

Artificial Intelligence in Medicine

next
AIM

Modality-independent explainable anomaly detection tool for neuroimaging

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next_AIM workshop on XAI techniques for medical data analysis

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ANOMALY DETECTION

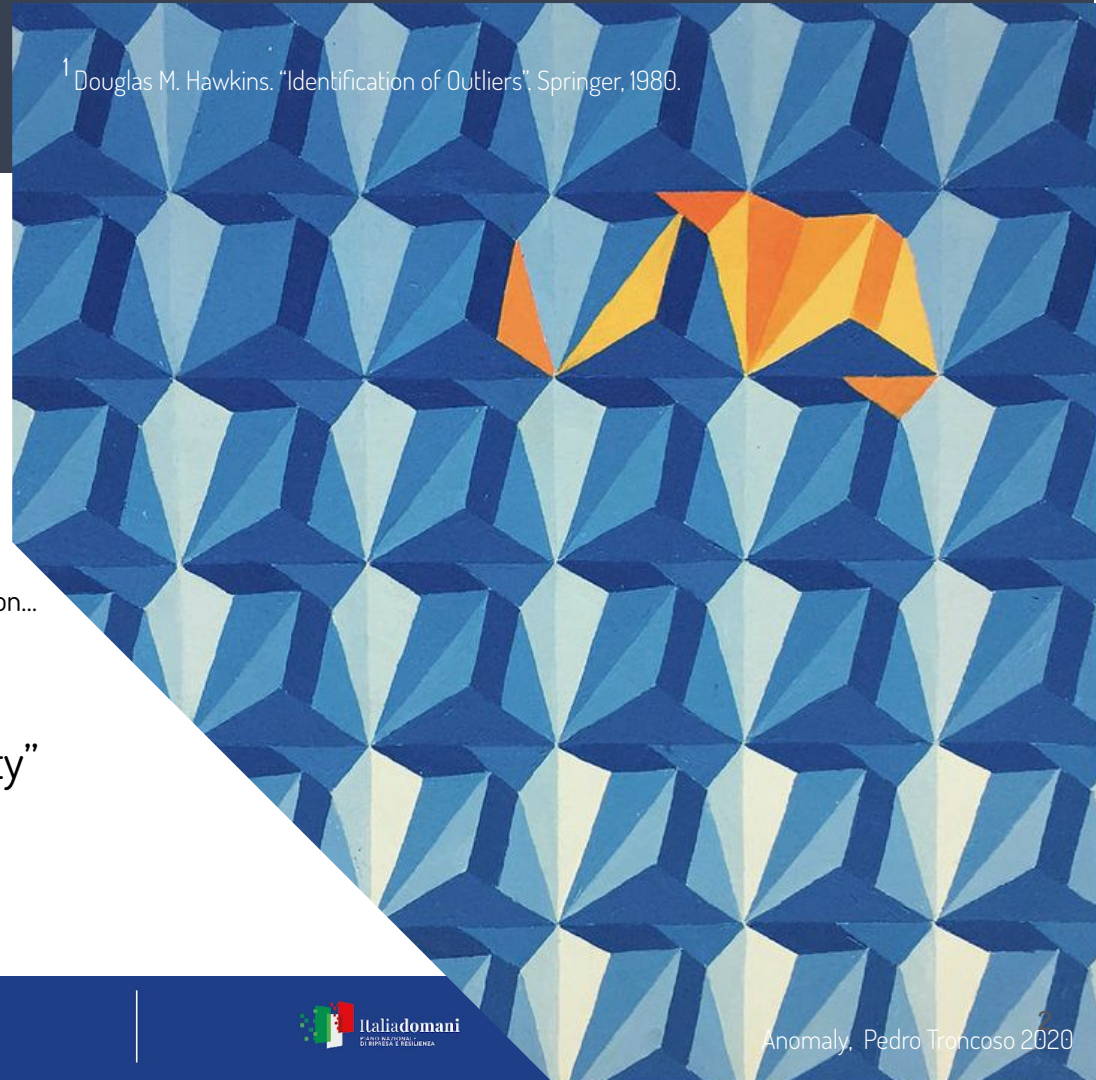
¹ Douglas M. Hawkins. "Identification of Outliers". Springer, 1980.

The science of identifying outliers

"...observations that deviate so much from other observations as to arouse suspicion that they were generated by a different mechanism"¹

Most diverse domains: card fraud detection, industrial damage detection...

- Pathology as deviation from "normality"



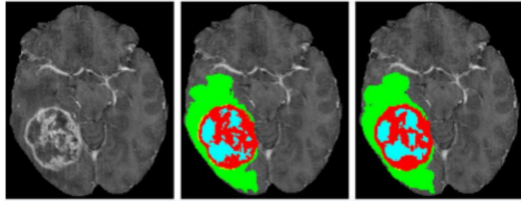
STATE OF THE ART

Unsupervised anomaly detection (clustering, Markov Random-fields, Dictionary Learning, ..)

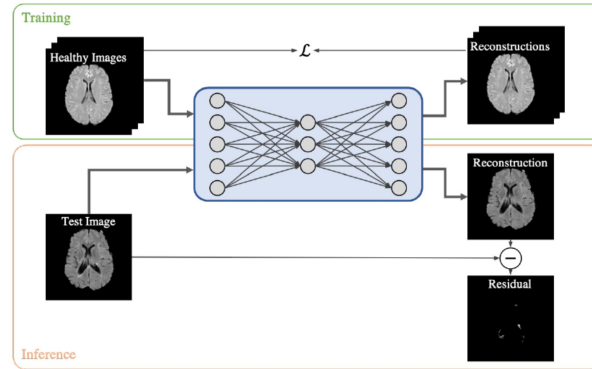
Supervised anomaly detection (Convolutional neural networks)

Semi-supervised anomaly detection (Auto-encoders)

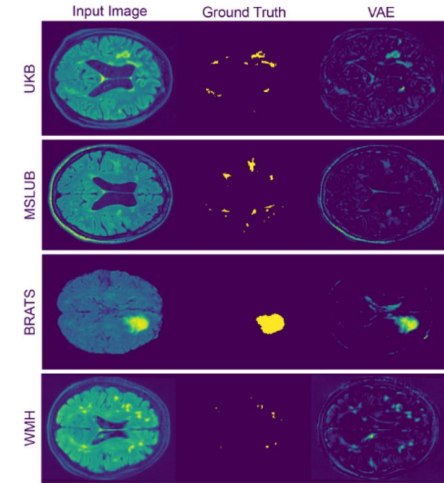
Try emulate the capability of the human eye to exploit the prior knowledge of how healthy brains should appear, in order to reach anomaly detection performance comparable to the ones of neuroradiologists



Pereira et al. "Brain Tumor Segmentation Using Convolutional Neural Networks in MRI Images", 2016



Auto Encoder + GAN



Pinaya et al, 2022

PROPOSED METHOD

A framework for general purpose & modality agnostic Anomaly Detection.
The main outputs of our machine-learning algorithm are anomaly score and probability maps

- **Explainable:** merely practical motivation: might need to justify the decision to someone (patient, ..)
- **Generalizable** might not know a priori what is to be found
- **Applicable to small data sets** it can be “localized” on centers data

Recipe:

- 1) Choose metrics to measure distance from a normative dataset (1-to-many, voxel-per-voxel)
- 2) Define “normality” boundaries
- 3) Assign anomaly score o probability

DISTANCE METRICS > PCA-based

Find normative set eigenvectors \rightarrow Project target image \rightarrow Measure recon. error $(I_{\text{orig}} - I_{\text{rec}}) / \sigma_{\text{normative}}$

Linear version of an auto-encoder

Good sensibility to small intensity differences

Decent sensibility to texture differences

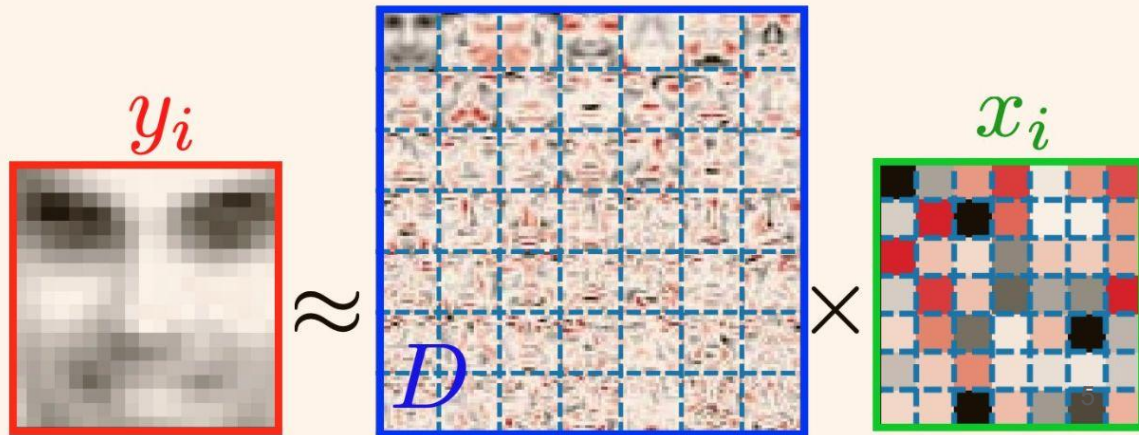
Typically we have: $N_{\text{normative}} \times d \Rightarrow d \times (N_{\text{normative}} - 1)$ if $N_{\text{normative}} < d$

Principal Component

Analysis (SVD):

$$\mathcal{X} = \{X ; XX^T = \text{Id}\}$$

$$\mathcal{D} = \{D ; D^T D = \text{Id}\}$$



DISTANCE METRICS > NMF-based

Find normative set basis \rightarrow Project target image \rightarrow Measure recon. error $(|I_{\text{orig}} - I_{\text{rec}}|) / \sigma_{\text{normative}}$

Unlike PCA, the elements of the base are non-negative and sparse: they represent the individual parts of the data

Poor sensibility

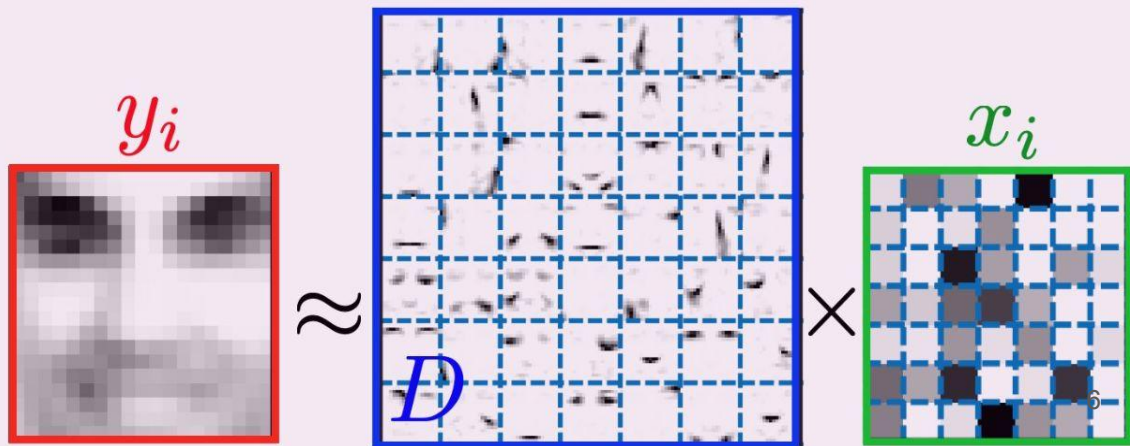
No mirror artefacts

We chose: $\sqrt{N_{\text{normative}}}$ basis images

Non-negative Matrix
Factorization (NMF):

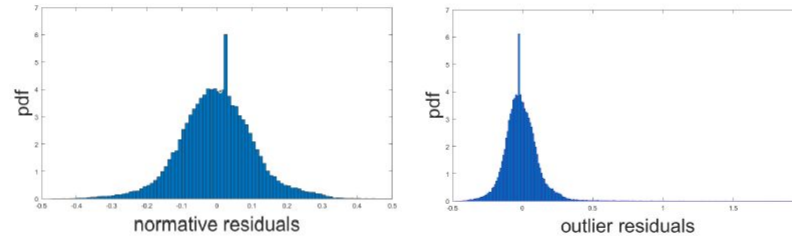
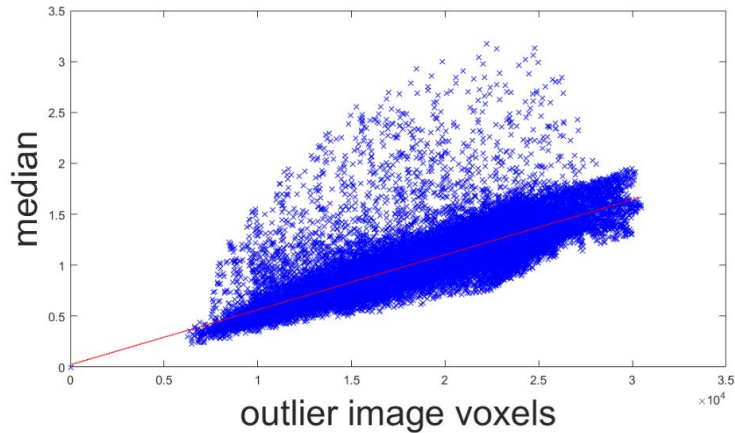
$$\mathcal{X} = \{X ; X \geq 0\}$$

$$\mathcal{D} = \{D ; D \geq 0\}$$



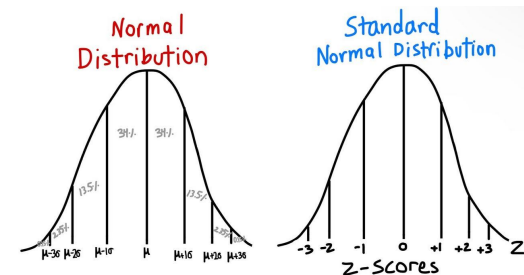
DISTANCE METRICS > Res, Z-score

Standardized residuals \rightarrow (vertical distance between the point and the fitting line) / $\sigma_{\text{normative}}$



Example: residuals of normative images are distributed as a Gaussian, while the pdf of the outlier image residuals has a pronounced right tail

Z-score \rightarrow distance from normative set mean in σ units

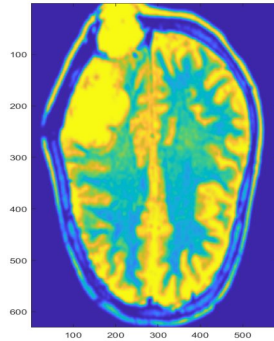


DISTANCE METRICS > STD, H

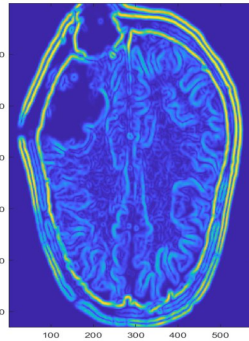
“Texture” metrics: capture pattern-based anomalies. Defined on a 5x5x5 voxel volume.

Standard deviation metric $\frac{STD_A(i,j,k) - M(i,j,k)}{S(i,j,k)}$

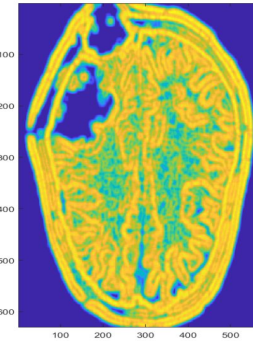
Entropy metric $\frac{H_A(i,j,k) - M(i,j,k)}{S(i,j,k)}$



original MRI image (brain tumor)



Entropy image



STD image

LOCAL OUTLIER FACTOR

Local Outlier Factor: comparing the local density of a point with the densities of its k -nearest neighbors. A point that has a much lower density than its neighbors is considered outlier.

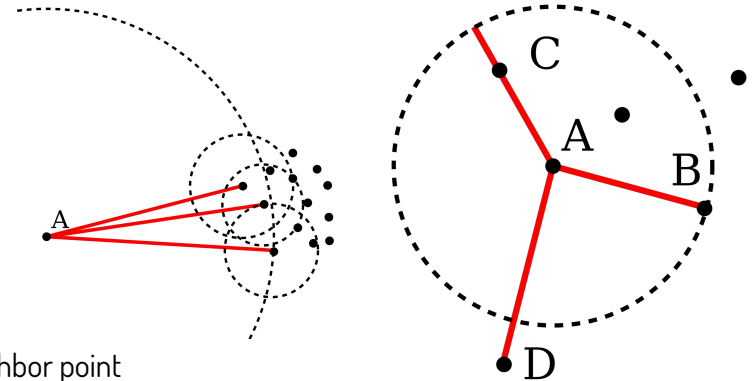
K-distance (D) is the distance of a point to its k -th neighbor

Reachability distance (RD) is the distance need to travel from particular point to its neighbor point

$$\max(k\text{-distance}(B), \text{distance}(A, B))$$

Reachability distance (LRD) is the inverse of the average RD of its neighbors

LOF score is the average LRD of the neighbors divided by object's own LRD



$$LRD_k(x) = 1 / \left(\frac{\sum_{o \in N_k(x)} d_k(x, o)}{|N_k(x)|} \right)$$

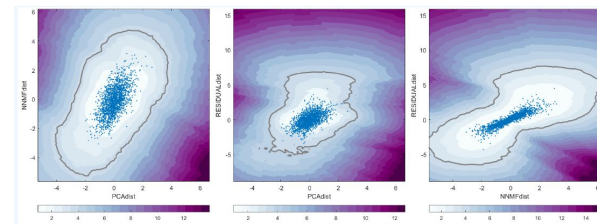
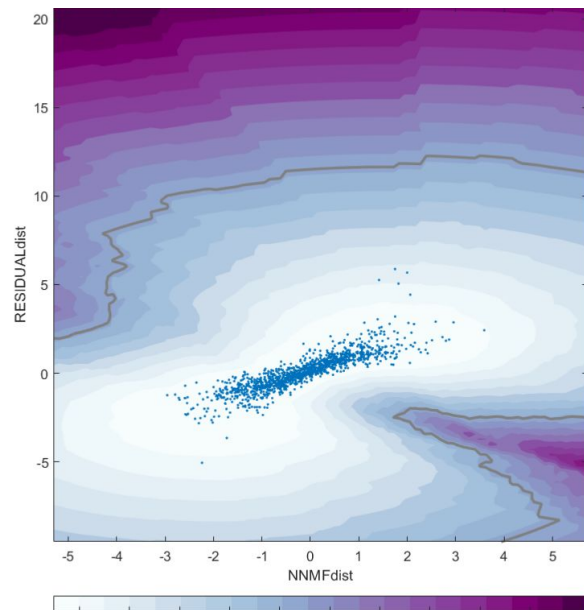
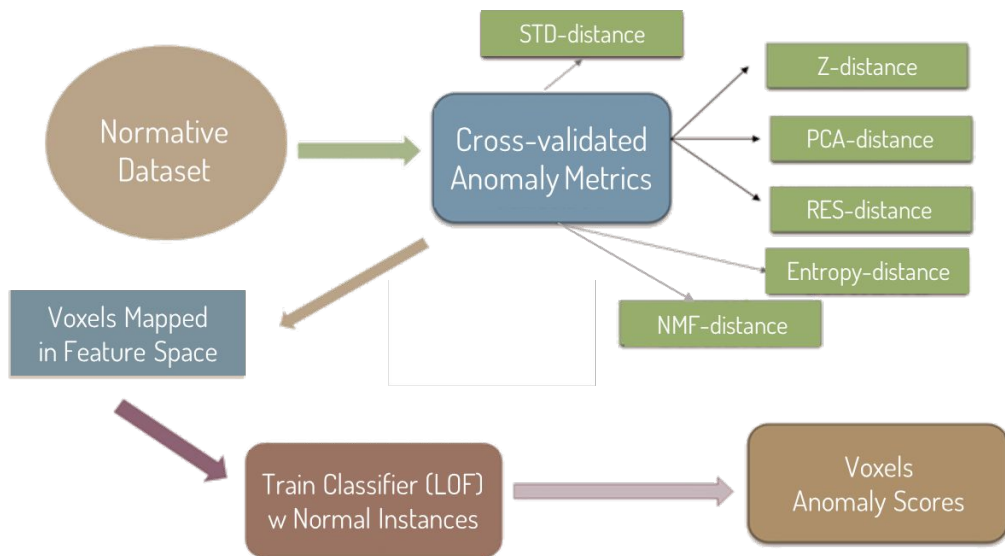
$$LOF(x) = \frac{\sum_{o \in N_k(x)} \frac{LRD_k(o)}{LRD_k(x)}}{|N_k(x)|}$$

TRAINING

Distance images are created from normative instances:

LOF operates in 2D feature subspaces (e.g., NMF-distance vs RES-distance)

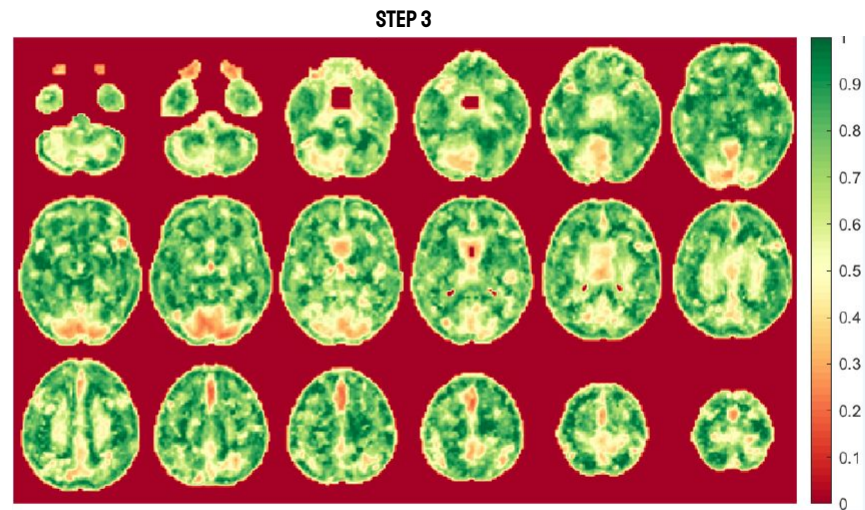
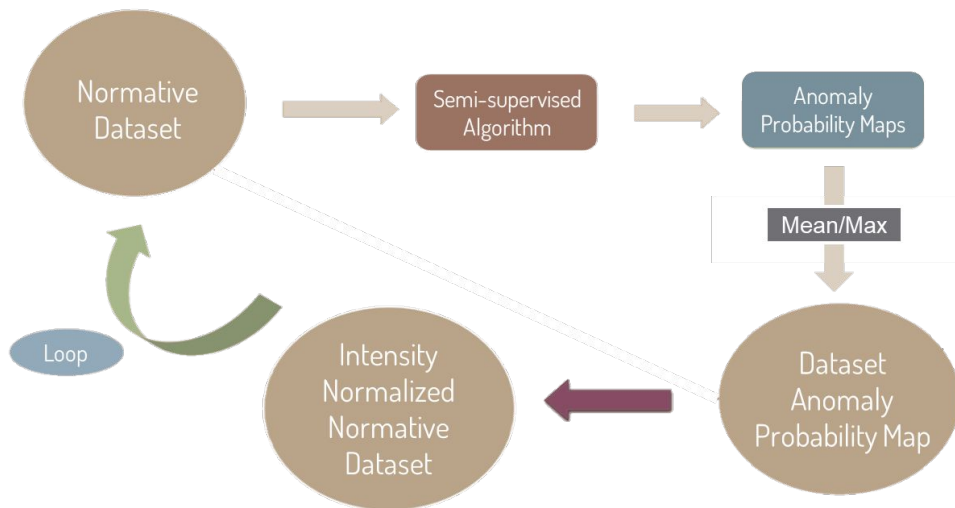
The system assigns an anomaly score to each pixel, and those above a certain threshold (determined by the algorithm) are classified as anomalies



INTENSITY NORMALIZATION

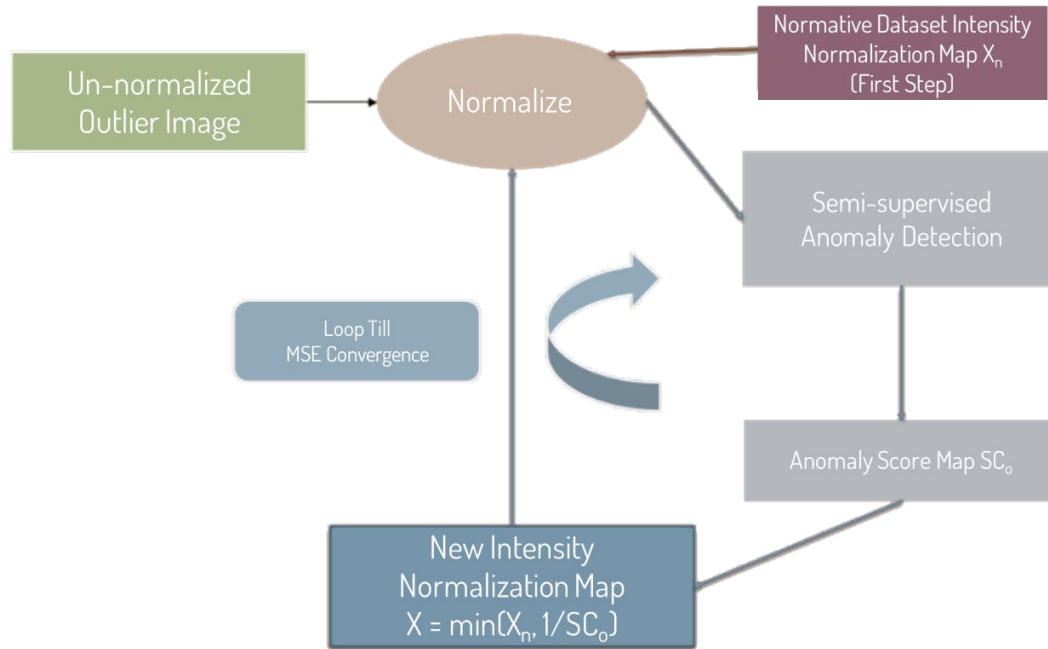
Intensity normalization is typically region-based (e.g., segmentation, non-affected region), whole-brain or limited to normal subjects. Risks: pathology dependent, sensitive to outliers..

To remain general, we chose to stick with total counts in data-driven masks (auto-calibration)



Auto-calibration for normative dataset (a *faster* version is also available..)

TESTING



Auto-calibration for test image

Test images undergo a similar procedure

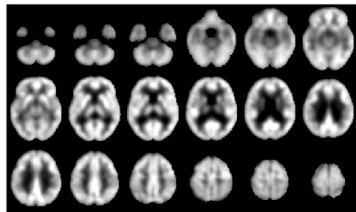
Intensity normalization is so that normative dataset intensity normalization map X_n is combined to with SC_o to obtain an intensity normalization where anomalous regions have a lower weights

$$x(i) = \min \left(X_n(i), \frac{1}{SC_o(i)} \right)$$

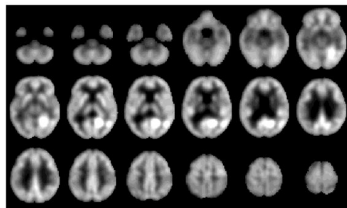
SYNTH FDG-PET DATA

The anomaly images are created by adding pseudo-Gaussian intensity anomalies onto images of the normative dataset

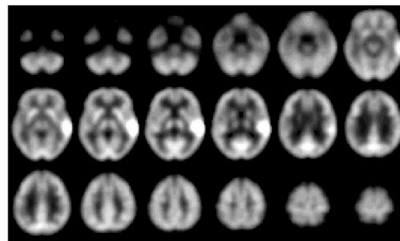
$$H(x, y, z) = a \exp\left(-\left(\frac{x - x_0}{\sigma}\right)^s\right) \exp\left(-\left(\frac{y - y_0}{\sigma}\right)^s\right) \exp\left(-\left(\frac{z - z_0}{\sigma}\right)^s\right)$$



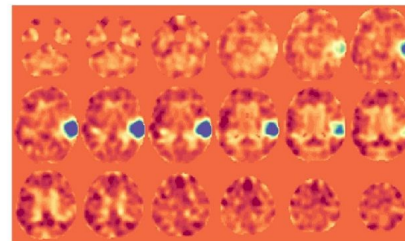
(a) ORIGINAL



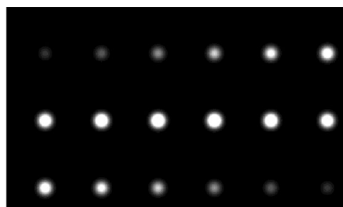
(b) synthA



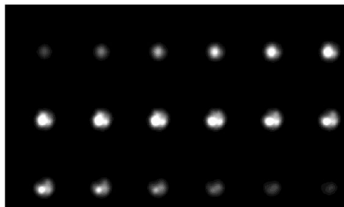
(a) SynthA



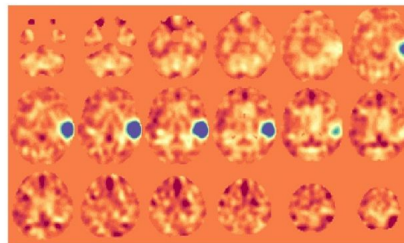
(b) NMF-distance



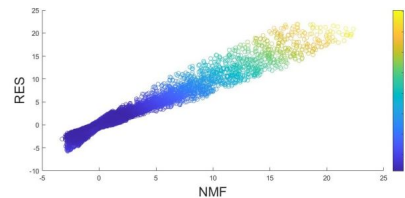
(a) synthH



(b) delta

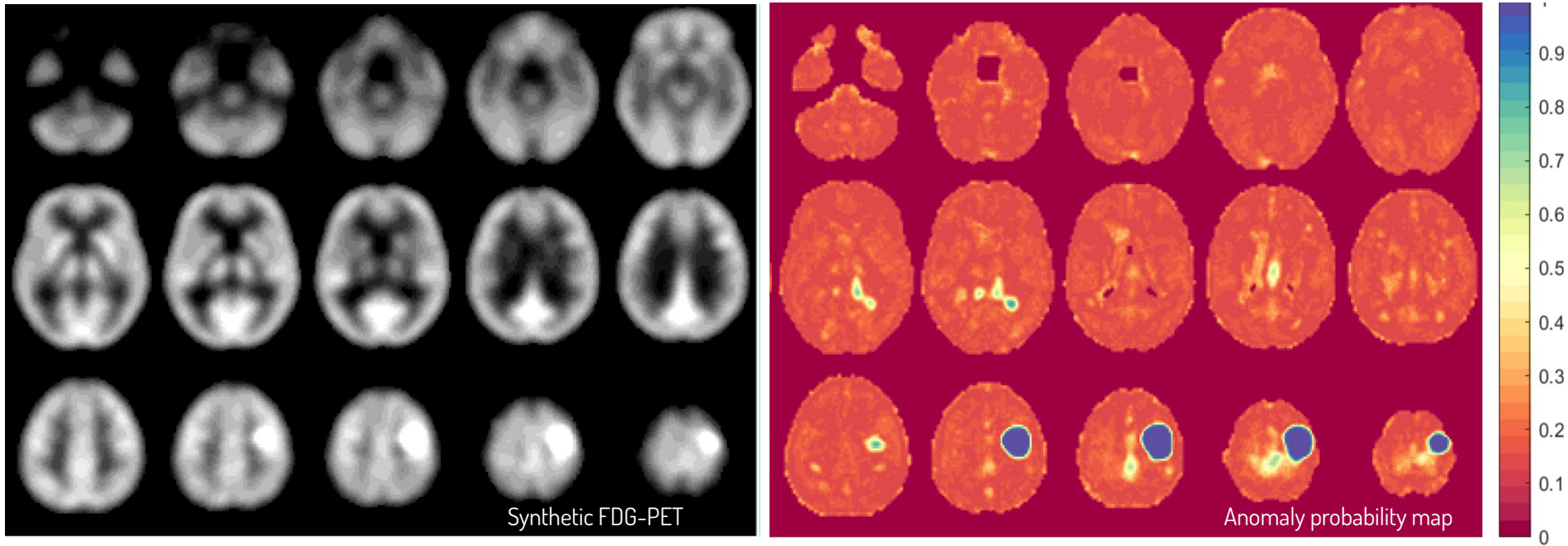


(a) RES-distance



(b) LOF scores

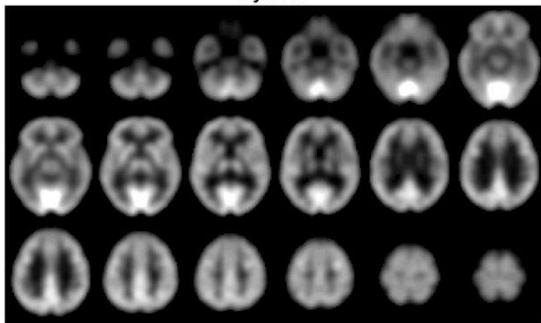
SOME RESULTS



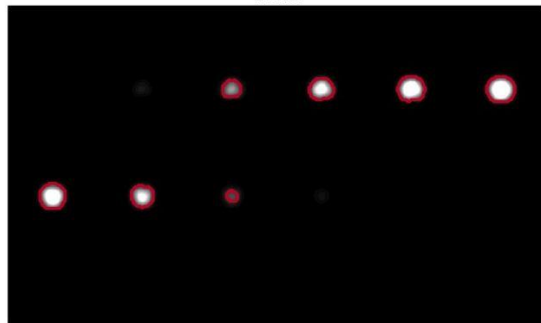
100 synthetic FDG-PET images created from 125 real FDG-PET of healthy subjects (San Martino Hospital, Genoa). Example shows a high accuracy in hyper-metabolism detection.

SOME RESULTS

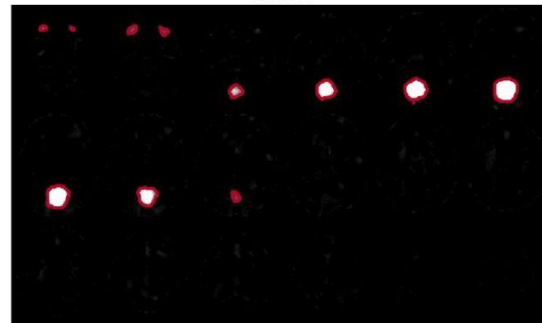
synthA



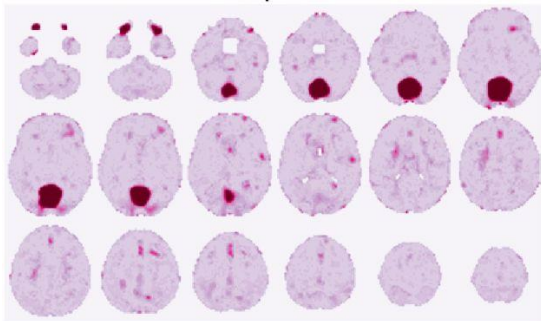
delta



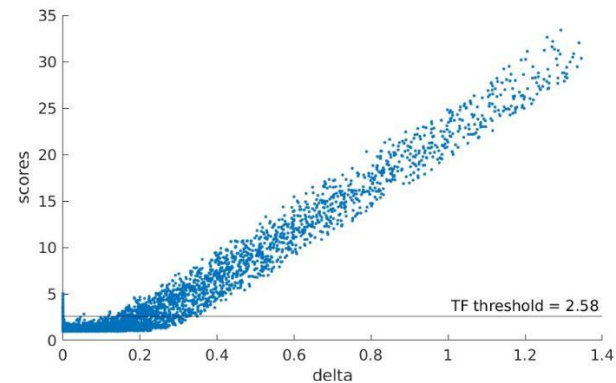
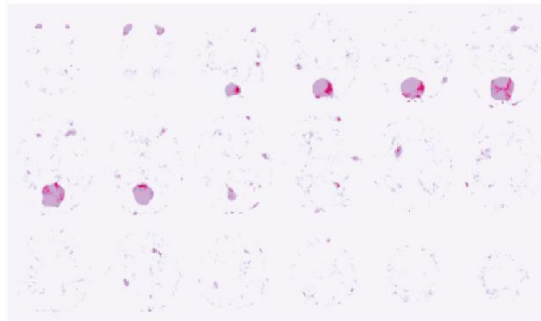
scores



anprob



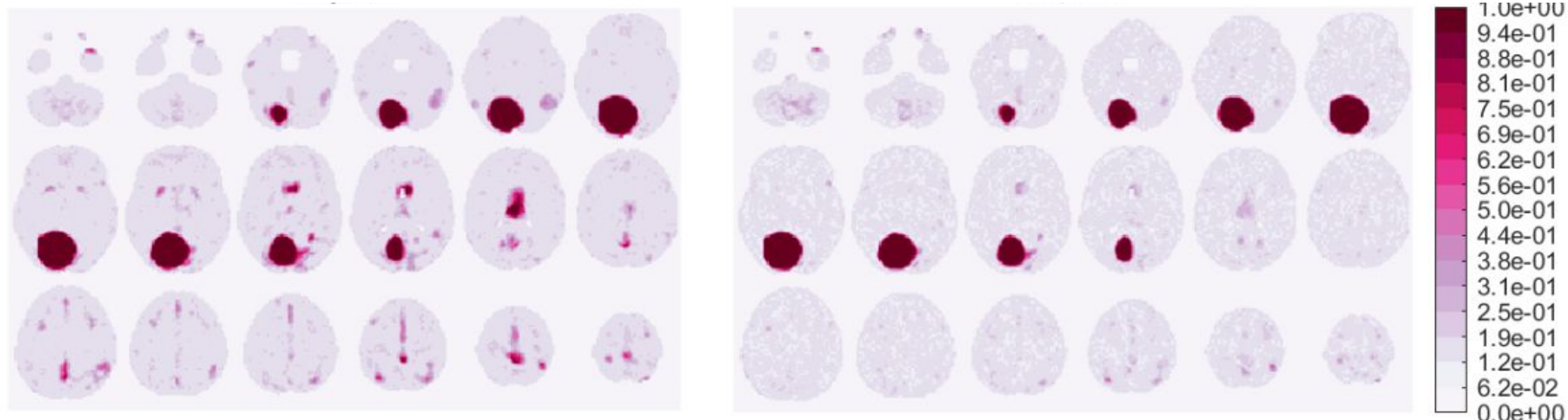
LR



SOME RESULTS

Auto-calibration proves to be best suited in this context: anomaly probability maps come out cleaner

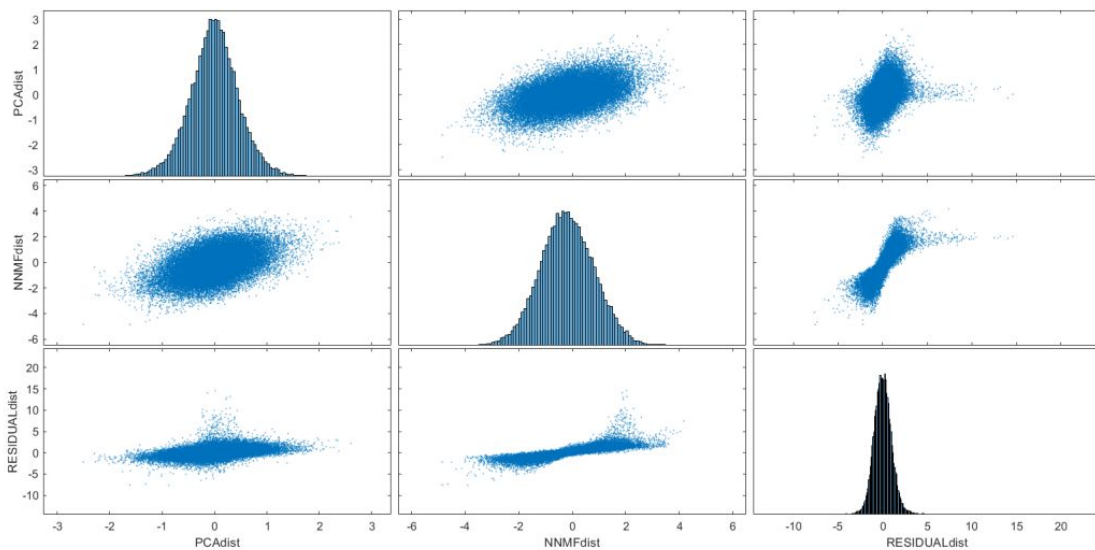
Whole-brain normalized (NMF vs RES) - Auto-calibrated



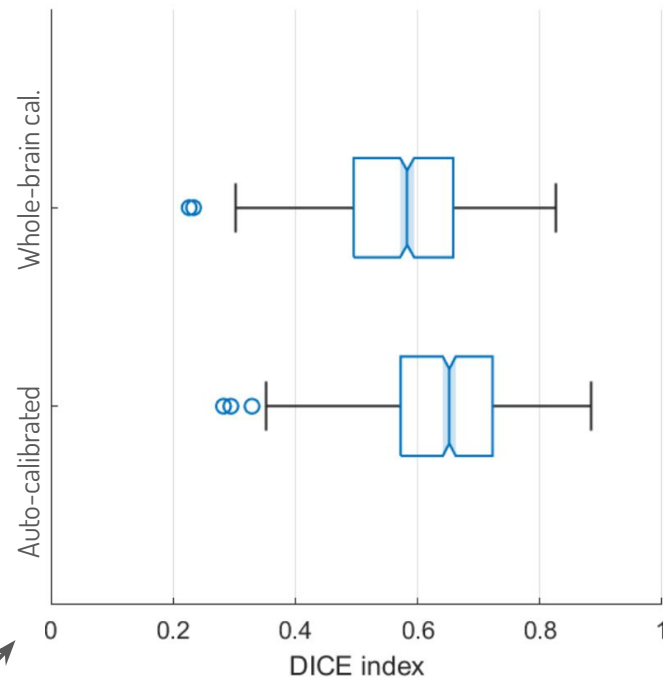
Anomaly probability

SOME RESULTS

Histogram shapes show discrepancies in metrics comparison

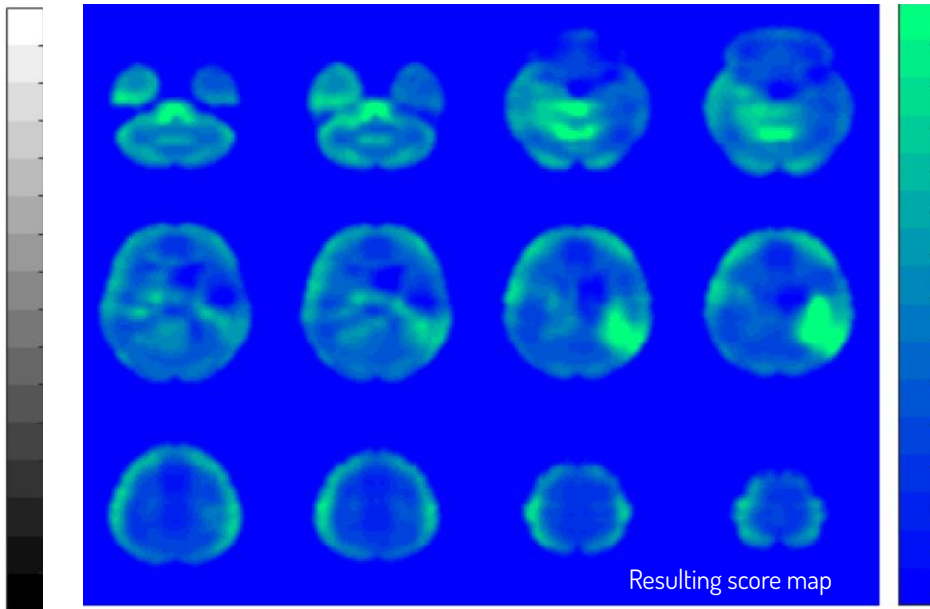
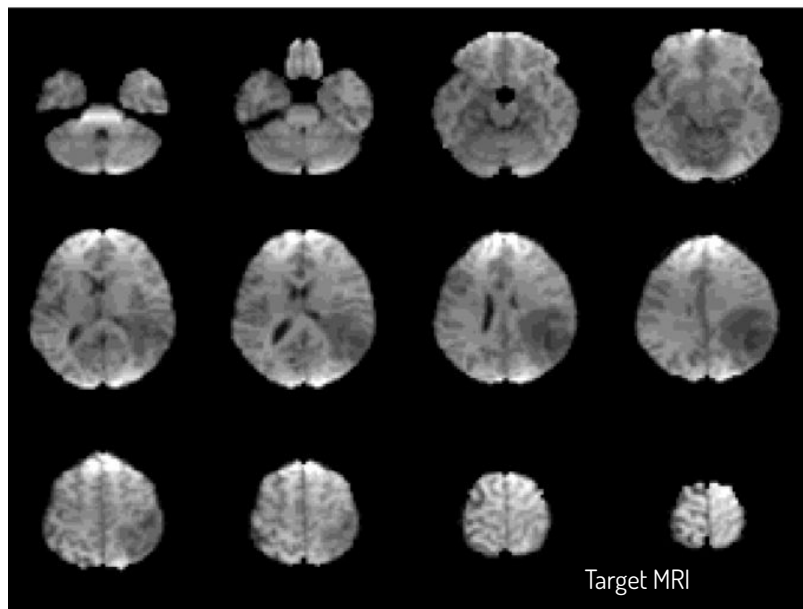


Importance of intensity normalization



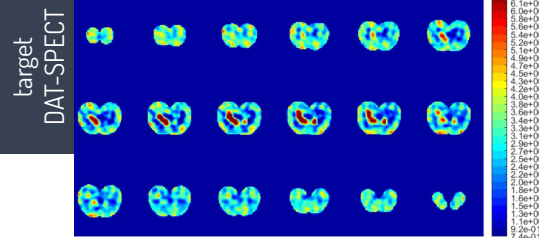
$$cDICE = 1 - \exp \frac{\sum x(y < 0)}{\sum x(y > 0) \log(0.5)}$$

MRI DATA



20 MRI of glioma affected patients; system trained on 75 healthy subjects (San Martino Hospital, Genoa). Example shows the accuracy in detection. The task was complicated by the fact that anomaly is not ipo nor hyper-intense

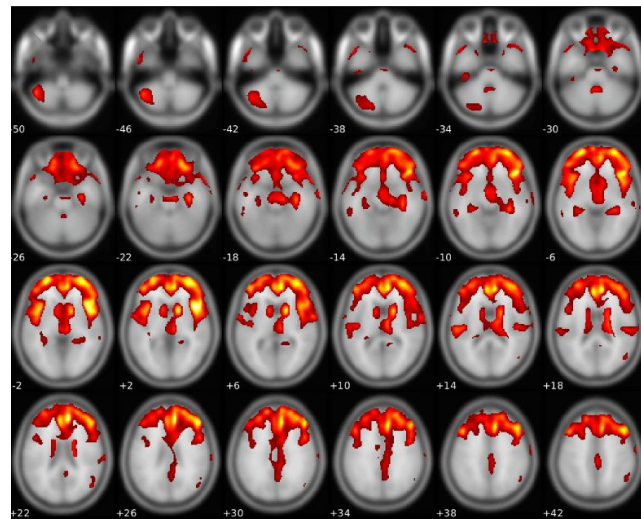
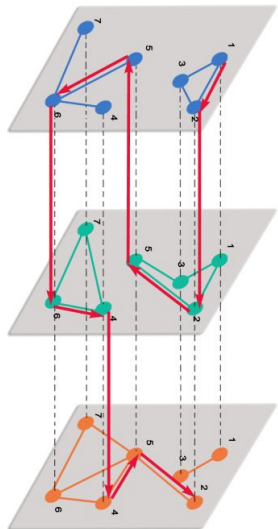
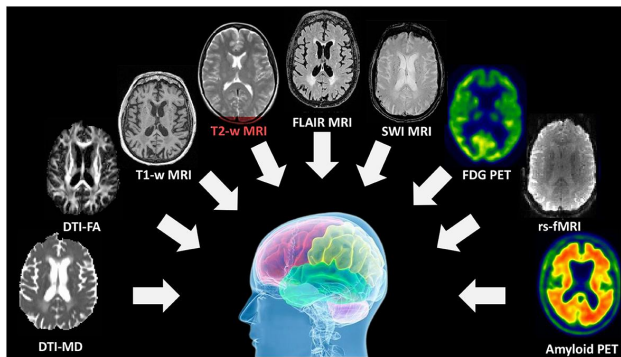
PERSPECTIVES



To test: Different metrics, alternatives to Local Outlier Factor

To test: Compare with well-known voxel-based morphometry software (FDG-PET)

To study: Score maps from different modalities composed into multi-layered matrix to study pathology models?



Thank you for your attention

