

Alghero Geant4 Summer School









Geant4 Monte Carlo simulations for the design of new imaging devices: MediPROBE4 and T4-QCT

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8 giugno 2023

Geant4 based optimization for semiconductor hybrid pixel detector for nuclear medicine imaging

A **portable gamma camera** is a small, light-weight gamma ray detector that can be used for pre- and intra-operative clinical procedures, tipically with Tc-99m radiotracers

→ sentinel lymph node scintigraphy







Hybrid pixel detectors Semiconductor sensor bump-bonded to a readout chip.

MediPROBE2 (2011)

<u>Medipix2 ASIC (256 x 256 pixels, 55 µm pitch).</u> 1-mm-thick <u>CdTe sensor</u> (sensitive area 1.98 cm²). Readout mode: frame based (Imaging). <u>FOV</u>: 40 x 40 mm² at 50-mm skin-to-collimator distance. <u>Spatial Resolution</u>: 5.5 mm FWHM (0.94 mm pinhole) at 50-mm skin-to-collimator distance.

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Geant4 based optimization for semiconductor hybrid pixel detector for nuclear medicine imaging

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 \rightarrow sentinel lymph node scintigraphy





Image of two lymph nodes acquired with MediPROBE2 (pinhole 0.94 mm aperture)

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MediPROBE4 (2022) with <u>Timepix4</u>

<u>Timepix4 ASIC</u> (448 x 512 pixels, 55 µm pitch). 0.3-mm-thick <u>Si sensor</u> (sensitive area 6.93 cm²). Readout modes: Frame based + Data Driven (tracking). Coupled to a Coded Aperture (CA) collimator.



With CA mask, from 2D data, one can obtain a 3D reconstruction of the emitting object (through a deconvolution algorithm).

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Monte Carlo simulations with Geant4



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Laboratory tests with Timepix4

Spectral imaging of radioactive sources (Timepix4 coupled to a coded aperture collimator)

- Timepix4v1 bump bonded with a **300 µm Silicon** sensor
- Spidr4 hardware and in-house software (Nikhef)
- Coded aperture collimator physically available at the lab (NTHN MURA mask, rank 31, 0.08 mm holes, 0.110 mm thickness)
- Radioactive source: Ba-133 (0.6 mm diameter)

Geant4 simulations

Imaging of a monoenergetic source taking into account interactions inside the sensor.

- **300 µm Silicon** sensor (energy deposition in the sensor are computed each 10µm along the ionization track)
- Coded aperture collimator (NTHN MURA mask, rank 31, 0.08 mm holes, 0.110 mm thickness)
- Monoenergetic source 30.85 keV (planar round source, 0.6 mm, placed at 5mm from the FOV center)



Experimental test CNR = 36

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Comparison between MC simulation and 100 experimental test for a ¹³³Ba source @63 mm from the collimator 80 60 **Pixel value** 40 MC simulation 20 Exp Test (clean) 0 --20 6 8 10 12 14 16 18

Position along the line profile (mm)

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Laura A. Cerbone

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Moving to a new project...

T4-QCT

A spectral quantitative photon counting CT for the assessment of bone density losses



High-Resolution peripheral quantitative CT (HR-pQCT)

Capable of resolving the micrometric trabecular structure of bones (≈50 µm)

Analyzed Wrist (Radius) anatomical Ankle (Tibia) compartments Heel

Commercially available HR-pQCT

- Isotropic spatial resolution $\approx 60 \ \mu m$
- Cone beam (scan time 2-4 minutes)
- 4 µSv effective dose to patient per scan (9 mm scan lenght, 12 cm FOV)
- \approx 600 kg (NOT portable, of course)



Osteoporotic



3D image of the radius of a 68 years old patient obtained with a commercial HR-pQCT

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Spectral quantitative CT for the assessment of bone density losses

Our purpose is to realize the first prototype of a spectral (color) CT scanner using the Timepix4 read-out ASIC and a microfocus x-tay tube, for bone densitometry by scanning peripheral parts of the body (wrist, tibia, fingers).

The patient will insert one limb inside the bore using a 3D-printed holder for the forearm or the leg (not shown).



I4-QC

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Spectral quantitative CT for the assessment of bone density losses ^{10/12}

- Isotropic high spatial resolution ($\approx 60 \, \mu m$)
- Photon counting detector
- Field of View of 10-12 cm at isocenter
- Photon counting & Spectral capabilities → possibility to separate bone from soft tissue without a dual-energy scan
- Expected patient effective dose $<10 \,\mu$ Sv
- 30% 60% reduction of radiation dose with respect to energy-integrating CT



Monte Carlo simulations goals

- Reproduce the detection system: the Timepix4 hybrid pixel detector
- Establish which is the optimal geometrical configuration for the system:
 - 1. Magnification
 - 2. Extention of the sensible area (trade-off between costs and FOV)
 - 3. Spatial resolution (must be micrometric to resolve the trabeculae)
- Dose assessment











Thank you for your attention!



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