# A 3D imaging system for dosimetry in FLASH radiotherapy

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#### Motivations and challenges **Proposed detector** Why plastic scintillators? [2] To develop a detector for <u>online 3D</u> Linear response within high dynamic The detector consists in a **monolithic block <u>dosimetry</u>** in quality assurance protocols range, suitable for FLASH applications [3] of plastic scintillator EJ200 read out by and beam characterization for **FLASH-RT**, a Spatial resolution ~ 100 µm four scientific cameras, each measuring a new radiotherapy modality characterized by different projection of scintillating light. Time response in ~ ns Ultra High Dose Rate >40 Gy/s, whereas conventional radiotherapy 1 Gy/min. The acquisition of four light projections **<u>Prompt readout</u>**, if coupled to a camera enables a tomographic reconstruction of **□** → **Linearity** at high-dose-rate Good for treatment plan verification: the volumetric dose distribution released by a **3D measurement** with high resolution ĕ→ tissue equivalent 9-MeV electron beam within the scintillator $\mathcal{S} \rightarrow \text{Real-time}$ capability reusable and cost-effective **GEANT4** simulation P1 P2 P3 **P4** transversal dose distribution **longitudinal dose distribution P1** 5.0

2.5 -





2.5

**Parallel projection** of the volumetric dose distribution Dose Per Pulse = 1 Gy, Voxel =  $1 \text{ mm}^3$ 

#### **Tomographic reconstruction and comparison**

- Iterative methods, such as Maximum Likelihood Expectation Maximization MLEM, due to the limited number of projections [4]
- **Poissonian likelihood** to account for the nature of scintillation-generated photons



### **Experimental results**







Longitudinal map with no selection on photon angle emission

#### References

[1] F. Romano et al., 2022, Med. Phys., vol. 49 [2] M. R. Ashraf et al., 2020, Frontiers in Physics, vol.8 [3] E. Ciarrocchi et al.,2024, Physica Medica, vol. 121 [4] F. Kroll et al., 2012, Medical Physics, vol. 40



Specific tests on reconstruction, including scintillation photon emission modeling and

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## Conclusions

- Despite the low number of projections, the tomographic algorithm reproduces the simulated signal with < [0.1] Gy difference
- Major discrepancies at the distribution edges, particularly in the PDD map (slice x = 0) cm) at the scintillator entrance (up to 0.3 Gy over 10 pixels)
- Improvement expected with reduced sampling step, using a scientific camera with resolution better than 1 mm
- accelerator data acquisition, are necessary.