

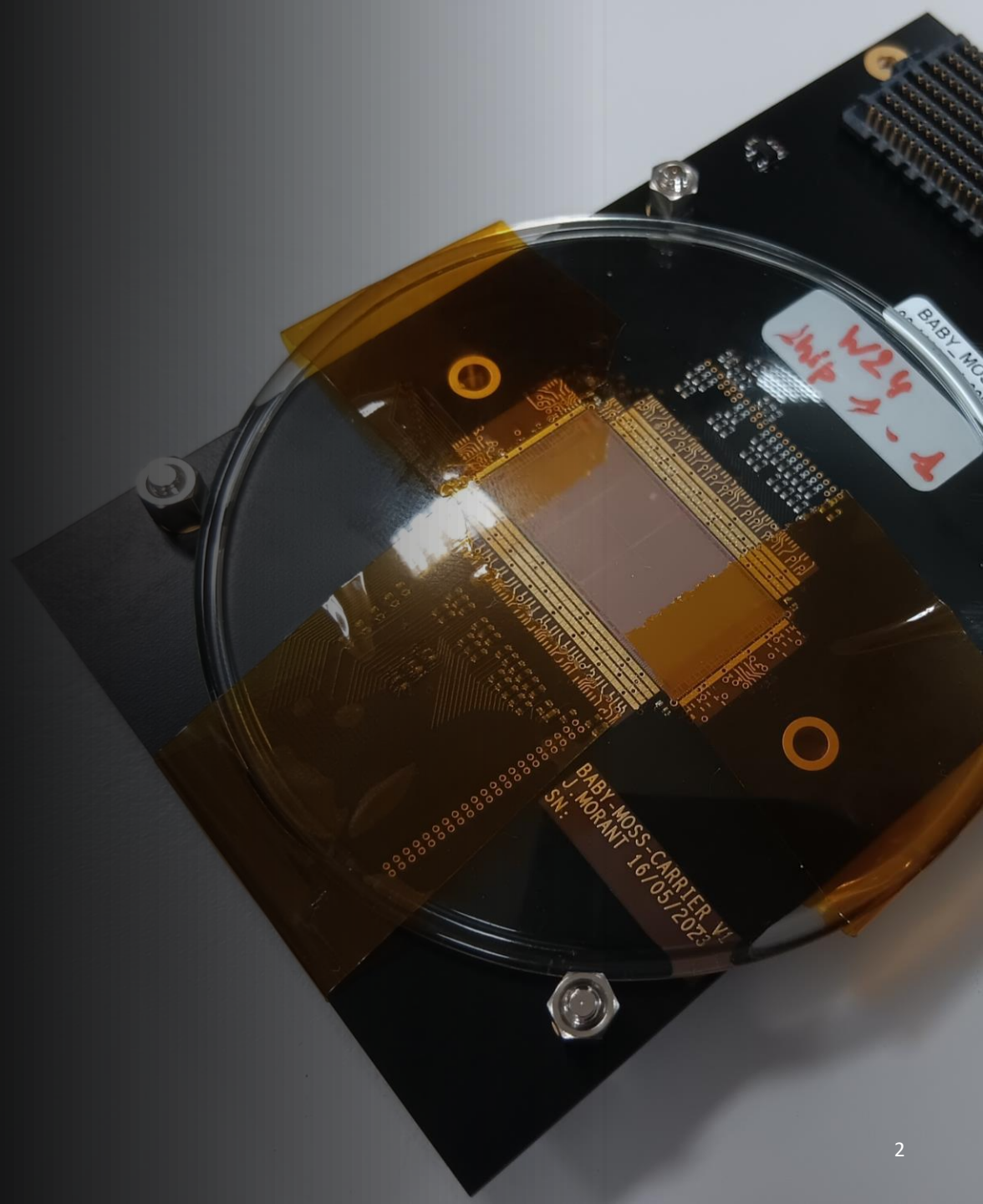
Studies on MAPS devices for medical applications.

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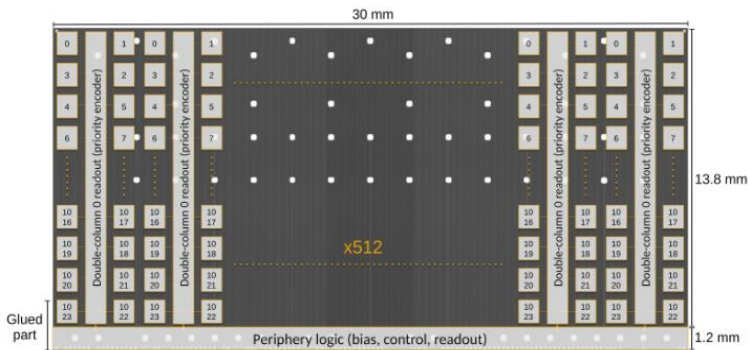
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The ALice Pixel DEtector.



The ALICE Pixel DEtector



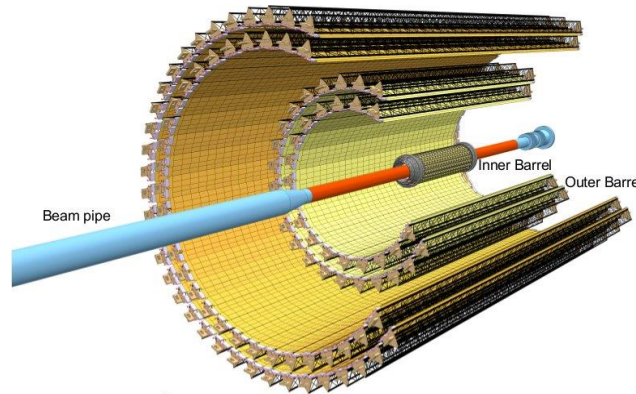
- Developed for the particle tracking of ALICE experiment at CERN (detection unity of the current ITS2).
- High performing MAPS, based on CMOS technology.
- 5×10^5 pixels (512 rows x 1024 columns).
- Pixel size = $29.24 \times 26.88 \mu\text{m}^2$.
- Total area = $15 \times 30 \text{ mm}^2$.

Performance in HEP:

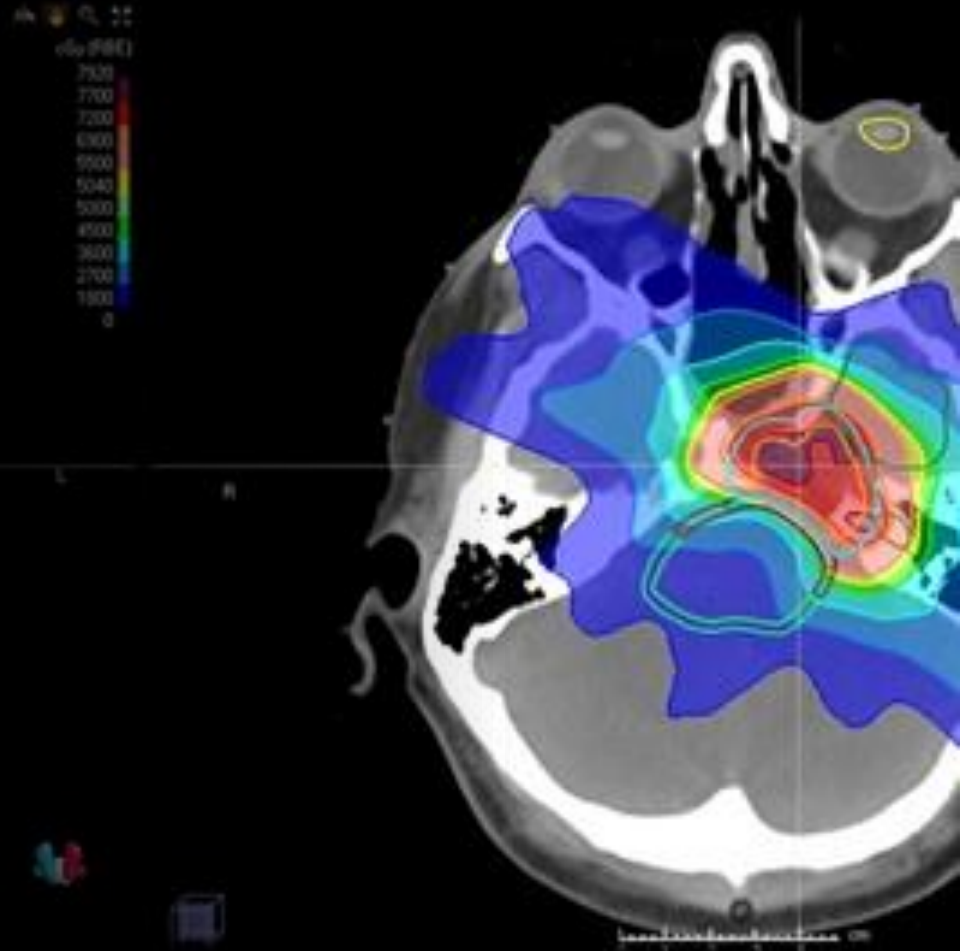
- Detection efficiency $> 99\%$
- Fake hit probability $\ll 10^{-6}$
- Spatial resolution $\approx 5 \mu\text{m}$
- Designed for operating at high rates and particle density environments.



A varied range of medical applications can benefit of the technological evolution of MAPS as commercial devices.

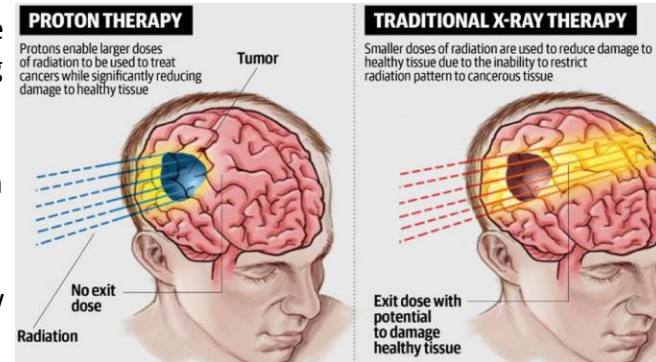
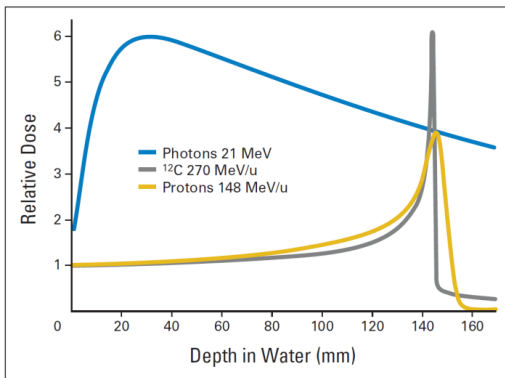


System for computerized tomography with a proton beam [ref1].



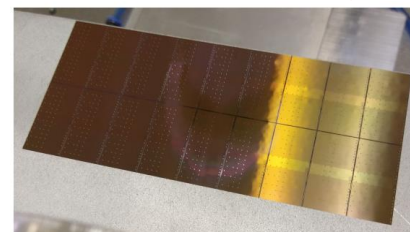
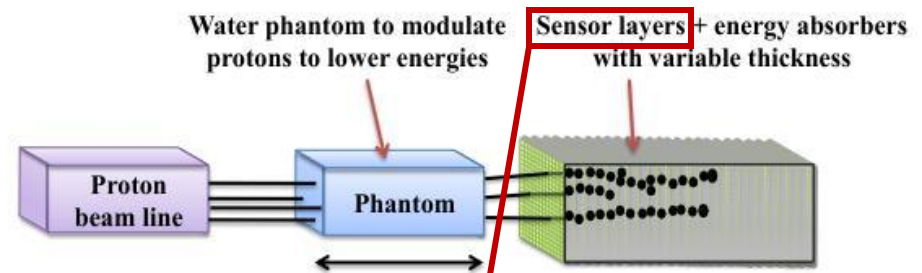
System for computerized tomography with a proton beam.

- Protons experience a continuous slow down as they cross matter, until they stop and release a large fraction of their initial energy, originating the Bragg pick at the end of their path.
- From measuring the energy loss of the protons in the tissues, a pCT can be performed.
- Dose delivered to the patient with a pCT (few mGy).
At least an order of magnitude lower than traditional X-ray CT (10–100 mGy).



Hybrid calorimeter with layers of pixelated silicon sensors.

- Single technology for both tracking and residual energy measurement would simplify the system assembly and guarantee stable operation in a clinical environment.
- Needs to fulfill the requirements to handle pencil beams with therapeutic characteristics:
 - High particle rate and localized dose depositions.
 - Readout speed fast enough to handle many tracks at the same time.
 - Accurate determination of the ranges of individual protons.



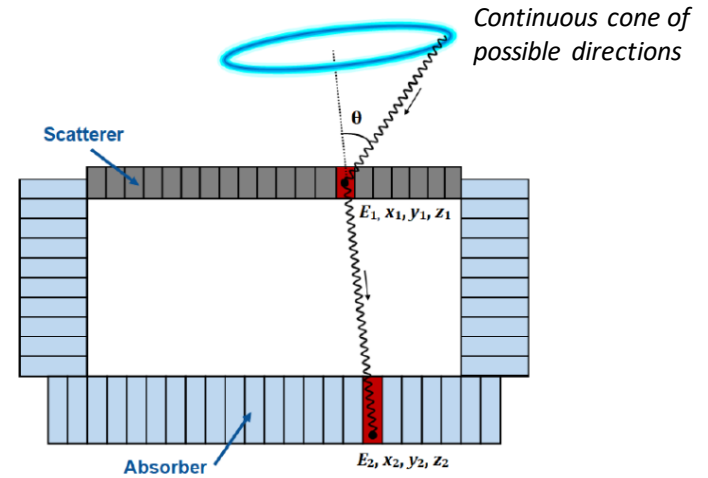
Prototype of a silicon pixel detector with area of $138 \times 60.1 \text{ mm}^2$ and thickness of $40 \mu\text{m}$.

Compton
Camera for
hadron-therapy
with a 3D silicon
Pixel Chamber
[ref2, 3].

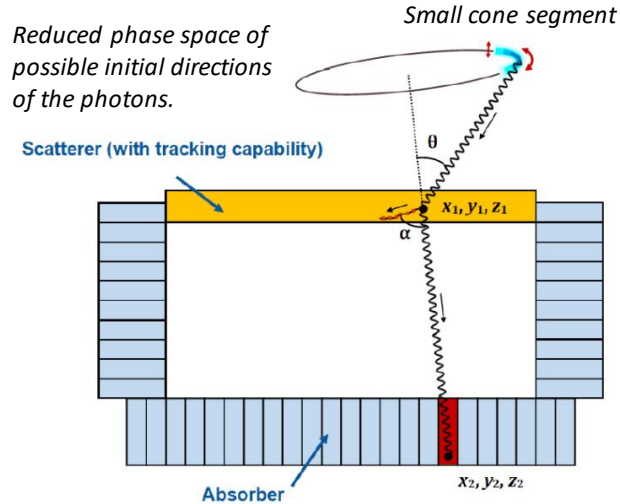


Compton Camera for hadron-therapy with a 3D silicon Pixel Chamber.

- Compton Cameras can perform in vivo beam monitoring during hadrontherapy treatments.
- High-resolution imaging of direct gamma sources is required to perform a precise monitoring over a time of a few seconds.
- Several gammas from the same source point are needed to reconstruct the source position (The direction of a single incident gamma cannot be determined univocally).

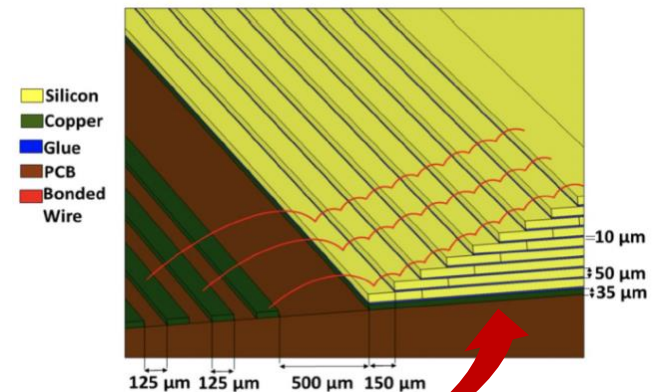


New concept of Compton Camera with a Pixel Chamber as the scatterer



- Reconstruction of the trajectory of the recoil electron.
- More constraint on the reaction plane of the Compton interaction.
- Reduction by order(s) of magnitude the numbers of gammas required for a precise source imaging.
- The acquisition time would match the needs for in vivo monitoring during hadrontherapy

Stack of ultra-thin ALPIDE on top of each other to provide a continuous three-dimensional tracking.



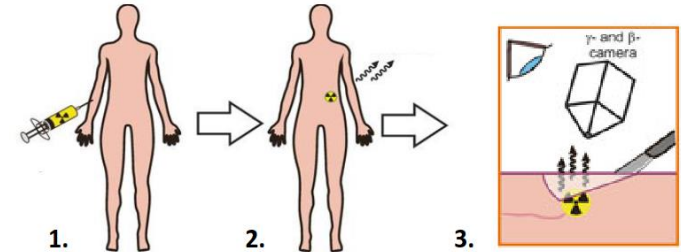
The high granularity, low thickness and high spatial resolution makes ALPIDE an excellent candidate for the Pixel Chamber.

Radio-Guided
Surgery with
 β -emitting
radio-tracers
[ref4].



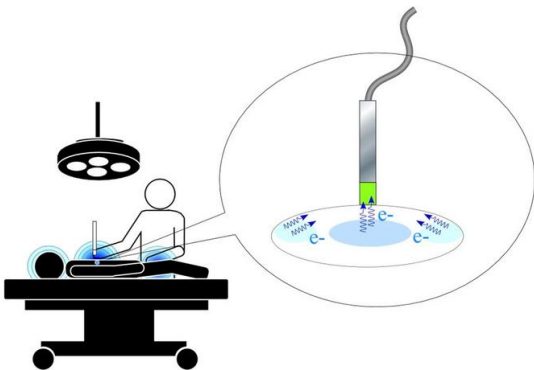
Radio-Guided Surgery with β -emitting radio-tracers

- The goal is to allow the surgeon to localize tumoral masses in real time.
 - Before the intervention, a dose of a radiotracer, preferentially absorbed by tumoral cells, is administered to the patient.
 - By detecting the emissions of the radiotracer with a dedicated probe, it is possible to identify the primary tumor.
- The usage of a probe with imaging capabilities may allow the surgeon to identify the borders of the tumoral masses with great precision.



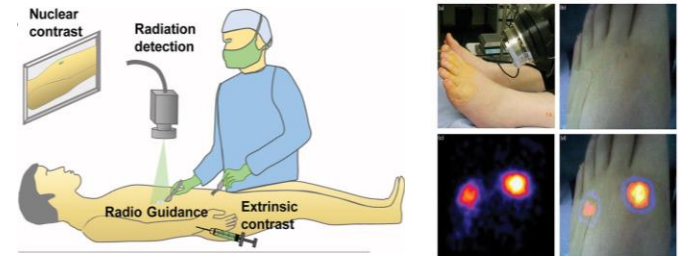
β -emitting radio-tracers:

- Limited background because their short range in human tissue (few mm at $E \approx 200$ KeV.) compared to γ -emitting radio-tracers (≈ 10 cm at $E \approx 200$ KeV).
- Higher spatial resolution ensures precise delineation of radioactive tissue.



β^+
The annihilation of positrons produce a background of 511 KeV γ with larger penetrating power.

β^-
Limited availability of the radiotracer and of suited detecting probes.



MAPS as intraoperative probes for RGS can satisfy the requirements:

- High e^- detection efficiency.
 - Low fake-hit rate.
 - Readout electronics inside the pixel.
 - Low power consumption (not need of a sophisticated cooling system).
- Possibility of realizing compact, handheld probes .



Excellent performance with β^- -emitting radio-tracers.

- Low sensitivity to photons \rightarrow Suited to be used with β^+ -emitting radiotracers).
- Excellent spatial resolution \rightarrow Optimal for a usage as imaging probes.



Thank you

List of projects:

- [1] RIPARTI, "Feasibility study of a system for computerized tomography with a proton beam"
- [2] PRIN 2022, "A pioneering Compton Camera for hadrontherapy with a 3D silicon Pixel Chamber"
- [3] Dipartimento di Eccellenza "Quantum Sensing and Modeling for One-Health (*QuaSiModO*)"
W.P.1.2, "Quantum and Innovative Particle Detectors for Health"
- [4] PRIN 2022 "Development of an innovative silicon pixel detector for imaging applications in radioguided surgery"