



Collagen micro-architecture investigation in tumor sections by means of second harmonic generation signal multiphasor analysis coupled with non-supervised machine learning techniques

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Collagen role in diseased tissues

AIM

Retrieving and exploiting features able to describe the collagen fibrils microstructure to separate tumor from healthy regions into the tissue.





It is characterized by non centrosymmetric microscopic structure.

The collagen micro-architecture is different depending on tissue and in presence of pathologies (aging, fibrosis, <u>tumor growth</u>)

Collagen can be exploited as an <u>early</u> <u>diagnostic marker</u>

Polarization Dependent Second Harmonic Generation (P-SHG)



Model:

SHG is a non linear coherent optical process, <u>label-free signal</u>, sensitive to molecular symmetry and <u>polarization</u>.

$$P_i^{(2)}(2\omega) = \sum_j \sum_k \chi_{ijk}^{(2)}(\omega, \omega) E_j(\omega) E_k(\omega)$$
$$\gamma = \chi_{zzz}^{(2)} / \chi_{zxx}^{(2)}$$

Williams, R. et al. Biophys. J. 88, 1377–1386 (2005)

$$I(\theta_L^n) = k \left\{ \sin^2 \left[2(\theta_L^n - \theta_F) \right] + \left[\sin^2 (\theta_L^n - \theta_F) + \gamma \cos^2 (\theta_L^n - \theta_F) \right]^2 \right\}$$
Moon fibril existation

Mean fibril internal disorder

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Microscopic Multiparametric Analysis by Phasor projection of Polarization dependent SHG (µMAPPS)



Radaelli et al. Sc.Rep. 7, 17468, 2017

<u>Pixel-by-pixel</u> retrieval of features able to describe the collagen microstructure, <u>without fitting procedures</u>.

$$g_{\theta} = \frac{\sum_{n=0}^{N-1} I(\theta_{L}^{n}) \cos(\theta_{L}^{n} K_{\theta})}{\sum_{n=0}^{N-1} I(\theta_{L}^{n})} \qquad \begin{array}{l} K_{\theta} = 2\pi (N \Delta \theta)^{-1} \\ \theta_{L}^{n} = n \Delta \theta \\ N = \frac{\pi}{\Delta \theta} \\ N = \frac{\pi}{\Delta \theta} \\ 0 \le \theta_{L} \le \frac{3}{2} \pi \end{array}$$





Microscopic Multiparametric Analysis by Phasor projection of Polarization dependent SHG (µMAPPS)

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Radaelli et al. Sc.Rep. 7, 17468, 2017

<u>Pixel-by-pixel</u> retrieval of features able to describe the collagen microstructure, without fitting procedures.

$$g_{\gamma} = \frac{\sum_{n=0}^{\left(\frac{N}{2}\right)-1} I(\theta_{L}^{n} + \theta_{F}) \cos((\theta_{L}^{n} + \theta_{F}) K_{\theta})}{\sum_{n=0}^{N-1} I(\theta_{L}^{n} + \theta_{F})}$$

$$s_{\gamma} = \frac{\sum_{n=0}^{\left(\frac{N}{2}\right)-1} I(\theta_{L}^{n} + \theta_{F}) \sin((\theta_{L}^{n} + \theta_{F}) K_{\theta})}{\sum_{n=0}^{N-1} I(\theta_{L}^{n} + \theta_{F})}$$

$$\theta_{L}^{n} = n\Delta\theta \quad N = \frac{\pi}{\Delta\theta} \quad K_{\theta} = 2\pi (N(\Delta\theta + \theta_{F}))^{-1} \quad \theta_{F} \le \theta_{L} \le \theta_{F} + \frac{\pi}{2}$$

$$d_{e-RC} = \sqrt{(g_e - g_{RC})^2 - (s_e - s_{RC})^2}$$
$$\gamma_e = \gamma_{RC|min(d_{e-RC})}$$

Tumor section analysis by μMAPPS θF-values Map

350 μm

0° 350 μm 180°

Skin

Ізнс Map







θF-values Histograms





Tumor section analysis by µMAPPS

D

γ-values Map





Skin

Isнg Map





γ-values Histograms





Clustering Procedure

Assignment phase



Aggregation phase



Id Pixel	ρ	
180	1501	
792	1407	
33.5		
- B.	•	
47	0	

 θc = Theta radius γc = Gamma radius $\Delta \theta_{ij}$ = Point-point distance in theta phasor space

 $\Delta \gamma_{ij}$ = Point-point distance in gamma phasor space

ROI-based procedure, which exploits both θ_F and γ values.



Results

PicroSirius Red Staining



Fibril Entropy (H) Map



Tumor/Skin Map



New feature: FIBRIL ENTROPY (H)



X_i = # elements of the i-cluster X_k = # total clustered elements

Accuracy (%)	True Negative	True Positive
Colon carcinoma	83.0 ± 4.5	91.8 ± 4.4
Breast carcinoma	87.5 ± 3.9	91.0 +- 6.0

Scodellaro et al. Front. Oncol. 9:527, 2019

Perspectives

Fast microstructural analyses to assist the histo-pathological evaluation.

In-situ diagnosis of pathologies and diseases.

Cluster-based machine learning algorithms with diagnostic capability of tumors.

Application to 3D samples.

Our team



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