

Fast Detectors Viewed from a Different Angle: Scintillators and SiPMs for Photon-Counting CT

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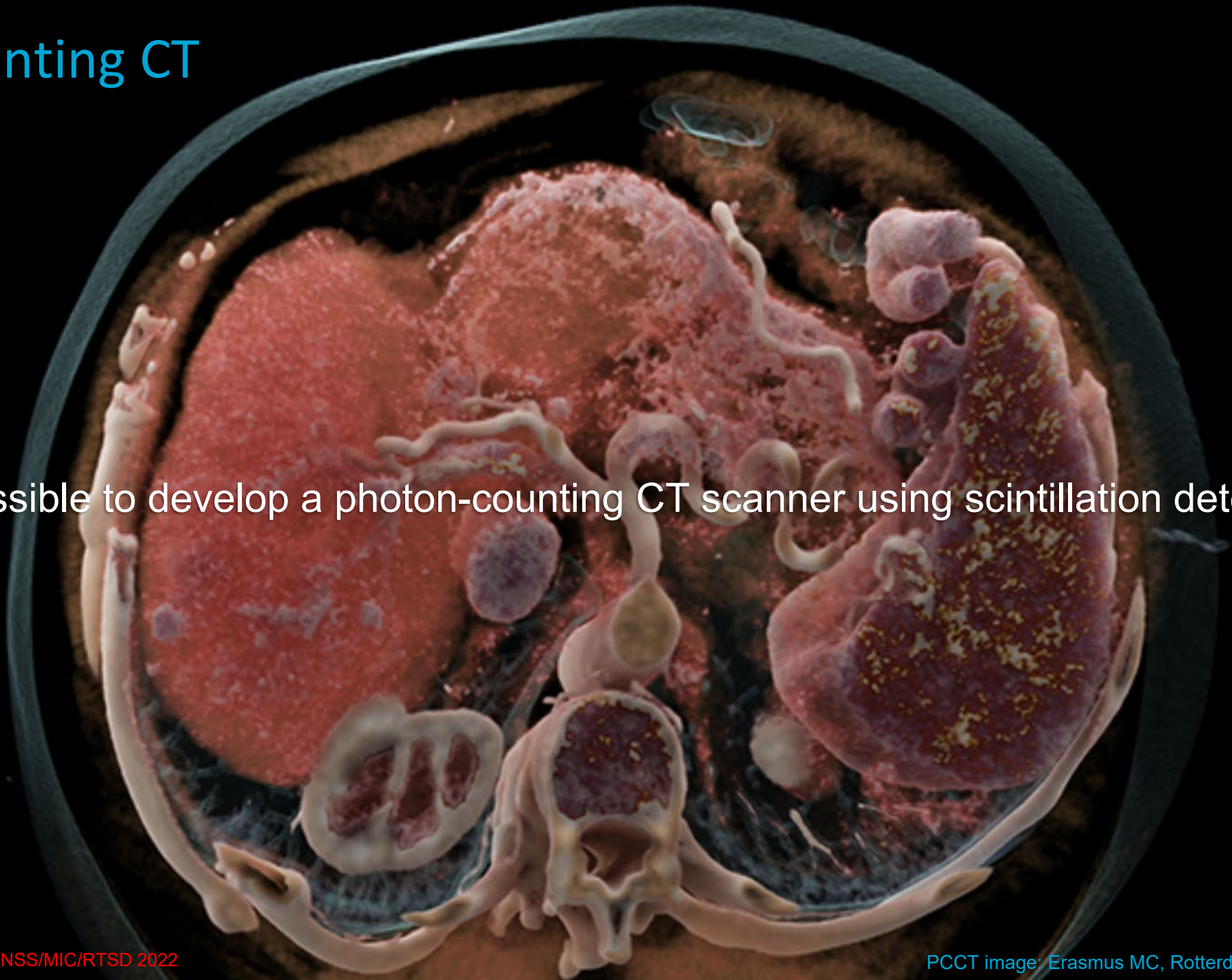
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Photon-counting CT

“It is ~~not~~ possible to develop a photon-counting CT scanner using scintillation detectors”



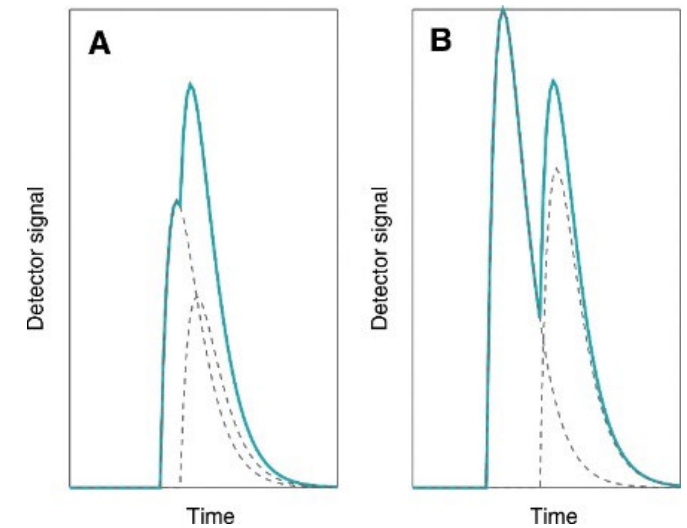
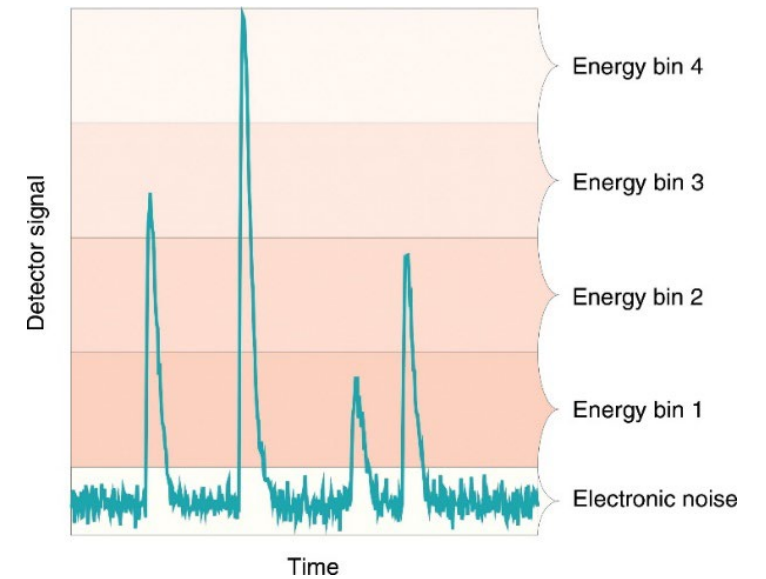
X-ray photon counting

Photon-counting instead of energy-integrating detectors:

- Count individual photons & assign them to energy bins
- Current PCCT systems are based on room temperature semiconductor detectors (RTSD), such as CdTe, CZT or Si

Challenges:

- X-ray absorption efficiency (energies ≤ 150 keV)
- Pulse pile-up (fluence rate > 100 Mcps/mm² in clinical PCCT scanners)
- Cost-effective production; stable and reliable detector performance



Photon-counting detectors: state of the art

Requirements (medical: [25, 150] keV)

Count rates > 100 Mcps/mm²

Sufficient energy resolution

X-ray detection efficiency

Room temperature

- Stable and reliable operation:
 - High purity materials
 - Low defect concentration
 - Optimized anode contacts

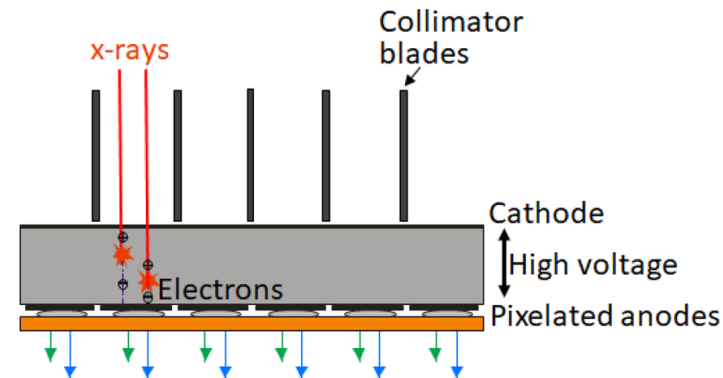
RTSDs (CdTe/CZT)

Short pulses (10s of ns) & small pixels (≤ 500 μ m)

~ 8 -20% @ 60 keV

$\rho = 5.8$ g cm⁻³ & $Z_{\text{eff}} \approx 50$ (1.5 – 3.0 mm)

Yes

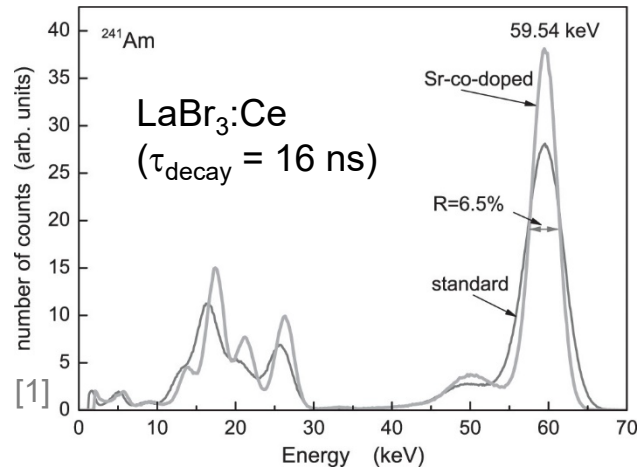


Why scintillation detectors are a rational choice for PCCT

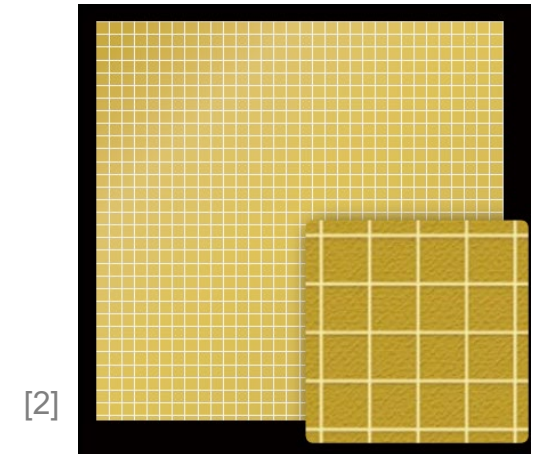
- Inorganic scintillators
 - Widely used in X-ray and nuclear imaging systems
 - High mass density and atomic number
 - Fast response & high energy resolution available
 - Sub-mm pixels are possible
- Silicon photomultiplier (SiPM)
 - SiPMs are state-of-the-art in PET
 - High internal gain ($> 10^5$)
 - Fast response ($\tau_{\text{recharge}} < 10$ ns is possible)
 - SiPMs can be miniaturized to sub-mm level



Images: Philips.com



$\text{LaBr}_3:\text{Ce}$ energy spectrum @ 60 keV

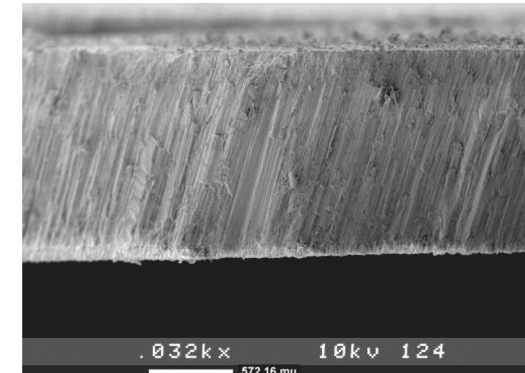
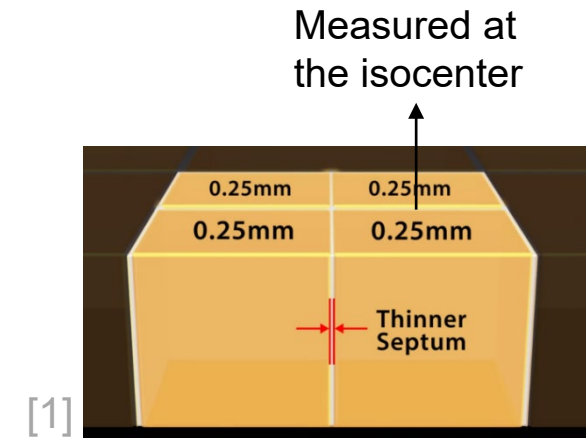


0.25 mm scintillator array

Finely pixelated scintillation detectors

Example of a commercial system with a finely pixelated detector:

- Canon's Aquilion Precision (energy-integrating) CT scanner
- 50% finer scintillator pixel, reflective septa, and collimator blades
- Dose-efficiency of conventional systems therefore maintained
- More examples of finely pixelated detectors in research projects:
 - $430 \times 430 \mu\text{m}^2$ pixels with a $50 \mu\text{m}$ thick reflector [2]
 - $220 \times 220 \mu\text{m}^2$ pixels with a $63 \mu\text{m}$ thick reflector [3]
 - $312.5 \times 312.5 \mu\text{m}^2$ pixels with a $38 \mu\text{m}$ thick reflector [4]
 - $250 \times 250 \mu\text{m}^2$ pixels with a $50 \mu\text{m}$ thick reflector [5]
 - Laser-induced optical barriers [6]
 - Columnar microstructure [7]



[1] Canon, "Aquilion Precision CT", https://global.medical.canon/products/computed-tomography/aq_precision. (24 Jan 2022)

[2] Godinez, F. et al., "Development of an ultra ..., IEEE TRPMS 2:7-16 (2017). doi: [10.1109/TRPMS.2017.2765486](https://doi.org/10.1109/TRPMS.2017.2765486)

[3] Cherry, S.R. et al., "High resolution PET with 250 ..., (2012), <https://www.osti.gov/servlets/purl/1032741> (8 June 2022)

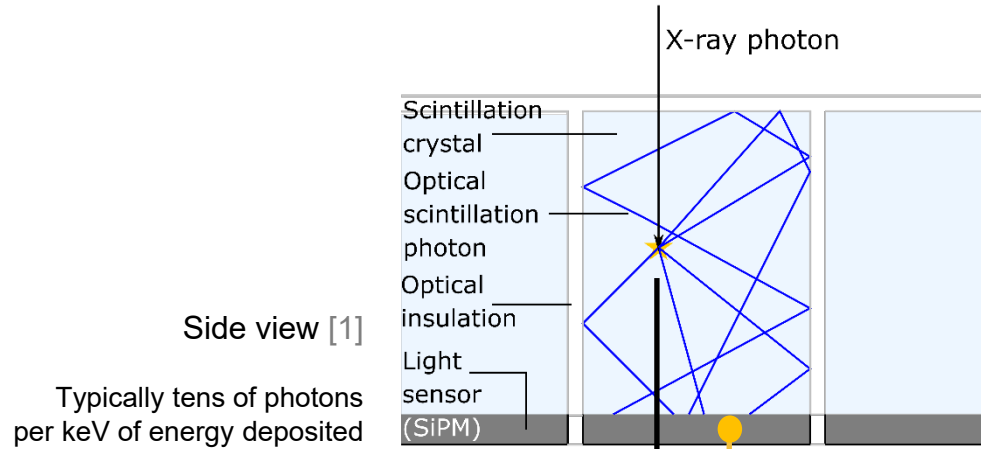
[4] Imai, Y. et al., "Development and performance ..., Medical Physics 36:1120-1127 (2009). doi: [10.1118/1.3086117](https://doi.org/10.1118/1.3086117)

[5] Shimadzo, K. et al., "Performance of custom fine-pitch SiPM-scintillator based photon counting detectors," IEEE NSS-MIC 2024

[6] Bläckberg, L. et al "Exploring light ...", Phys Med Biol 64: 095020 (2019). doi: [10.1088/1361-6560/ab1213](https://doi.org/10.1088/1361-6560/ab1213)

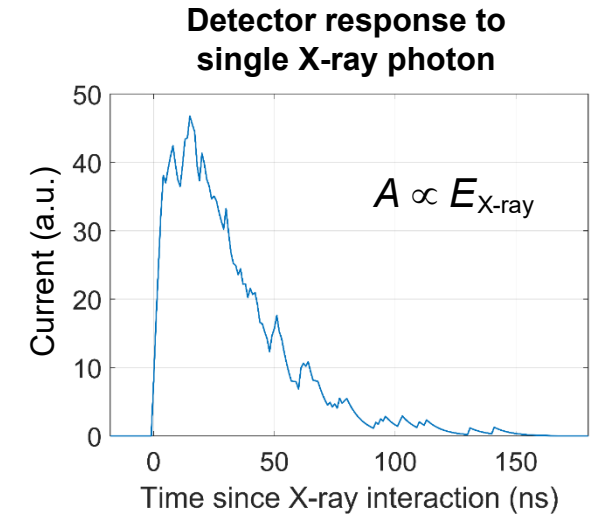
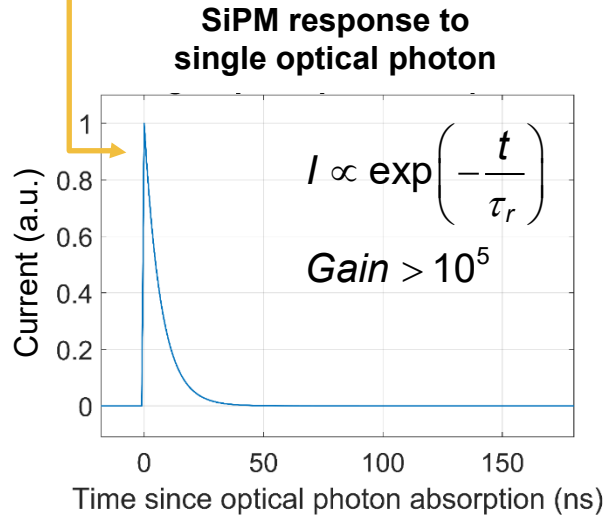
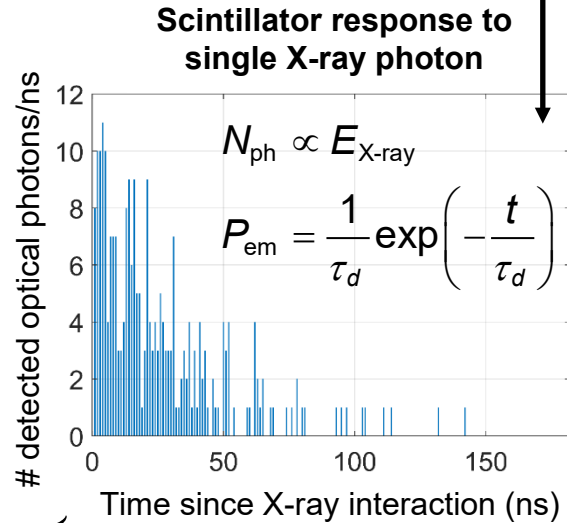
[7] Bhandari, H.B. et al, "Large-Area Crystalline ...", IEEE TNS 60(1), 3-8 (2013). doi: [10.1109/TNS.2012.2213612](https://doi.org/10.1109/TNS.2012.2213612)

SiPM-based scintillation detector array (analog case)

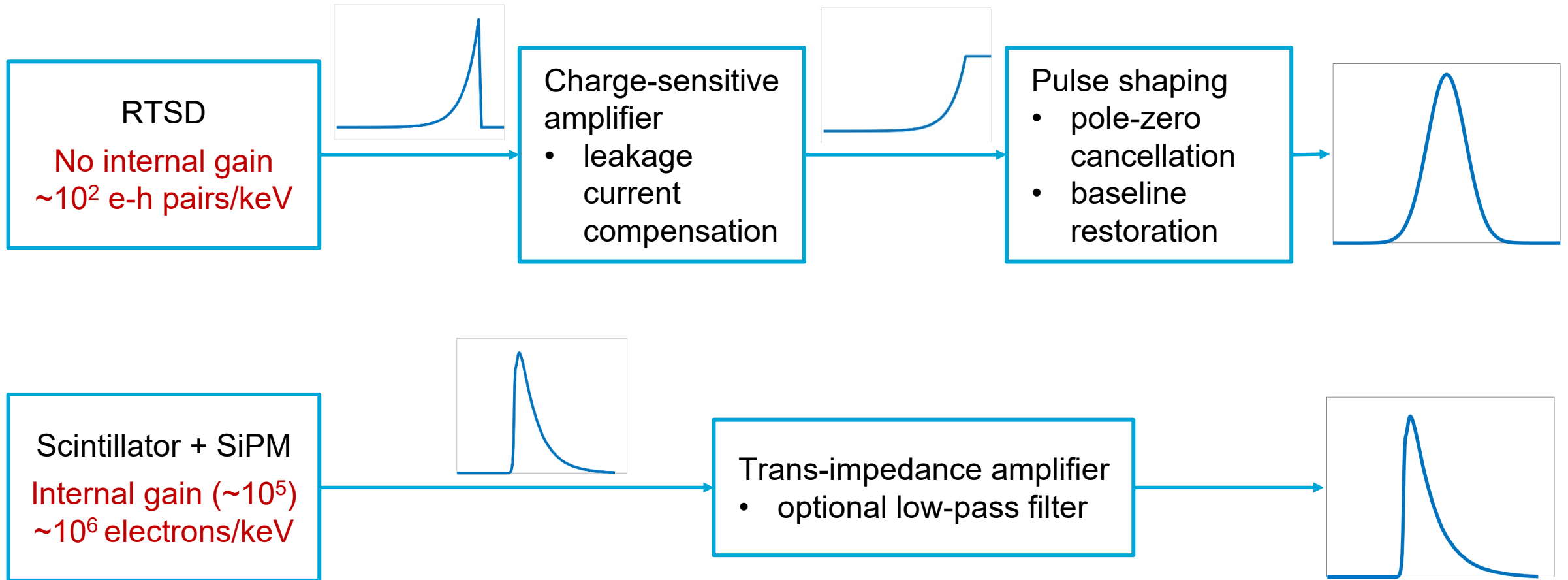


Pulse width mainly determined by two parameters:

- Scintillator decay time τ_d (e.g. 16 ns for LaBr₃:Ce)
- SiPM recharge time τ_r (< 10 ns is possible)

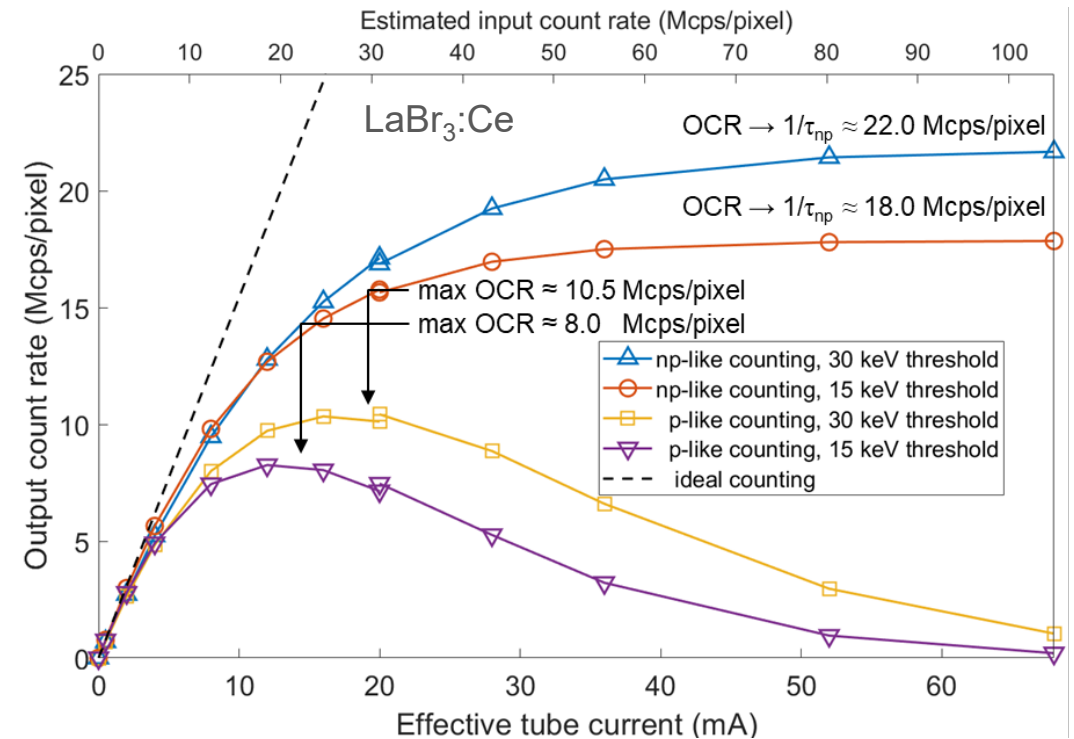
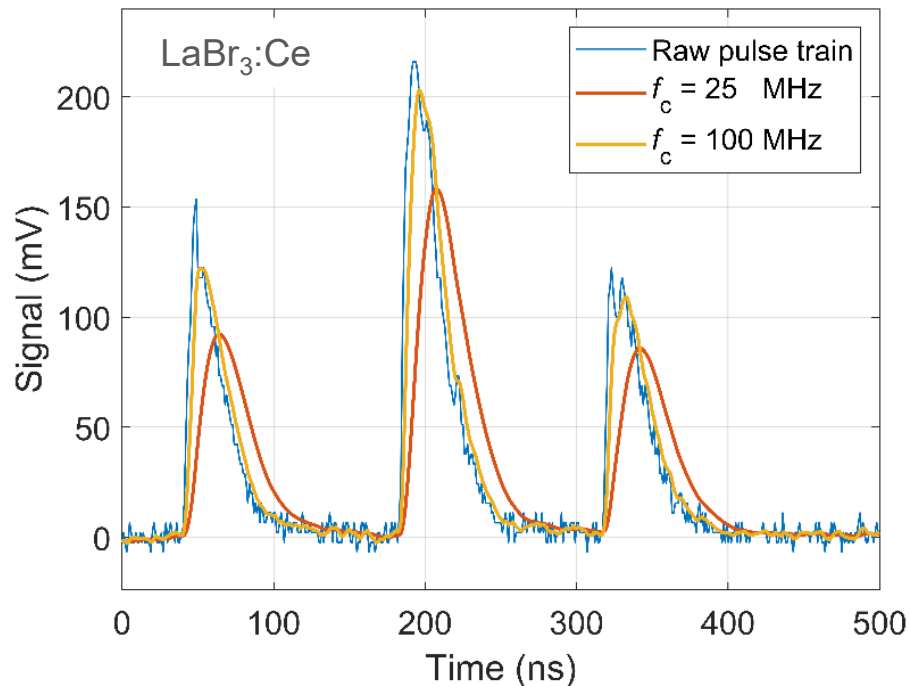
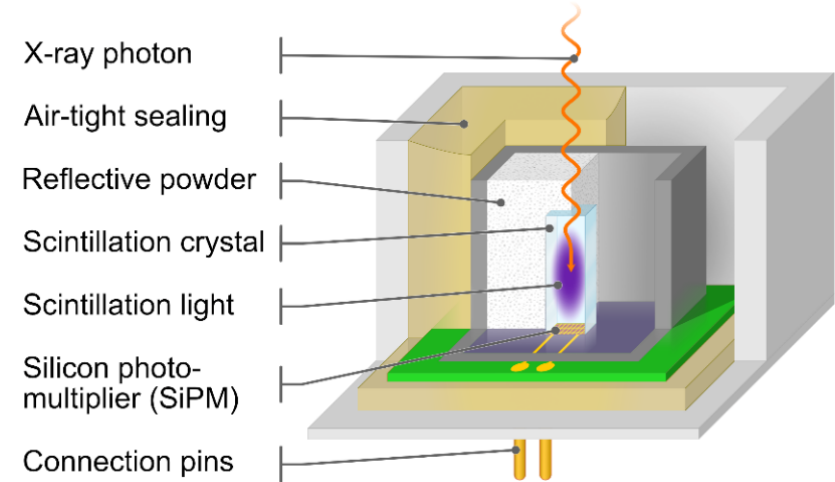


RTSD vs SiPM-based detection chains



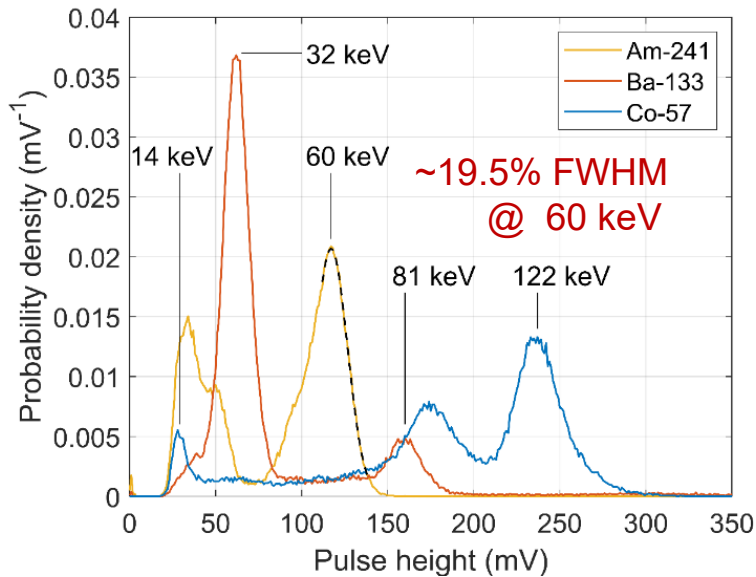
Single-pixel experiments

- $0.9 \times 0.9 \times 3.5 \text{ mm}^3 \text{ LaBr}_3\text{:Ce}$ ($\rho = 5.1 \text{ g/cm}^3$, $\tau_{\text{decay}} = 16 \text{ ns}$)
- Ultrafast SiPM prototypes: $15 \text{ }\mu\text{m}$ SPADS, PDE 20-30%, $\tau_{\text{recharge}} = 7 \text{ ns}$
- Trans-impedance amplifier \rightarrow digital scope
- 2nd order low-pass filter with various cut-off frequencies
- X-ray tube (120 kVp, tungsten target, 3.0 mm Be, 7.5 mm Al)
- **$\sim 20 \text{ Mcps/pixel} \times \sim 10 \text{ pixels/mm}^2 = \sim 200 \text{ Mcps/mm}^2$**

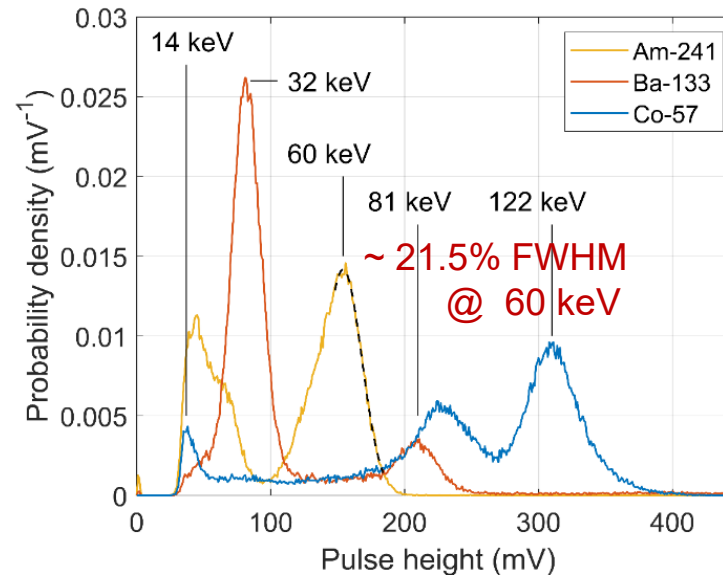


LaBr₃:Ce spectral performance

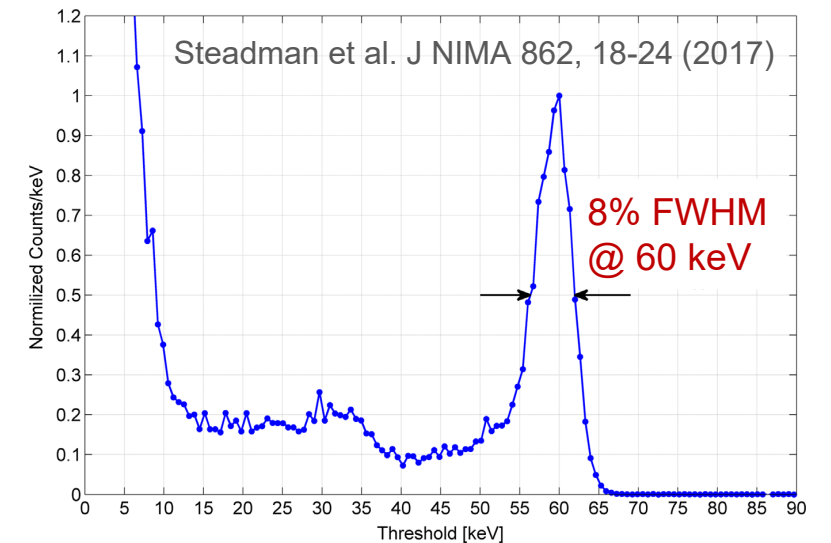
LaBr₃:Ce, $f_c = 25$ MHz



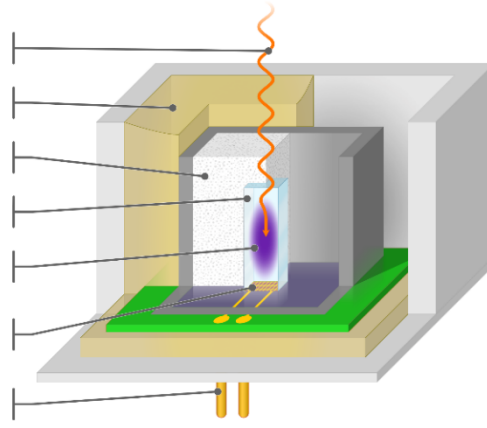
LaBr₃:Ce, $f_c = 100$ MHz



0.5 x 0.5 x 2.0 mm³ CZT pixel



- X-ray photon
- Air-tight sealing
- Reflective powder
- Scintillation crystal
- Scintillation light
- Silicon photo-multiplier (SiPM)
- Connection pins



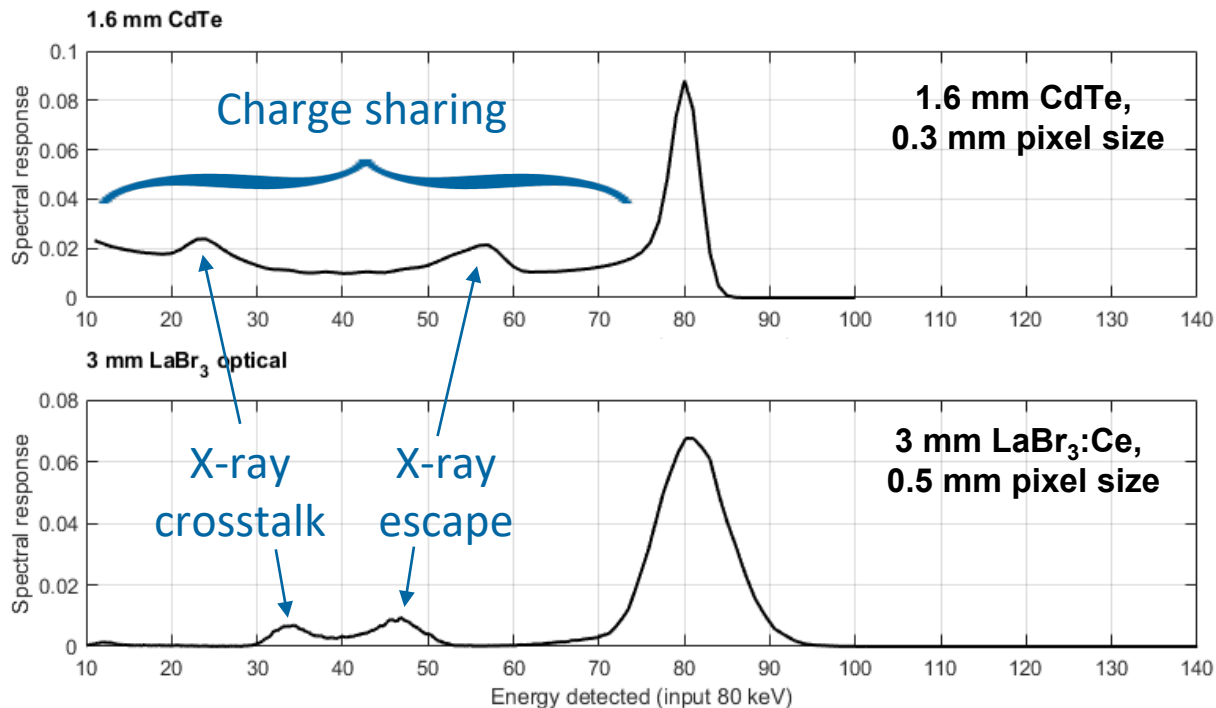
Upgrade of SiPM: PDE x 2 \Rightarrow Energy resolution x 1/ $\sqrt{2}$

Literature (Alekhin et al Appl. Phys. Lett. 102, 161915, 2013):

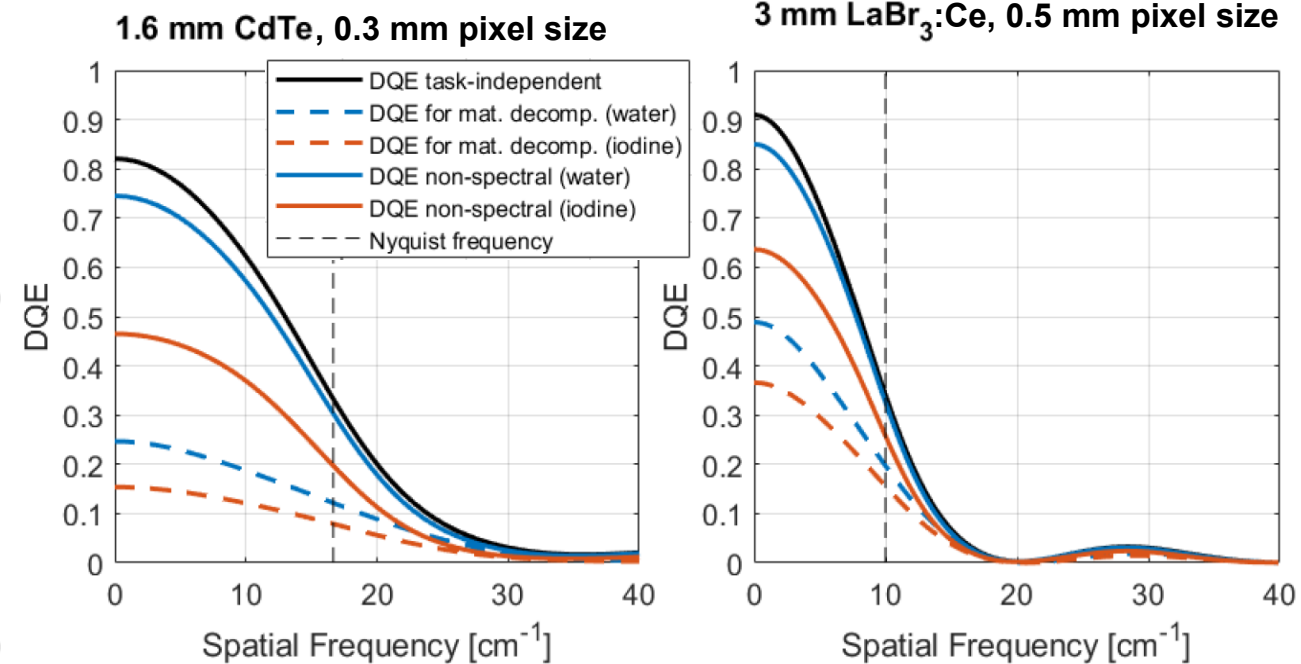
- 9.4% FWHM @ 60 keV for LaBr₃:Ce ($\tau_{\text{decay}} = 16$ ns)
- 6.5% FWHM @ 60 keV for LaBr₃:Ce,Sr ($\tau_{\text{decay}} = 18$ ns)

A closer look at spectral performance: influence of crosstalk

Simulated pulse height spectra of 1.6 mm CdTe (top) and LaBr₃:Ce (bottom) upon irradiation with 80 keV X-rays [1]

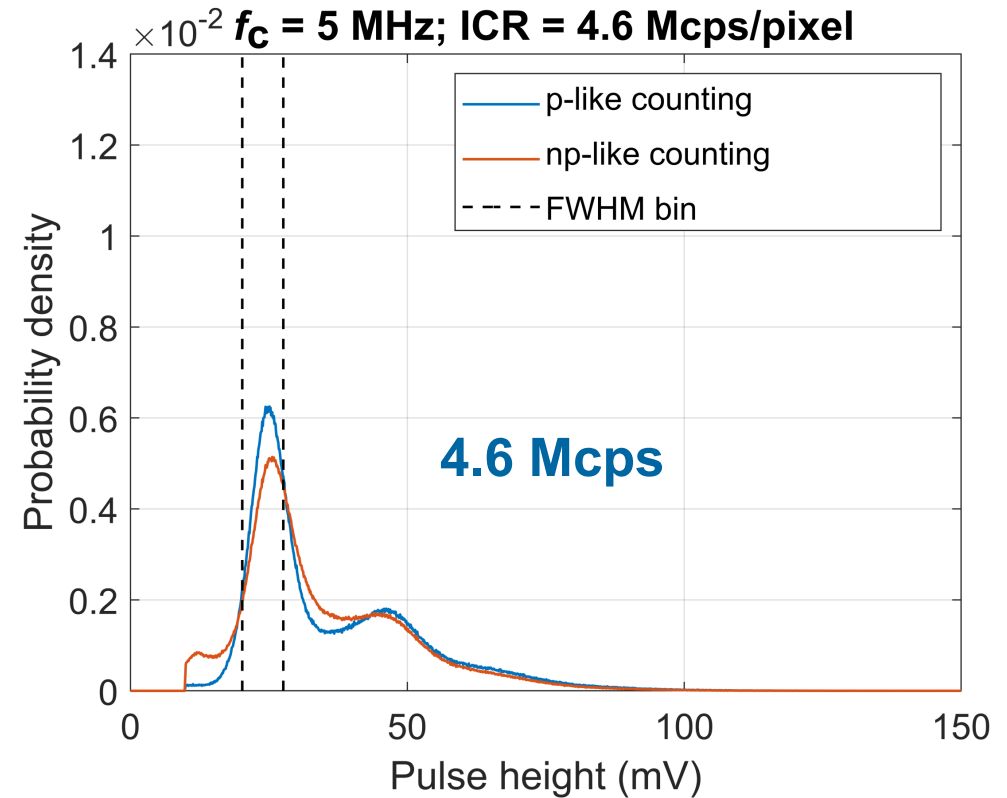
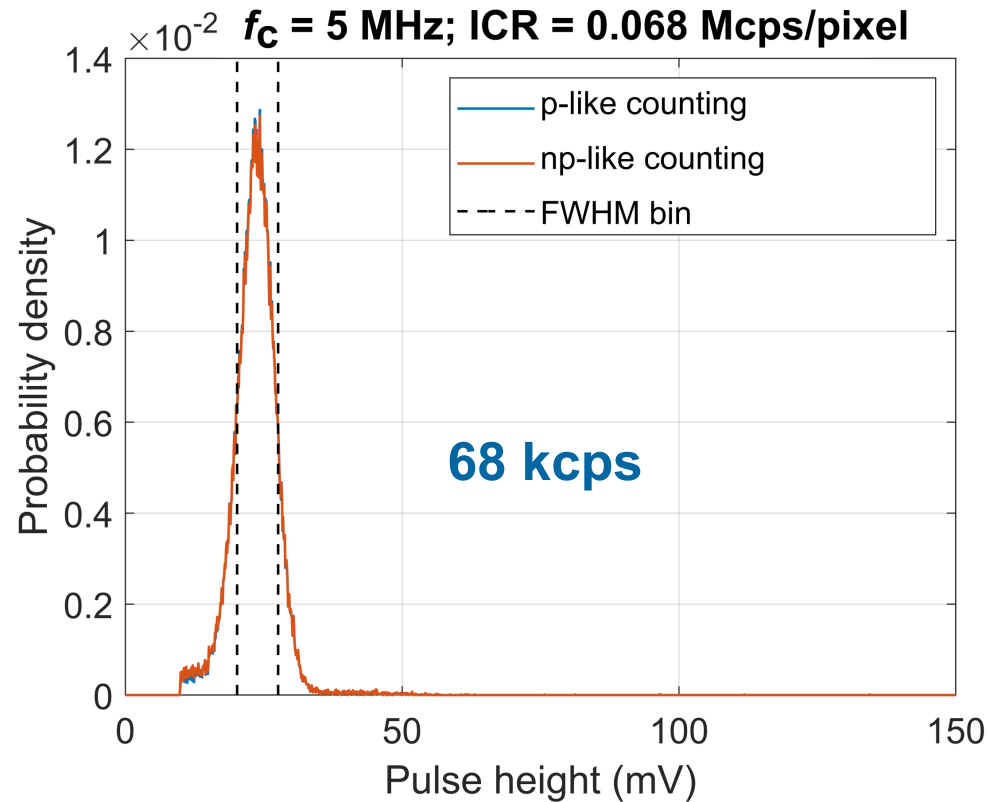


Spectral DQE of 1.6 mm CdTe (left) and LaBr₃:Ce (right) [2]

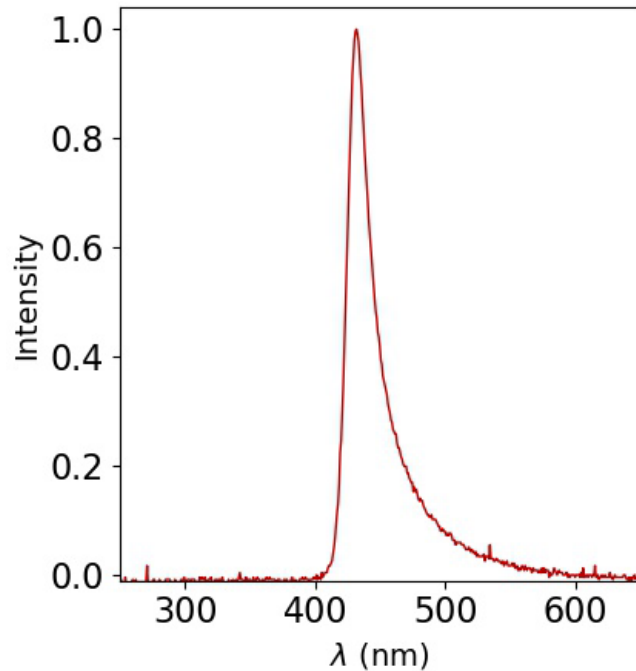


A closer look at spectral performance: influence of pile-up

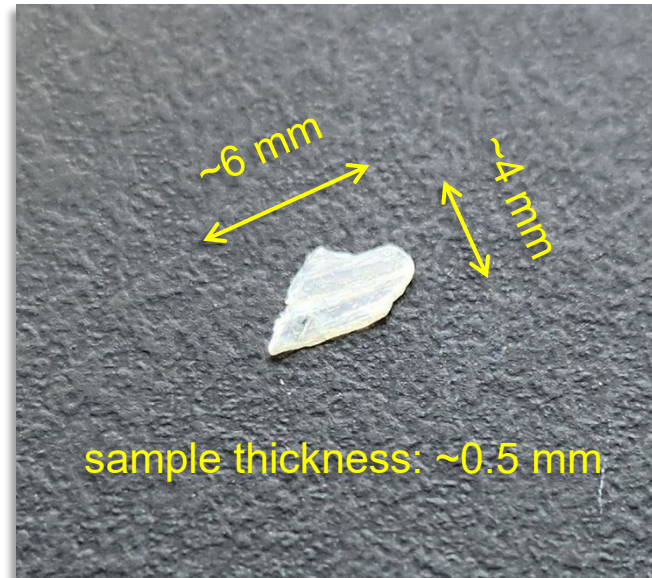
Measured spectra of a LYSO:Ce detector upon irradiation with 60 keV X-rays at different incident count rates (ICR)



Benzylammonium lead bromide - $(\text{BZA})_2\text{PbBr}_4$



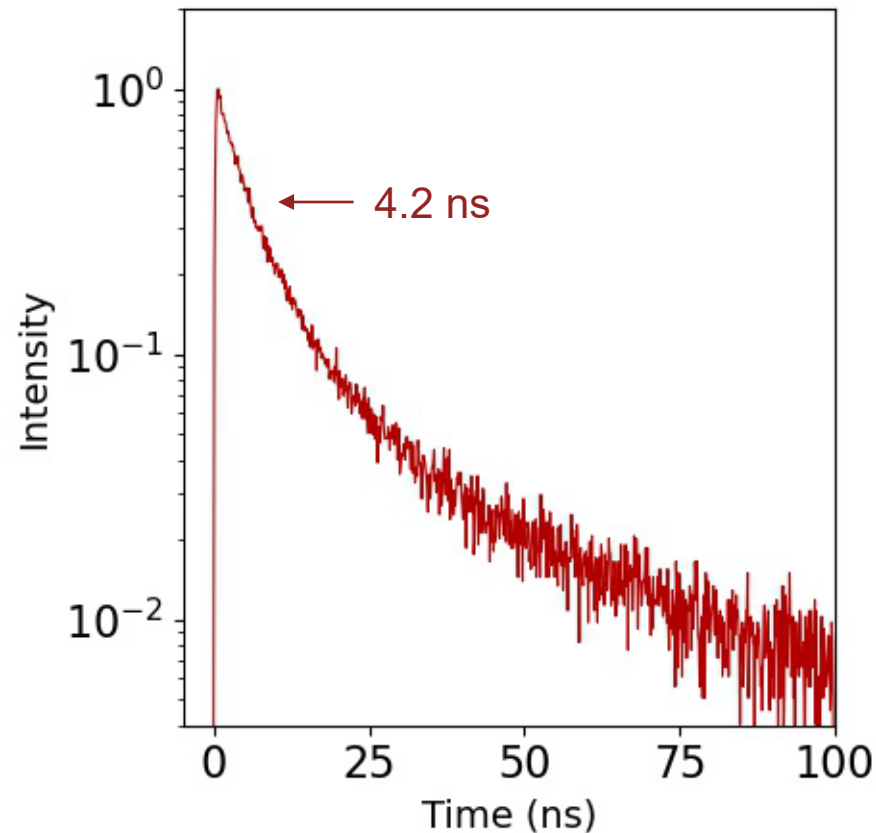
$(\text{BZA})_2\text{PbBr}_4$ X-ray excited emission spectrum at 300K.



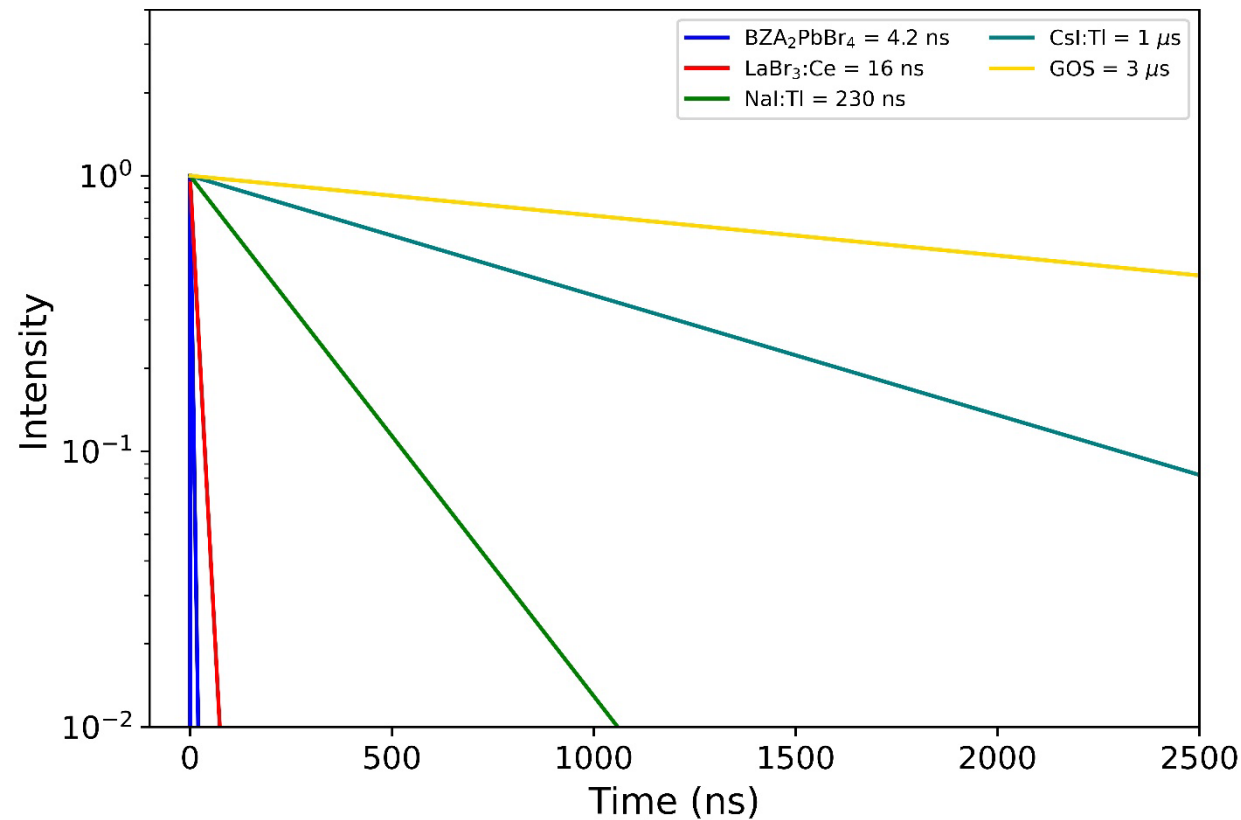
Photograph of the investigated sample.

Material:	2D hybrid organic-inorganic perovskite (HOIP)
Formula:	$(\text{C}_7\text{H}_{10}\text{N})_2\text{PbBr}_4$
Emission:	432 nm
Density:	2.23 g/cm^3
Hygroscopic:	No
Production:	Solution growth

$(\text{BZA})_2\text{PbBr}_4$ X-ray excited decay



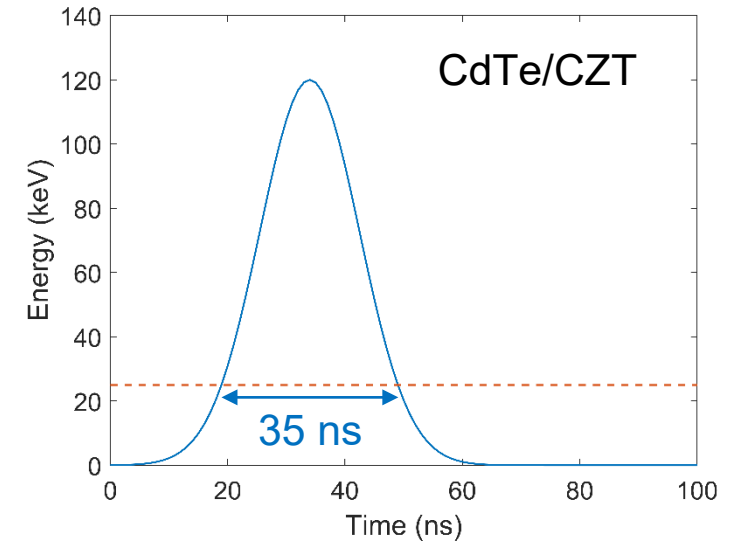
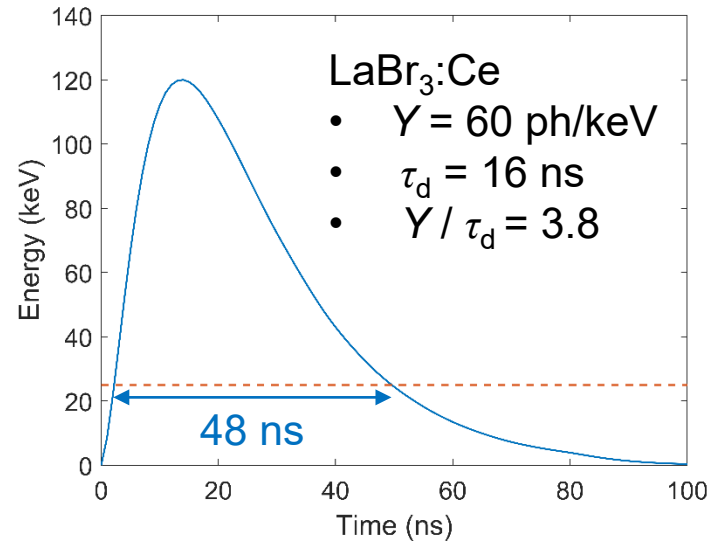
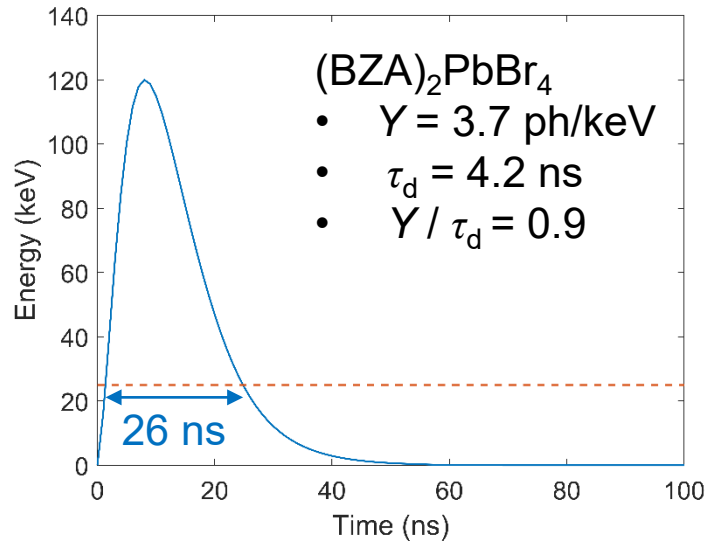
Pulsed X-ray excited decay spectrum of $(\text{BZA})_2\text{PbBr}_4$ at 300 K



Decay spectrum of $(\text{BZA})_2\text{PbBr}_4$ compared to other frequently used scintillators

Expected count rate performance

Comparison of simulated pulses ($E_{\text{x-ray}} = 120 \text{ keV}$, $f_c = 100 \text{ MHz}$, $E_{\text{thr}} = 25 \text{ keV}$)



	(BZA)₂PbBr₄	LaBr₃:Ce	CdTe / CZT
Max count rate with np-like counting	38.5 Mcps/pixel ($\tau_{\text{np}} = 26 \text{ ns}$)	20.8 Mcps/pixel ($\tau_{\text{np}} = 48 \text{ ns}$)	28.6 Mcps/pixel ($\tau_{\text{np}} = 35 \text{ ns}$) [1]

Conclusions

- Count rate of scintillator-based X-ray photon-counting detectors can be similar to that of CdTe/CZT detectors; potentially even better with new ultrafast scintillation materials
- The spectral fidelity of scintillator-based X-ray photon-counting detectors may be better than that of CdTe/CZT detectors due to the absence of charge sharing
- Scintillator-based X-ray photon-counting detectors may have a bright future!

Thank you!