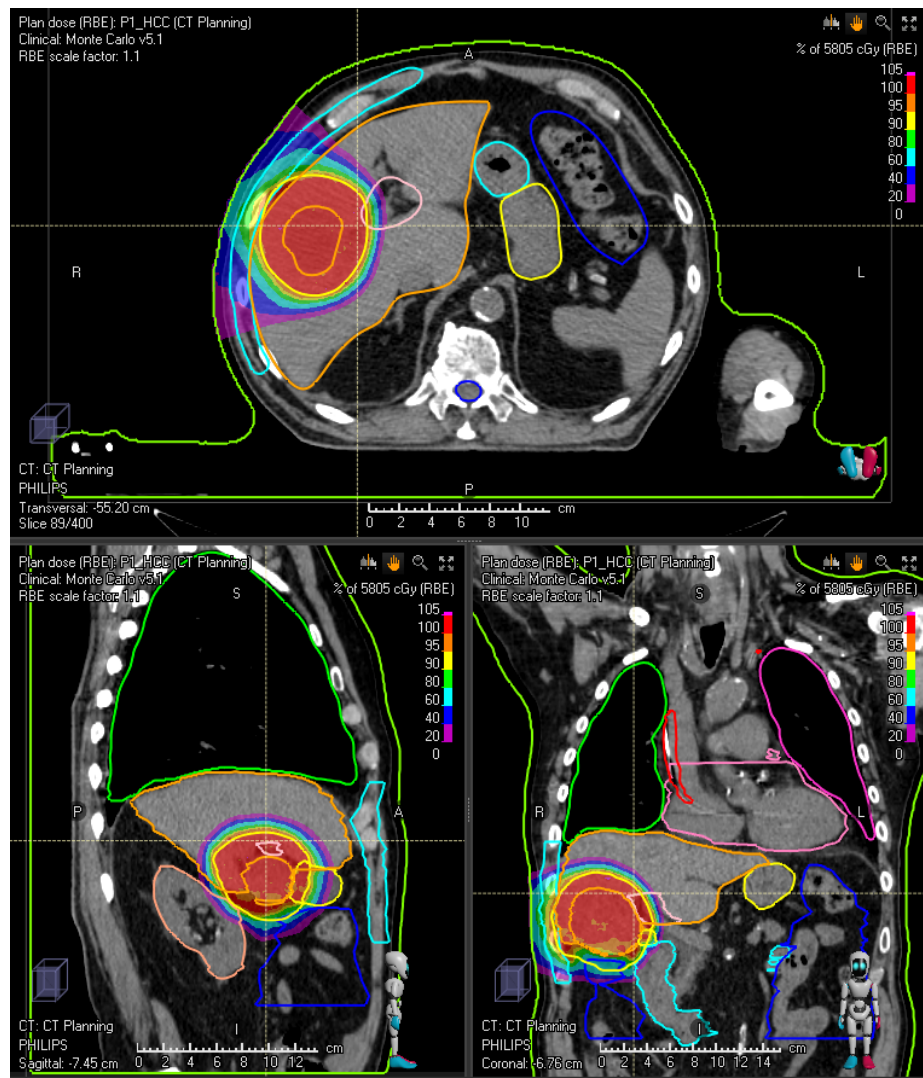


Range Modulators for proton beams

F. Tommasino
(most slides from R. Cristoforetti)

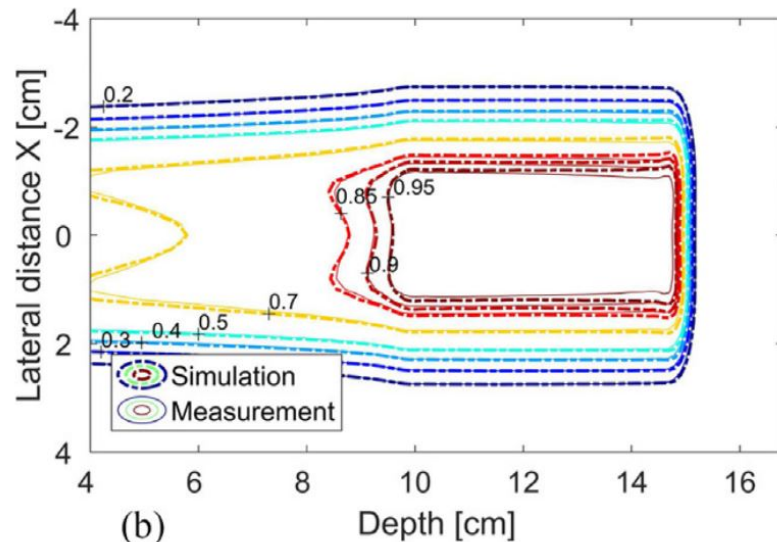
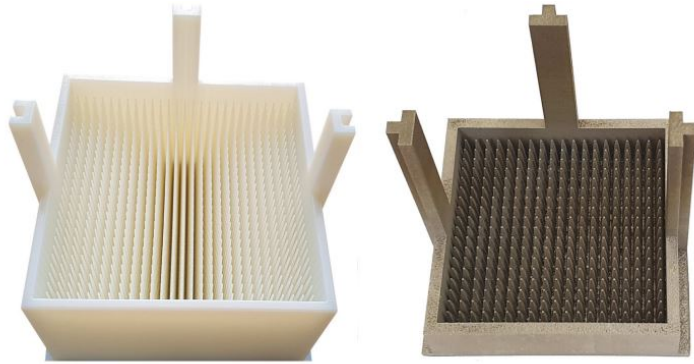
Case study: liver cancer



- Energy change requires times in the order of **seconds**
- Up to **30** energy layers per field...
- ... and more than one field
- Severely affected by **target motion**, so breath hold techniques need to be exploited

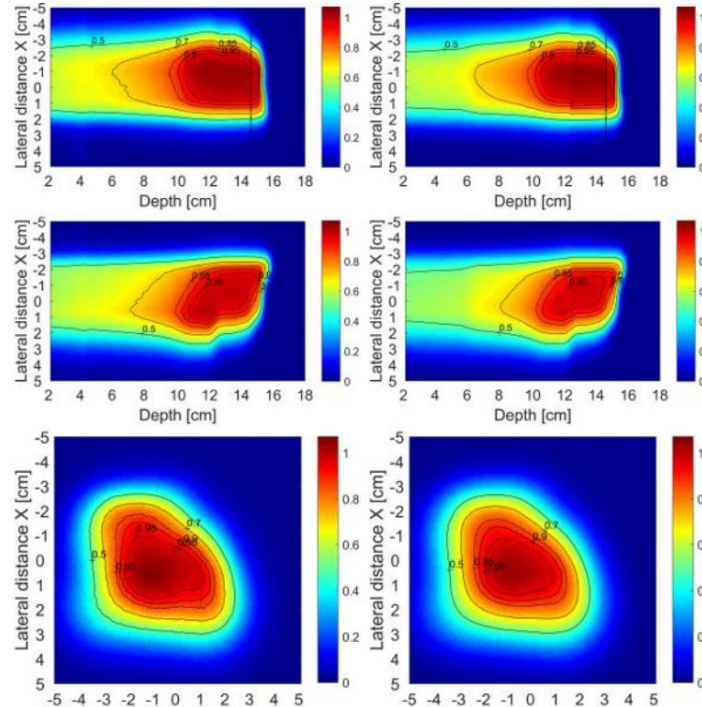
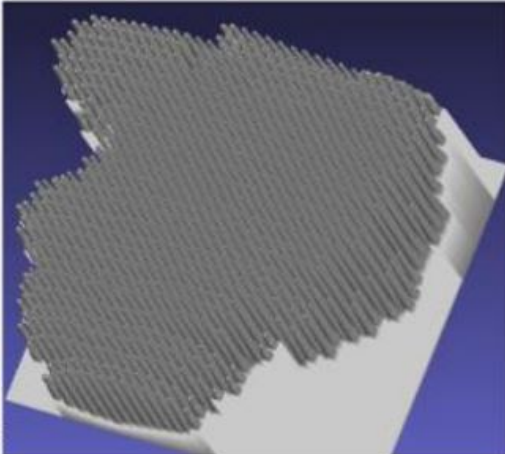
The use of Range Modulators (RMs) avoids the energy selection process

2D vs 3D Range Modulators



- Pins are all **identical**
- Dose distribution controlled only on the **depth-dose profile**
- **Not** useful for clinical applications

2D vs 3D Range Modulators

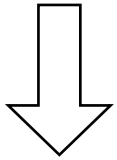


Simeonov et al. MC simulations and dose measurements of a patient-specific 3D range modulator for proton therapy.

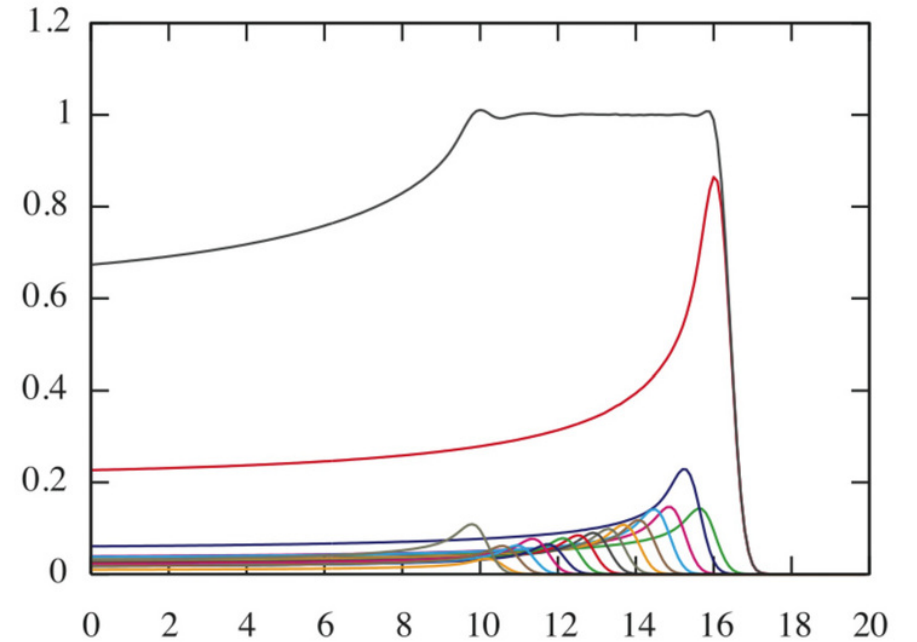
- All pins need to be **different** in order to exploit all available **degrees of freedom**
- Objective dose distribution is **conformal** to arbitrary shape
- **Scattering** becomes relevant
- Increased level of **complexity**

Numerical description

$$D_{SOBP}(i) = \sum_{j=1}^{N_s} w(j)D(i, j)$$



$$\begin{bmatrix} D[1] & \dots & D[N_s] \\ \vdots & \ddots & \vdots \\ D[N_z] & \dots & D[N_s + N_z] \end{bmatrix} \cdot \begin{bmatrix} w[1] \\ \vdots \\ w[N_s] \end{bmatrix} = \begin{bmatrix} D_{SOBP}[1] \\ \vdots \\ D_{SOBP}[N_z] \end{bmatrix}$$

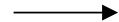


- D_{SOBP} = SOBP profile
- D = Single BP
- N_s = Number of BPs
- w = fluence weights
- N_z = Number of sampled depths

Workflow

For 2DRMs

Numerical
Optimization



Monte Carlo
Simulation

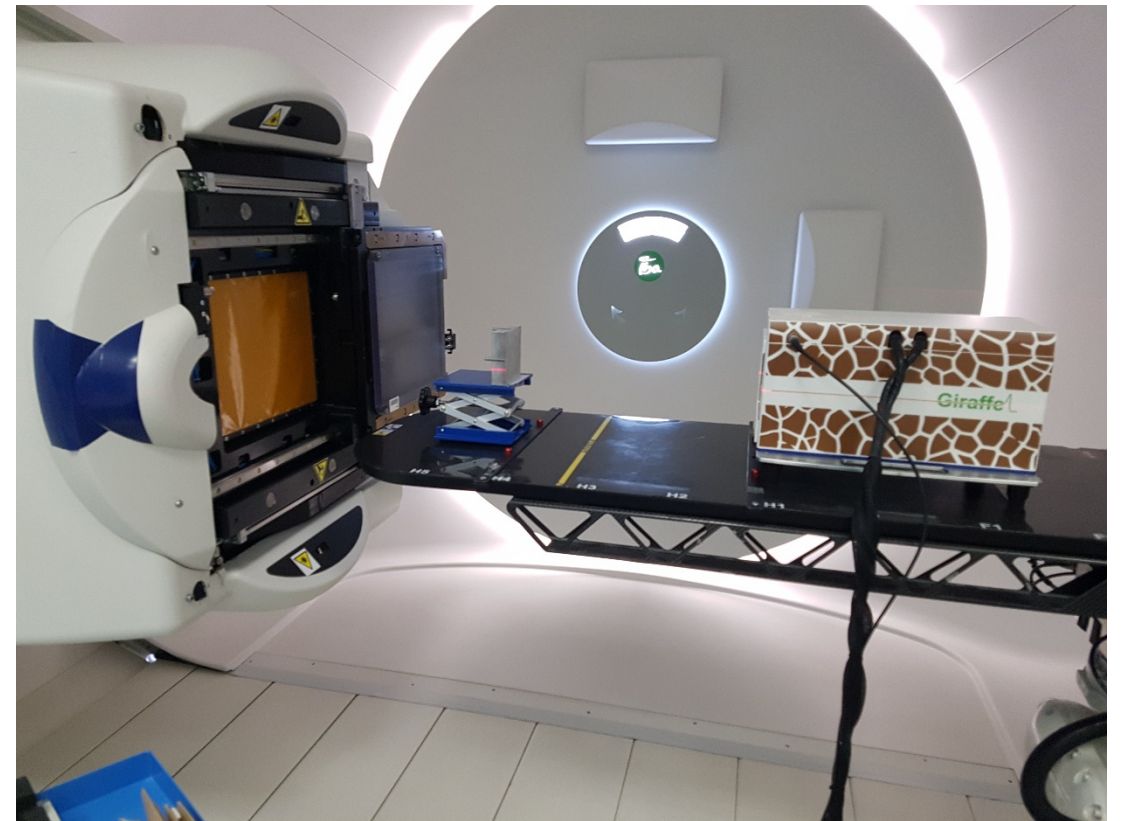
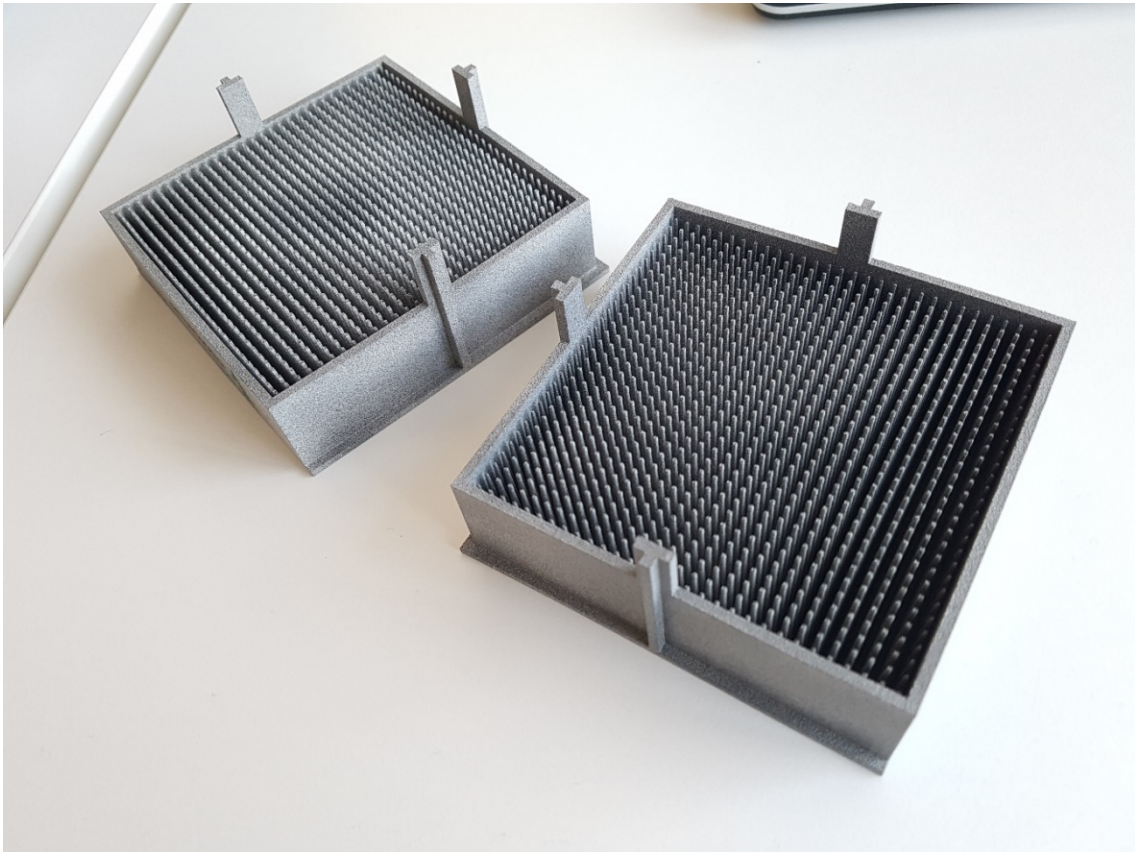


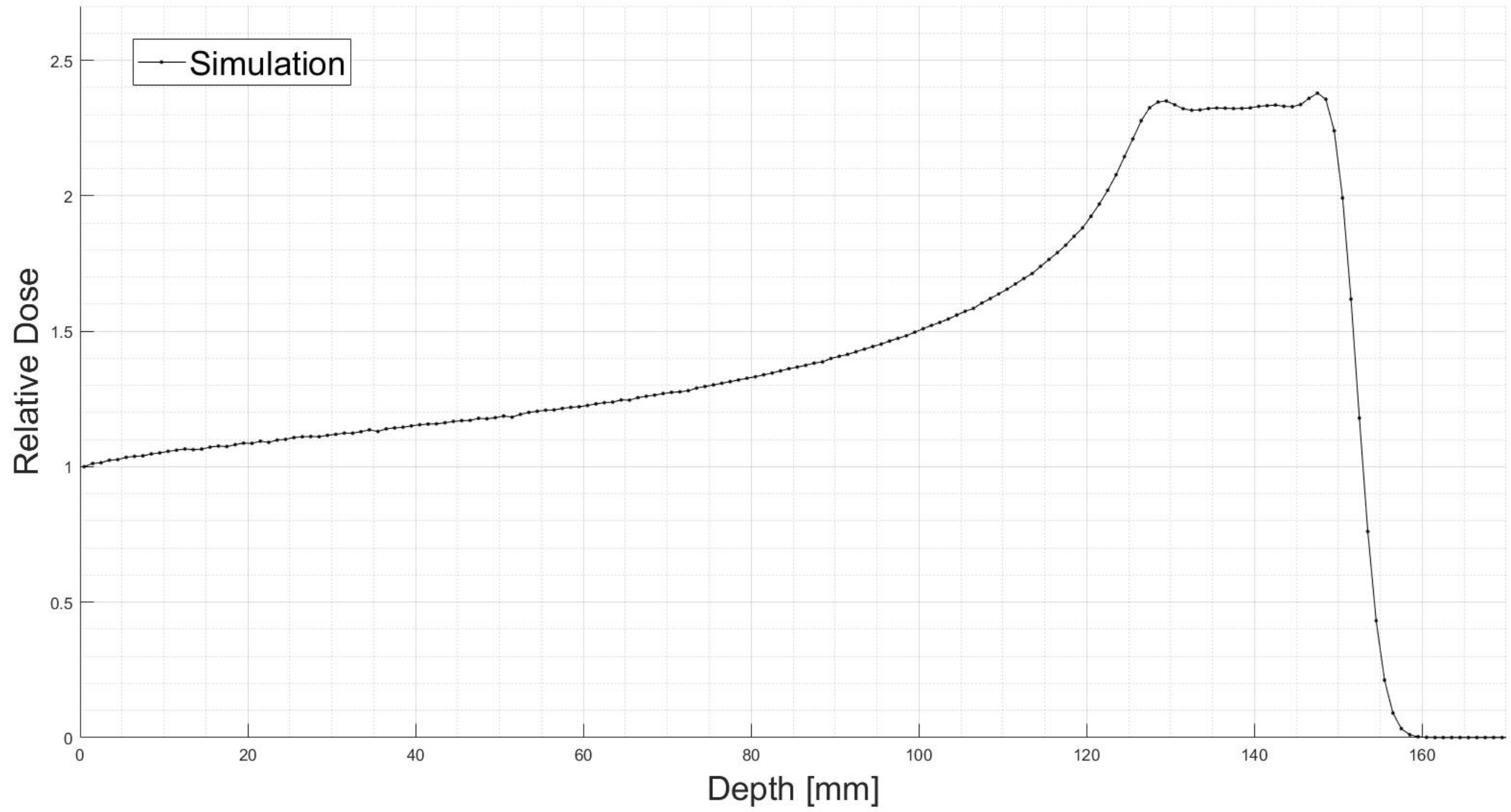
Printing & Validation

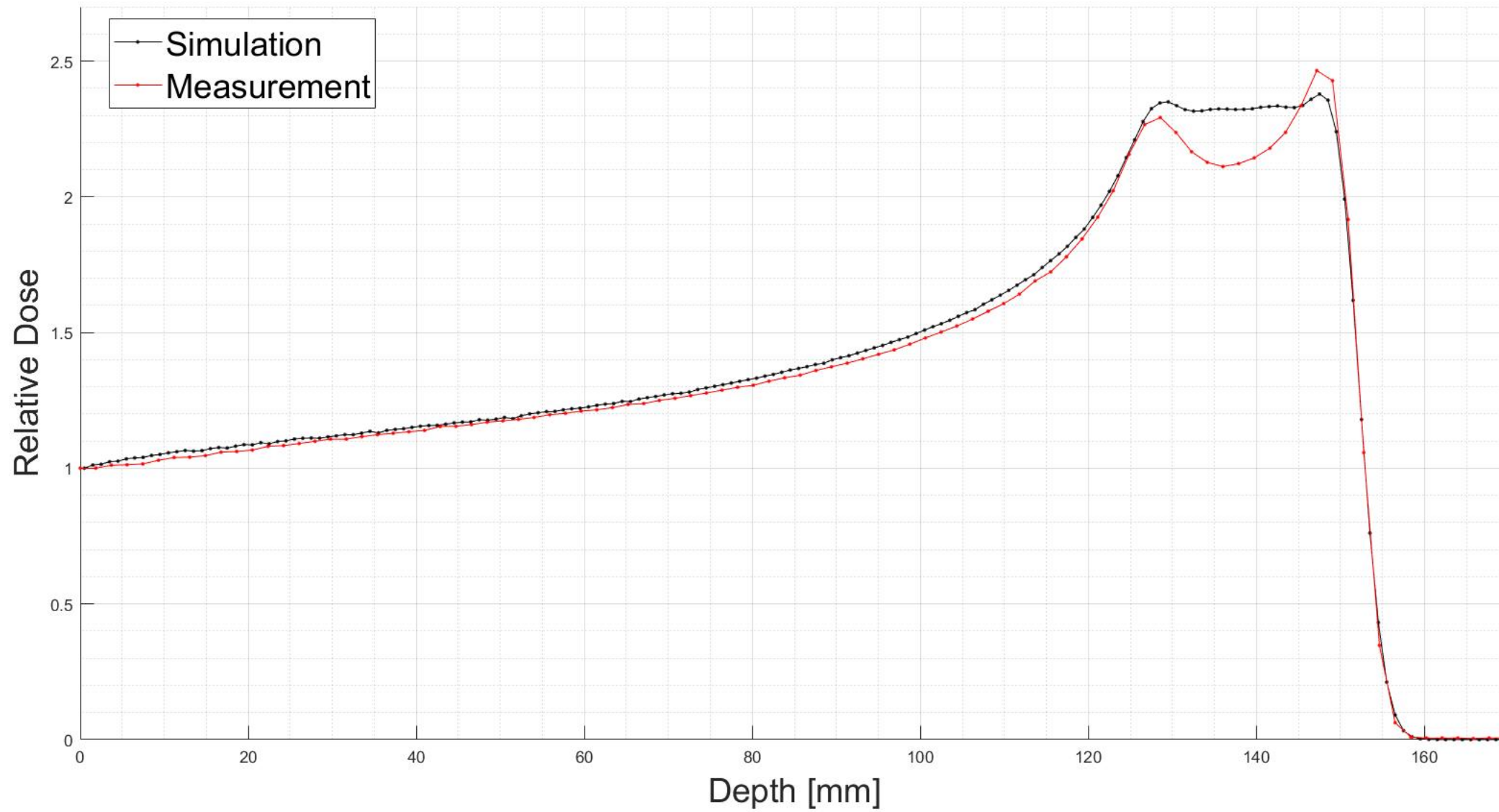


REALIZATION AND EXPERIMENTAL VALIDATION

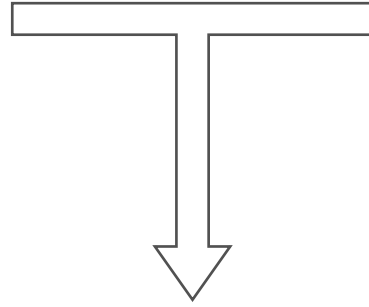
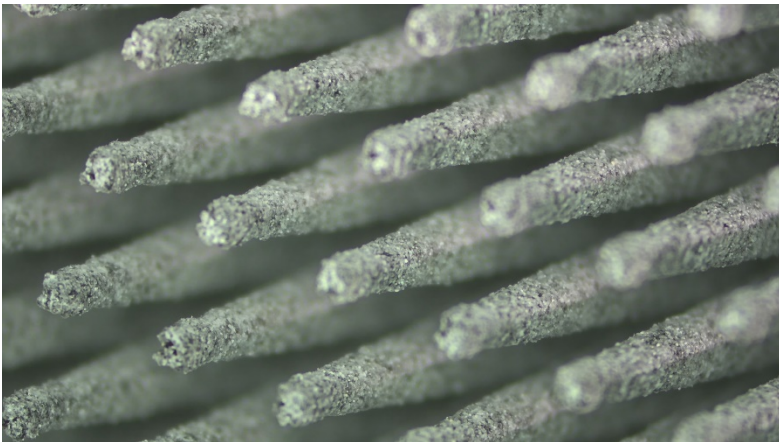
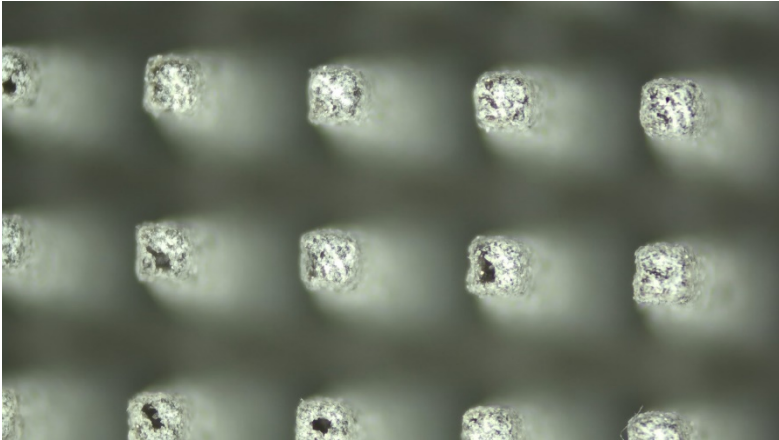
First prototypes: PA12 Range Modulators





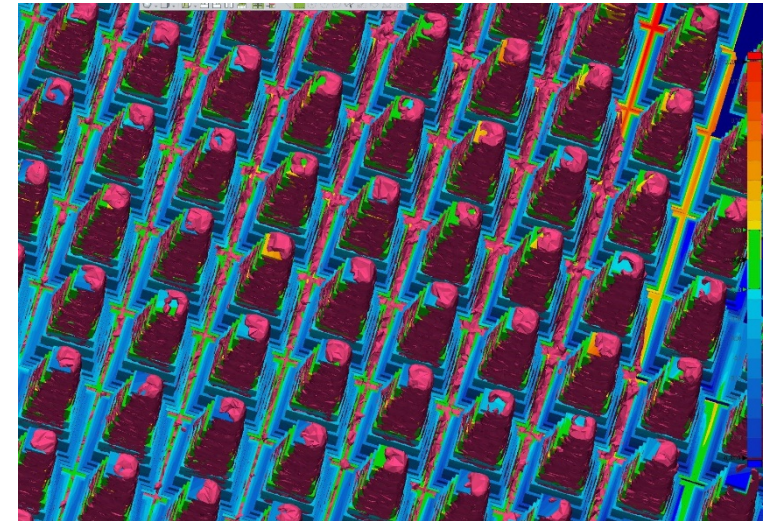


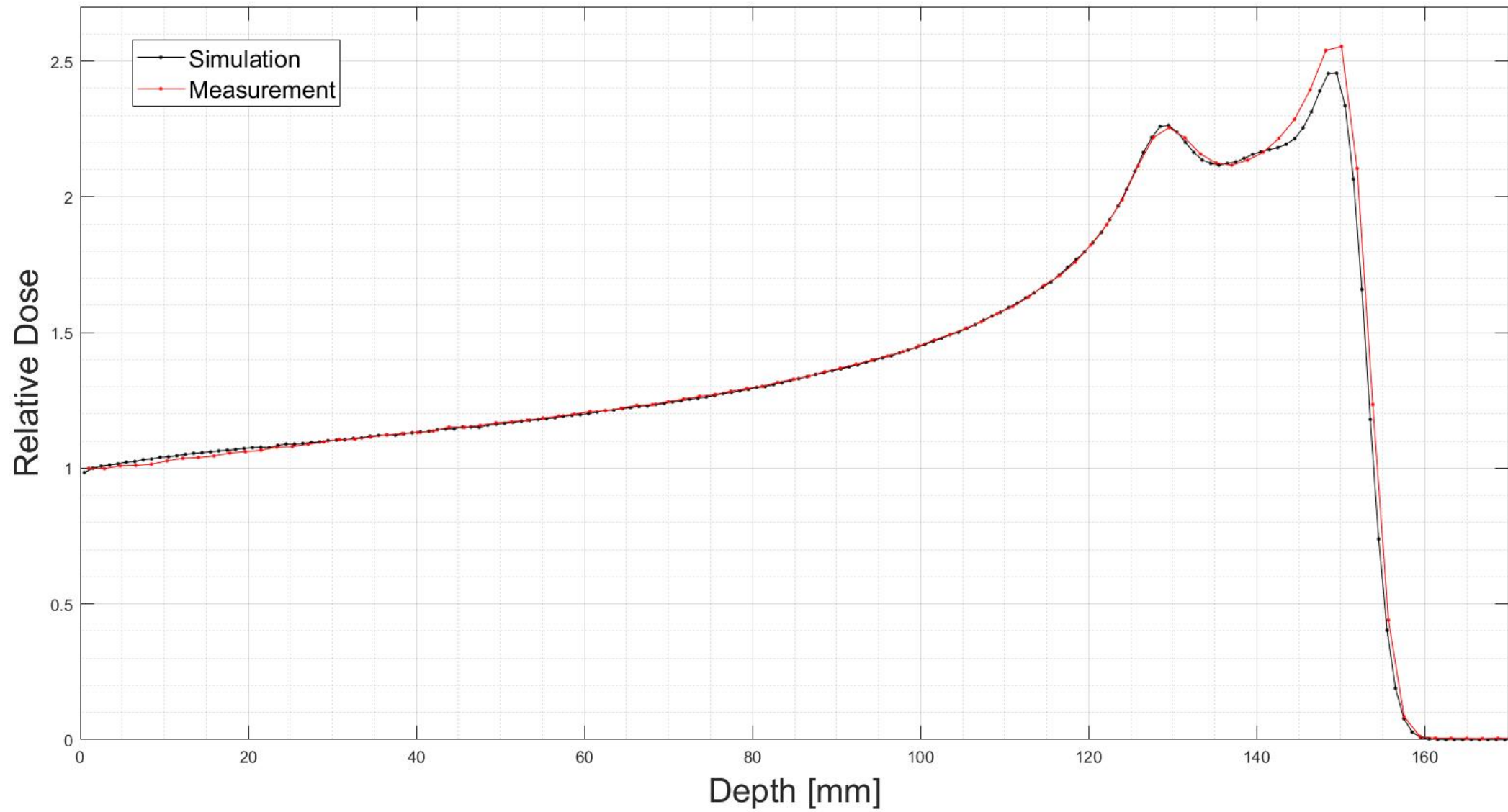
Stereo Microscope
(Visual Inspection)



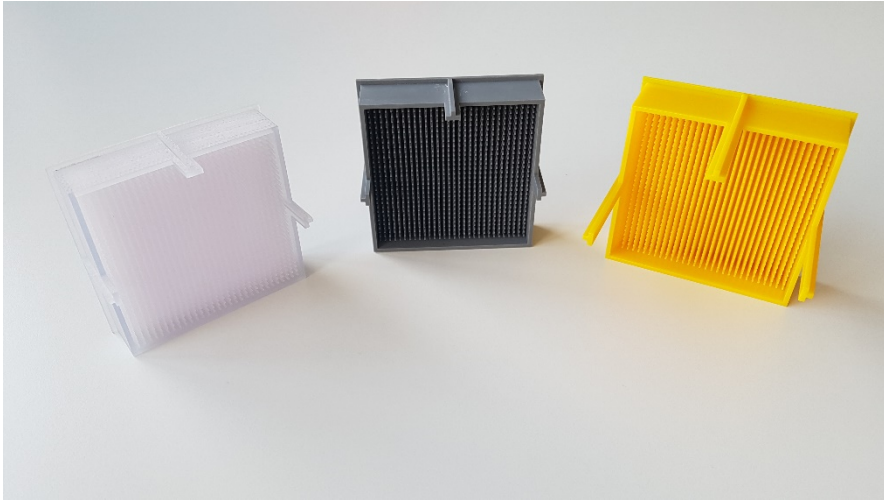
Industrial Tomograph
(Quantitative estimation)

- Porosity
- Irregularities
- **Systematic deviations**





Solution: change material and printing technique

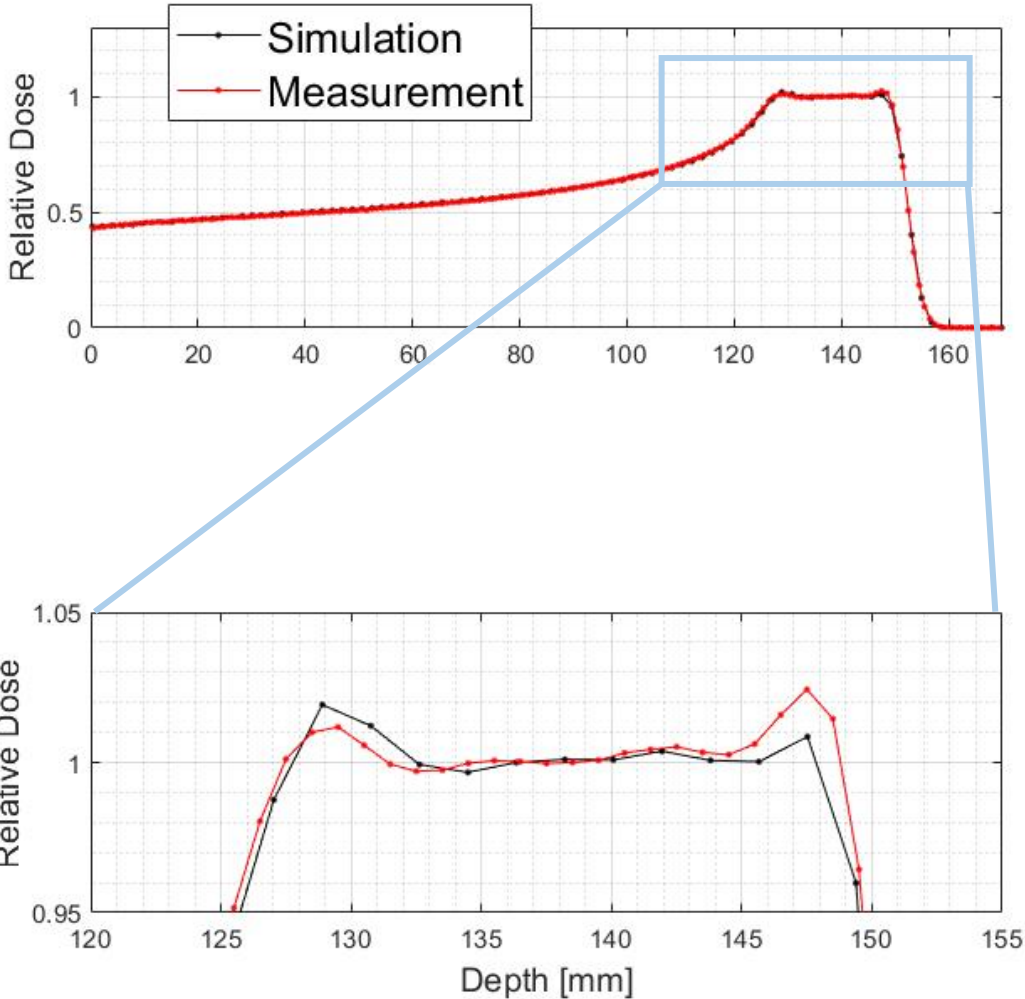


Stereolithography with three different resins:

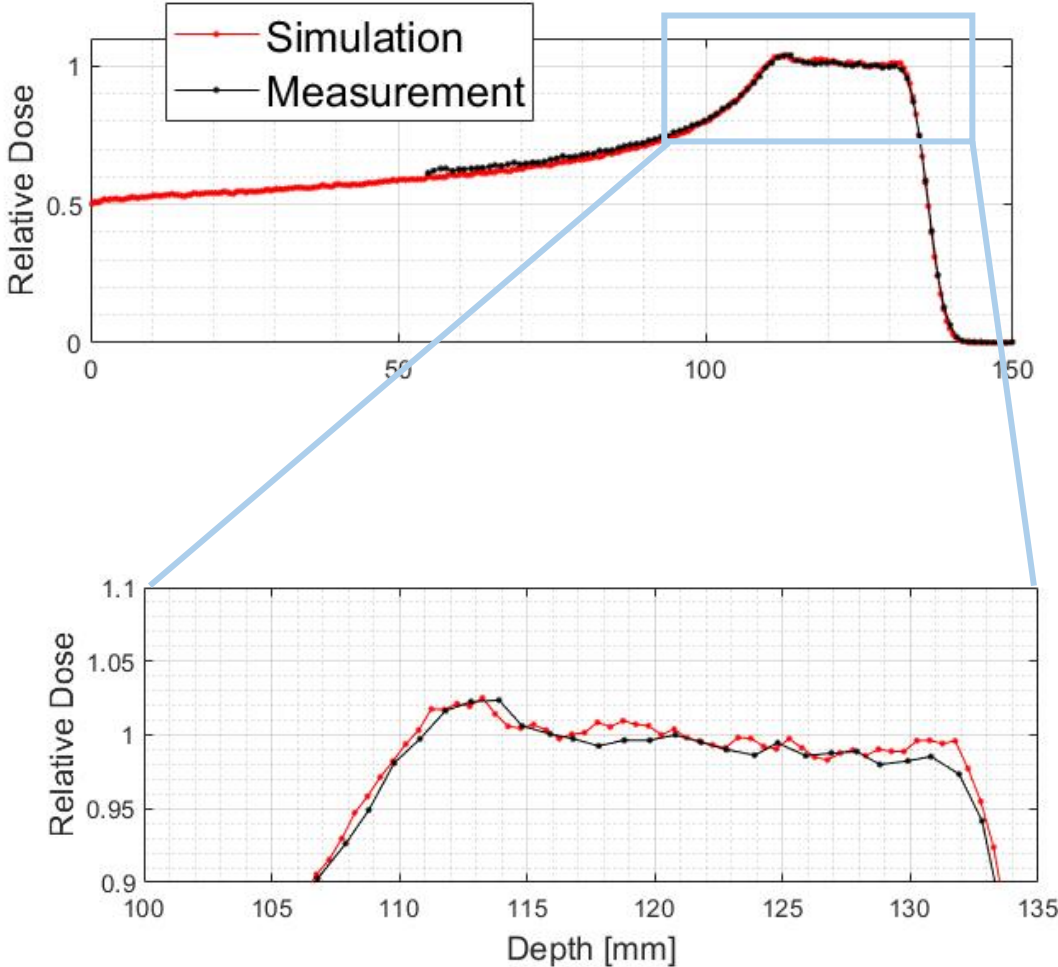
- Vitra
- DWS
- Vero Yellow

Results

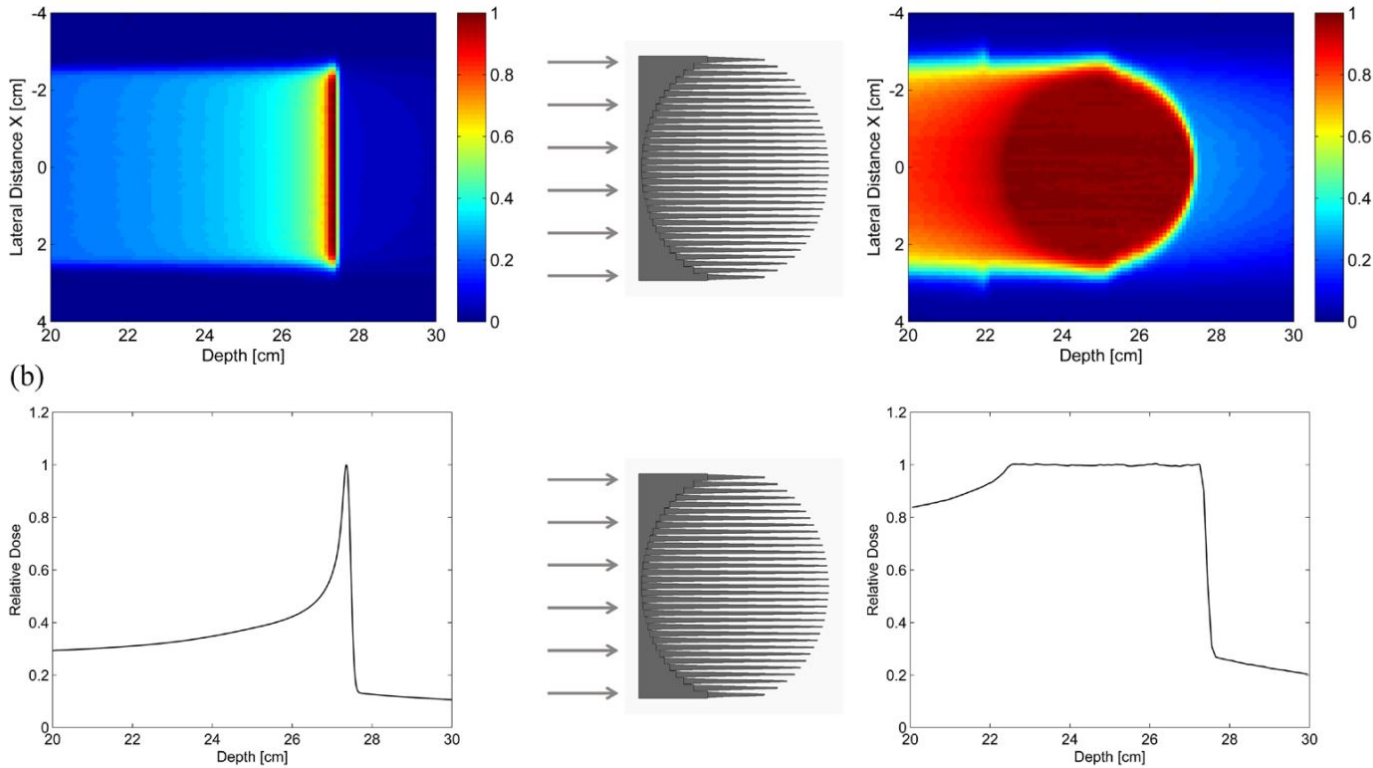
Gantry



Research Area



3D Range Modulators

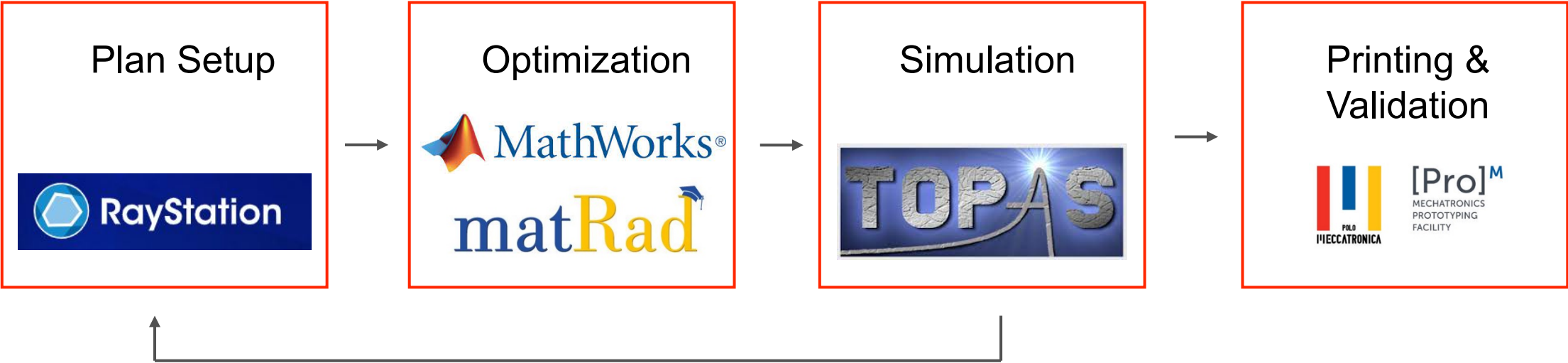


Y. Simeoneov et al, 3D range-modulator for scanned particle therapy: development, Monte Carlo simulations and experimental validation

- All pins need to be **optimized**
- Increased number of degrees of freedom required
- Need to control **beam scattering** and **optical divergence**
- Up to several thousands of optimization variables
- Linear combination of **full dose distributions** instead of single depth dose profiles

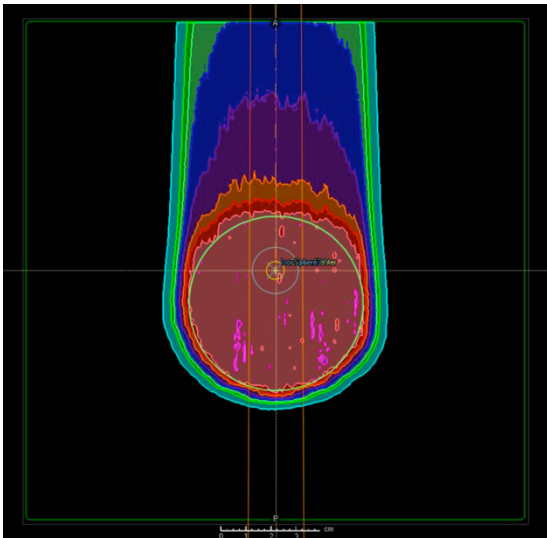
Workflow

For 3DRM



3D Range Modulators: spherical target in water

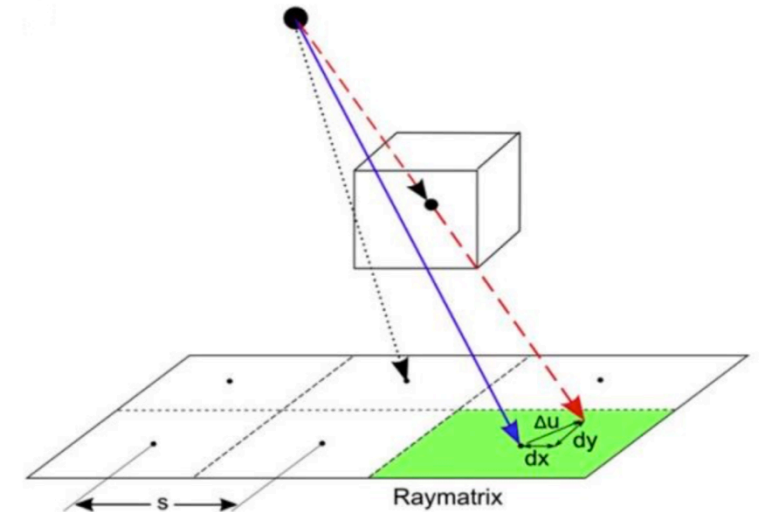
1. Target definition and RS plan



Export DICOM RP, RD, RS

Switch to Matlab/matRad

2. RM “macroscopic” geometry definition



At this stage, we get how many pins we need and “where”

3D Range Modulators

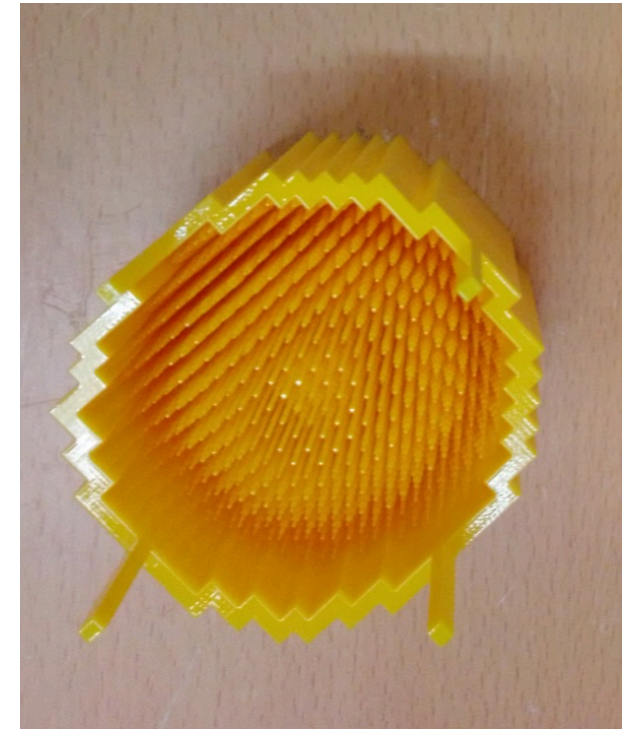
3. Pre-computed Dose Influence Matrix

$$D[i] = \sum_{j=1}^{N_s} d[i][j]w[j]$$

$i \rightarrow$ voxel
 $j \rightarrow$ spot

Optimization to get weights

4. Weights converted into pin geometry and sent to printer

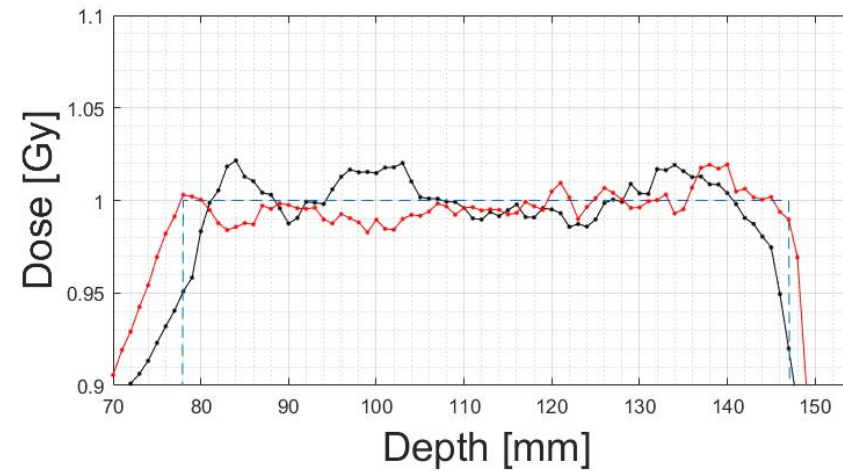
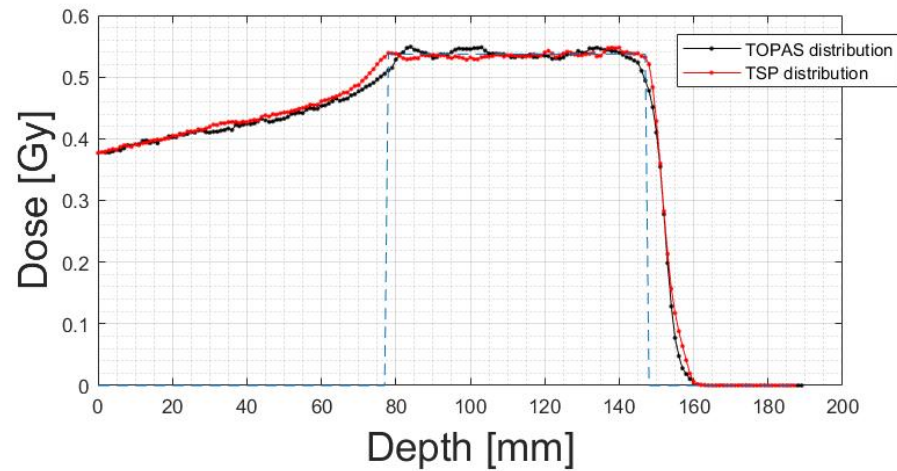
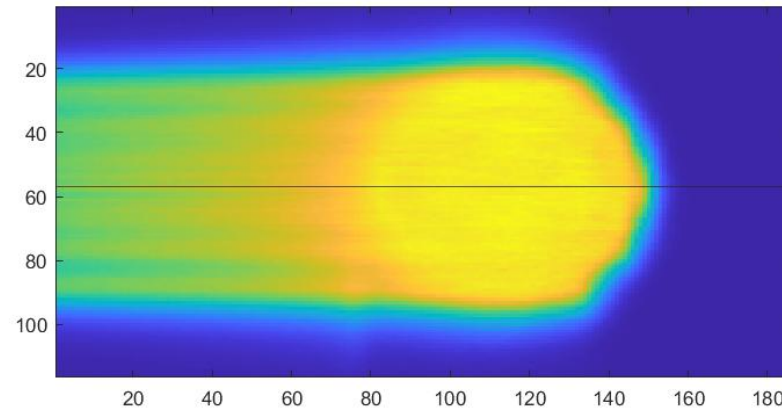


6. Fluence map optimization

5. Monte Carlo (TOPAS) re-calculation of $D(i)$

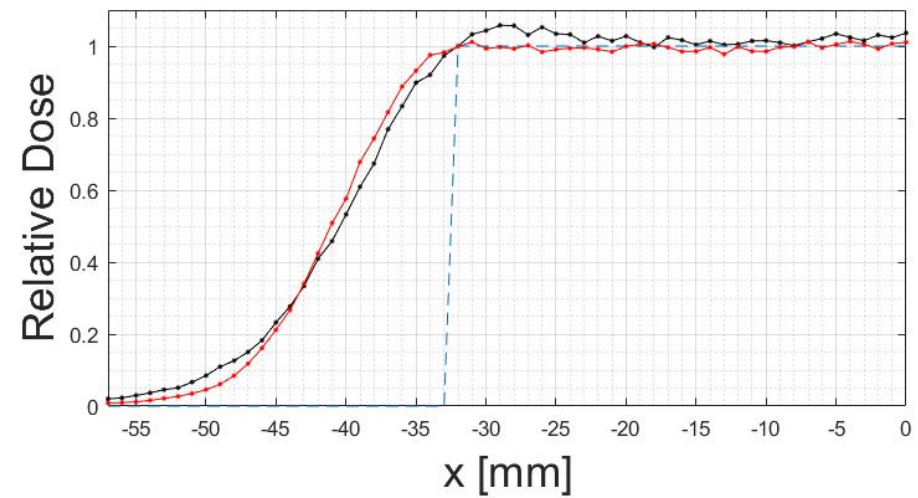
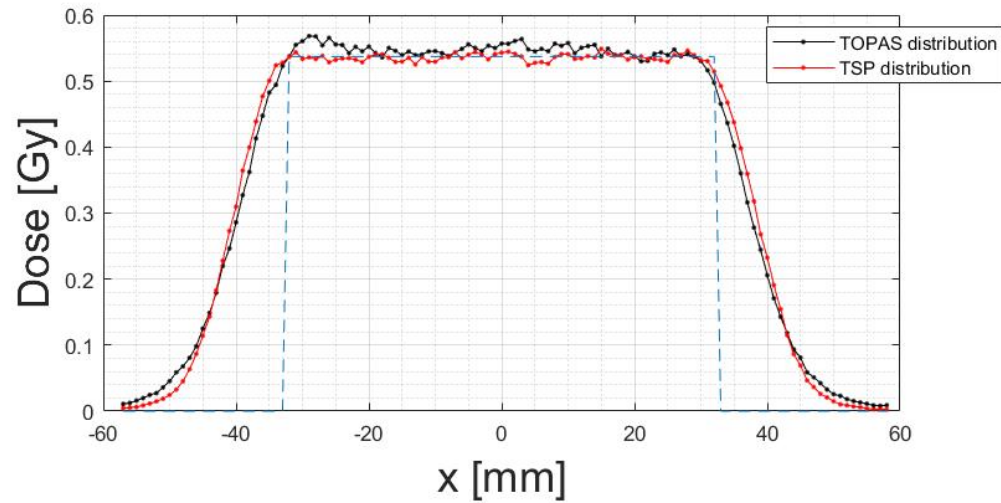
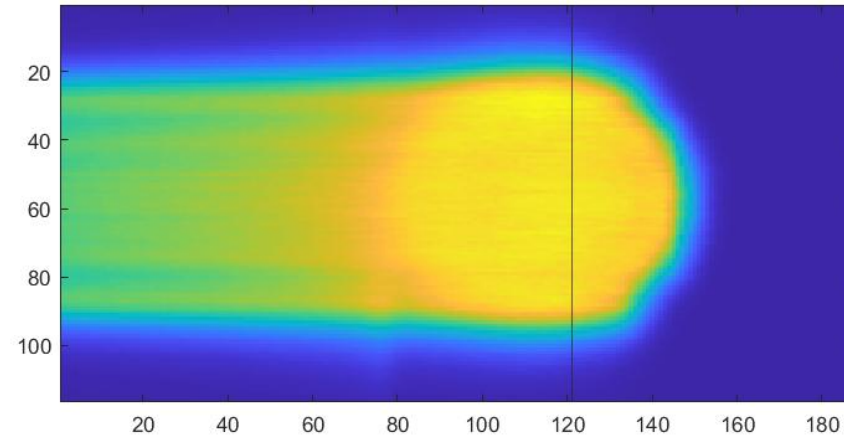
Simulation

Simulation



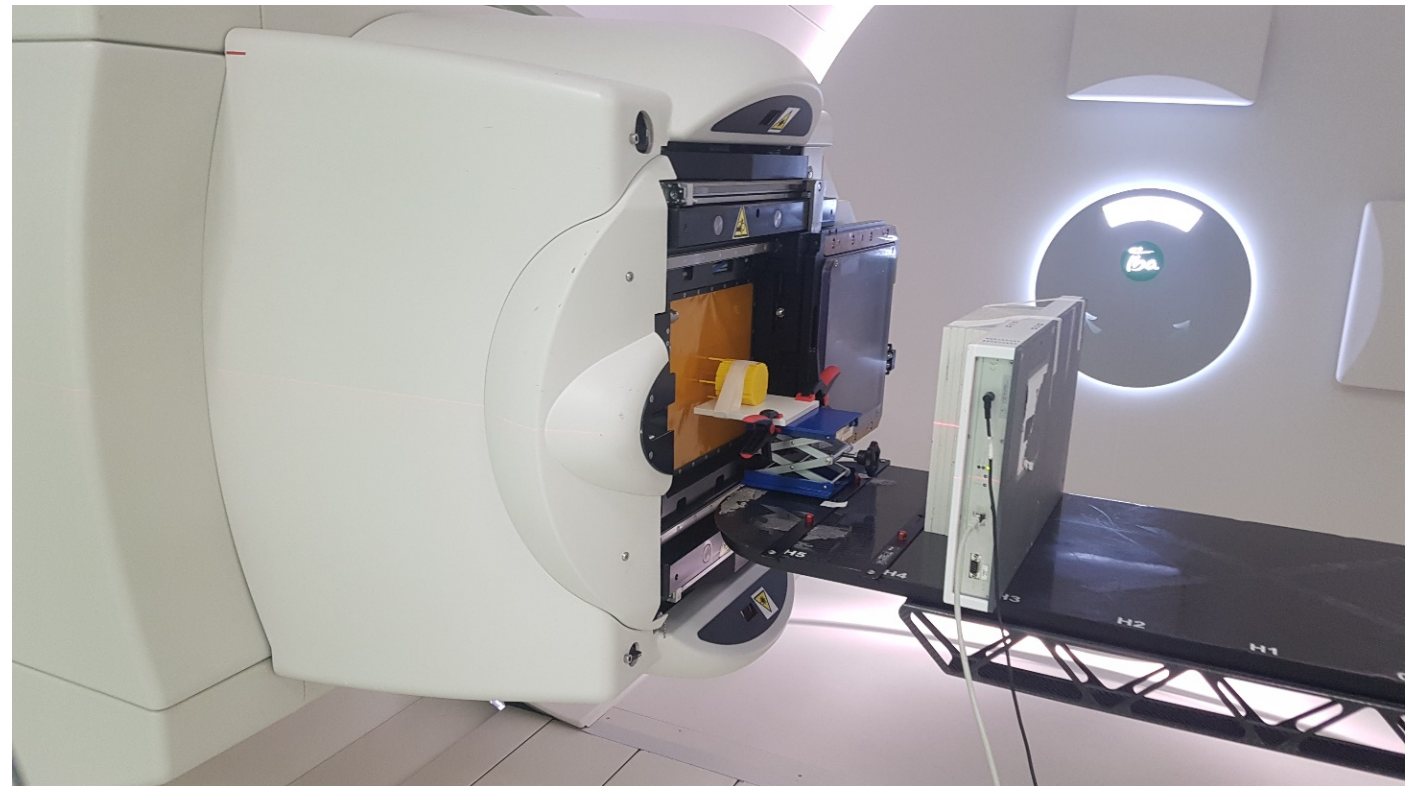
Simulation

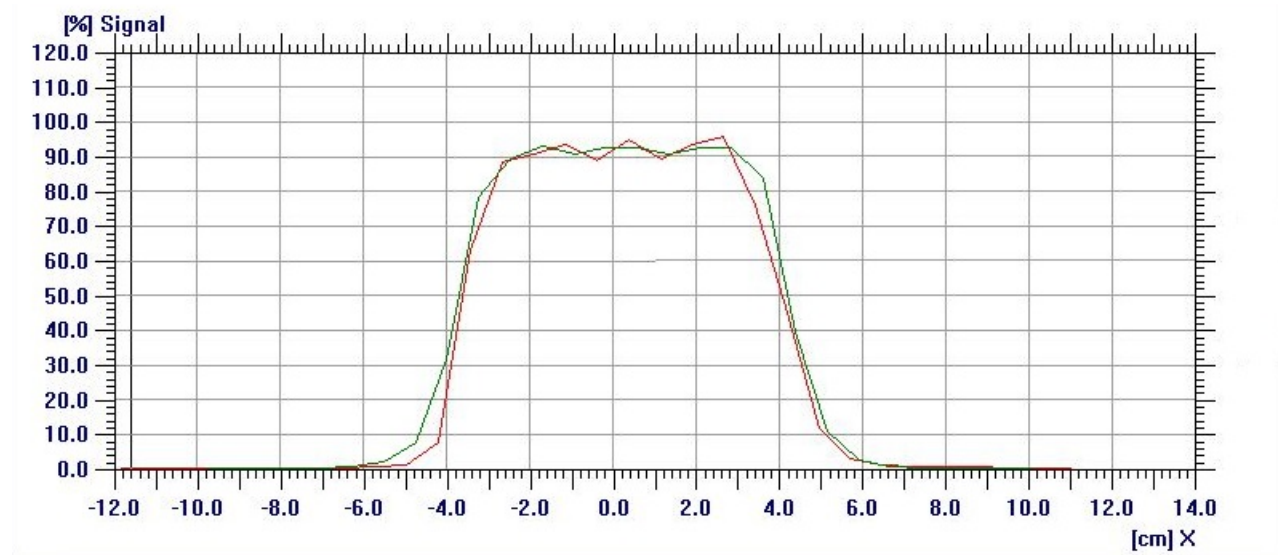
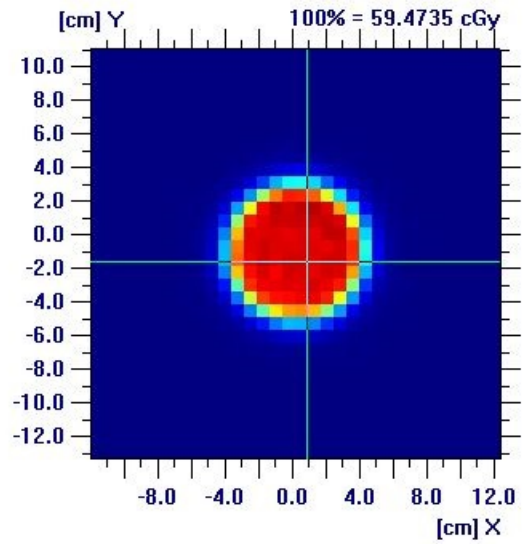
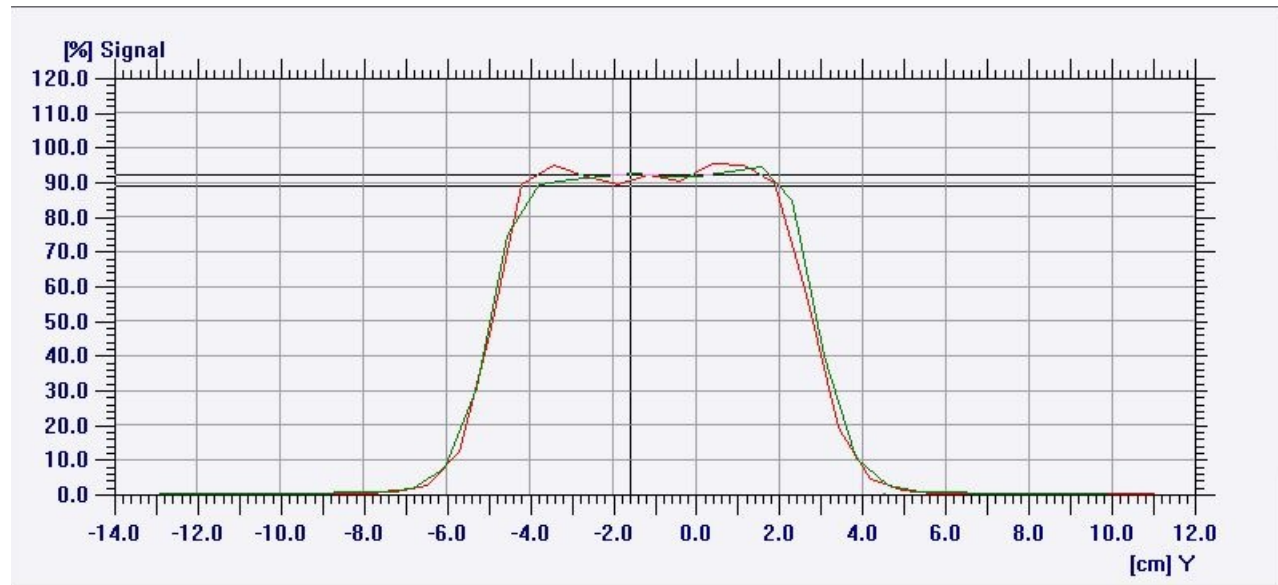
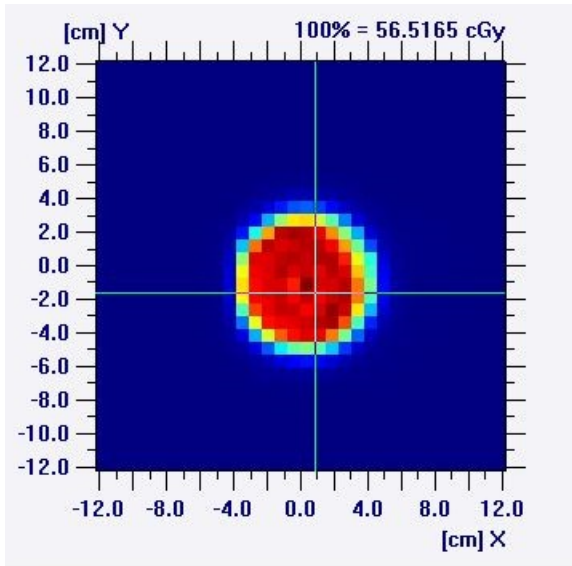
Simulation



First prototype

Printing &
Validation





Outlook

- Further **testing** of the 3DRM prototype (on the short term)
- Best setup for 3D RM implementation?
- Improvement of the 3DRM optimization **procedure**
- Evaluation of dose rate distributions
- Implementation of DMF and SDDRO