

# MONTE CARLO APPLICATIONS @ MEDAUSTRON

The use of Monte Carlo Computation Tools in the Hadron Therapy Facility MedAustron

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*Photos / Graphics: MedAustron, Thomas Kästenbauer, Freepik/MedAustron, Kästenbauer/Ettl*

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- Introduction and status of MedAustron
- FLUKA in Radiation Protection Services
- FLUKA in Accelerator and Beam Physics
- GEANT4 in Medical Physics (Beam Delivery and Monte Carlo)

# FACILITY OVERVIEW

## Clinical Irradiation Rooms

Three rooms for patient treatments

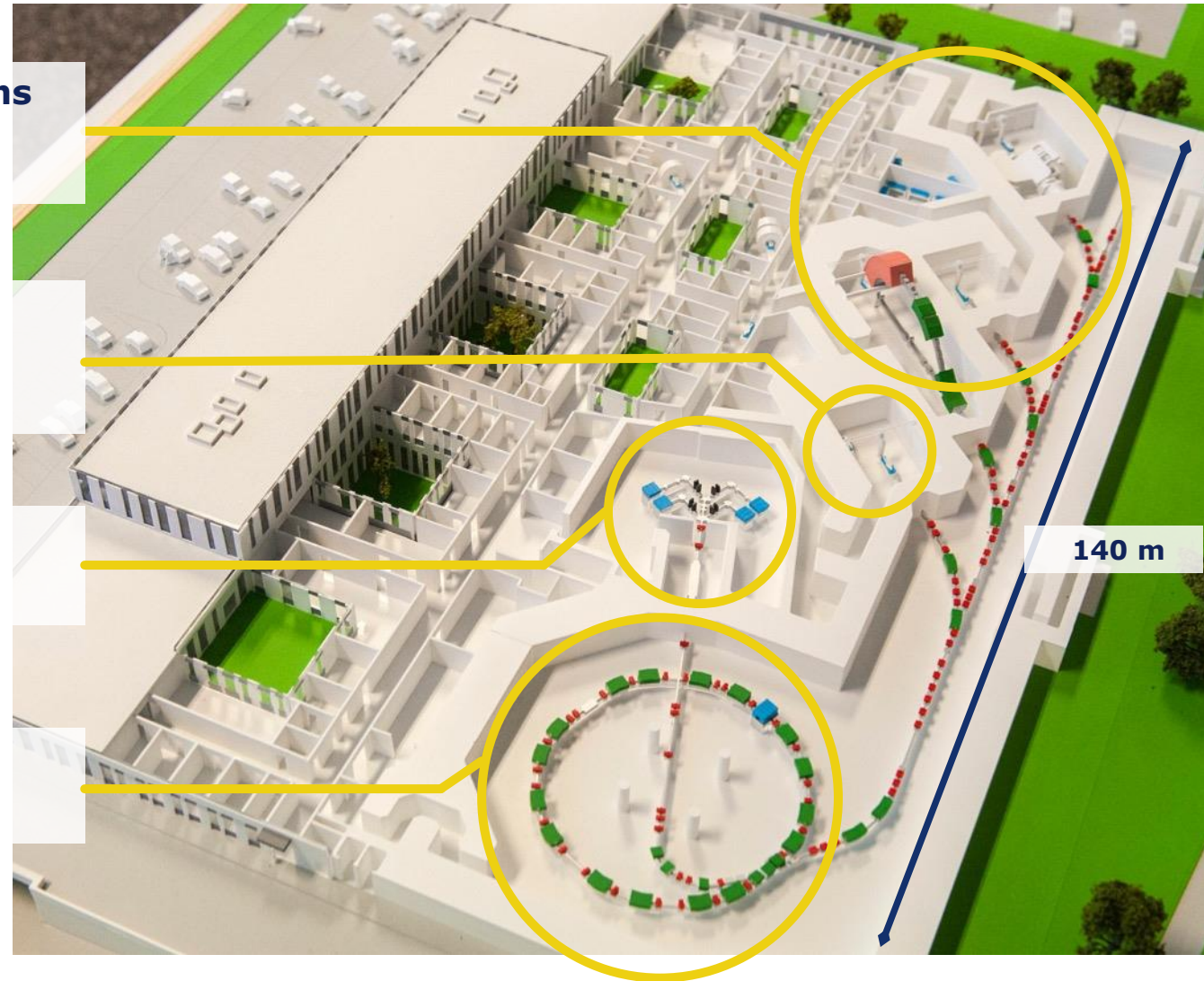
## Research

Irradiation room for non-clinical use

## Ion Sources

and linear accelerator

## Synchrotron

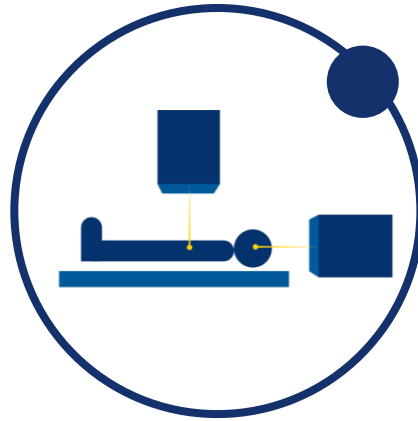


# INTERNATIONALITY



## TEAM

~300 employees from  
20 different countries



## CLINIC

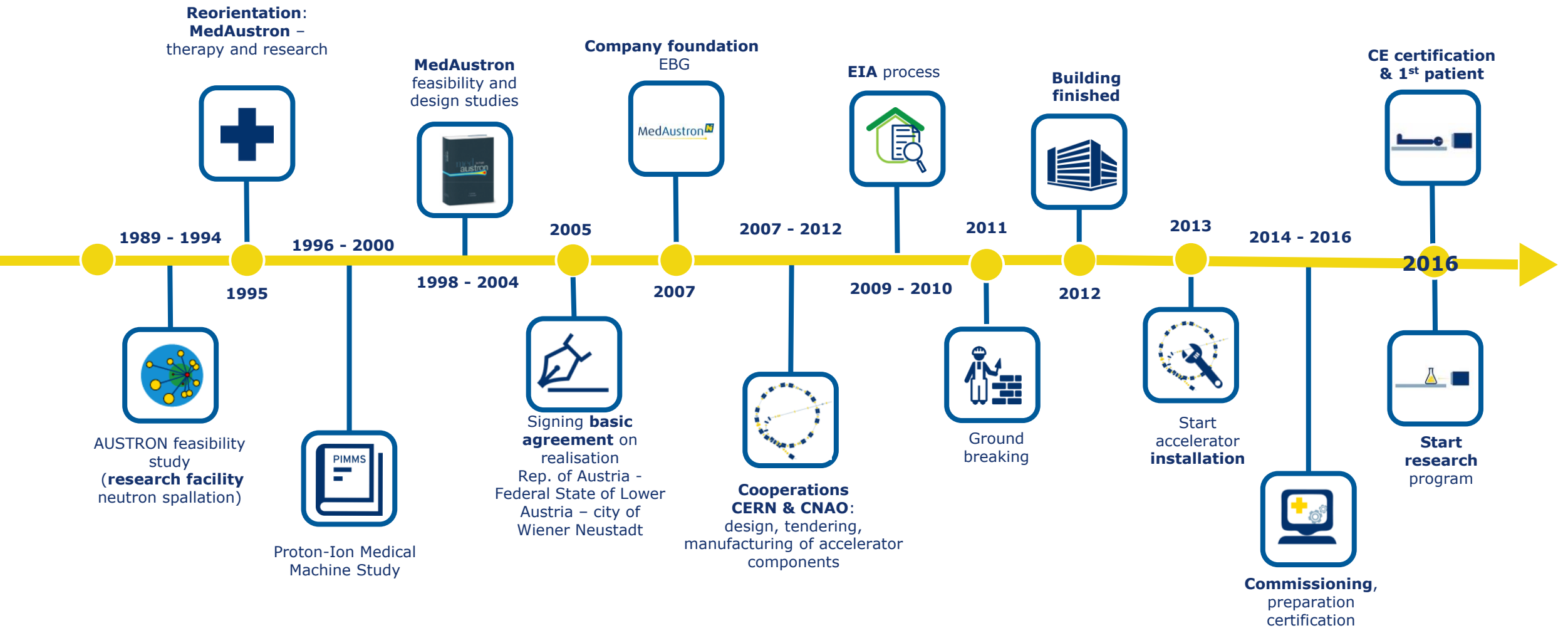
Patients from all over  
Austria and abroad



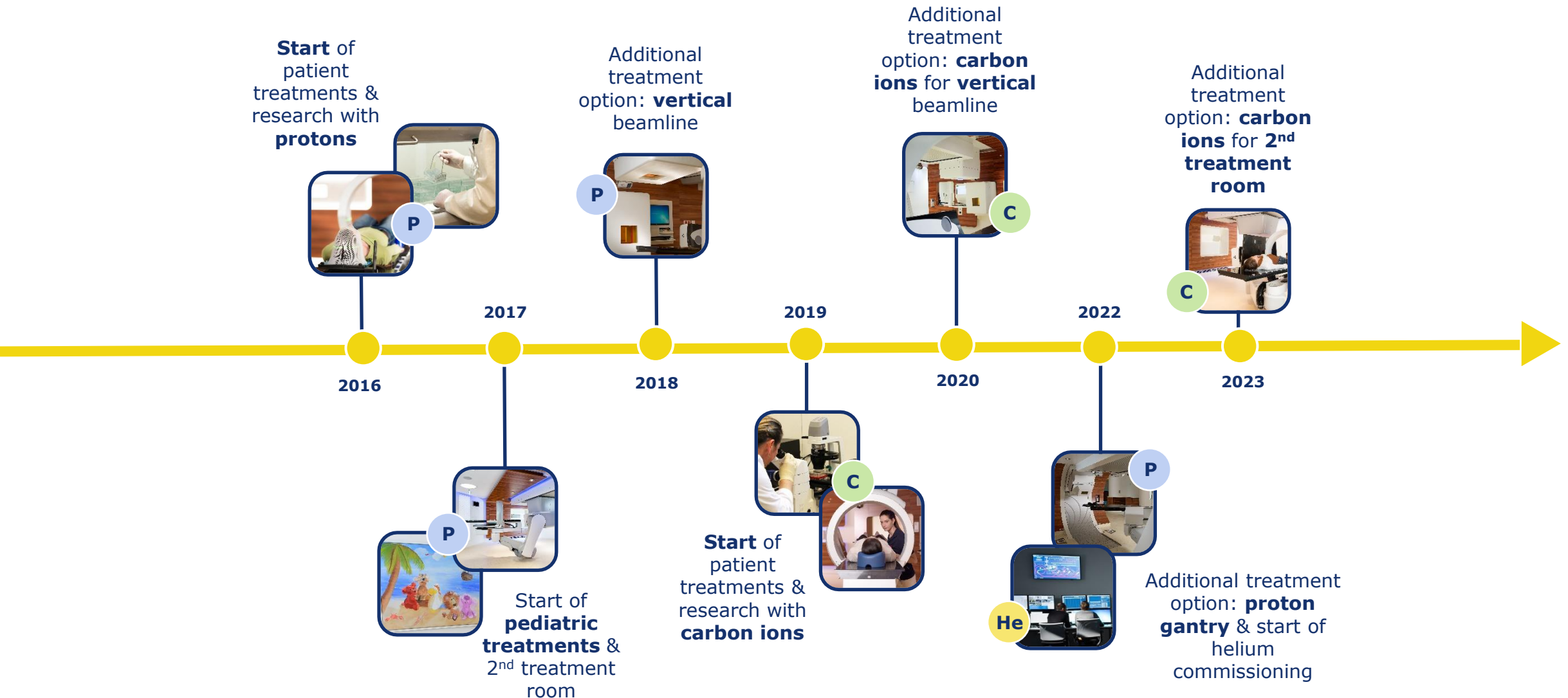
## COOPERATIONS

With institutes,  
companies,  
professional societies  
worldwide

# COMPANY HISTORY TO FIRST PATIENT

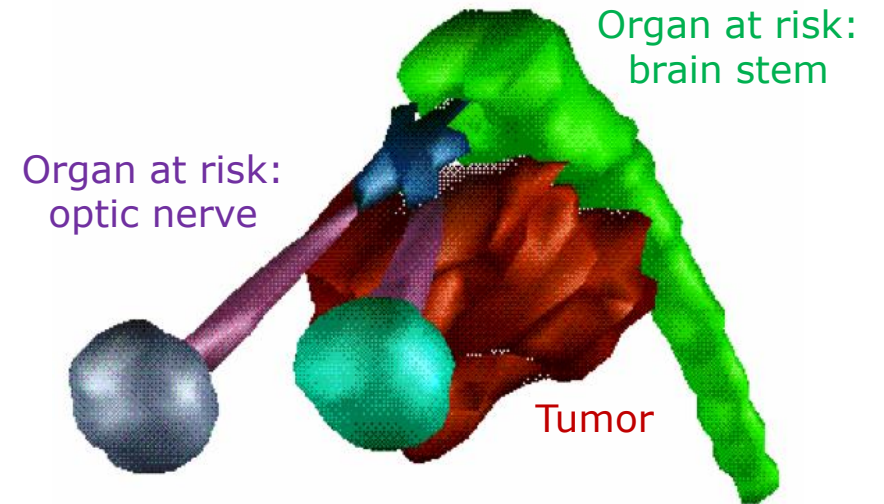


# MILESTONES SINCE FIRST PATIENT

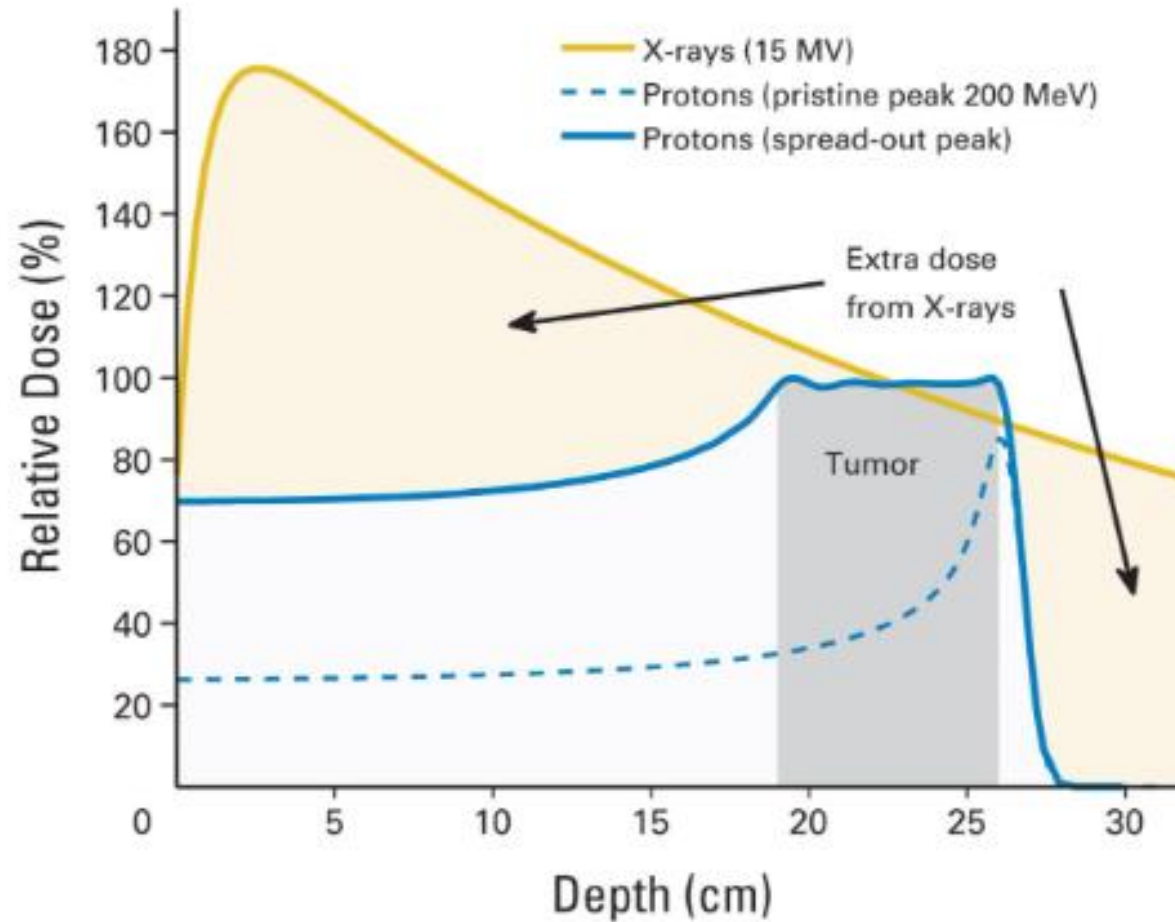


# RADIOTHERAPY IN GENERAL

- The aim is to **prevent further proliferation** of the tumor cells
- This requires a **high radiation dose** in the tumor cells
- **Organs at risk** tolerate only a low radiation dose



# THE PRINCIPLE OF PARTICLE THERAPY

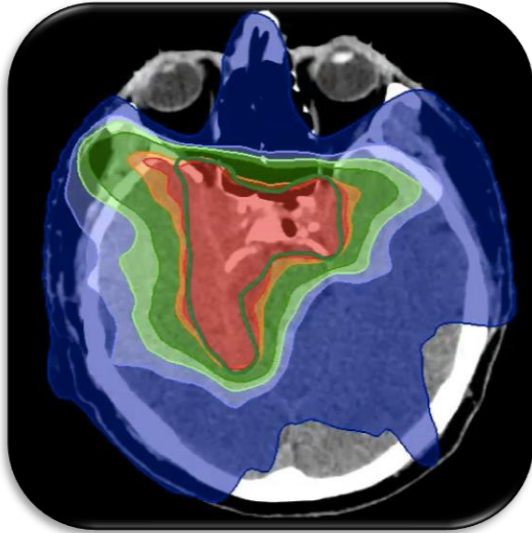




# TREATMENT PLANNING - COMPARISON

## PHOTONS

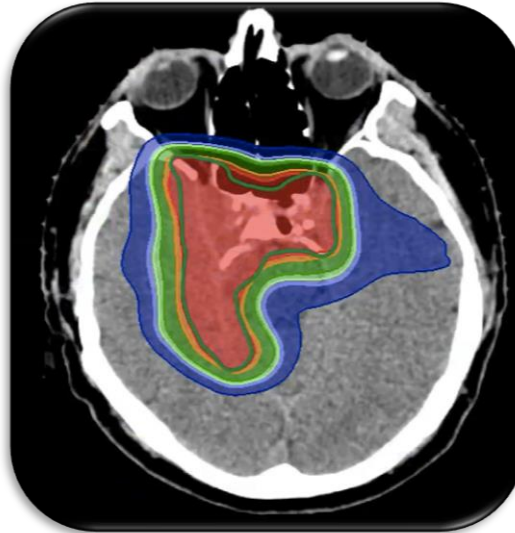
IMRT, VMAT, SBRT



Several fields, entry and exit dose

## PROTONS

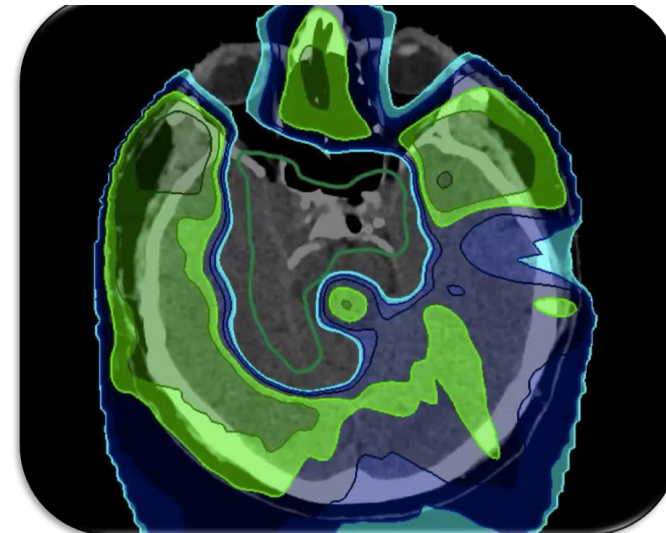
IMPT



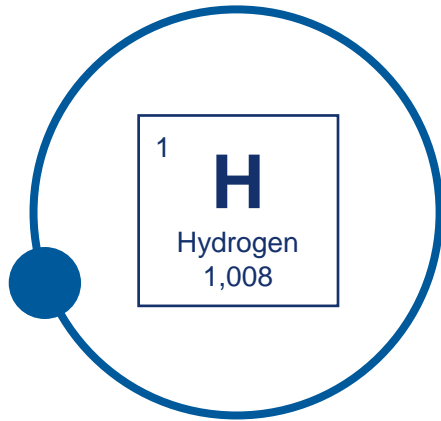
Fewer fields, reduced entry dose, no exit dose

## DOSE DIFFERENTIAL

Photons minus Protons



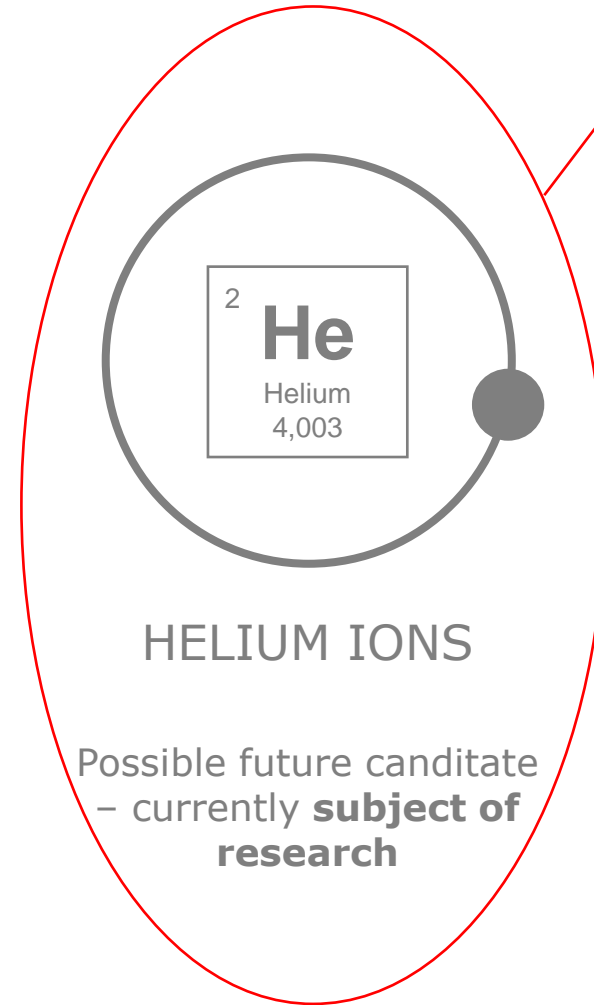
# PARTICLE TYPES AT MEDAUSTRON



PROTONS



CARBON IONS



HELIUM IONS

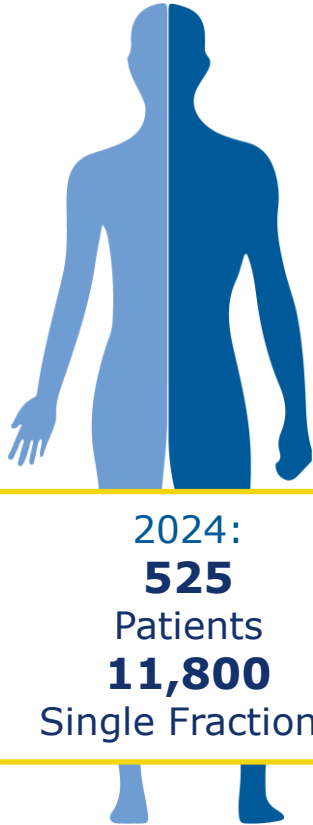
Possible future candidate  
– currently **subject of research**

Update in the upcoming presentation by C. Lenauer

**Sparing** of organs at risk and healthy tissue

Higher dose in the tumor / application in **radioresistant tumors**

# INDICATIONS TREATED AT MEDAUSTRON



2024:  
**525**  
Patients  
**11,800**  
Single Fractions

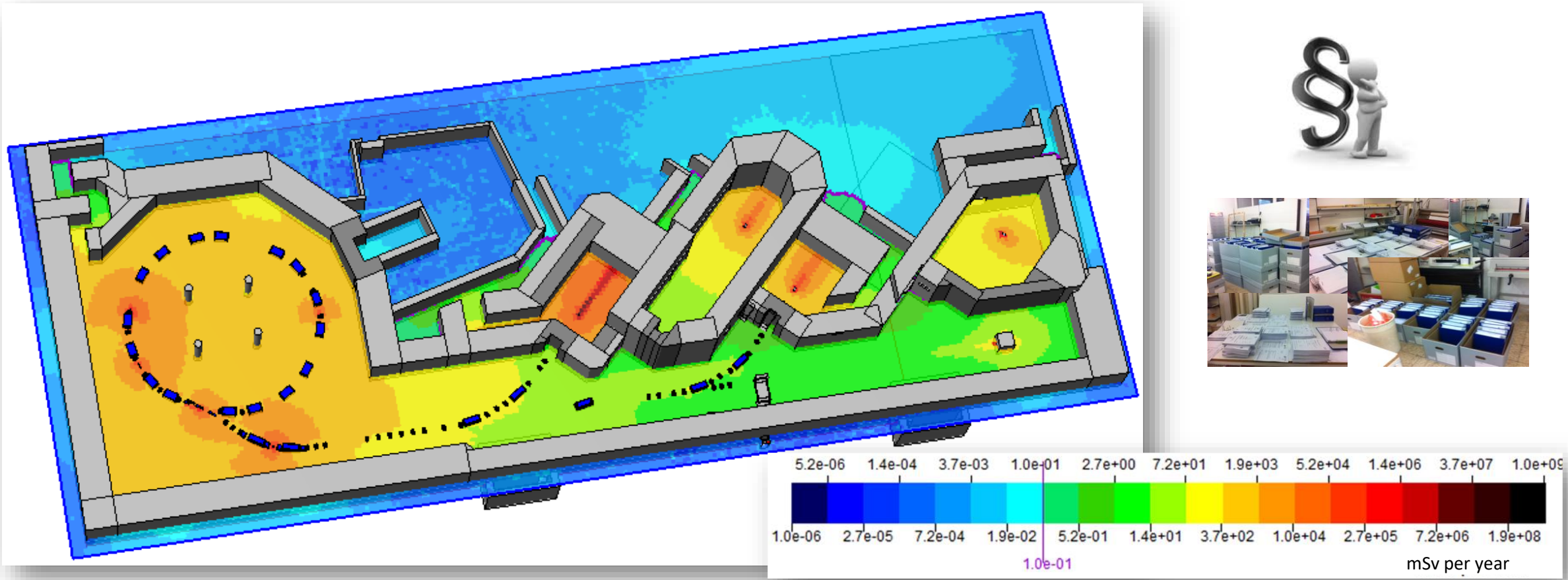
<b>CNS</b>	<b>25%</b>
<b>Head &amp; Neck</b>	<b>20%</b>
<b>Re-Irradiation</b>	<b>16%</b>
<b>Pediatrics</b>	<b>16%</b>
<b>Sarcoma</b>	<b>12%</b>
<b>Skull Base</b>	<b>5%</b>
<b>Prostate</b>	<b>3%</b>
<b>Gastrointestinal (upper)</b>	<b>2%</b>
<b>Thorax</b>	<b>1%</b>
<b>Gastrointestinal (lower)</b>	<b>&lt;1%</b>
<b>Urogenital Tumors</b>	<b>&lt;1%</b>
<b>Breast/Mamma-Ca</b>	<b>&lt;1%</b>
<b>Gynecological Tumors</b>	<b>&lt;1%</b>

Values (rounded) as of April 2024

# Radiation Protection Project

## INITIAL AUTHORITY APPROVAL FOR THE FACILITY

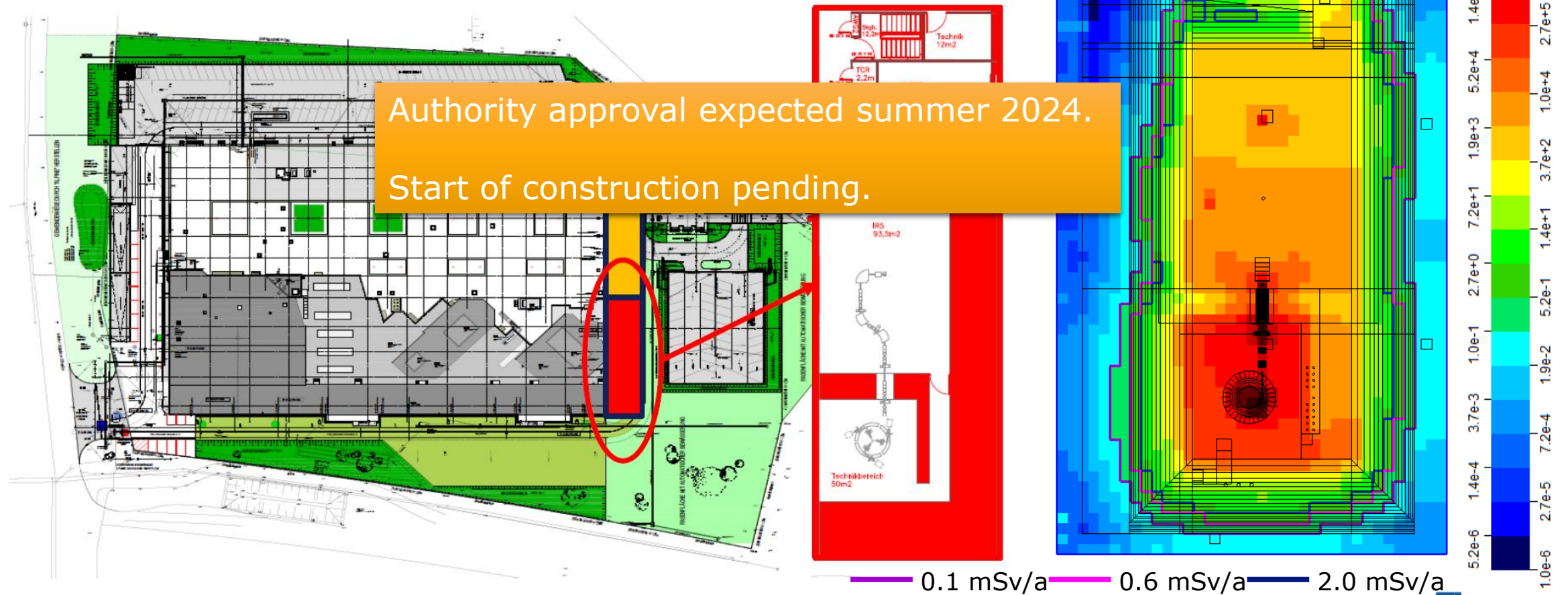
*SHIELDING CONCEPT IS PART OF AN ENVIRONMENTAL IMPACT ASSESSMENT*



# Radiation Protection Project

## AUTHORITY APPROVAL FOR AN ADDITIONAL IRRADIATION ROOM

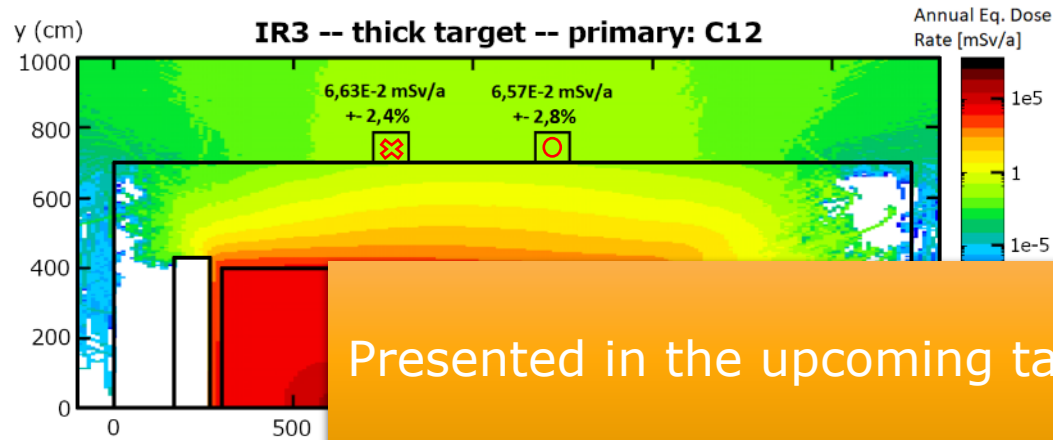
A COMMERCIAL SYNCHRO CYCLOTRON FOR PROTON THERAPY



# Radiation Protection Project

## EXTENSION OF APPROVED ION SPECIES

*EFFECTS ON THE SHIELDING*



Nr of primary particles of ion species A

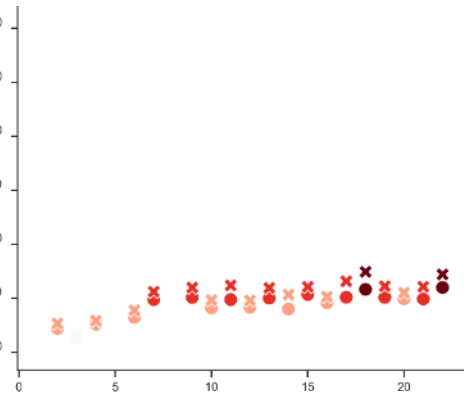
$$D_{ges} = \sum_{A=1}^{A_{max}} N_A \cdot D_A$$

...les of ion species A

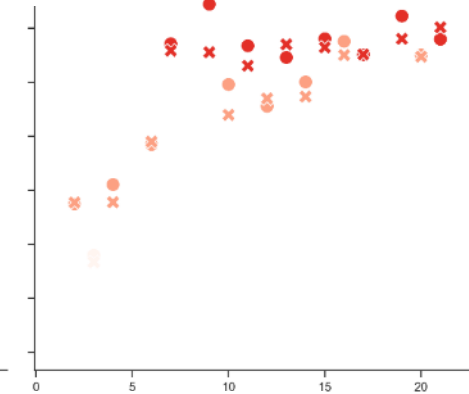
Presented in the upcoming talk by C. Lenauer

Room with heavy concrete

Doseequ./prim.  
(zSv/p)



Room with normal concrete



Excess neutrons

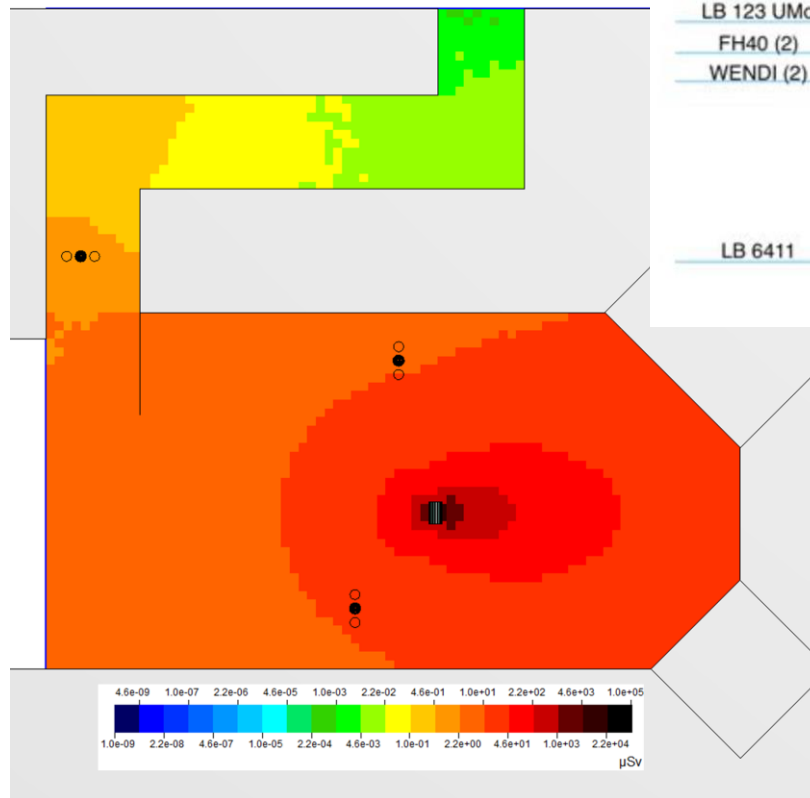
- -1.0
- 0.0
- 1.0
- 2.0
- Detektor
- far
- ✱ close

Mass Number of primary particle

# Radiation Protection Project

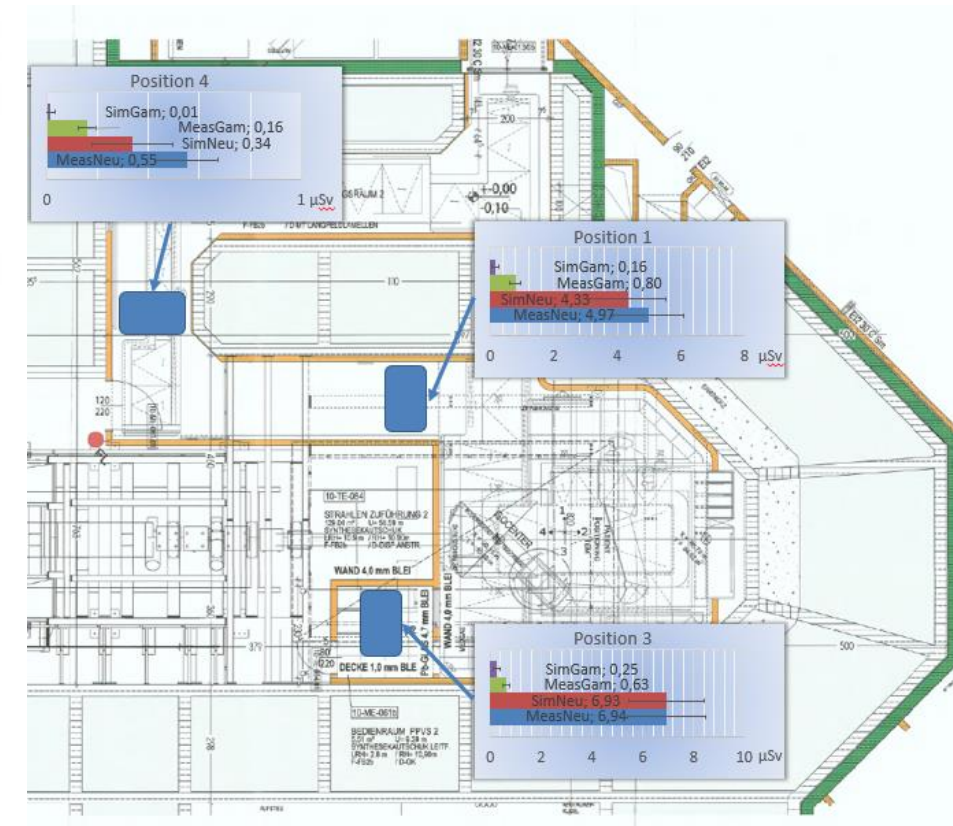
## MEASUREMENTS AND SIMULATIONS IN IR DURING PATIENT TREATMENT

CAN FLUKA BE USED TO ASSESS DOSE TO PERSON IN THE ROOM IN CASE OF THIS INCIDENT?



Reasonable agreement  
btw measurements  
and simulations

-> Method might be  
valid to assess  
personal dose

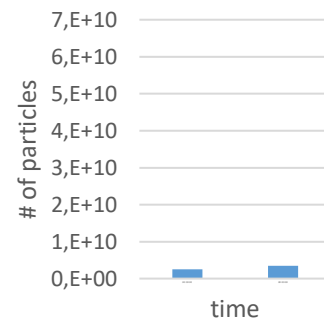
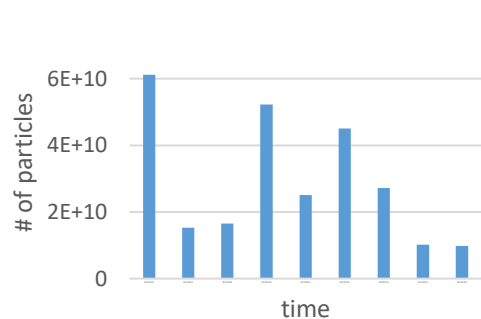
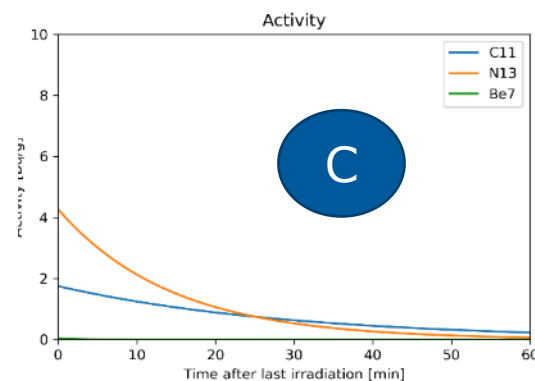
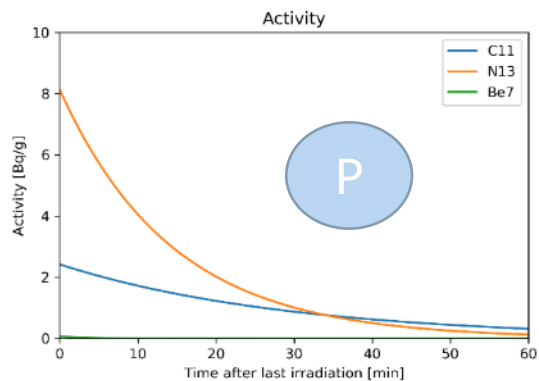


# Radiation Protection Project

## ACTIVATION OF WATER

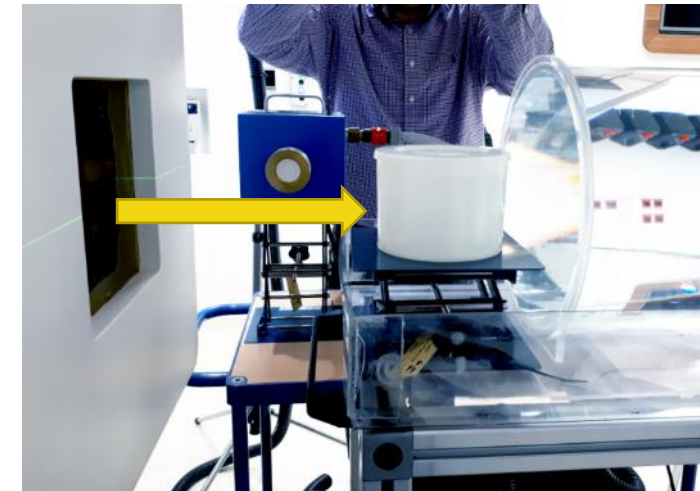
ARE CARBON IONS MORE DANGEROUS THAN PROTONS?

(Bq/g)	After protons			After carbon		
Nuclide	Activity	$\sigma$	MDA	Activity	$\sigma$	MDA
Be-7	0.07	0.01	0.0066	0.04	0.03	0.0099
C-11*	2.42	0.31	0.0138	1.75	0.22	0.0102
N-13*	8.14	1.04	0.0465	4.27	0.55	0.0248



Typical treatment plans:

- Less Particles
- Less Activation of phantoms (or immobilization equipment, etc.)

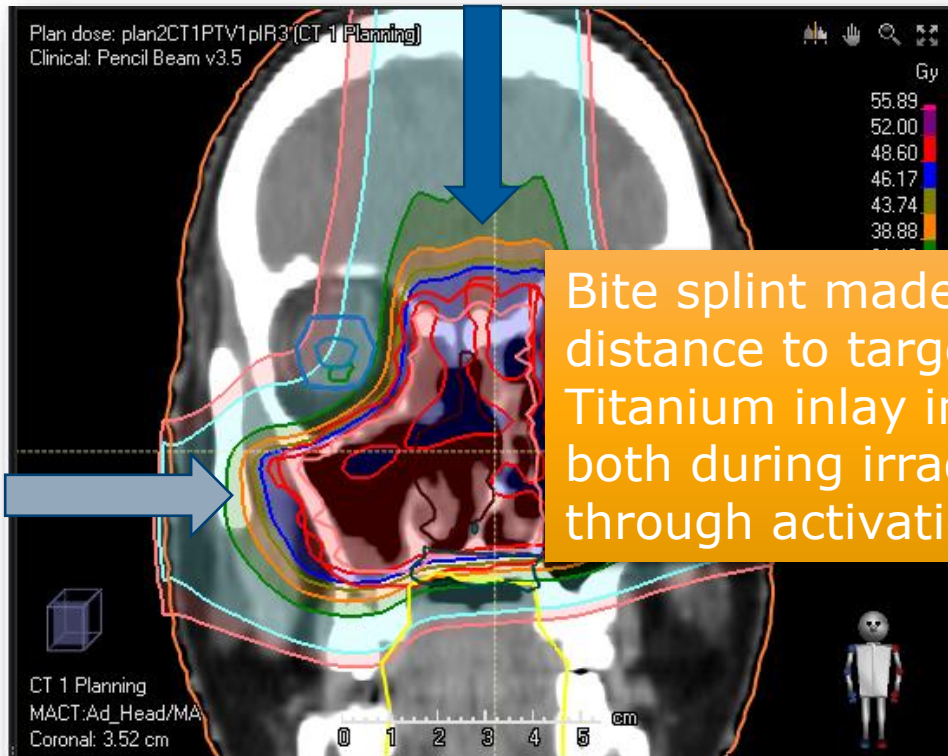




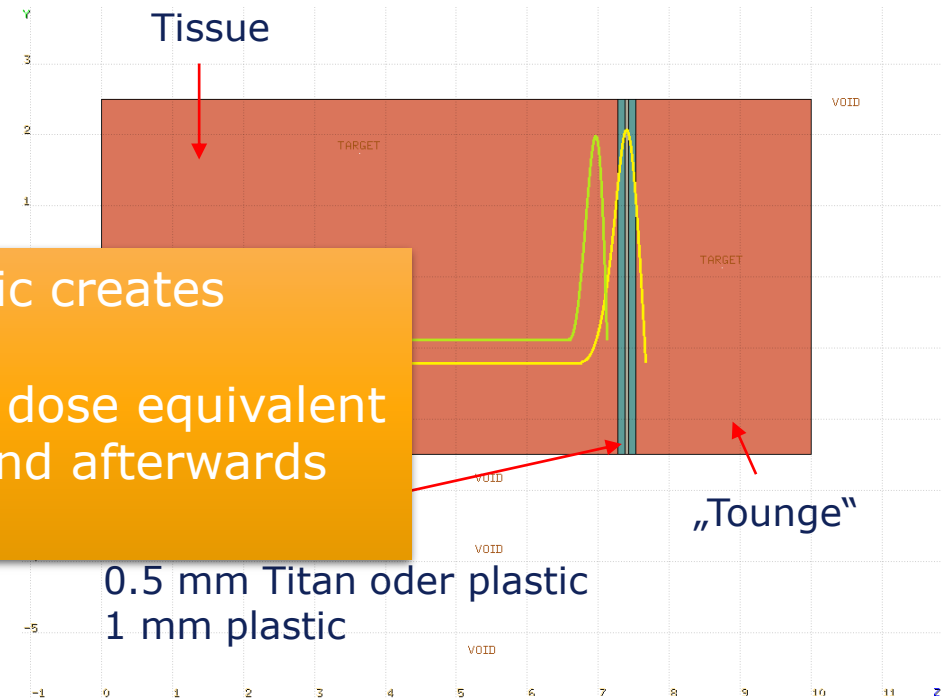
# Radiation Protection Project

## OPTIMIZATIONS FOR SINUS IRRADIATION

IS A TITANIUM LAYER IN THE BITE SPLINT USEFUL TO REDUCE DOSE EQUIVALENT TO THE PATIENT?

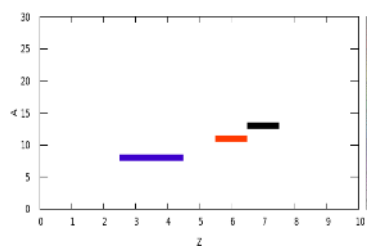


Bite splint made of plastic creates distance to target area - Titanium inlay increases dose equivalent both during irradiation and afterwards through activation

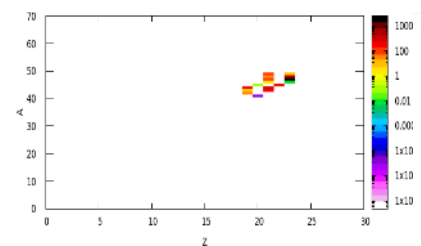


0.5 mm Titan oder plastic  
1 mm plastic

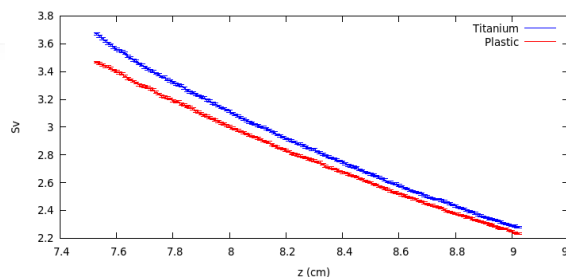
Activation without Ti



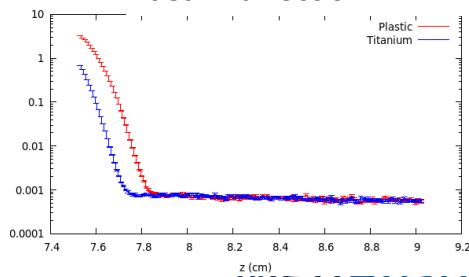
Activation with Ti



Dose Equivalent in beam direction



Energy dose in beam direction

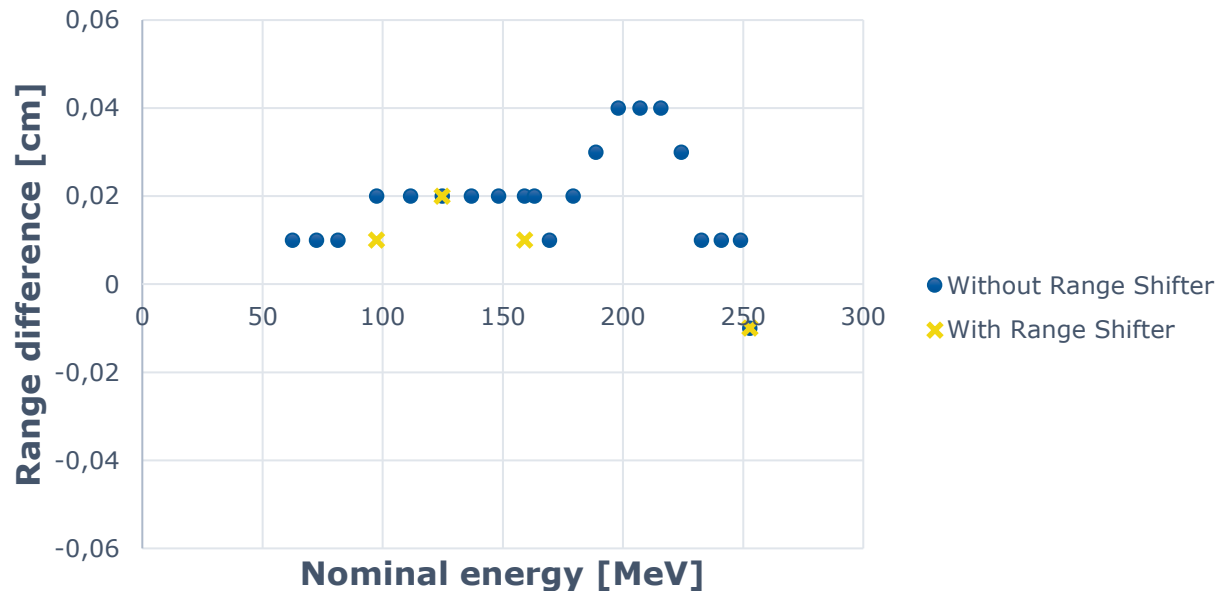


# Radiation Protection Project

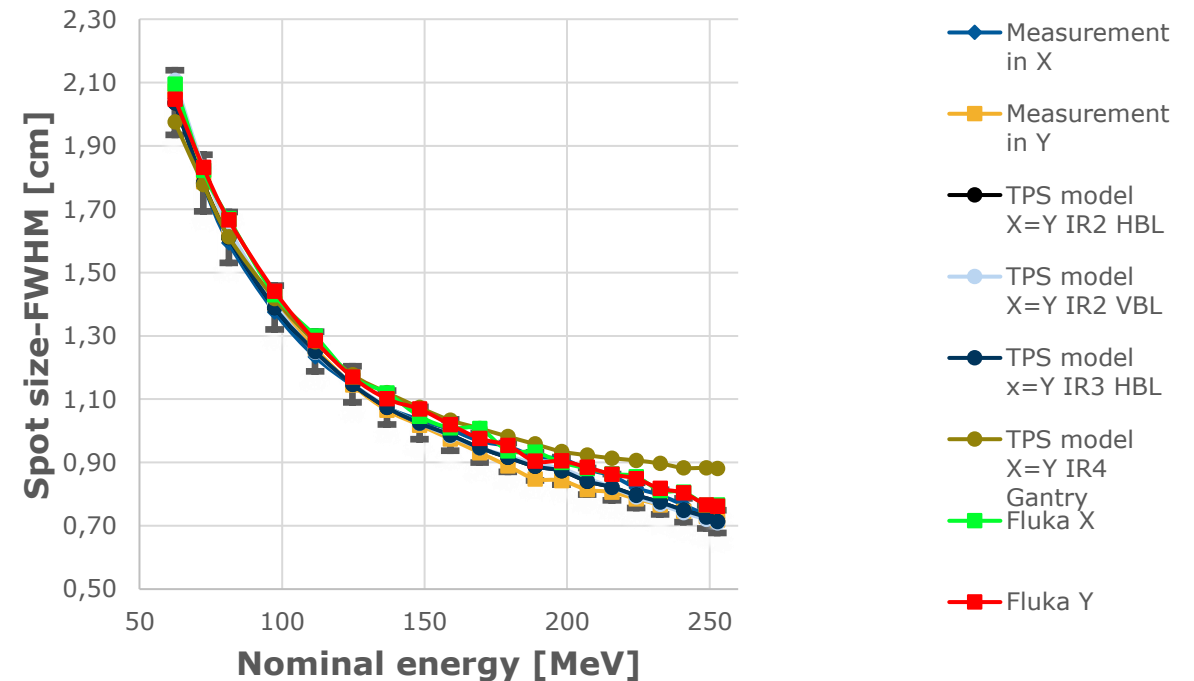
## COMMISSIONING OF THE PROTON BEAM MODEL IN FLUKA

FOR ADDITIONAL EVALUATION OF SPECIAL TREATMENT SITUATIONS (E.G. IMPLANTS)

Differences in range (R80) between measurements and FLUKA for proton beams of different energies (current beam model)



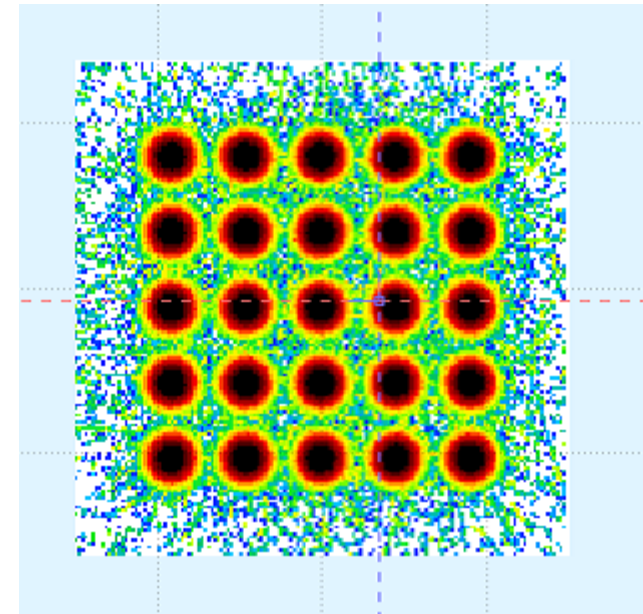
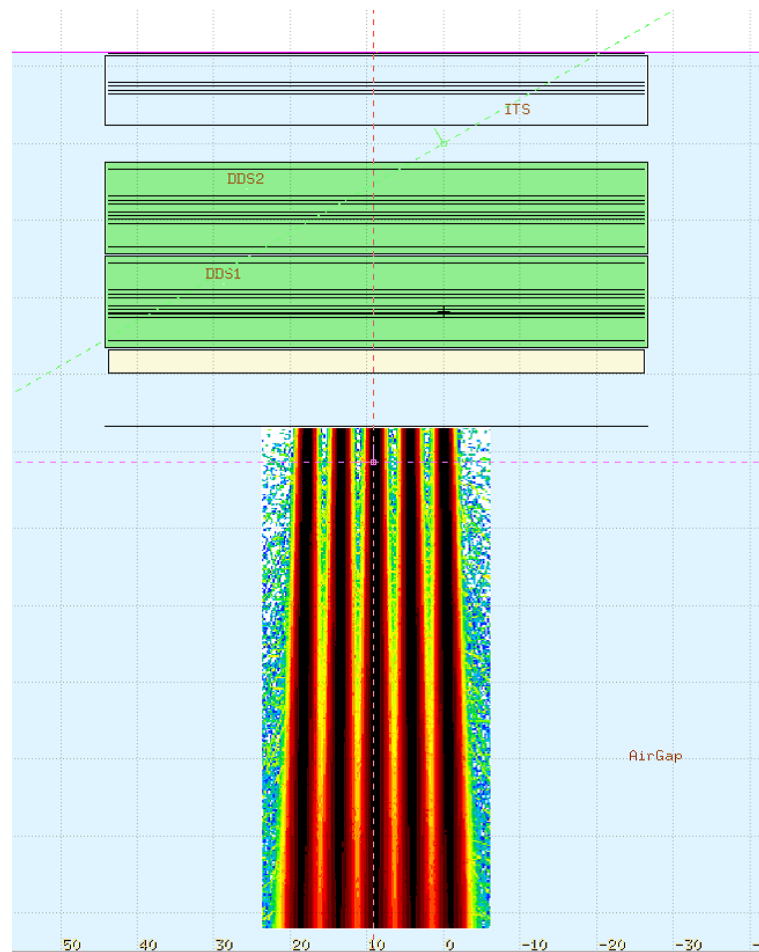
Spot size at isocenter - Measurements versus TPS baseline and FLUKA



# Radiation Protection Project

## EVALUATION OF PROFILES IN AIR – 5X5 SPOTS PLAN

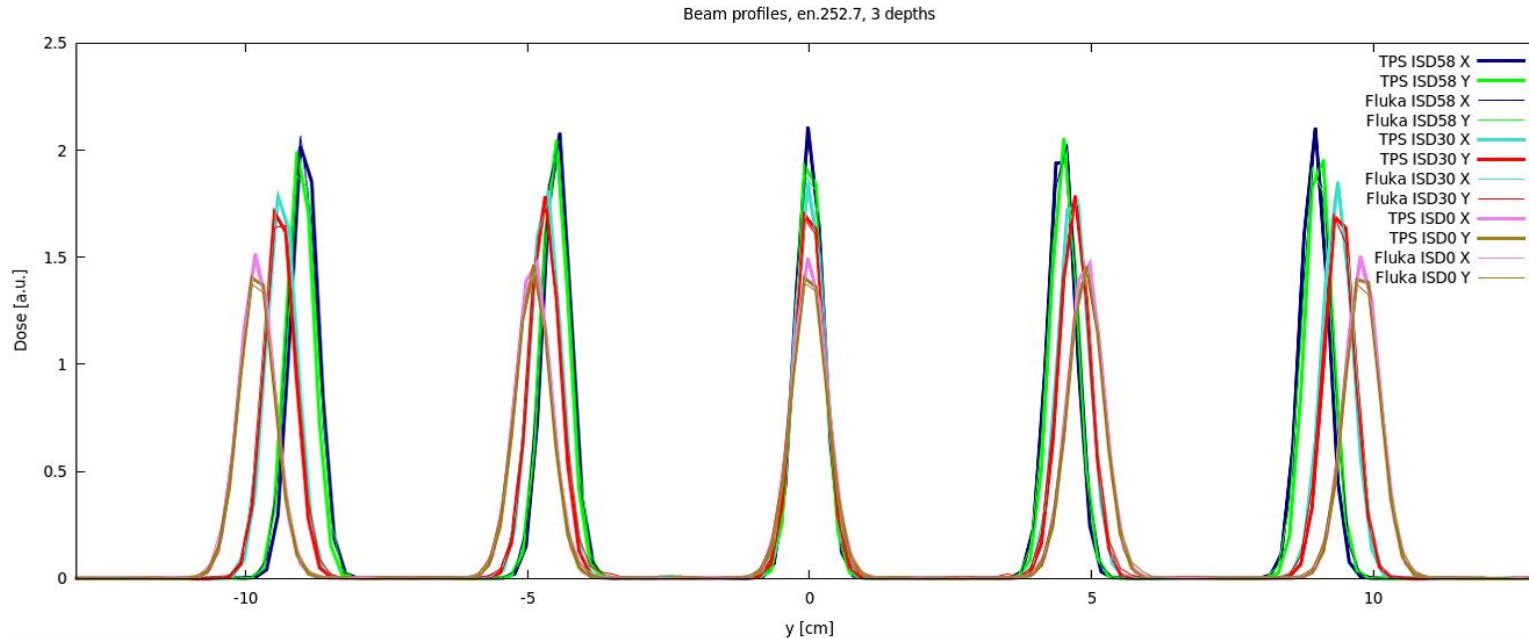
*BEST RESULT IF VACUUM WINDOW IS NOT IMPLEMENTED*



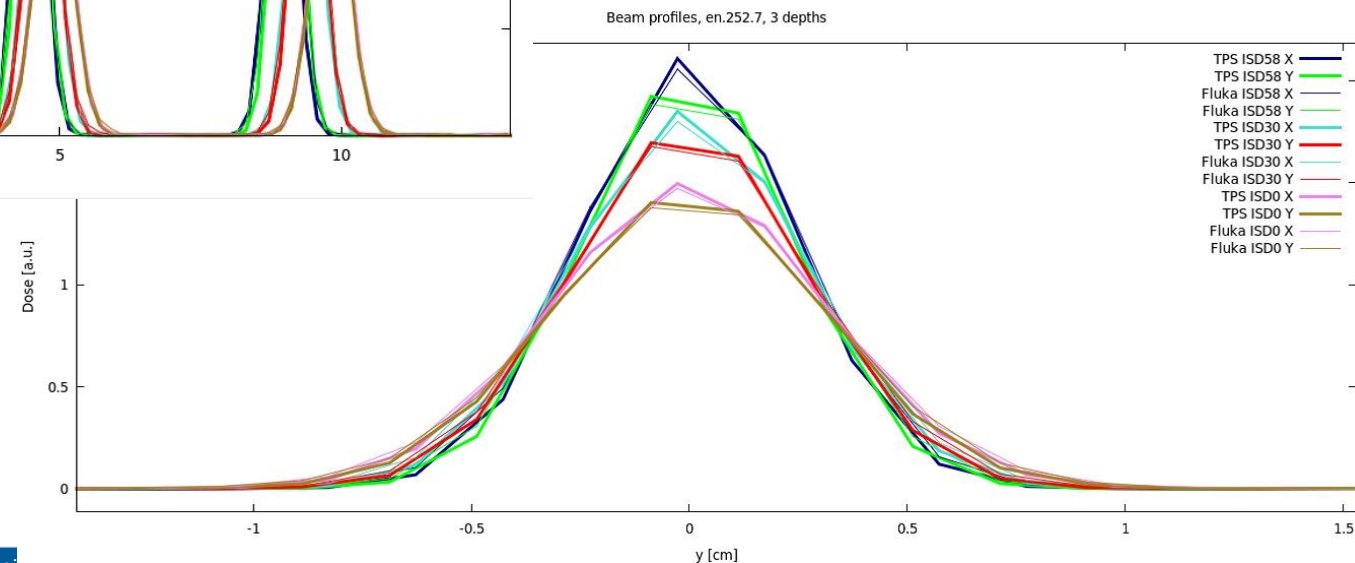
# Radiation Protection Project

## EVALUATION OF PROFILES IN AIR – 5X5 SPOTS PLAN

SHOWN FOR 252,7 MEV PROTON BEAM



For ISD58, ISD30 and ISD0 (at isocenter) FWHMs in agreement (inside 0.6 mm difference from measurements)



# Radiation Protection Project

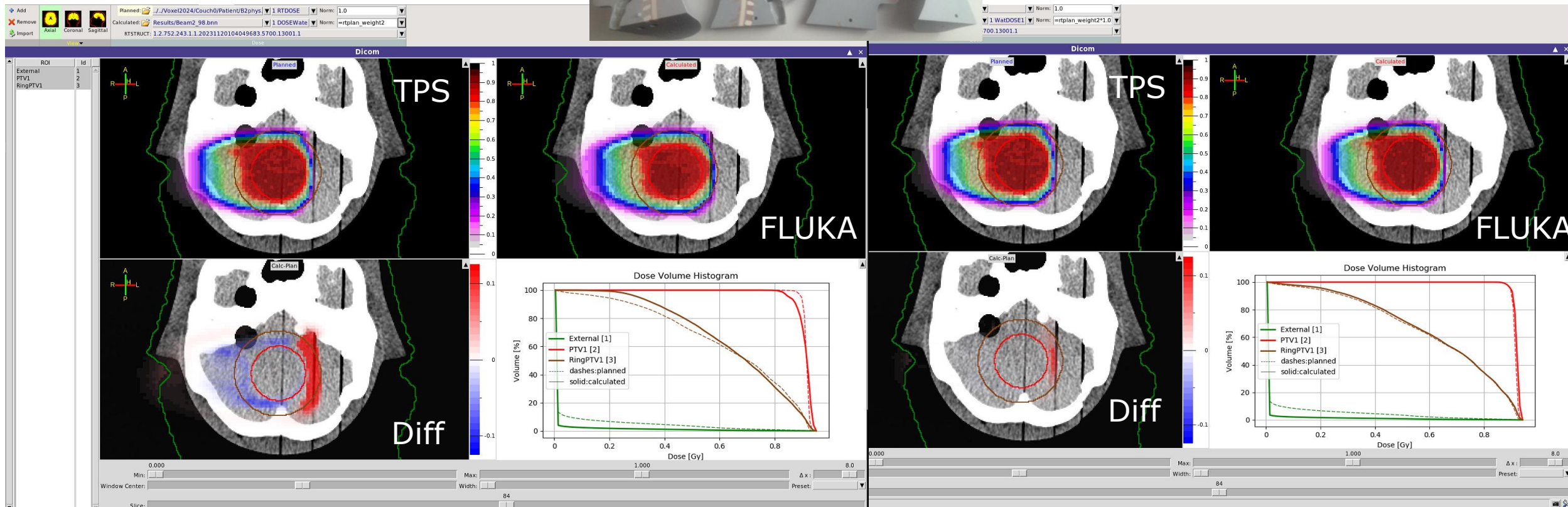
## APPLICATION OF BEAM MODEL IN A TREATMENT PLAN

LEFT WITHOUT BEAM MODEL IMPLEMENTED, RIGHT WITH OPTIMIZED BEAM MODEL FOR PROTONS

Without beam model



With beam model



# Radiation Protection Project

## APPLICATION OF

LEFT WITHOUT BEAM MODEL

Without beam model

Good agreement between FLUKA and commercial TPS for proton beams.

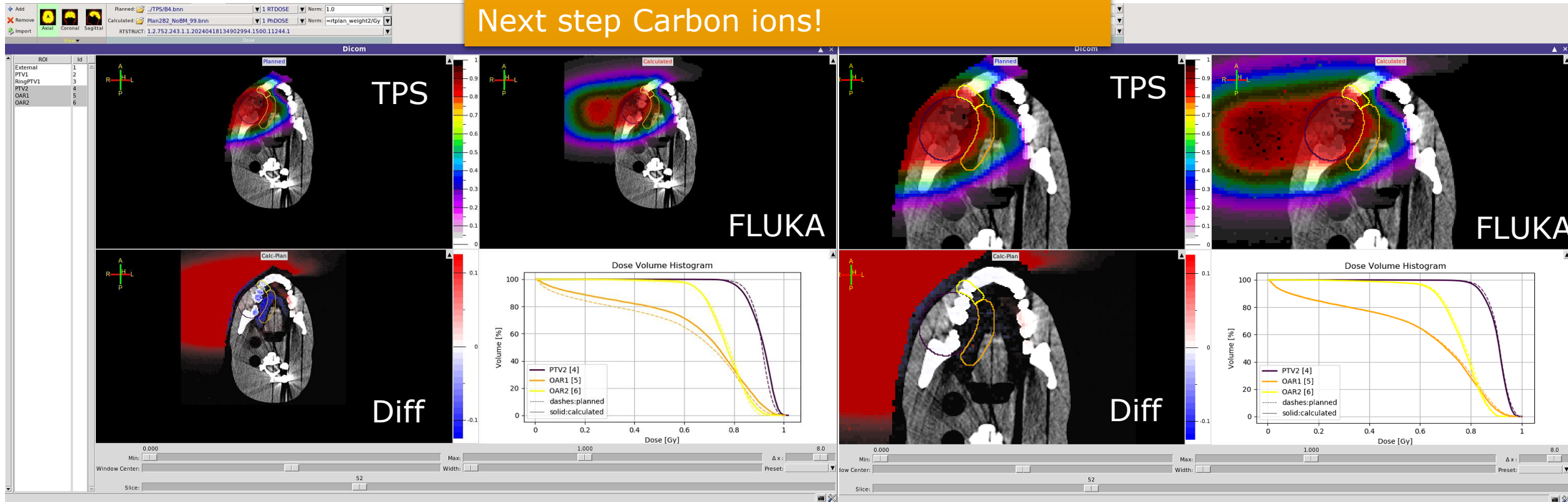
Beam model still needs optimization concerning effective energy in iso center.

Next step Carbon ions!

## MENT PLAN

MODEL FOR PROTONS

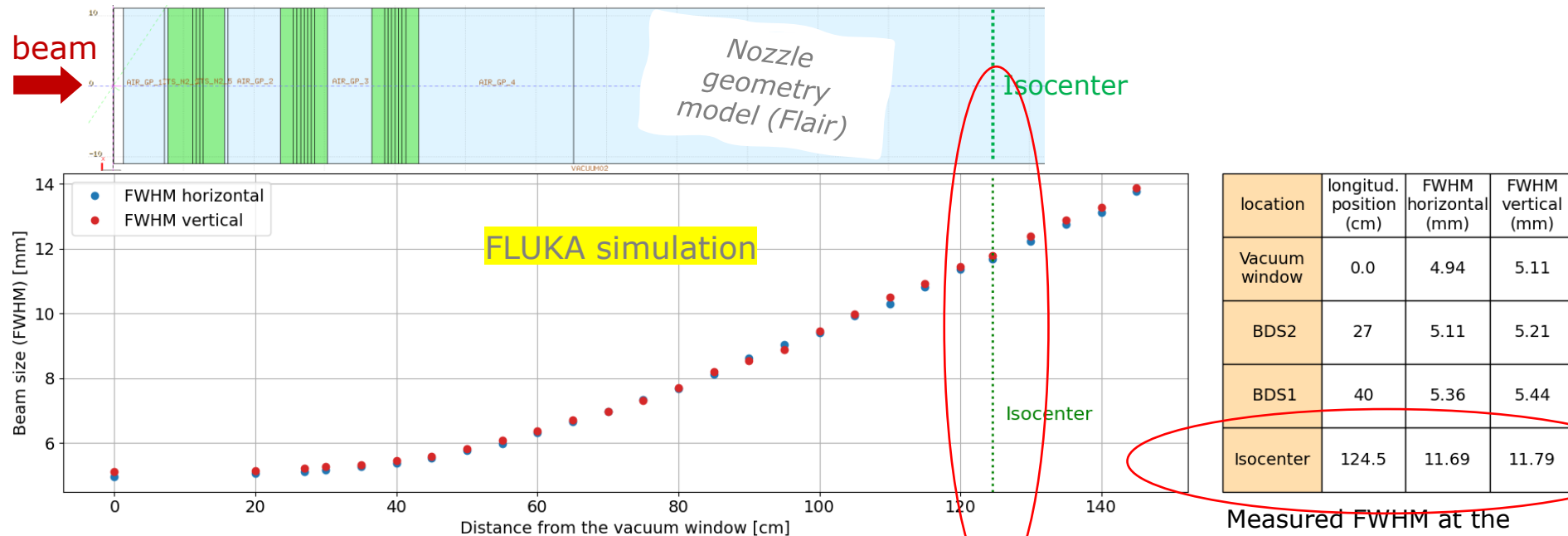
With beam model



# Accelerator and Beam Physics Project

## FLUKA SIMULATION OF BEAM SCATTERING IN THE NOZZLE

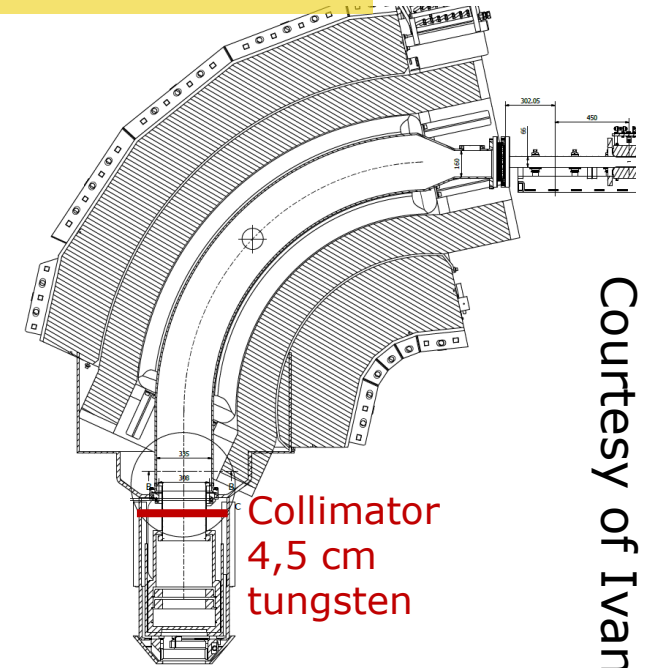
- MAD-X/PTC particle tracking in the accelerator beam line → recorded particle coordinates.
- Output of MAD-X/PTC at the vacuum window → FLUKA input via the SOURCE sub-routine.
- Beam delivery monitors consist of thin metal and plastic foils with gaps filled by gasses.
- Detailed nozzle model was built using Flair to simulate the beam scattering using FLUKA.
- MULSOPT card included → MCS optimization & single scattering activated.
- Below → FLUKA simulation of the 136.8 MeV proton beam passing through the nozzle.



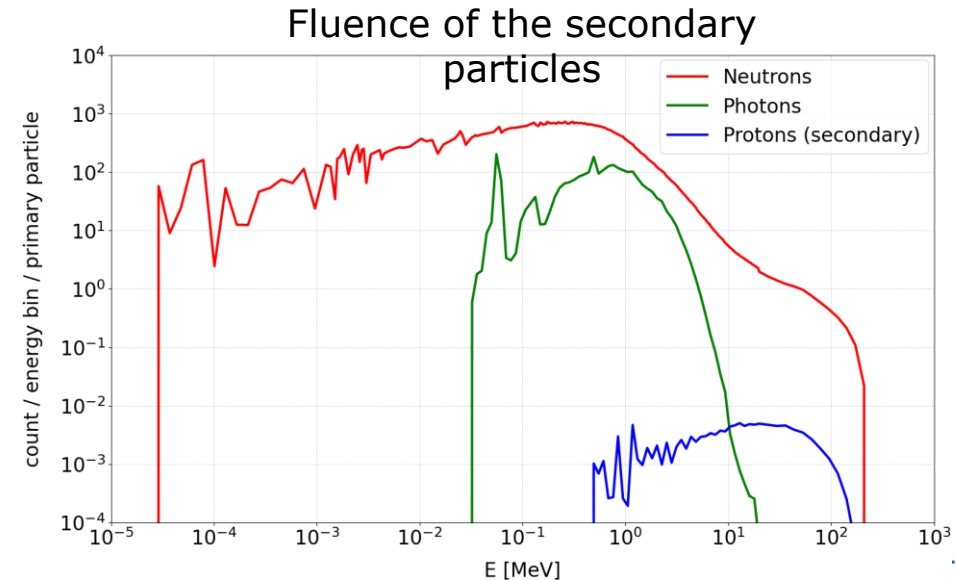
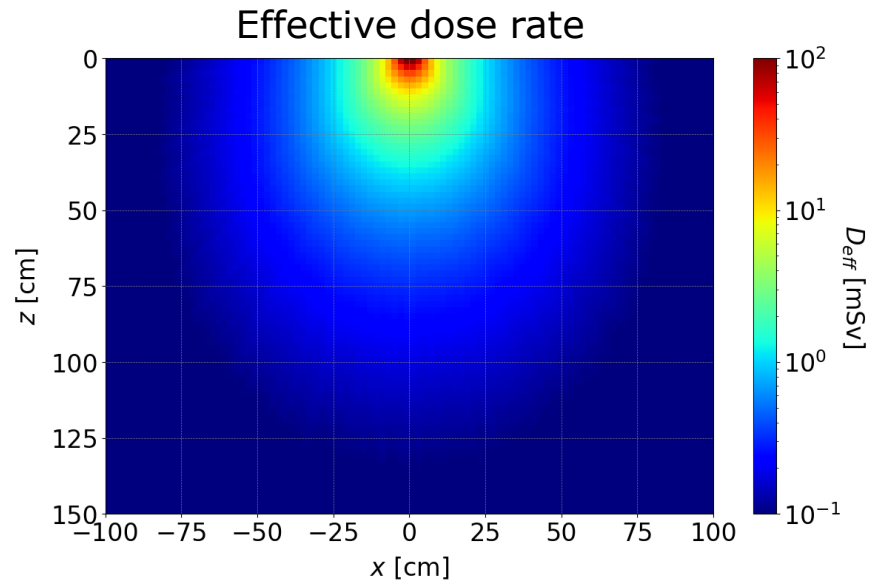
Measured FWHM at the isocenter = 11.7 mm (average)

## COLLIMATOR DESIGN USING FLUKA

- FLUKA was used to design a protective collimator in the gantry irradiation room.
- The collimator shall protect the patients in case of a failure of the last dipole magnet -> IEC 60601-2-64 clause 201.10.2.101.4.6. – non primary radiation under fault condition
- FLUKA simulations were used to determine the collimator parameters (dimensions, material, ...).
- Secondary particles generated by the beam which accidentally hits the collimator, are also evaluated.
- Below are presented FLUKA simulations of the 252.7 MeV proton beam impacting on the collimator.



Courtesy of Ivan Strasik & Mauro Pivi

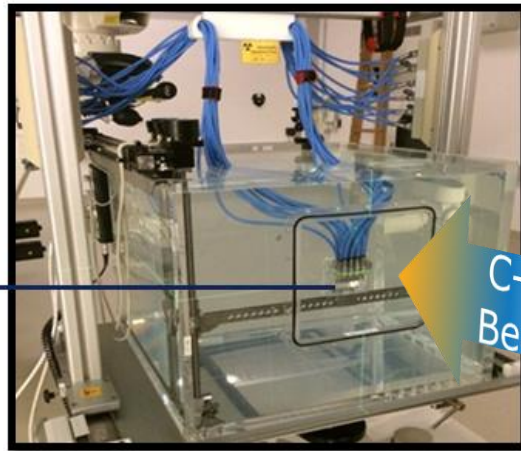
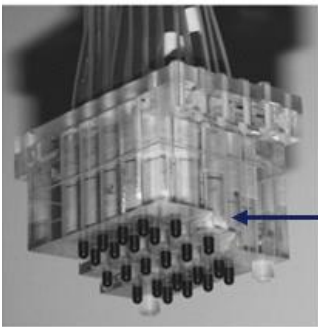




## MOTIVATION

*SAVING BEAM TIME!*

- Experimental **patient-specific quality assurance (PSQA)**
  - To verify dose calculation in clinical treatment planning system (**TPS**)
  - **Non-human** standardized geometry and material
  - Limited **sensitivity** to errors in planned/delivered dose
  - **Time consuming**



C-12  
Beam

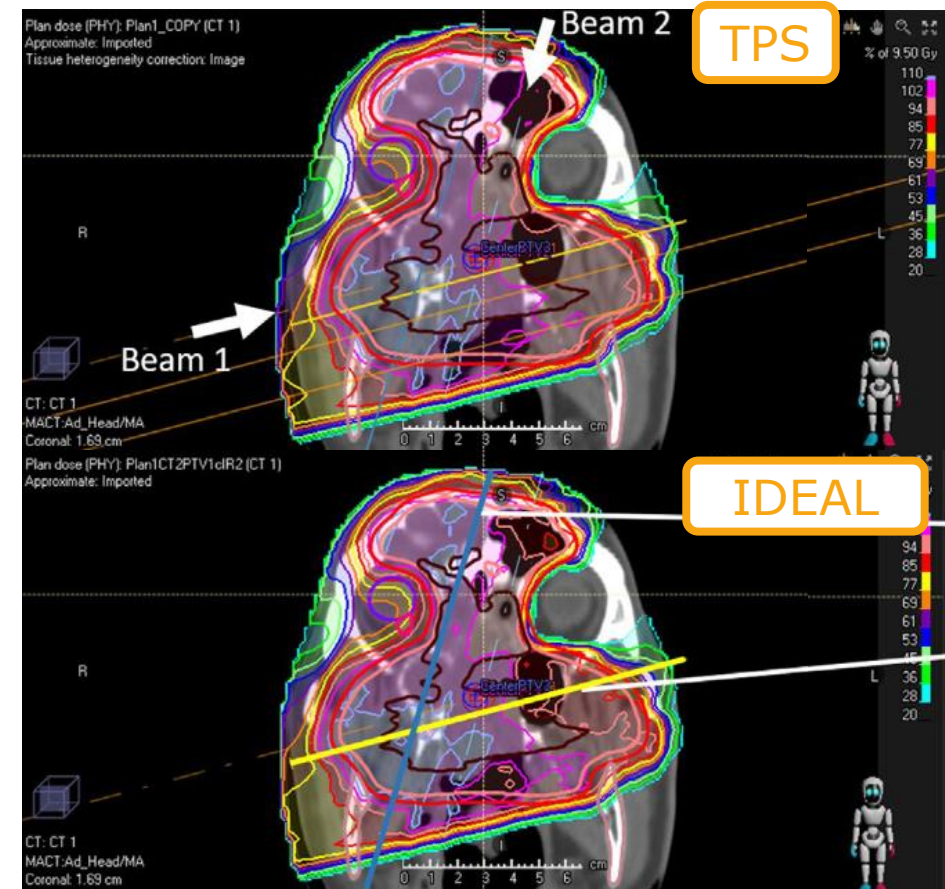
Independent system to  
recalculate dose in  
patient geometry

24 PinPoint ICs fixed to the PTW 3D detector block holder  
in a PTW MP3-P water phantom

## IDEAL



- **Independent** **Dose** **calculation** system for **Light ion beam therapy**
- Wrapper for GATE-RTion v1.0/Geant4.10.3.p3
  - GATE-RTion: well validated release of GATE for clinical usage, release cycle ~ 5 years
- Designed for **daily clinical usage**  
→ automatic workflow
- Integration of IDEAL into **myQA iON**
  - Collaboration with IBA Dosimetry
- First step
  - Absorbed dose validation
- Next step
  - RBE weighted dose validation



Grevillot et al. 2021

Courtesy of Andreas F. Resch & Yihan Jia

THANK YOU FOR YOUR INTEREST!

