

A 3D imaging system for dosimetry in FLASH radiotherapy

E. Ravera^{1,2}, R. Anzalone^{1,2}, A. Cavalieri¹, E. Ciarrocchi^{1,2}, D. Del Sarto^{1,2}, F. Di Martino^{3,4,2}, M. Morrocchi^{1,2}, and M. G. Bisogni^{1,2}

1) Università di Pisa, 2) Istituto Nazionale di Fisica Nucleare - sezione di Pisa, 3) U.O. Fisica Sanitaria, 4) Azienda Ospedaliera Universitaria Pisana

eleonora.ravera@phd.unipi.it



Motivations and challenges

To develop a detector for **online 3D dosimetry** in quality assurance protocols and beam characterization for **FLASH-RT**, a new radiotherapy modality characterized by Ultra High Dose Rate >40 Gy/s, whereas conventional radiotherapy 1 Gy/min.

- Issues [1]
- Linearity at high-dose-rate
 - 3D measurement with high resolution
 - Real-time capability

Proposed detector

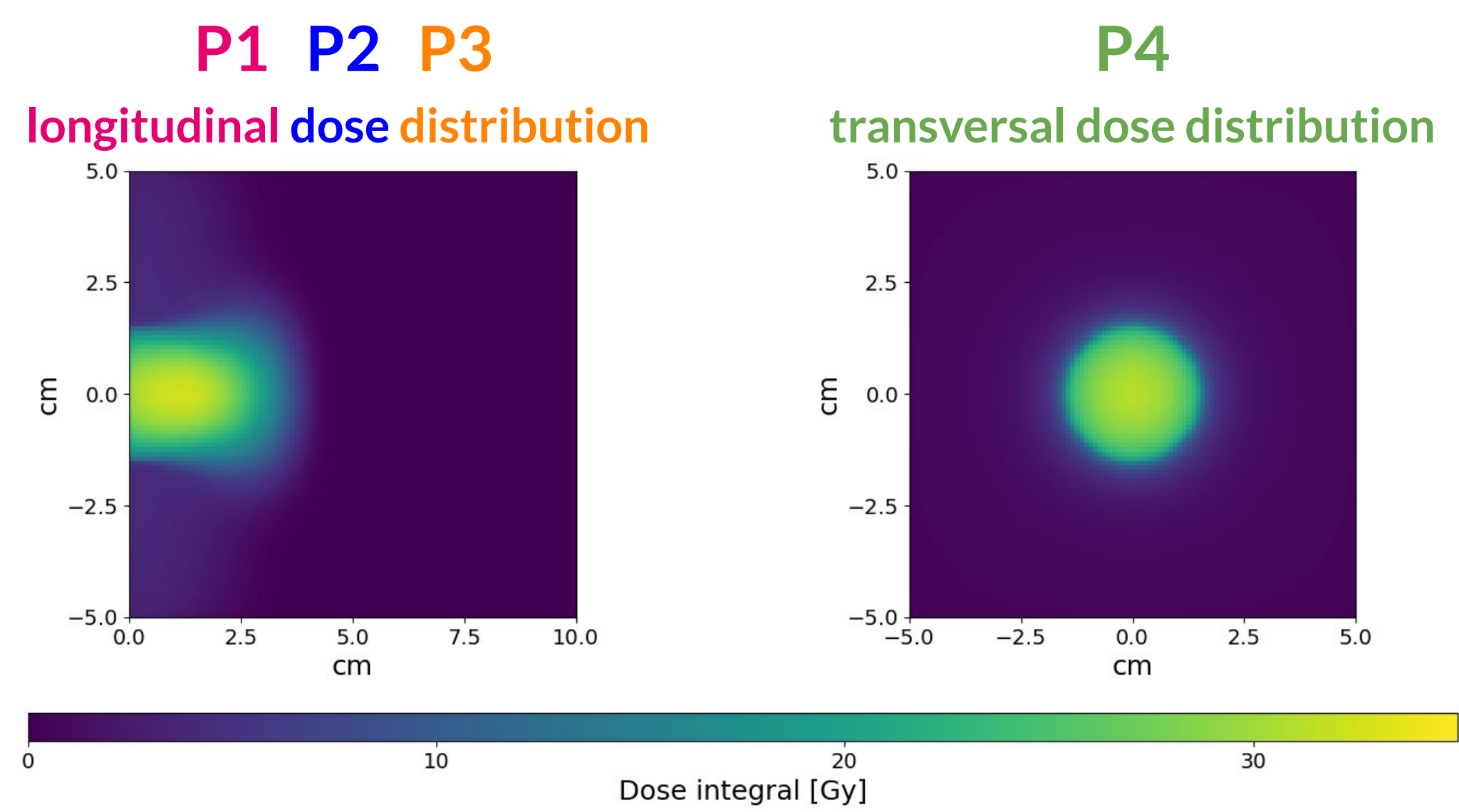
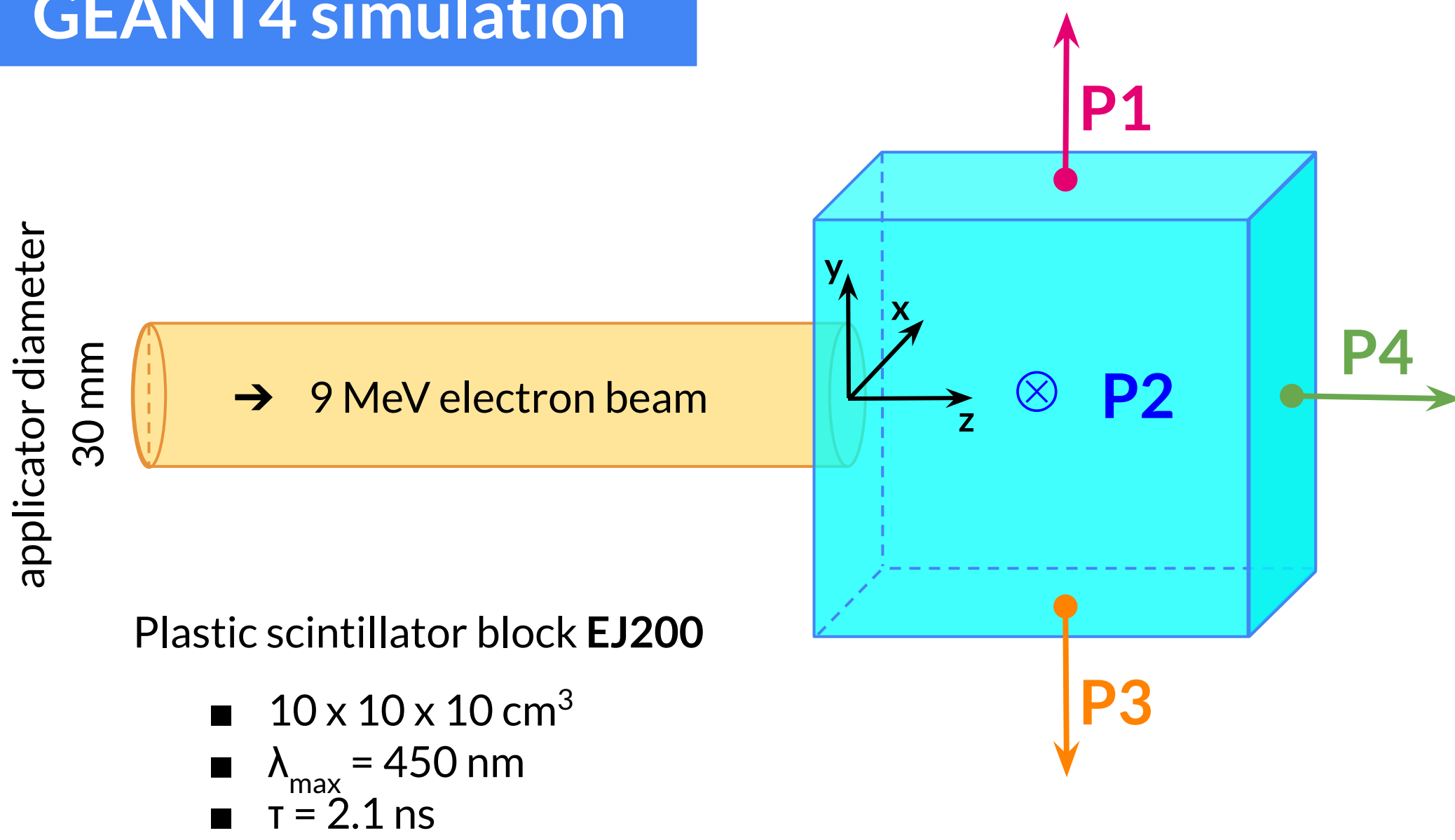
The detector consists in a **monolithic block of plastic scintillator EJ200** read out by four scientific cameras, each measuring a different projection of scintillating light.

The acquisition of four light projections enables a **tomographic reconstruction** of the volumetric dose distribution released by a 9-MeV electron beam within the scintillator

Why plastic scintillators? [2]

- ✓ **Linear response** within high dynamic range, suitable for FLASH applications [3]
- ✓ Spatial resolution **$\sim 100 \mu\text{m}$**
- ✓ Time response in **$\sim \text{ns}$**
- ✓ **Prompt readout**, if coupled to a camera
- + Good for treatment plan verification:
 - ✓ tissue equivalent
 - ✓ reusable and cost-effective

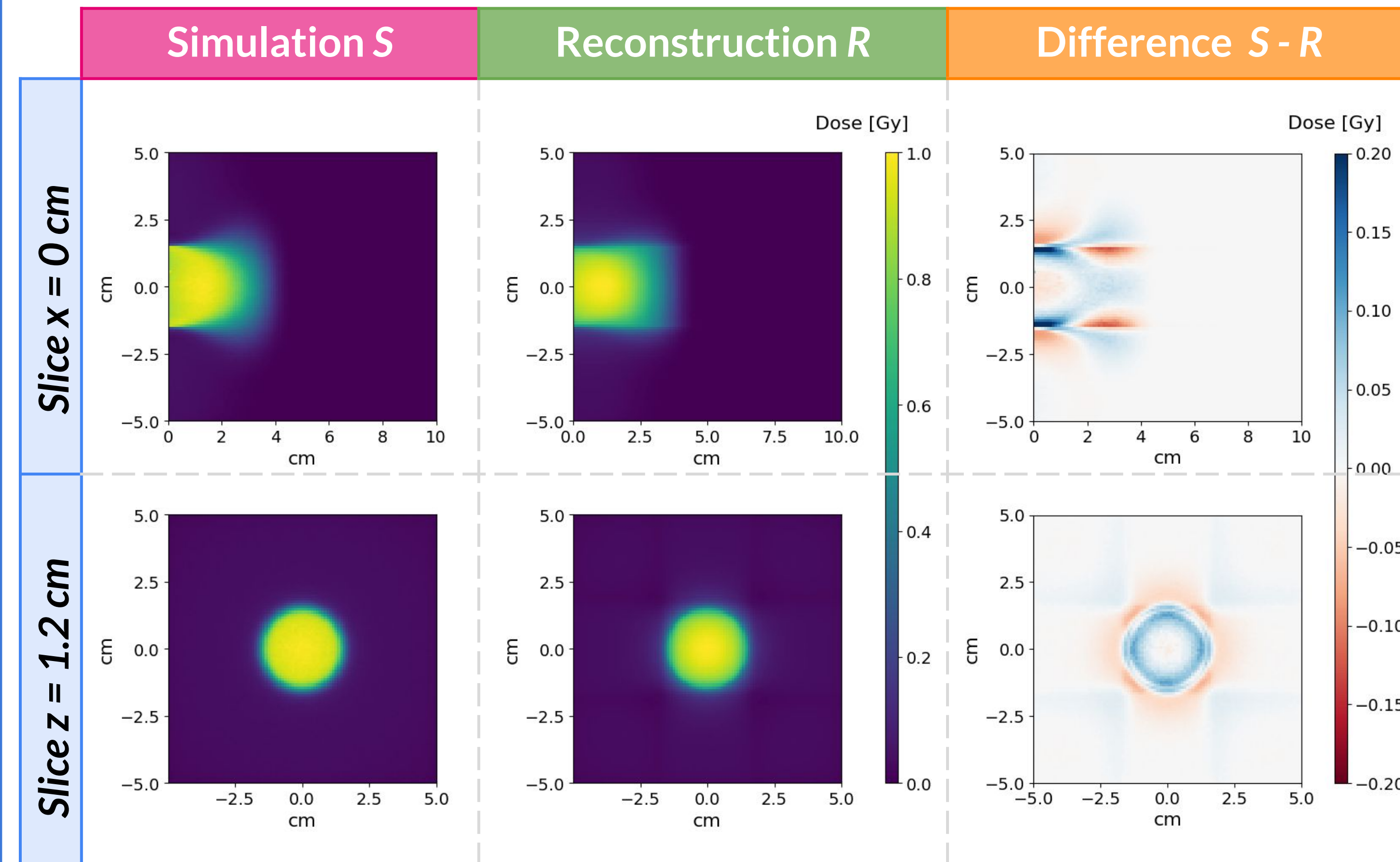
GEANT4 simulation



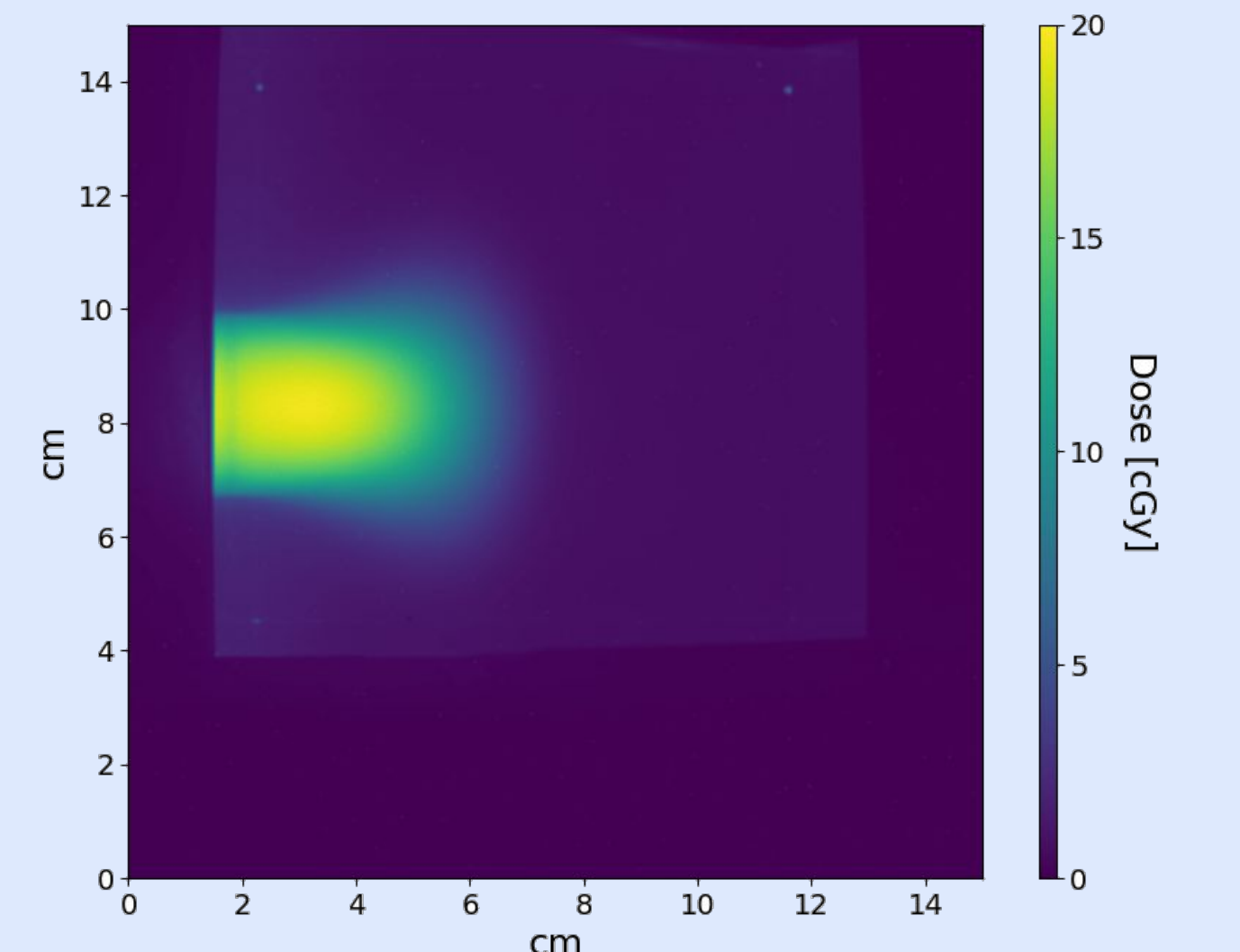
Parallel projection of the volumetric dose distribution
Dose Per Pulse = 1 Gy, Voxel = 1 mm^3

Tomographic reconstruction and comparison

- Iterative methods, such as Maximum Likelihood Expectation Maximization **MLEM**, due to the limited number of projections [4]
- **Poissonian likelihood** to account for the nature of scintillation-generated photons



Experimental results



Conclusions

- Despite the low number of projections, the tomographic algorithm reproduces the simulated signal with **$< |0.1|$ Gy difference**
- Major discrepancies at the distribution edges, particularly in the PDD map (slice $x = 0$ cm) at the scintillator entrance (up to 0.3 Gy over 10 pixels)
- Improvement expected with reduced sampling step, using a scientific camera with resolution better than 1 mm
- Specific tests on reconstruction, including scintillation photon emission modeling and accelerator data acquisition, are necessary.

References

- [1] F. Romano et al., 2022, Med. Phys., vol. 49
- [2] M. R. Ashraf et al., 2020, Frontiers in Physics, vol.8
- [3] E. Ciarrocchi et al., 2024, Physica Medica, vol. 121
- [4] F. Kroll et al., 2012, Medical Physics, vol. 40

