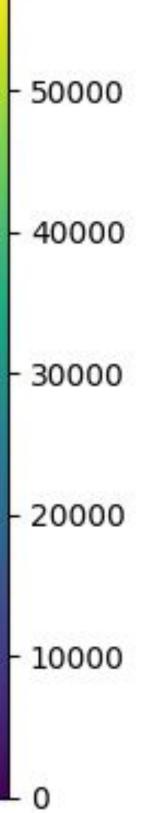


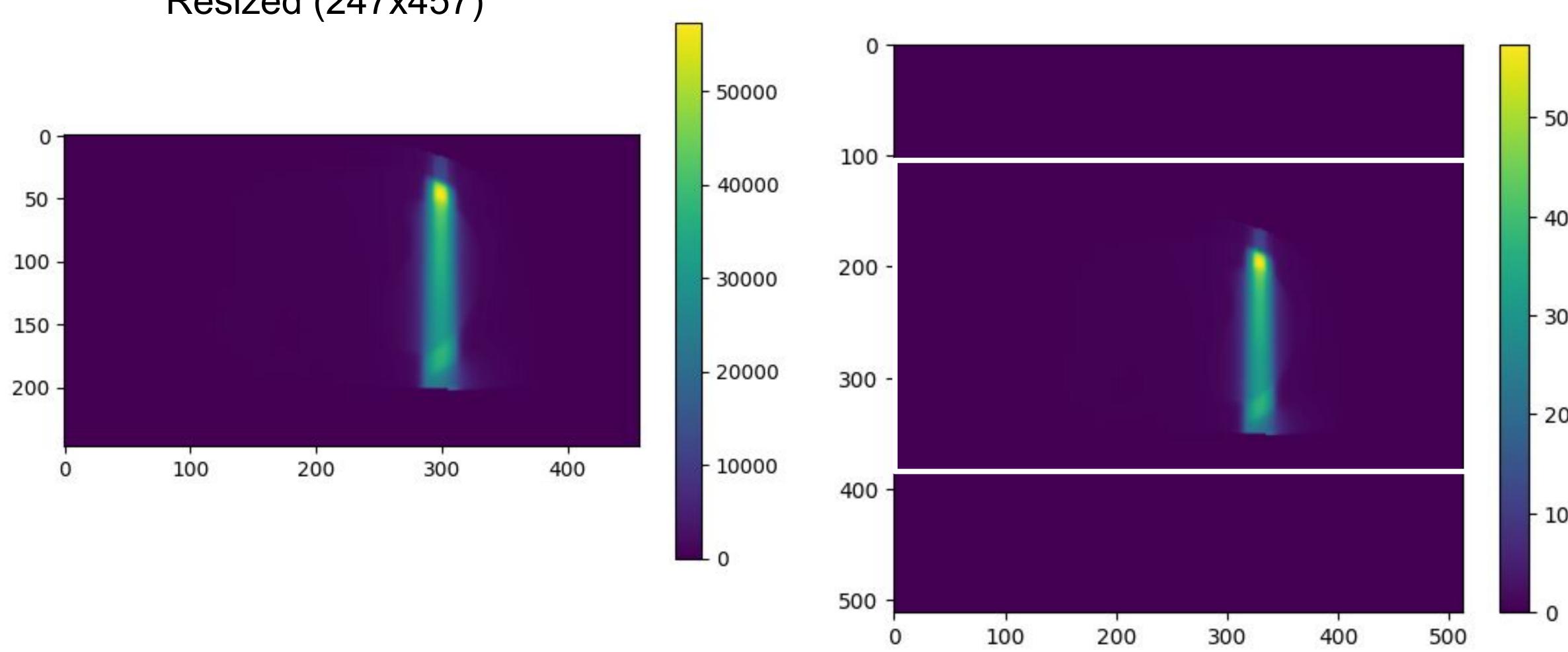
Original image (128x268)



Resized (247x457)





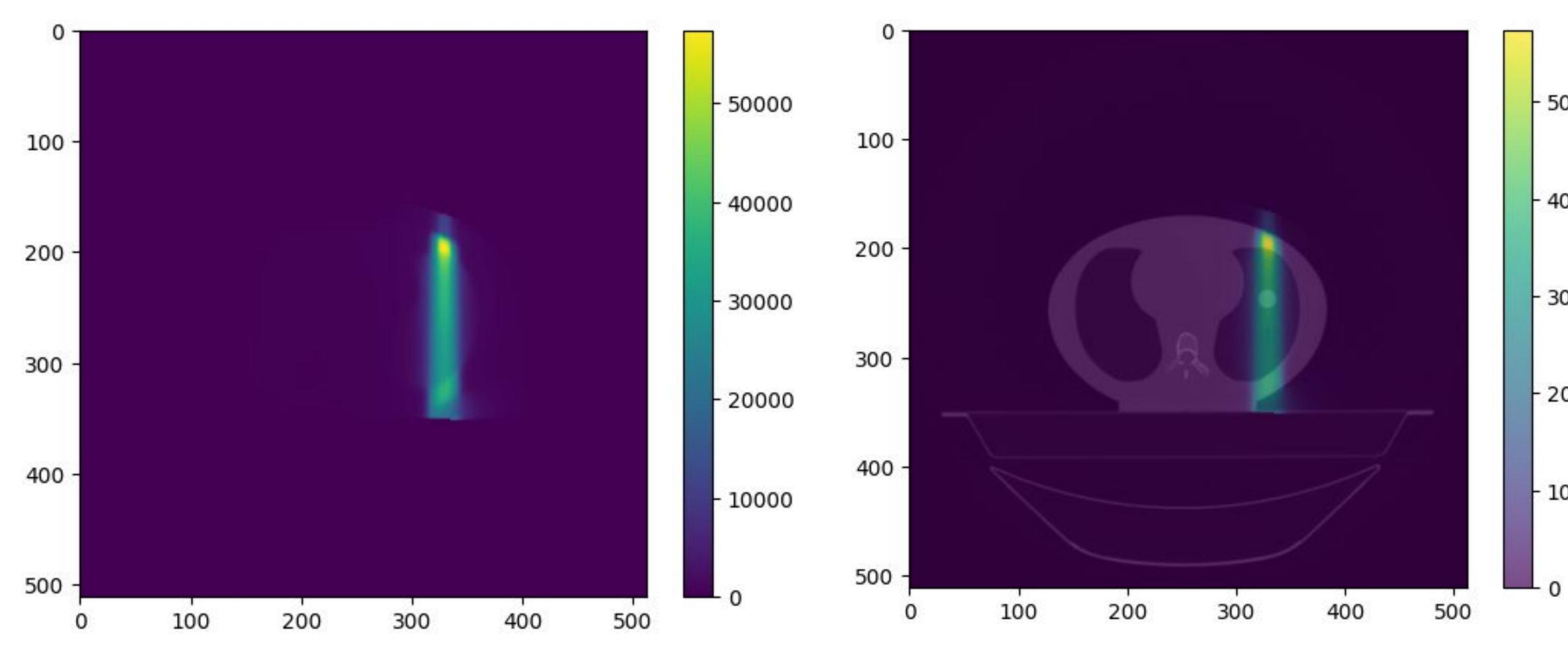


Resized (247x457)

Overlay on a zeros matrix (512x512)



Overlay on a zeros matrix (512x512)



Overlay on a CT slice (512x512)

