

High Precision X-ray Measurements 2023

19-23 June 2023, Laboratori Nazionali di Frascati, Italy

Detectors for beam monitoring and dosimetry at ultra-high dose rates for FLASH Radiotherapy



University Medical Center Groningen

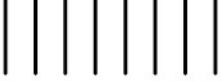
partrec

Francesco Romano

Istituto Nazionale di Fisica Nucleare - Sezione di Catania, Italy
and

Particle Therapy Research Center (PARTREC), Department of Radiation Oncology,
University Medical Center Groningen, The Netherlands

High Precision ~~X-ray~~ Measurements 2023



Disclosures:

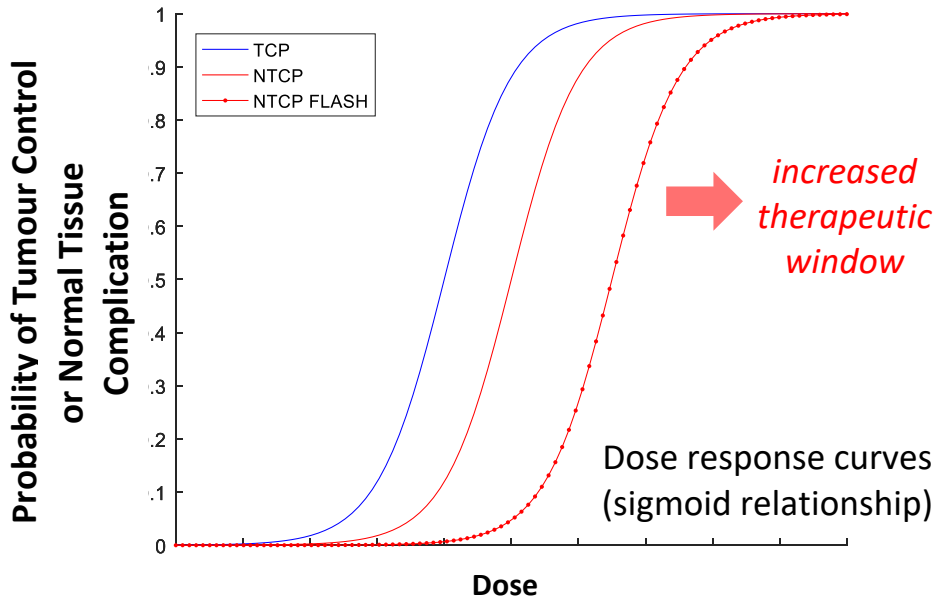
I won't talk about X-ray measurements!

I will talk about high-precision particle measurements!

Decreasing toxicity maintaining tumor control: FLASH effect

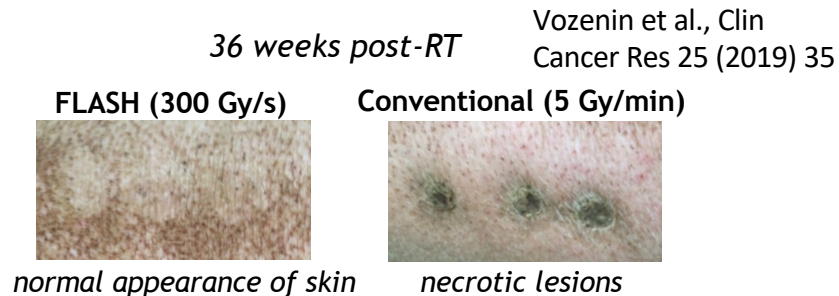


- FLASH radiotherapy: a promising cancer treatment modality under development → almost instantaneous delivery of a high radiation dose in a few radiation pulses of ultra-high dose rate (UHDR)



TCP = Tumour Control Probability

NTCP = Normal Tissue Complications Probability



CONVENTIONAL RADIOTHERAPY

Dose: ~2 Gy/fract. (x 30 fractions)

Dose Rate: ~ Gy/min

Irradiation Time: few minutes

FLASH RADIOTHERAPY

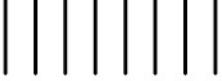
Dose: > 8 Gy (x 1 fraction?)

Dose Rate: > 40 Gy/s

Irradiation Time: <200 ms

- Biological mechanism producing the FLASH effect not yet fully understood

FLASH Radiotherapy: open questions



Several non-mutually exclusive hypothesis → role of oxygen depletion, immune response, ...

Is the FLASH effect only dependent on the **average dose-rate** along the irradiation duration?

Which are the relevant physical parameters?

Total dose → **D** (>8 Gy)

T (<200ms) → Average dose rate → **D/T** (> 40 Gy/s)

Dose-per-pulse? → **d** (→ relevant for ion chambers)

Dose rate (averaged) in the pulse? → **d/t** (< MGy/s)

Instantaneous dose rate? → **\dot{d}**

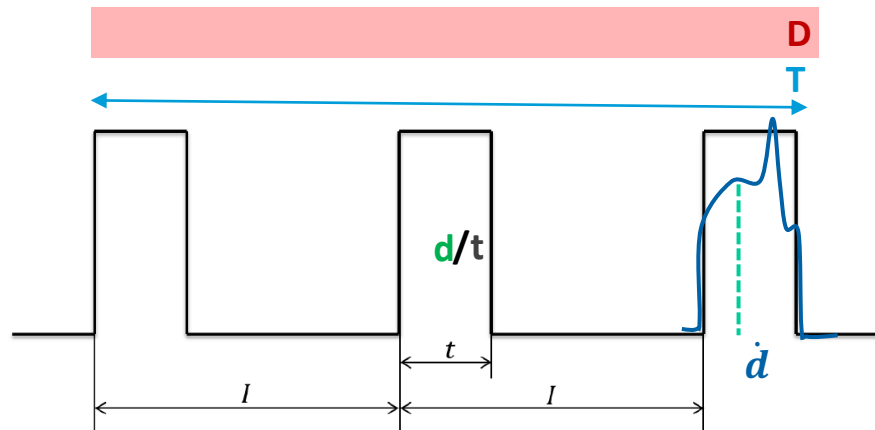
...basic questions (for medical physicists):

Are we able to accurately perform absorbed dose measurements for FLASH Radiotherapy

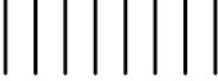
→ *all relevant parameters?*

With the level of accuracy required for clinical translations? → Which detectors?

Are we able to accurately *real-time monitor* the dose delivery at the irradiation point?



Realization of FLASH radiation beams



Year	Radiation type	Machine	Energy (MeV)	Average dose rate (Gy/s)	Dose per pulse (Gy/pulse)	Pulse repetition rate (Hz)	Field size	Purpose	Dosimetry method
1995	Photon ³⁰	Brookhaven National Laboratory (USA)	0.08 mean	310–620	Not provided	52 MHz	4 × 0.02/0.04 mm 0.075/0.2 × 7 mm	Rat neuro-study	IC, RCF, TLD
2014	Electron ⁴	Kinetron Linac ³⁷ (Switzerland)	4.5	60	5 × 10 ⁶	19	Ø 1.2 cm 1.8 cm × 2.0 cm	Mouse study (bilateral thorax irradiation)	Chemical dosimetry with blue methyl viologen
2017	Electron ⁵	Oriatron 6e Linac (Switzerland)	6	100	5 × 10 ⁶	100	Ø 1.7 cm	Mouse study (brain irradiation)	TLD
2017	Electron ¹⁷	Varian 21EX (USA)	9 and 20	35–210	1.7 × 10 ⁶	182	1–5 cm @ 90%	Feasibility study	EBT2 RCF
2018	Photon ⁷	European Synchrotron Radiation Facility (France)	0.102 mean	37	1.2 × 10 ⁴ Gy/s instantaneous	Continuous	2 × 2 cm (reference size)	Mouse study (brain irradiation)	IC ³⁹
2018	Proton ²⁰	IBA isochronous cyclotron (France)	138–198	40	N/A	106.14 MHz (quasi-continuous)	~1.2 cm @ 90%	Feasibility study	Cylindrical IC, EBT3 RCF
2019	Electron ¹⁸	ELEKTA Precise Linac (Sweden)	8	30–300	Not provided	200	Ø 2 cm (at the highest dose rate)	Feasibility study	EBT3 RCF
2019	Electron ⁶	Kinetron Linac and Oriatron 6e (Switzerland)	4.5 and 6	300	5 × 10 ⁶	Not provided	Ø 2.6 cm or 1.8–4.5 cm rectangular	Mini-pig (skin) and cat (nasal tumor) study	TLD, alanine pellets, EBT3 RCF
2019	Electron ³¹	Oriatron ERT6 Linac (Switzerland)	5.6	150	1 × 10 ⁶	100	Ø 3.5 cm 1.3 depth @ 90%	Human patient treatment (skin)	Alanine pellets, EBT3 RCF
2019	Proton ²¹	Varian isochronous cyclotron (USA)	245	40	N/A	Quasi-continuous	1 cm × 3 cm	Mouse study (whole thorax irradiation)	Not provided
2020	Proton ²²	IBA isochronous cyclotron (USA)	230	80	N/A	106.14 MHz (quasi-continuous)	~2 cm FWHM	Mouse study (abdomen irradiation)	Plane-parallel IC
2020	Proton ²⁴	Mevion synchrocyclotron (USA)	70	100–200	0.16–0.32 Gy/pulse (8–16 × 10 ³ Gy/s instantaneous)	648	~1.2 cm FWHM (5 mm @ 90% isodose)	Feasibility study	Plane-parallel IC, FC, MC simulation, and RCF

e-

Modified clinical LINACs

e-

Research LINACs

p

Isochronous cyclotrons

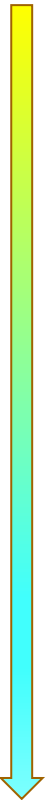
p

Synchro cyclotrons

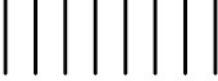
γ ions

Synchrotrons

> 40 Gy/s



Realization of FLASH radiation beams



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2020	Proton ³²	IBA isochronous cyclotron (USA)	227.5	130	N/A	106 MHz (quasi-continuous)	1.6 × 1.2 cm ² ellipse	Mouse (partial abdomen irradiation)	Plane-parallel IC, FC, MC simulation, EBT3 RCF
2020	Photon ³³	ANSTO Australian Synchrotron	0.07 and 0.09 mean	40–350 (at treatment depth and filtration)	200 (at 20 mm reference depth and filtration)	Continuous	2 × 2 cm (reference dosimetry size)	Rat study (brain cancer irradiation)	Pinpoint IC (reference), silicon semiconductor, and MC
2021	Proton ²⁵	Mevion synchrocyclotron (USA)	60	120–160	0.22 Gy/pulse (9.3 × 10 ³ Gy/s instantaneous)	750	Ø 1.1 cm FWHM (5 mm @ 90% isodose)	Feasibility of SOBPs beam using a synchrocyclotron	IC, FC, MC simulation, and EBT-XD RCF
2021	Electron ³⁴	Varian Clinac 2100 C/D (USA)	10	240–260	0.81 Gy/pulse	360	Ø 1–1.5 cm	Feasibility of UHDR at the machine's isocenter	EBT-XD RCF
2021	Proton ³⁵	Research isochronous cyclotron (Germany)	68	75	N/A	20 MHz	Ø 1.3 cm	Preclinical setup for mouse irradiation	IC and RC
2021	Proton ³⁶	COMET ³⁸ isochronous cyclotron (Switzerland)	170–250	9000 (for a single spot)	N/A	72.85 MHz	~2.3–5 mm (16 × 1.2 cm ² by scanning)	Feasibility study	FC
2021	Helium ion ²⁶	Synchrotron (Germany)	145.74 MeV/u	185	N/A	Quasi-continuous	1 cm ² (by spot scanning)	In vitro study of dose, LET, and O ₂ concentration	Parallel-plate IC
2021	Carbon ion ²⁷	Synchrotron (Germany)	280 MeV/u	70	N/A	Quasi-continuous	1 cm ² (by spot scanning)	Dosimetry and in vitro study	IC and EBT3 RCF

> 40 Gy/s

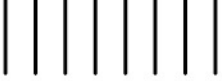
e- Modified clinical LINACs

e- Research LINACs

p Isochronous cyclotrons

p Synchro cyclotrons

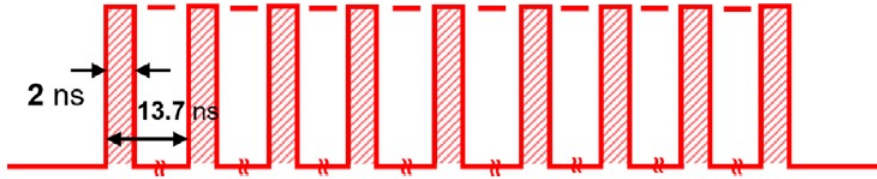
γ Synchrotrons



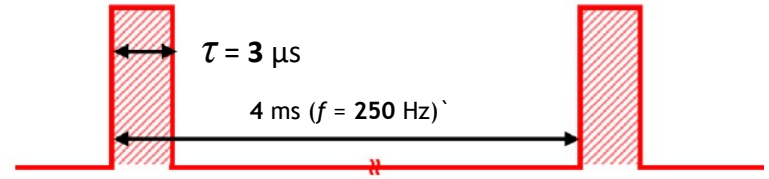
protons $\dot{d} < 500 \text{ Gy/s}$

electrons

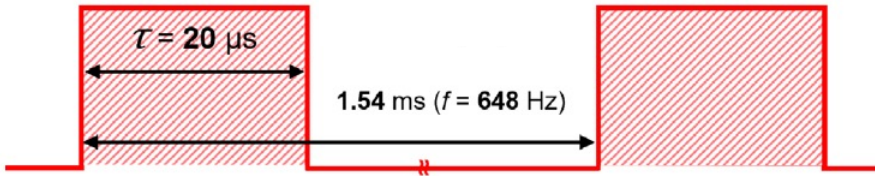
Isochronous cyclotron (quasi-continuous radiation)
($f=72.8 \text{ MHz}$, 2nd Harmonic)



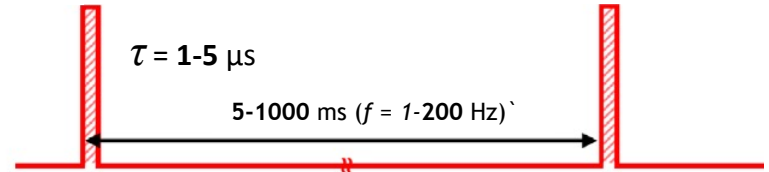
$\dot{d} < 100 \text{ kGy/s}$
Clinical LINAC for Radiotherapy (modified)



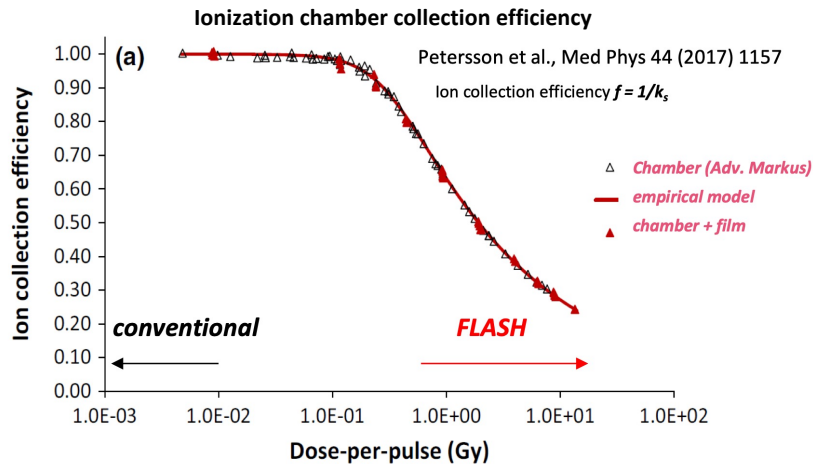
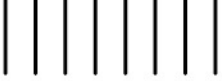
Synchrocyclotron (FLASH dose rate) $\dot{d} < 10 \text{ kGy/s}$



$\dot{d} < 5 \text{ MGy/s}$
Research LINAC for pre-clinical studies



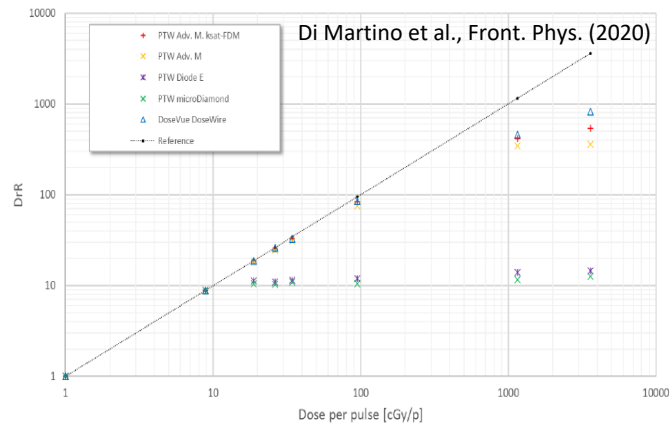
FLASH Radiotherapy: dosimetric challenges



*Ionization chambers: recommended by protocols
for reference dosimetry for Radiotherapy*

Tools and methods established in dosimetry for conventional RT are not suitable for FLASH-RT:

- Alternative active detectors to be developed
- New protocols for reference dosimetry



Other commercially available detectors

Uncertainties in dosimetry:

- under/over/not estimate different biological response between conventional irradiation and ultra-high dose rate irradiation
- no proper assessment and investigation of the FLASH effect.

European initiatives

UHDpulse EMPIR project

6 Metrology institutes
3 Hospitals
5 Universities
5 Research institutes
6 Companies
+ Proton therapy network

Metrology for advanced radiotherapy using particle beams with ultra-high pulse dose rates

Type:	Joint Research Project
Duration:	2019-2023
Start:	1. Sept. 2019
Funding:	2.1 M €
Coordinator:	Andreas Schüller (PTB)
Topic:	Tools for traceable dose measurements for:



- **FLASH radiotherapy**
- **VHEE radiotherapy**
- **Laser driven accelerators**

<http://uhdpulse-empir.eu/>



The EMPIR initiative is co-funded by the European Union's Horizon 2020 research and innovation programme and the EMPIR Participating States

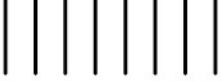
The European Metrology Programme for Innovation and Research (EMPIR):

- **traceable reference standards** and **validated reference methods** for dose measurements at ultra-high pulse dose rates
- characterization of detector systems, development of traceable and validated methods **for relative dosimetry**
- contribution to **codes of practice**

Follow-up normative project submitted soon

Courtesy of A. Schueller

Italian initiatives



The INFN “FRIDA” project



WP1

The FLASH mechanism

WP3

Beam/dose monitoring

WP2

Beam delivery

WP4

Treatment planning

Units

CT – F. Romano
LNS – G. Cirrone
MI – D. Giove
PI – G. Bisogni
RM1 – A. Sarti (PI)
TIFPA – E. Scifoni
TO – A. Vignati

Goal of “FRIDA” (FLASH Radiotherapy with high Dose-rate particle beams) is to make a step forward in all the crucial areas... Four WPs [mechanism modelling & radio-bio experiments; beam delivery; beam monitoring; treatment planning] working in parallel, >25 FTEs, 7 INFN units with know-how in the fields and a solid international network of research centres and companies (SIT, STLab) are the resources to accomplish the research program.

- **Test few promising techniques for FLASH beam monitoring and dosimetry applications**
 - Adapting existing techniques for FLASH conditions
 - Developing from scratch some other novel approaches.

Task 1 Development and test of new Beam Monitoring systems

- Task 3.1.1: Air Fluorescence monitor (Roma1)
- Task 3.1.2: Integrating Current Transformer (LNS)
- Task 3.1.3: Silicon/Diamond detectors (To)
- Task 3.1.4: SiC detectors (in-kind) (CT)

Task 2 Development and test of new dosimetric systems

- Task 3.2.1: Portable Calorimeter (CT)
- task 3.2.2: Scintillator based dosimeter (PI)
- Task 3.2.3: SiC for relative dosimetry (in-kind) (LNS)

Task3 Intercomparisons, calibrations and codes of practice

- Task 3.3.1 Dosimetric characterization of the beams with available BM systems (dual gap chamber, SEM, FC) and reference dosimeters (Faraday cup, alanine, RCF, IC)
- Task 3.3.2 Intercomparisons and calibrations of the developed BMs and dosimeters
- Task 3.3.3 Dosimetric codes of practice for the dosimetry of FLASH beams

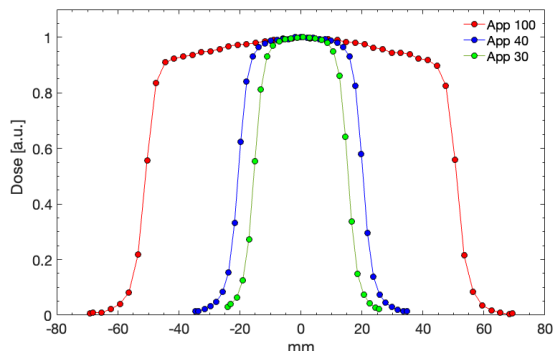
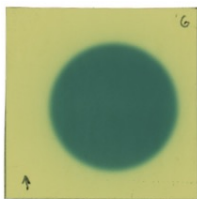
Possible dosimetric approaches for FLASH RT: passive detectors



Dosimeter	Real time	In vivo dosimetry	Absolute/reference dosimetry	Beam monitoring	Spatial resolution	Temporal resolution	2D dosimetry	Accuracy at conventional dose rates ^a	Other considerations
Ion chamber	Yes	No	Yes	Yes	Several mm	10–200 μ s	Array	1%–2%	Significant ion recombination at UHDRs
Semiconductor	Yes	Yes	No	Yes	Sub-mm (or μ m)	1–10 ns	Yes	2%–5%	Angular dependency, radiation damage, LET dependence
TLD	No	Yes	Yes	No	Several mm	N/A	No	3%–10%	Energy dependence, time consuming, LET dependence
OSLD	No	Yes	Yes	No	Sub-mm to mm	N/A	Array	3%–5%	Energy dependence, quenching in high LET fields
Scintillator	Yes	Yes	Potentially	Potentially	Sub-mm to mm	ns to μ s	Array and sheet	3%–5%	Quenching in high LET fields, Cherenkov radiation
Gas scintillator	Yes	No	No	Yes	Sub-mm	N/A	Yes	1%	Beam centroid measurement
Calorimeter	Yes	No	Yes	No	cm to several mm	ms–10 ms	No	<1% at the primary standard level	Bulky, not easy to use, correction factors, time consuming
Film	No ^b	Yes	Potentially	No	Tens of μ m	N/A	Yes	3%–5%	Quenching in high LET fields
Fricke	No	No	Yes	No	cm to sub-mm	N/A	Potentially	<1% at primary standard level	Time consuming, complexity
Faraday cup	Yes (for charge measurements)	No	Yes	No	N/A	< μ s	No	2%–5% for commercial devices; 1%–2% for dedicated equipment ^c	Measures the total collected charge (other detectors are required for dose determination)
Nuclear track detector	No	Yes	No	No	mm; sub-mm with specialized equipment	N/A	Yes	5%–7%	Time consuming, energy dependence, LET dependence
Alanine	No	Yes	Yes	No	mm	N/A	No	2%–7% for doses larger than 10 Gy	Decreased accuracy for doses less than 10 Gy (minimum 2 Gy)
Integrated current transformer	Yes	Potentially	No	Yes	N/A	sub- μ s	No	<1% for charge measurements	Lack of 2D measurements, only charge measurements

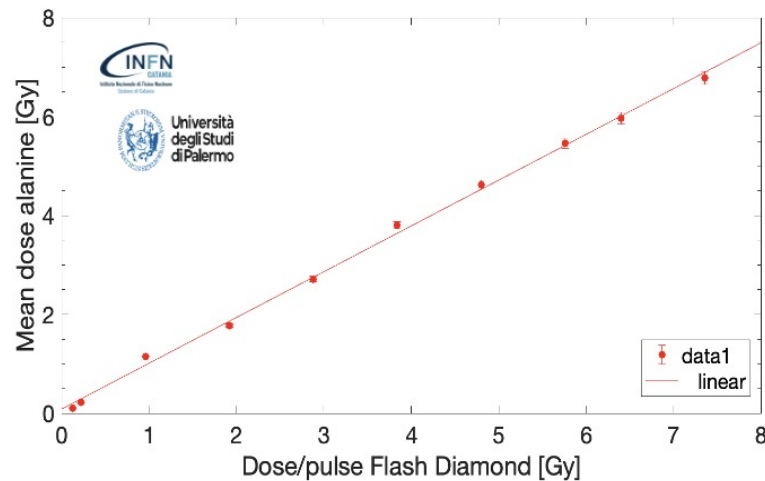
Possible dosimetric approaches for FLASH RT: passive detectors

Radiochromic films



Relative dosimetry

Alanine



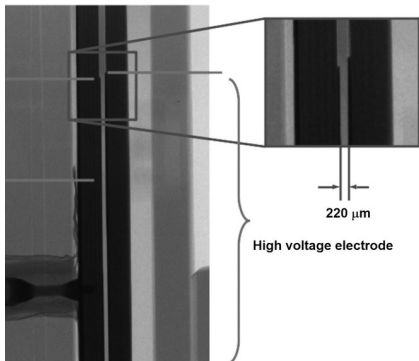
Absolute dosimetry

Possible dosimetric approaches for FLASH RT: ionization chambers



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Gas scintillator	Yes	No	No	Yes	Sub-mm	N/A	Yes	1%	Beam centroid measurement
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Possible dosimetric approaches for FLASH RT: ionization chambers

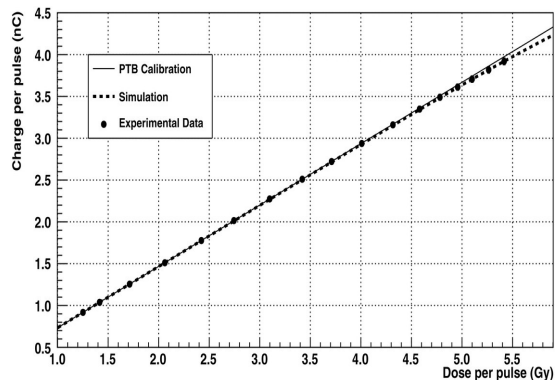


Which solutions for ion recombination at UHDRs?

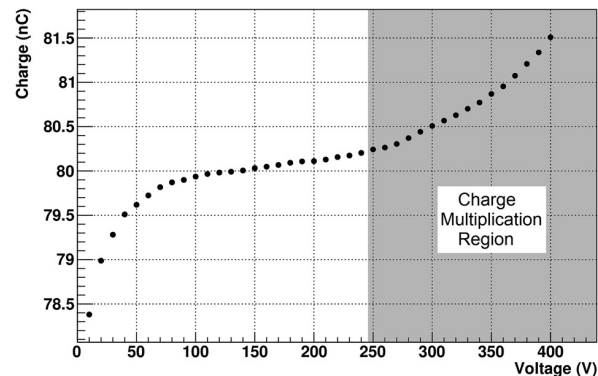
- Still using ionization chambers → k_{sat} to be decreased and/or properly determined

○ New chamber design with ultra-thin gap thickness (F. Gomez et al., Med. Phys. 2022)

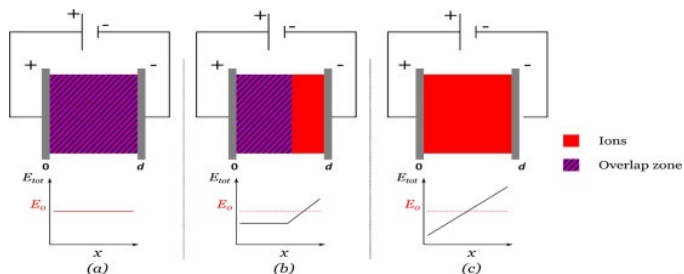
F. Gomez et al. Med Phys. 2022



Increasing applied V



Possible dosimetric approaches for FLASH RT: ionization chambers



Which solutions for ion recombination at UHDRs?

- Still using ionization chambers $\rightarrow k_{sat}$ to be decreased and/or properly determined

- Decreasing the gas pressure and changing the mixture (F. Di Martino et al., EJMP 2022)



A new solution for UHDP and UHDR (Flash) measurements: Theory and conceptual design of ALLS chamber

Fabio Di Martino^{a,b,d,*}, Damiano Del Sarto^b, Maria Giuseppina Bisogni^{b,c,d}, Simone Capaccioli^{b,c}, Federica Galante^e, Alessia Gasperini^{b,g}, Stefania Linsalata^a, Giulia Mariani^e, Matteo Pacitti^e, Fabiola Païar^{b,d,h}, Stefano Ursino^{b,d,h}, Verdi Vanreusel^{f,g}, Dirk Verellen^{f,g}, Giuseppe Felici^e

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^b Centro Pisano ricerca e implementazione clinica Flash Radiotherapy (CPFR@CISUP), Presidio S. Chiara, ed. 18 via Roma 67, Pisa, Italy

^c Department of Physics, University of Pisa, Largo B. Pontecorvo 3, I-57127 Pisa, Italy

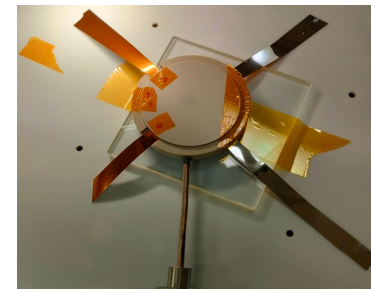
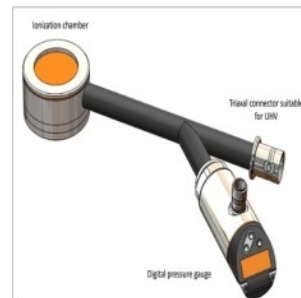
^d INFN, Sezione di Pisa, Largo B. Pontecorvo 3, I-57127 Pisa, Italy

^e SIT S.p.A., via del Commercio 1A, Aprilia (LT), Italy

^f Iridium Kanikerwerk, 2610 Antwerp, Belgium

^g Antwerp University, Faculty of Medicine and Health Sciences, 2610 Antwerp, Belgium

^h Radiation Oncology Unit, Department of Translational Research, University of Pisa, Pisa, Italy



Possible dosimetric approaches for FLASH RT: calorimeters



Dosimeter	Real time	In vivo dosimetry	Absolute/reference dosimetry	Beam monitoring	Spatial resolution	Temporal resolution	2D dosimetry	Accuracy at conventional dose rates ^a	Other considerations
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Scintillator	Yes	Yes	Potentially	Potentially	Sub-mm to mm	ns to μ s	Array and sheet	3%–5%	Quenching in high LET fields, Cherenkov radiation
Gas scintillator	Yes	No	No	Yes	Sub-mm	N/A	Yes	1%	Beam centroid measurement
Calorimeter	Yes	No	Yes	No	cm to several mm	ms–10 ms	No	<1% at the primary standard level	Bulky, not easy to use, correction factors, time consuming
Film	No ^b	Yes	Potentially	No	Tens of μ m	N/A	Yes	3%–5%	Quenching in high LET fields
Fricke	No	No	Yes	No	cm to sub-mm	N/A	Potentially	<1% at primary standard level	Time consuming, complexity
Faraday cup	Yes (for charge measurements)	No	Yes	No	N/A	< μ s	No	2%–5% for commercial devices; 1%–2% for dedicated equipment ^c	Measures the total collected charge (other detectors are required for dose determination)
Nuclear track detector	No	Yes	No	No	mm; sub-mm with specialized equipment	N/A	Yes	5%–7%	Time consuming, energy dependence, LET dependence
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Integrated current transformer	Yes	Potentially	No	Yes	N/A	sub- μ s	No	<1% for charge measurements	Lack of 2D measurements, only charge measurements

Possible dosimetric approaches for FLASH RT: calorimeters → expertise of PSDLs

Charge liberated in the medium results in an energy cascade - the liberated energy ends up as heat → measured as a temperature rise

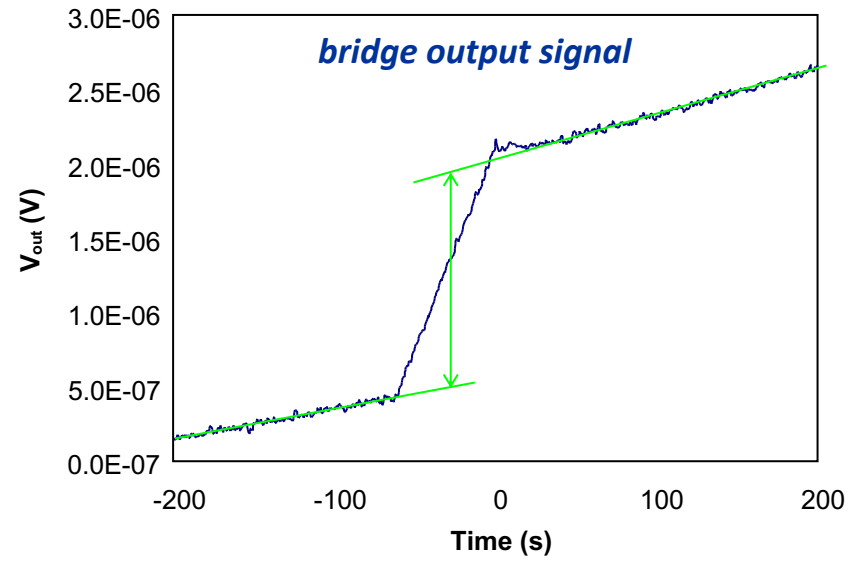
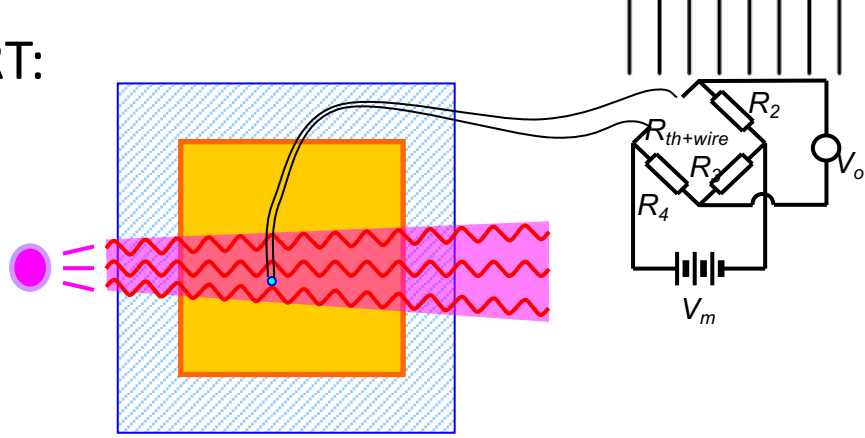
$$D_m = c_m \Delta T$$

Where c_m stands for the specific heat capacity of the material and ΔT for the temperature rise.

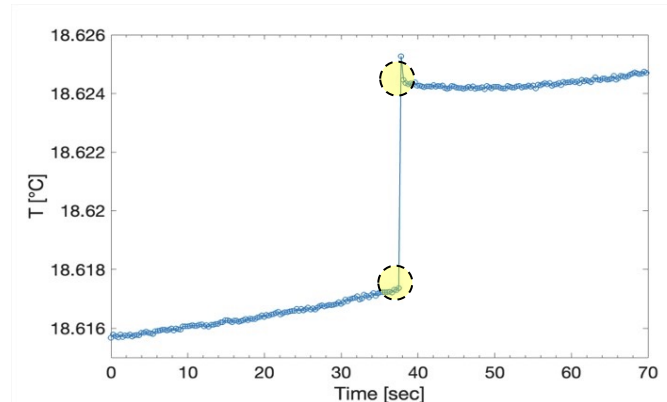
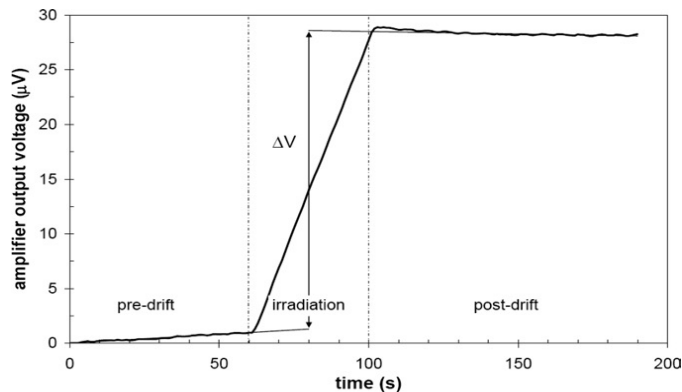
- Water calorimeters: bulky systems typically used as a primary standard for metrology
- The temperature rise of water is **very small**:

$$\Delta T (\text{water}) = 2.4 \times 10^{-4} \text{ K/Gy}$$

- **Graphite** calorimeters: higher temperature rise as respect to **water** (c_m six times smaller) → *portable!*



Possible dosimetric approaches for FLASH RT: calorimeters



Conventional Radiotherapy

FLASH Radiotherapy

A. Subiel and F. Romano, Br. J. Radiol. (2023)

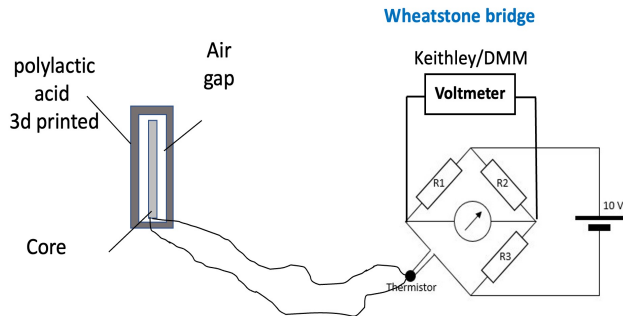
Calorimeter type	Beam & energy	Average dose rate	Dose-per-pulse	Pulse duration	Uncertainty ($k = 1$)
Transfer standard graphite calorimeter	200 MeV electrons	0.2–50 Gy/s	0.03–5.3 Gy/pulse	Approx. 100 ns	1.2% (no uncert. budget)
Small portable graphite calorimeter	15–40 MeV laser-driven protons	10^9 Gy/s (one ps pulse delivered)	1–3 Gy/pulse	Approx. ns	Not stated
Aluminium calorimeter*	50 MeV electrons	1–9 Gy/s	0.2–1.8 Gy/pulse	2.5 μ s	0.5% (no uncert. budget)
Aerrow graphite calorimeter*	20 MeV electrons	3–28 Gy/s	0.6–5.6 Gy/pulse	2.5 μ s	1.06 %
Al-core secondary standard calorimeter	6 MeV electrons	180 Gy/s	Approx. 0.45 Gy/s	4 μ s	1.25%

References

- McManus et al. Scientific Reports (2020)
- H. Palmans et al. PMB (2009)
- F. Romano et al. Journal of Physics (2020)
- A. Bourguin, Frontiers in Physics (2020)
- A. Bourguin, Med. Phys. (2022)
- G. Bass et al., Br. J. Radiol. (2023)

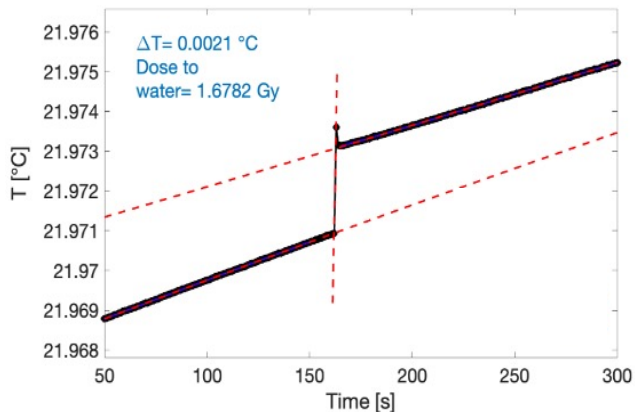


Secondary standard calorimeter

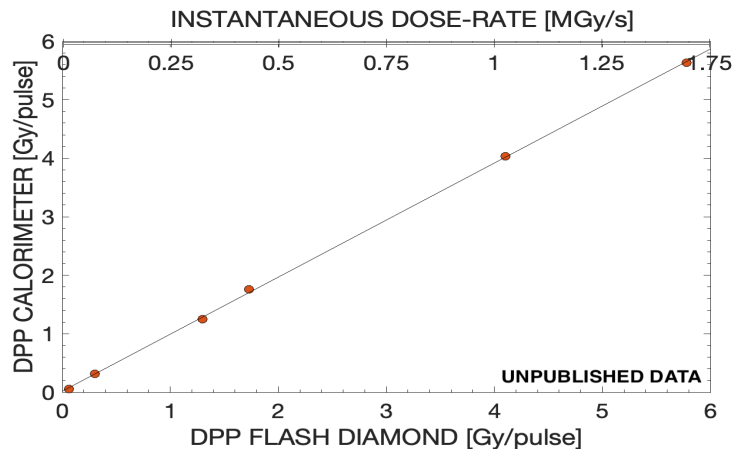


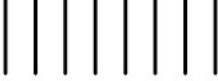
- Developed by NPL
- Simple usage and low cost
- 2 mm graphite core
- 1 single termistor connected to the Wheatstone bridge to measure the temperature increase
- IBA PPC05 ion chamber geometry (same holders)
- Tested at CPFR in Pisa (SIT e_FLASH linac)

SINGLE PULSE TEMPERATURE RISE

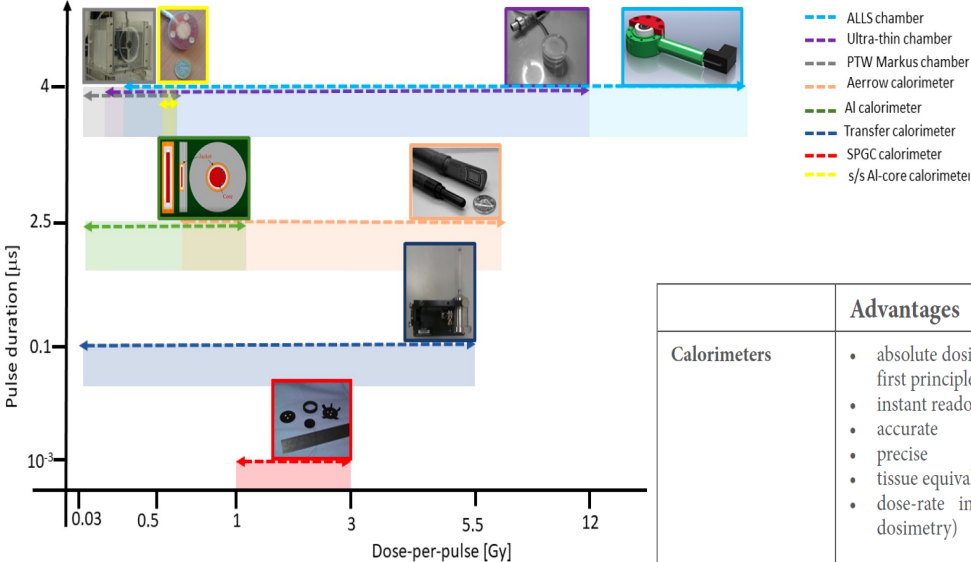


App 100-40, pulse length= 4 us





Possible dosimetric approaches for FLASH RT: calorimeters vs ion chambers



A. Subiel and F. Romano, Br. J. Radiol. (2023)

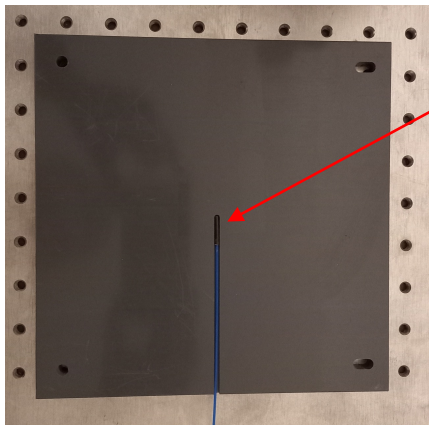
	Advantages	Disadvantages
Calorimeters	<ul style="list-style-type: none"> absolute dosimeter (absorbed dose determination from first principles) instant readout accurate precise tissue equivalence (water and graphite calorimeters) dose-rate independent detector (ideal for UHDR dosimetry) 	<ul style="list-style-type: none"> typically complex devices normally used in primary standard laboratories require post-processing to retrieve the absorbed dose several correction factors required conversion to dose to water required for non-water calorimeters low sensitivity (for water calorimeters) expensive devices (particularly when maintained as a primary standard)
Ionization chambers	<ul style="list-style-type: none"> simplicity easy operation instant readout precise recommended by international protocols for beam calibration long-term usage for radiation dosimetry in radiotherapy less expensive than calorimeters 	<ul style="list-style-type: none"> require calibration for determination of absorbed dose low density medium high voltage supply required from associated electrometer require many correction factors significant ion recombination effects in high dose-per-pulse beams

Possible dosimetric approaches for FLASH RT: scintillators



Dosimeter	Real time	In vivo dosimetry	Absolute/reference dosimetry	Beam monitoring	Spatial resolution	Temporal resolution	2D dosimetry	Accuracy at conventional dose rates ^a	Other considerations
Ion chamber	Yes	No	Yes	Yes	Several mm	10–200 μ s	Array	1%–2%	Significant ion recombination at UHDRs
Semiconductor	Yes	Yes	No	Yes	Sub-mm (or μ m)	1–10 ns	Yes	2%–5%	Angular dependency, radiation damage, LET dependence
TLD	No	Yes	Yes	No	Several mm	N/A	No	3%–10%	Energy dependence, time consuming, LET dependence
OSLD	No	Yes	Yes	No	Sub-mm to mm	N/A	Array	3%–5%	Energy dependence, quenching in high LET fields
Scintillator	Yes	Yes	Potentially	Potentially	Sub-mm to mm	ns to μ s	Array and sheet	3%–5%	Quenching in high LET fields, Cherenkov radiation
Gas scintillator	Yes	No	No	Yes	Sub-mm	N/A	Yes	1%	Beam centroid measurement
Calorimeter	Yes	No	Yes	No	cm to several mm	ms–10 ms	No	<1% at the primary standard level	Bulky, not easy to use, correction factors, time consuming
Film	No ^b	Yes	Potentially	No	Tens of μ m	N/A	Yes	3%–5%	Quenching in high LET fields
Fricke	No	No	Yes	No	cm to sub-mm	N/A	Potentially	<1% at primary standard level	Time consuming, complexity
Faraday cup	Yes (for charge measurements)	No	Yes	No	N/A	< μ s	No	2%–5% for commercial devices; 1%–2% for dedicated equipment ^c	Measures the total collected charge (other detectors are required for dose determination)
Nuclear track detector	No	Yes	No	No	mm; sub-mm with specialized equipment	N/A	Yes	5%–7%	Time consuming, energy dependence, LET dependence
Alanine	No	Yes	Yes	No	mm	N/A	No	2%–7% for doses larger than 10 Gy	Decreased accuracy for doses less than 10 Gy (minimum 2 Gy)
Integrated current transformer	Yes	Potentially	No	Yes	N/A	sub- μ s	No	<1% for charge measurements	Lack of 2D measurements, only charge measurements

Scintillators

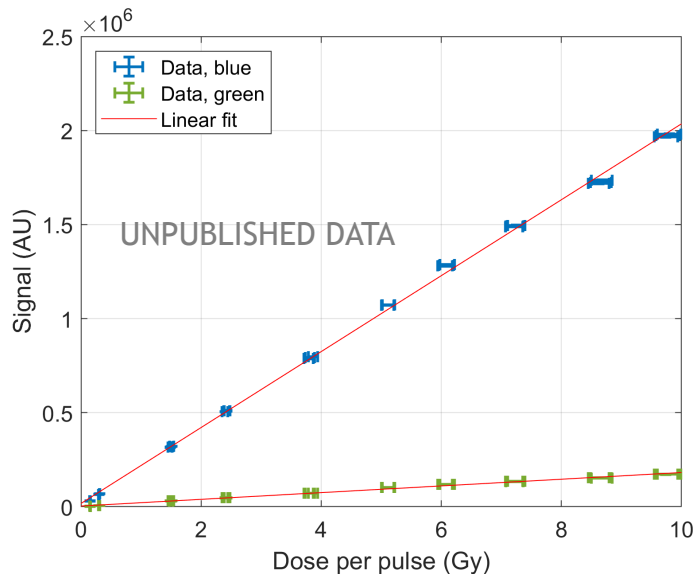


Plastic scintillator fiber
(d = 1 mm)



- **Plastic scintillators:**
- ✓ Minimal to no saturation at high dose per pulse (DPP) and dose rates
- ✓ Water and tissue-equivalent
- ✓ Allow sampling the pulse time structure
- ✓ **Fibers:** compact, easy-to-use, cost-effective, real-time detector prototypes for precise local dose measurements

UHDR e- beams



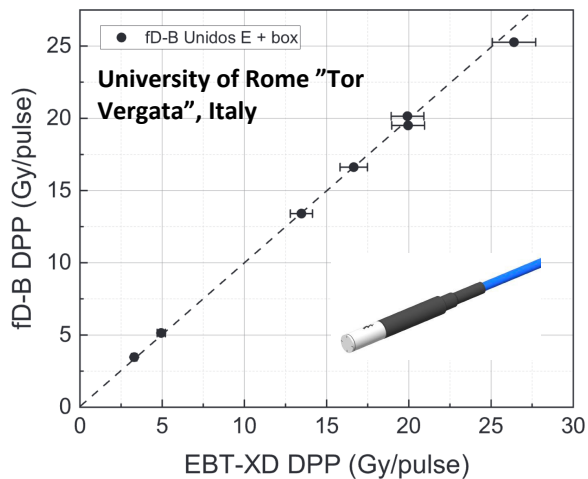
Possible dosimetric approaches for FLASH RT: semiconductors



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Semiconductor	Yes	Yes	No	Yes	Sub-mm (or μ m)	1–10 ns	Yes	2%–5%	Angular dependency, radiation damage, LET dependence
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Scintillator	Yes	Yes	Potentially	Potentially	Sub-mm to mm	ns to μ s	Array and sheet	3%–5%	Quenching in high LET fields, Cherenkov radiation
Gas scintillator	Yes	No	No	Yes	Sub-mm	N/A	Yes	1%	Beam centroid measurement
Calorimeter	Yes	No	Yes	No	cm to several mm	ms–10 ms	No	<1% at the primary standard level	Bulky, not easy to use, correction factors, time consuming
Film	No ^b	Yes	Potentially	No	Tens of μ m	N/A	Yes	3%–5%	Quenching in high LET fields
Fricke	No	No	Yes	No	cm to sub-mm	N/A	Potentially	<1% at primary standard level	Time consuming, complexity
Faraday cup	Yes (for charge measurements)	No	Yes	No	N/A	< μ s	No	2%–5% for commercial devices; 1%–2% for dedicated equipment ^c	Measures the total collected charge (other detectors are required for dose determination)
Nuclear track detector	No	Yes	No	No	mm; sub-mm with specialized equipment	N/A	Yes	5%–7%	Time consuming, energy dependence, LET dependence
Alanine	No	Yes	Yes	No	mm	N/A	No	2%–7% for doses larger than 10 Gy	Decreased accuracy for doses less than 10 Gy (minimum 2 Gy)
Integrated current transformer	Yes	Potentially	No	Yes	N/A	sub- μ s	No	<1% for charge measurements	Lack of 2D measurements, only charge measurements

Solid state detectors: semiconductors

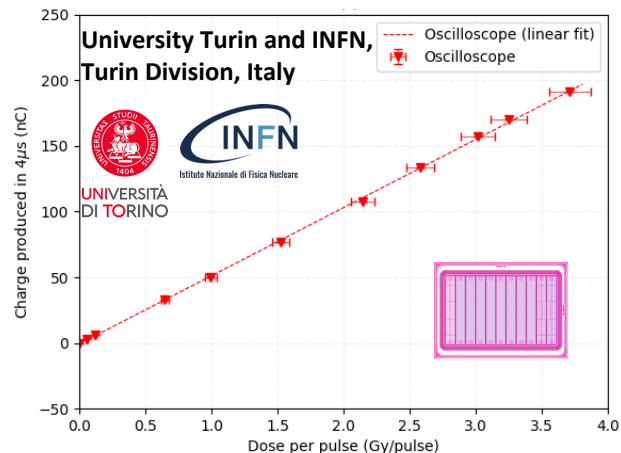
Diamond detectors (FLASH diamond)



M. Marinelli *et al.* Med. Phys. (2022)
G. Verona Rinati *et al.* Med. Phys. (2022)

- Linear response at UHDR
- Good stability (long-term response stability?)
- High spatial resolution (< 1 mm)
- Water equivalent
- Commercialized by PTW

Silicon detectors



- More mature technology
- Linear response at UHDR
- Good stability (long-term response stability?)
- High spatial resolution (< 500 µm)
- Pixellated and strip geometries

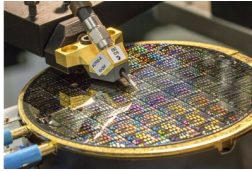


FRIDA

Silicon carbide detectors for dosimetry and monitoring



Silicon



+

Diamond



SiC

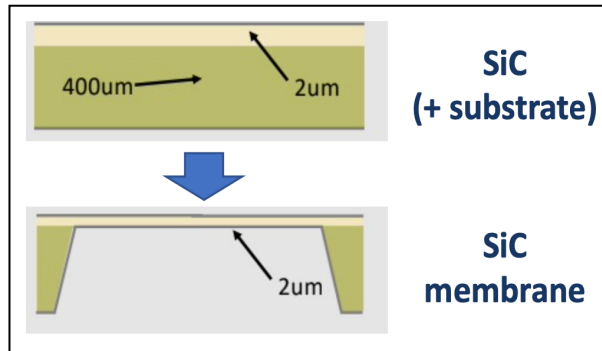
Radiation hardness
High signal to noise ratio
High time resolution (ns) and fast collection time
Large area devices

Standard with bulk devices



Freestanding membranes

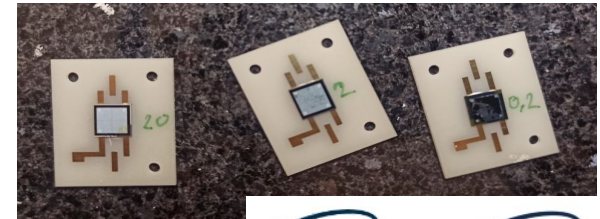
5x5 mm² 10x10 mm² 2x2 mm²



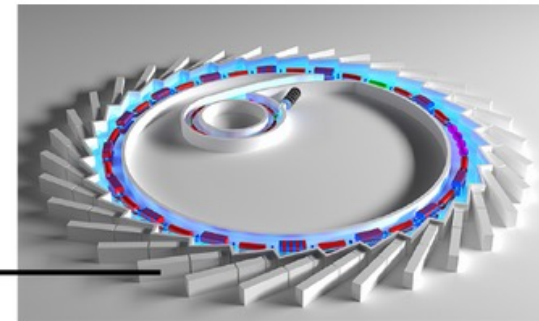
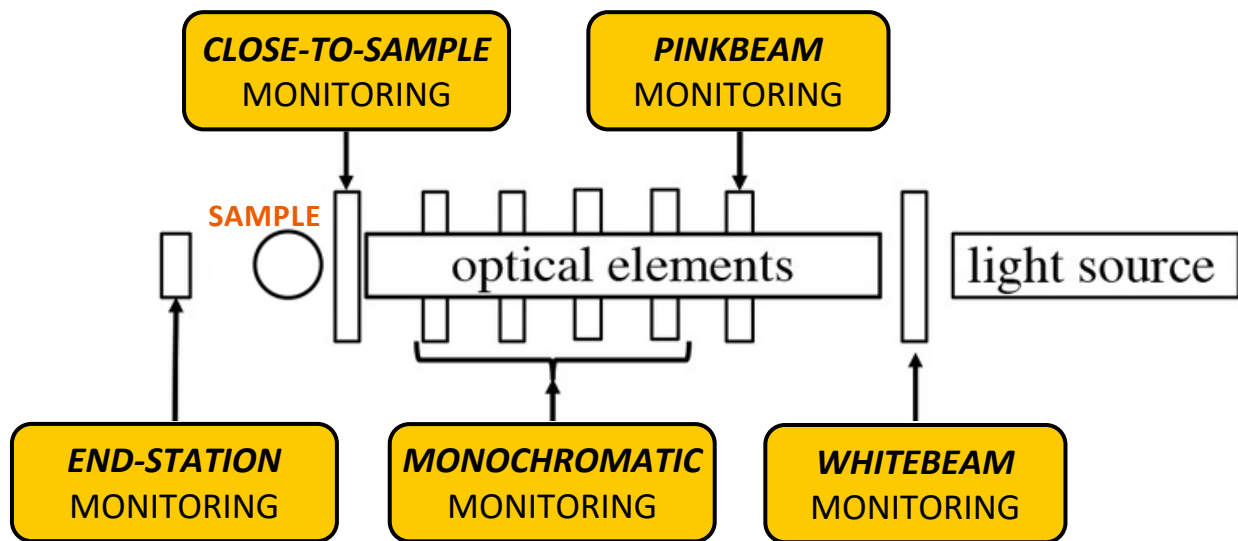
20um

2um

0.2um



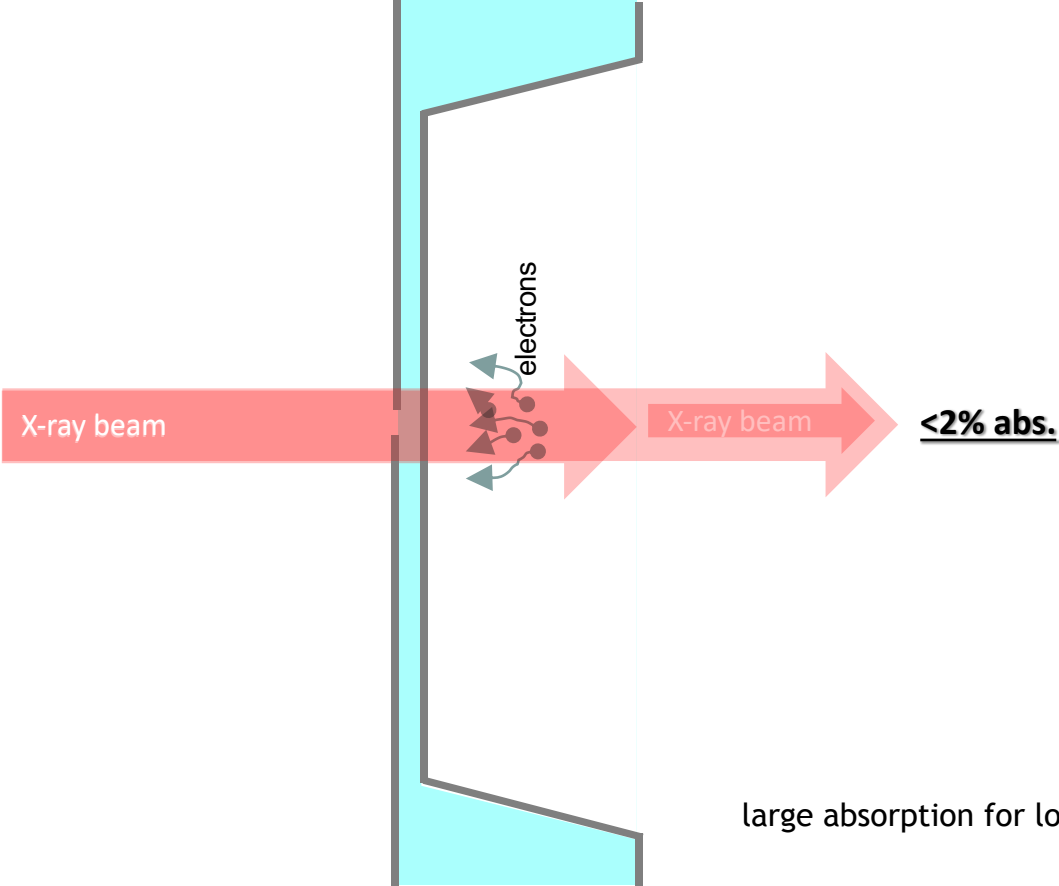
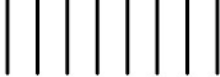
Generalities of Synchrotron Beam monitoring



Main requirements

- transparency (>98%)
- stability over time
- good lateral resolution (<um)
- fast response (<ms, <us)
- large active areas (mm²)

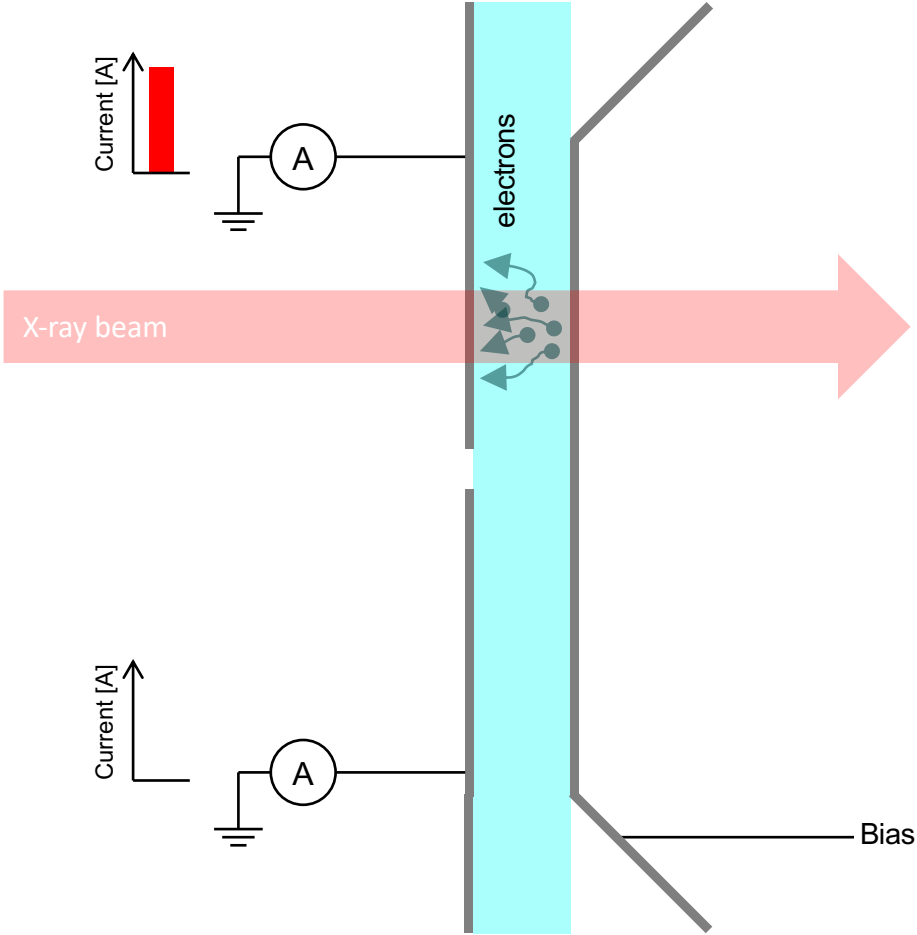
Standard "thin-membrane" solid state XBPM



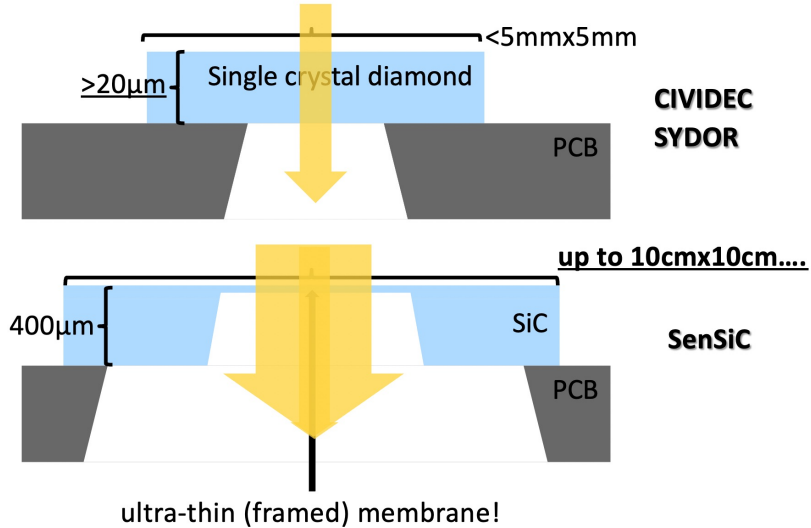
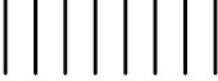
no information on beam position

large absorption for low energy X-rays

Standard "thin-membrane" XBPM

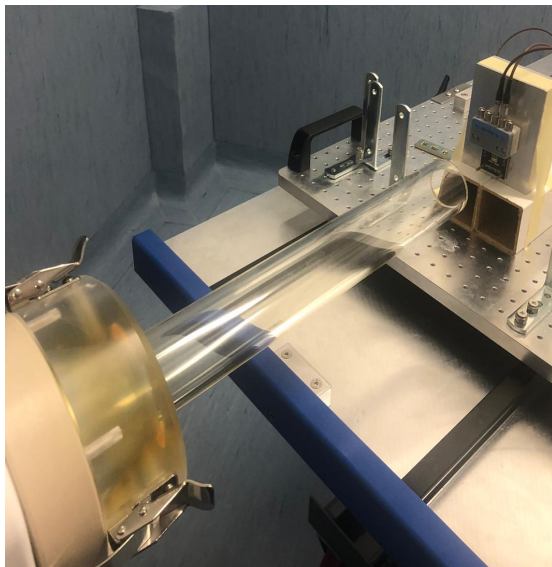


Why choose Silicon Carbide XBPMs?

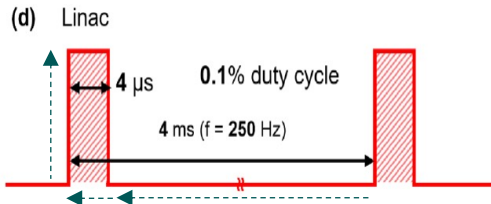


- Lower device costs
- Larger active areas (up to x9 time higher)
- Higher current signals / higher resolutions*
- Superior transparencies ($20\mu\text{m}$, $2\mu\text{m}$, $1\mu\text{m}$, $0.2\mu\text{m}$)
- easier installations:
 - zero bias operation
- Large number of devices quickly available

Characterization with Electron FLASH Linac accelerator @ CPFR

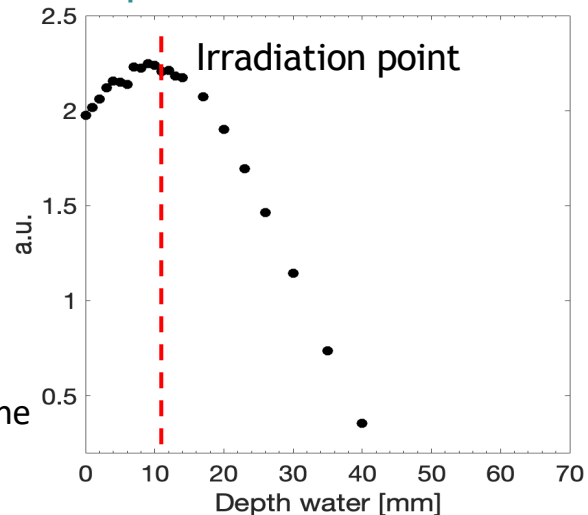


F. Romano *et al.* Med. Phys. (2022)



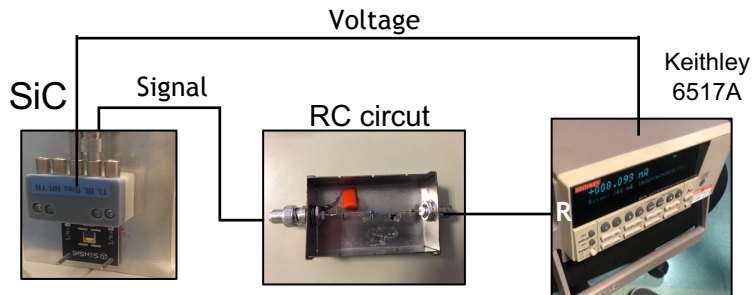
- $E = 9$ MeV
- **Single pulse duration: 0-5-4 μ s**
- PRF: 1-245 Hz
- **Dose per pulse: from 0.1-20 Gy**
- Average instantaneous dose rates in the single pulse up to **5 MGy/s**

Depth dose distribution with SiC



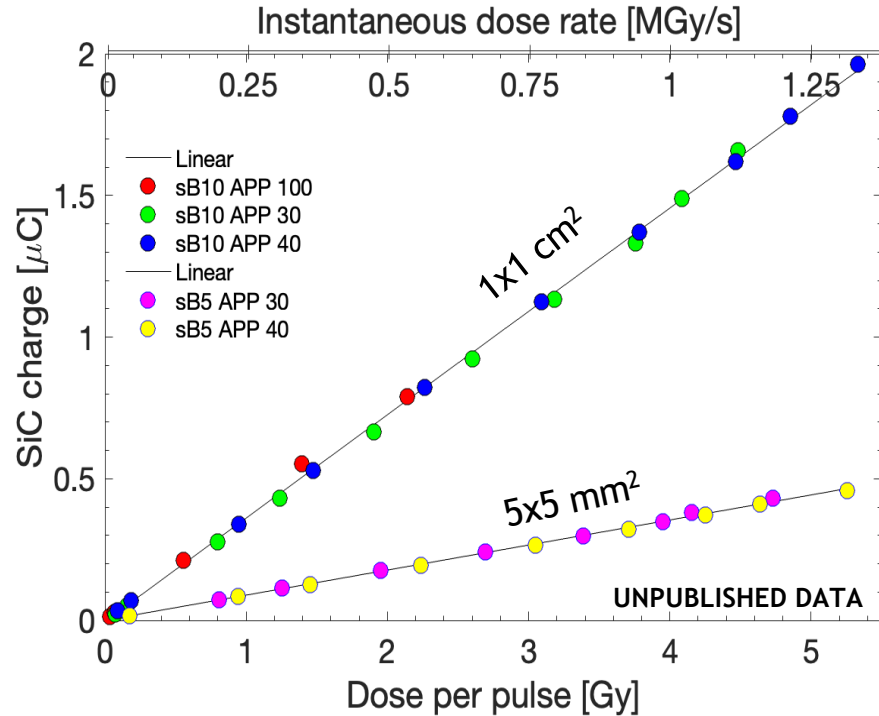
Experimental setup

- 10x10, 5x5, 3 mm² 10 μ m thick SiC with and without the substrate placed at the build-up connected to a Keithley electrometer
- Alanine dosimeters at the build-up
- **30,40,100 Applicator and Open Field**
- RC circuit connected to the detector

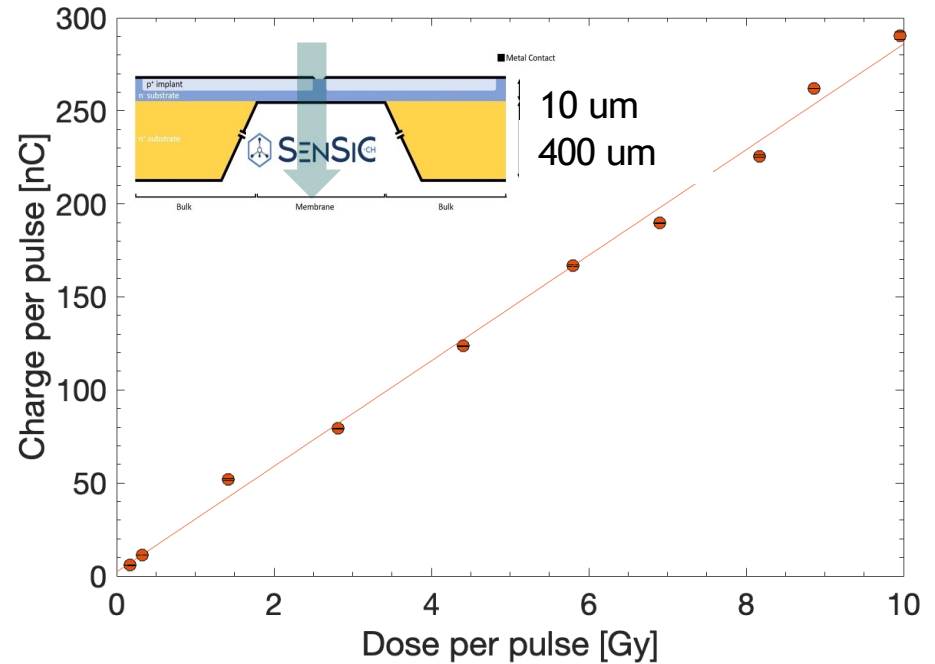


Independence with the instantaneous dose rate and dose per pulse

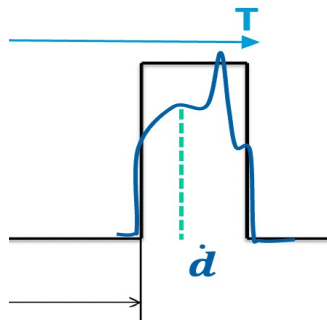
1x1 cm²- 5x5 mm² Bias Voltage: 200 V



10 μm thick free-standing membrane

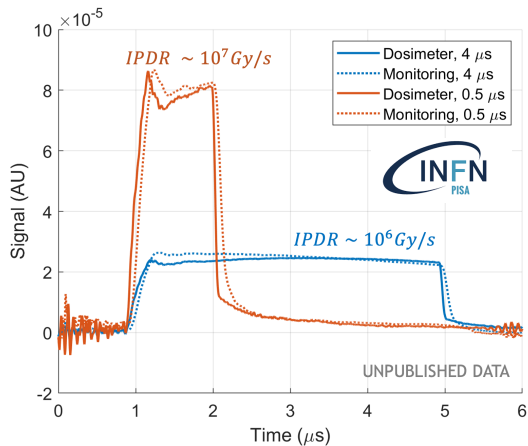


Instantaneous dose rate measurements for FLASH?

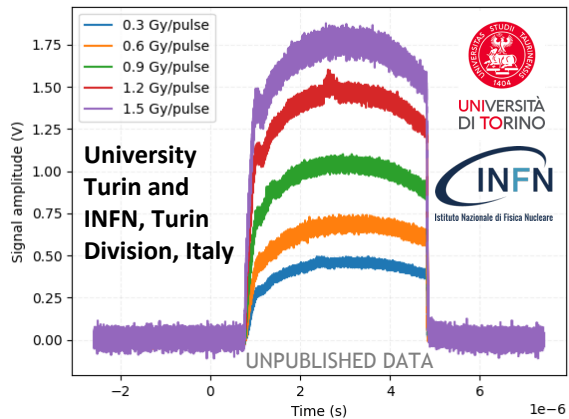


Temporal resolution from 1 to tens of ns,
allowing for "intra-pulse" instantaneous dose
rate measurements

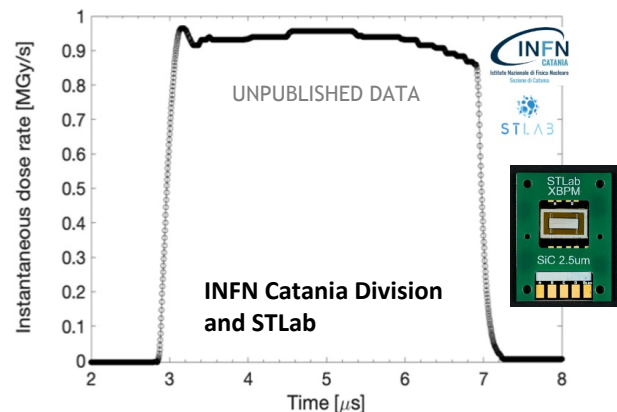
Scintillators



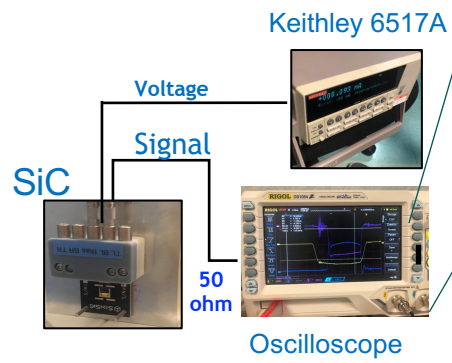
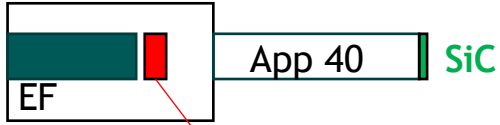
Silicon detectors



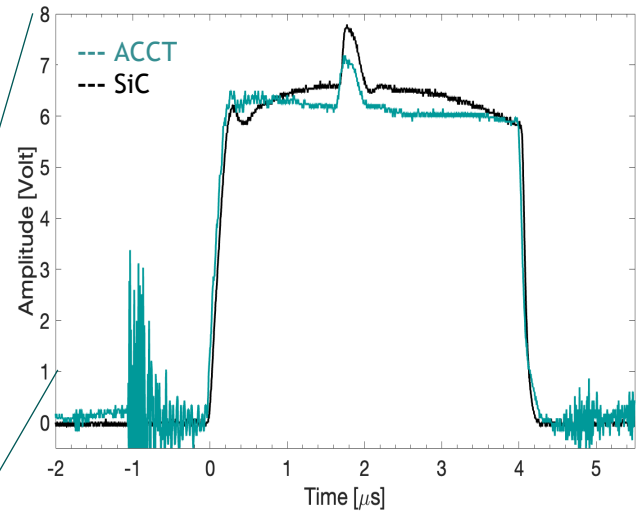
Silicon carbide (SiC)



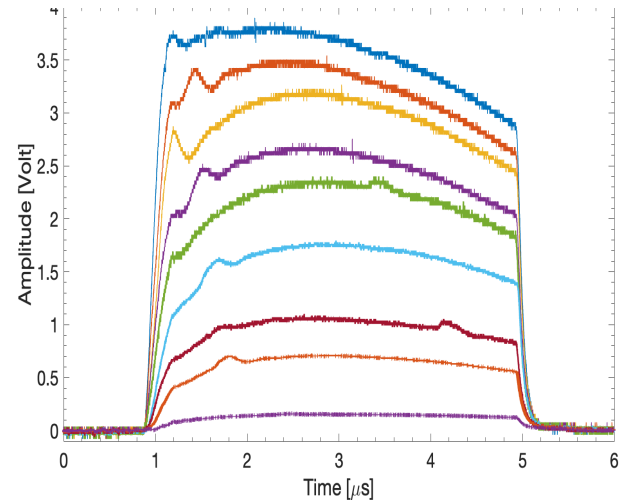
Measurements of the intra-pulse instantaneous dose rate with SiC



Single pulse real time current waveform



Instantaneous dose rate variation at irradiation point



- **Sensitivity** to fast variation in the beam current and energy spectrum during the pulse at the irradiation point
- Provided with the **dose calibration** the SiC detectors measure real-time the intra-pulse instantaneous dose-rate opening the possibility to monitor the single pulse delivery of the dose

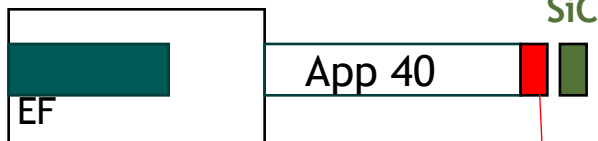
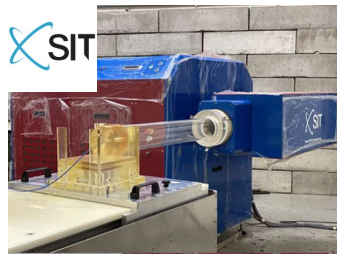
Real-time beam monitoring (@ SIT in Aprilia)



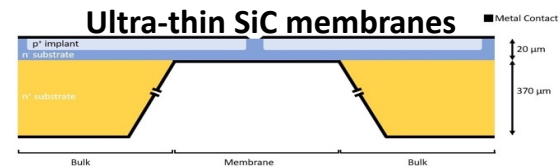
- Fast signals
- High temporal resolution
- Low beam perturbation

For UHDR **electron** beams in transmission ion chambers cannot be used → new approaches!

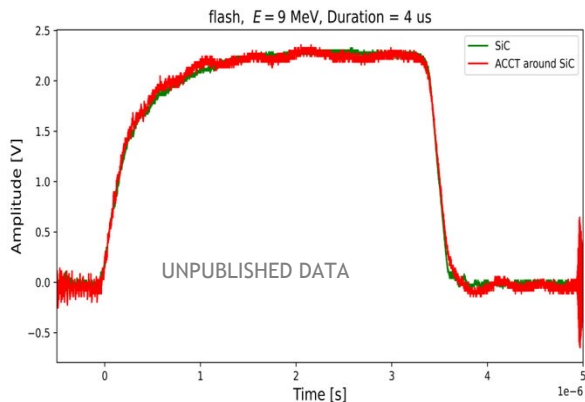
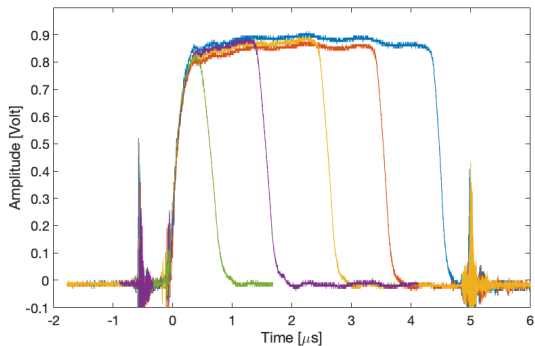
bergoz
INSTRUMENTATION

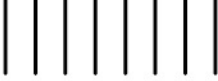


ACCT



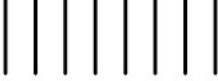
ACCT (AC current transformer)
(no position sensitive)





Summary and conclusions

- Radiochromic films to assess 2D dose distributions and alanine dose rate independent but passive detectors
- Ionization chambers still reference dosimeters for routine beam calibration measurements?
- Small portable calorimeters as an alternative reference instrument?
- Alternative dosimetric approaches with scintillators, silicon, diamond and SiC detectors
- Real-time beam monitoring additional challenges
- 2D configurations for both real-time beam monitoring and dosimetry to be developed in the perspective of a clinical translation of FLASH radiotherapy



Thank you for your attention

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G. Milluzzo (INFN-CT), M. Camarda (STLab), N. Amato (STLab), S. Both (UMCG), A. Gerbershagen (UMCG), M.-J. van Goethem (UMCG), S. Brandenburg (UMCG), F. Di Martino (CPFR), J. Pensavalle (SIT), L. Masturzo (SIT), G. Felici (SIT), S. McCallum (QUB), M. McManus (NPL), A. Vignati (INFN-TO), E. Medina (INFN-TO), G. Bisogni (INFN-PI), E. Ciarrocchi (INFN-PI), A. Subiel (NPL), R. Thomas (NPL), H. Palmans (NPL)