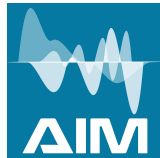


# Amyloid PET: quantification, classification and clinics

UPDATE

Enrico Peira



AIM general meeting

Pisa - February 3rd, 2020

# Aim

“to develop and validate new approaches for quantification and classification of amyloid PET that can be integrated into the clinical practice”

## Concluded projects:

quantification & grading  
a kinetic based approach to quantification

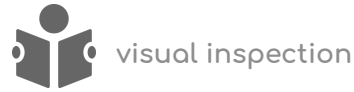
## Ongoing studies:

further validation of our methodologies  
regional accumulation: does it make sense?  
regional accumulation: how?  
EEG to amyloid

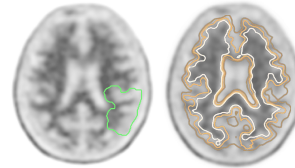
# Quantification & grading

study design & objectives

175 cases  
symptomatic outpatients  
age [62 - 88]  
MMSE  $\mu$  = 26.1



multicentric  
6 EADC centers, population matching  
cross-sectional data



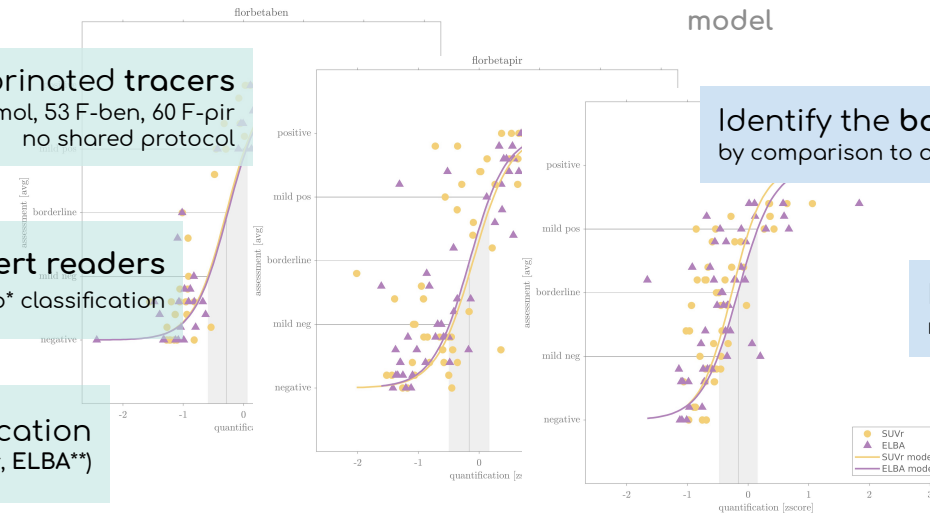
quantitative  
analysis

Test a more complex visual scale\*  
across different tracers

3 fluorinated tracers  
62 F-mol, 53 F-ben, 60 F-pir  
no shared protocol

5 independent expert readers  
quality, n/p and 5-step\* classification

2 quantification  
(cortico-cerebellar SUVr, ELBA\*\*)



Identify the **borderline zone** and **cut-off**  
by comparison to a **graded\*** visual assessment

Map function (SUVr, ELBA)  
regardless of tracer

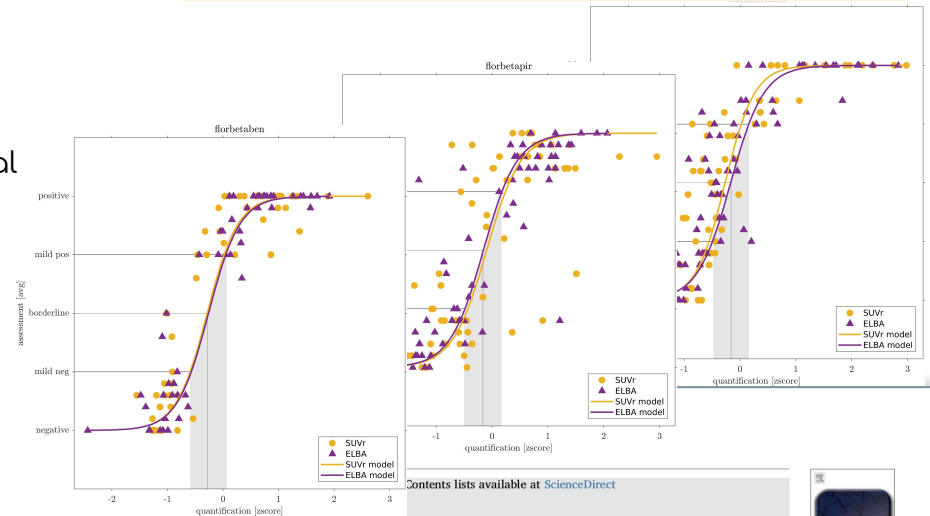
\* Paghera et al. Comparison of visual criteria for amyloid Positron Emission Tomography reading: could their merging reduce the inter-raters variability. *Q. J. Nucl. Med. Mol. Imaging*. 2019

\*\* Chincarini et al. Standardized uptake value ratio-independent evaluation of brain amyloidosis. *J. Alzheimers Dis*. 2016

- Thanks to a sigmoid model and to the 5-step visual scale it was possible to define **cut-offs** and **transition regions** (borderline) on all tracers
- It is possible to construct a **map** between different tracers and different **quantification** methods without resorting to ad-hoc acquired cases
- No tracer is the winner here, all are **equivalently discriminating** (means: equivalent contrast)

very little literature on tracer comparison with evaluation from the same set of readers

## results



NeuroImage: Clinical

journal homepage: [www.elsevier.com/locate/ynicl](http://www.elsevier.com/locate/ynicl)



Semi-quantification and grading of amyloid PET: A project of the European Alzheimer's Disease Consortium (EADC)

A. Chincarini<sup>a,\*</sup>, E. Peira<sup>a,d</sup>, S. Morbelli<sup>b,c</sup>, M. Pardini<sup>c,d</sup>, M. Bauckneht<sup>e</sup>, J. Arbizu<sup>e</sup>, M. Castelo-Branco<sup>f</sup>, K.A. Büsing<sup>g</sup>, A. de Mendonça<sup>h</sup>, M. Didic<sup>i</sup>, M. Dottorini<sup>j</sup>, S. Engelborghs<sup>k,l</sup>, C. Ferrarese<sup>m</sup>, G.B. Frisoni<sup>n,o</sup>, V. Garibotto<sup>o</sup>, E. Guedj<sup>p,q</sup>, L. Hausner<sup>r,s</sup>, J. Hugon<sup>t</sup>, J. Verhaeghe<sup>u</sup>, P. Mecocci<sup>v</sup>, M. Musarra<sup>w</sup>, M. Queneau<sup>x</sup>, M. Rivera<sup>y</sup>, I. Santana<sup>z</sup>, U.P. Guerra<sup>aa</sup>, F. Nobili<sup>ab</sup>

<sup>a</sup> Istituto Nazionale di Fisica Nucleare (INFN), Genova, Italy, <sup>b</sup> Dipartimento di Neuroscienze, Università della Genova, Genova, Italy, <sup>c</sup> Istituto Nazionale di Fisica Nucleare (INFN), Genova, Italy, <sup>d</sup> Dipartimento di Neuroscienze, Università della Genova, Genova, Italy, <sup>e</sup> Institut d'Investigacions Biomèdiques August Pi i Sunyer (IDIBAPS), Hospital de la Santa Creu i Sant Pau, Barcelona, Spain, <sup>f</sup> Instituto de Diagnóstico y Referencia Epidemiológica, Secretaría de Salud, México, <sup>g</sup> Department of Neurosciences, Rehabilitation, Ophthalmology, Genetics, Maternal and Child Health, University of Genoa, Genoa, Italy, <sup>h</sup> Department of Nuclear Medicine, University of Navarra, Clínica Universidad de Navarra, Pamplona, Spain

published in NeuroImage: Clinical

# A kinetics-based approach to quantification

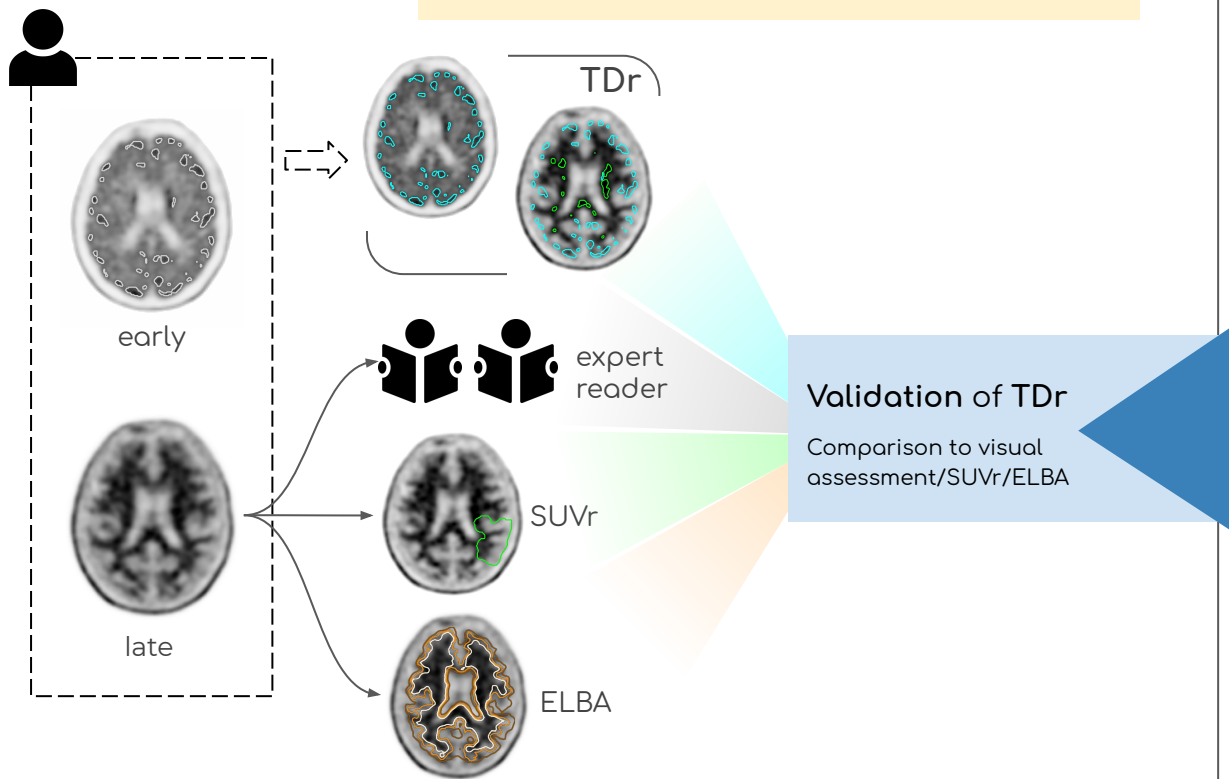
study design & objectives

143 cases  
symptomatic outpatients  
age [54-87]

2 acquisitions per patient  
early (0-5 min.) + late (50-70 min.)

1 tracer  
 $^{18}\text{F}$ -florbetapir

multicentric  
4 EADC centers  
cross-sectional data

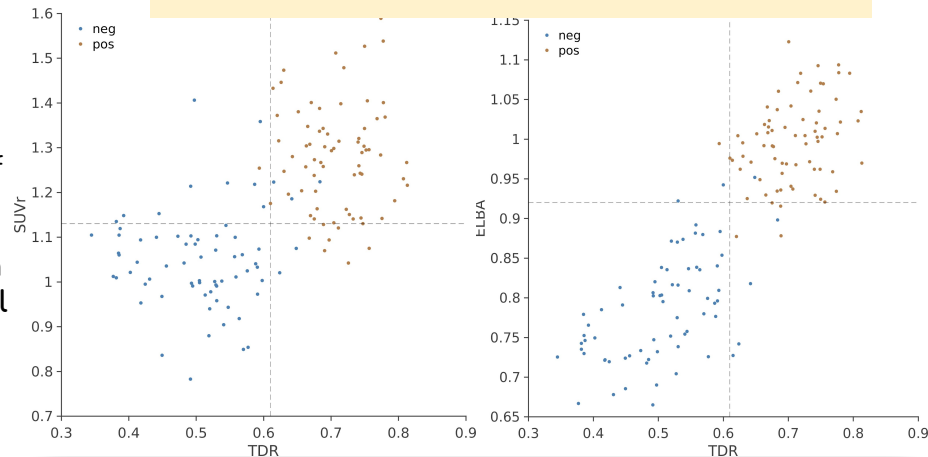


# A kinetics-based approach to quantification

- Novel kinetic-based approach to quantification of amyloid PET, tested on naturalistic population
- Based on dual-time point acquisition, tailored on individual patient anatomic and pathophysiological characteristics
- Excellent agreement with visual assessment
- Significantly correlates with the two validated methods (ELBA, SUVr)

TDr is a patented method

## results



European Journal of Nuclear Medicine and Molecular Imaging  
<https://doi.org/10.1007/s00259-020-04689-y>

ORIGINAL ARTICLE



### A kinetics-based approach to amyloid PET semi-quantification

A. Chincarini<sup>1</sup> • E. Peira<sup>1,2</sup> • M. Corosu<sup>1</sup> • S. Morbelli<sup>3,4</sup> • M. Bauckneht<sup>3,4</sup> • S. Capitanio<sup>3,4</sup> • M. Pardini<sup>2,4</sup> • D. Arnaldi<sup>2,4</sup> • C. Vellani<sup>5</sup> • D. D'Ambrosio<sup>6</sup> • V. Garibotto<sup>7,8</sup> • F. Assal<sup>7,9</sup> • B. Paghera<sup>10</sup> • G. Savelli<sup>11</sup> • A. Stefanelli<sup>11</sup> • U. P. Guerra<sup>11</sup> • F. Nobili<sup>2,4</sup>

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#### Abstract

**Methods** The TDr method requires two static scans per subject: one early (~0–10 min after the injection) and one late (typically 50–70 min or 90–100 min after the injection, depending on the tracer). High perfusion regions are delineated on the early scan and the PET data from the late scan are subtracted from the early scan. The resulting difference image is then used to estimate the TDr. The TDr is a novel method for amyloid PET semi-quantification. It is based on the difference between the two static scans. The TDr is a novel method for amyloid PET semi-quantification. It is based on the difference between the two static scans. The TDr is a novel method for amyloid PET semi-quantification. It is based on the difference between the two static scans.

published in European Journal of Nuclear Medicine and Molecular Imaging

# Further validation of our methodologies

90 cases

symptomatic outpatients  
age [67 - 82]

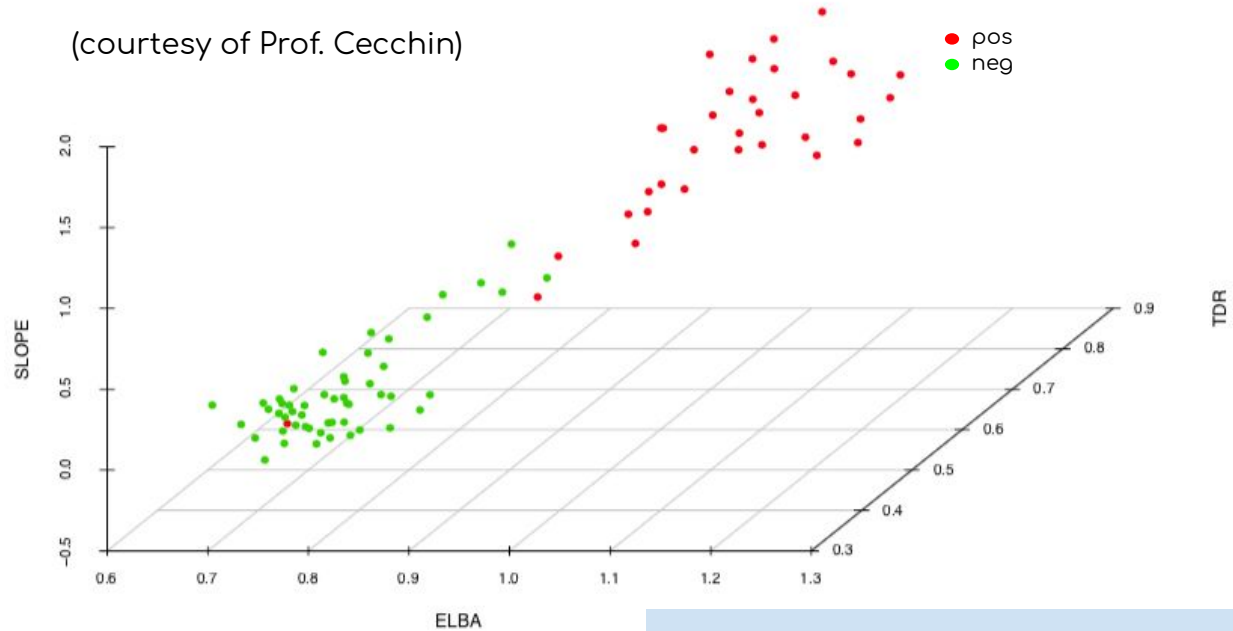
2 acquisitions per patient

early (0-5 min.) + late (50-70 min.)  
1 Tracer ( $^{18}\text{F}$ -florbetaben)

2 quantification  
(TDr, ELBA, SLOPE)

2 independent  
expert readers

(courtesy of Prof. Cecchin)



Compare ELBA and TDr to SLOPE\*

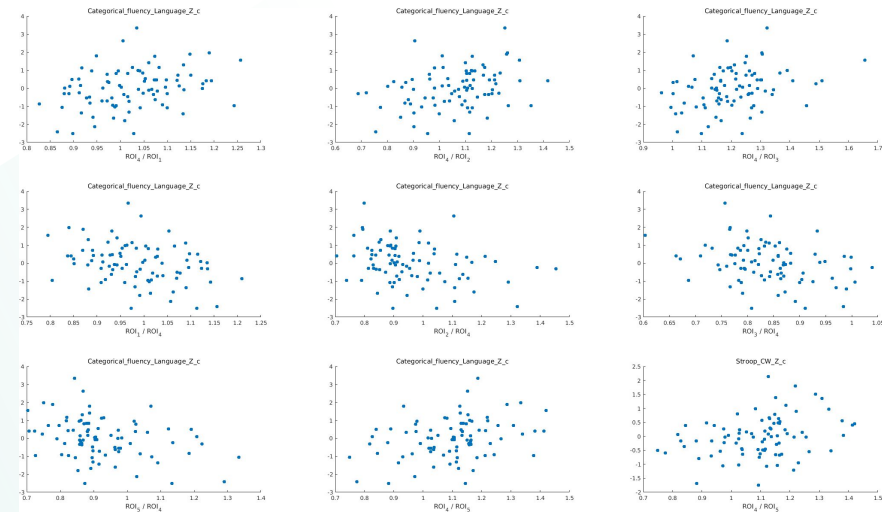
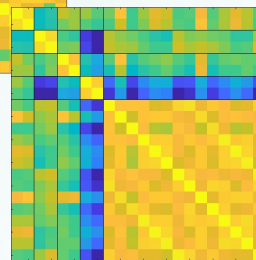
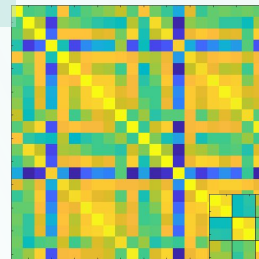
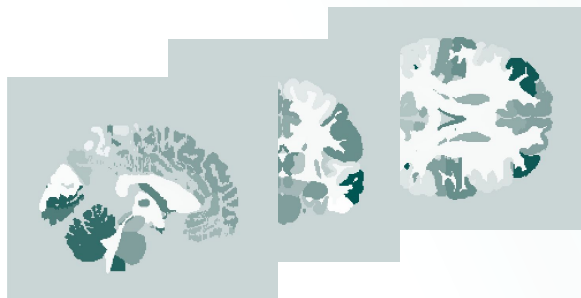
\* Cecchin et al. A new integrated dual time-point amyloid PET/MRI data analysis method. EJNMMI. 2017

# Regional amyloid accumulation: does this make sense?

84 cases  
symptomatic outpatients  
age [54 - 87]

Amyloid PET  
Neuropsychological assessment  
[ MMSE, RAVLT, TMT-A, TMT-B, Stroop, ...]

ELBA + SUVR quantification  
[ template 11 ROI]

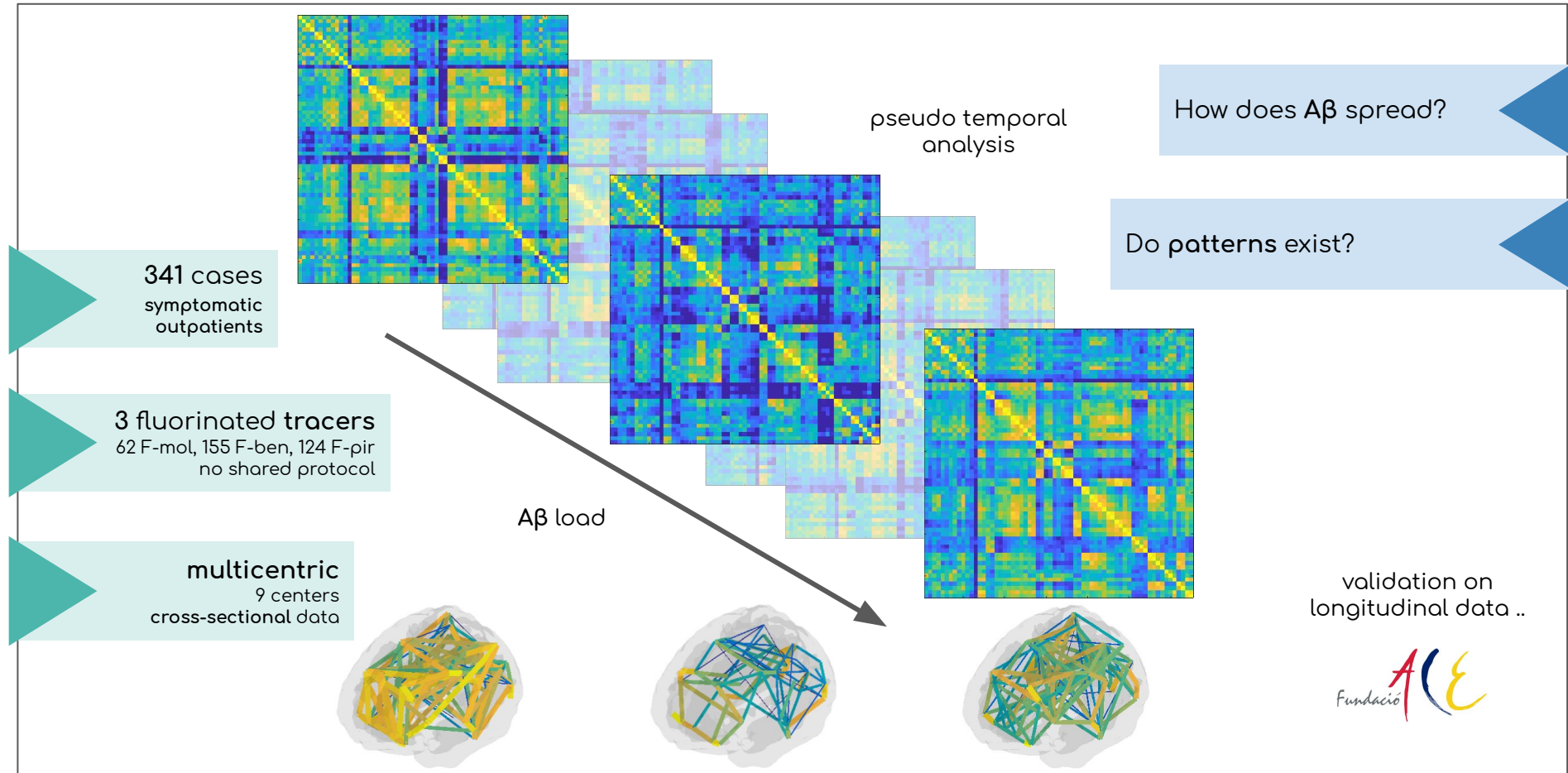


Does  $A\beta$  accumulation affect brain regions differently?

Clinical implications?



# Regional amyloid accumulation: how it happens?



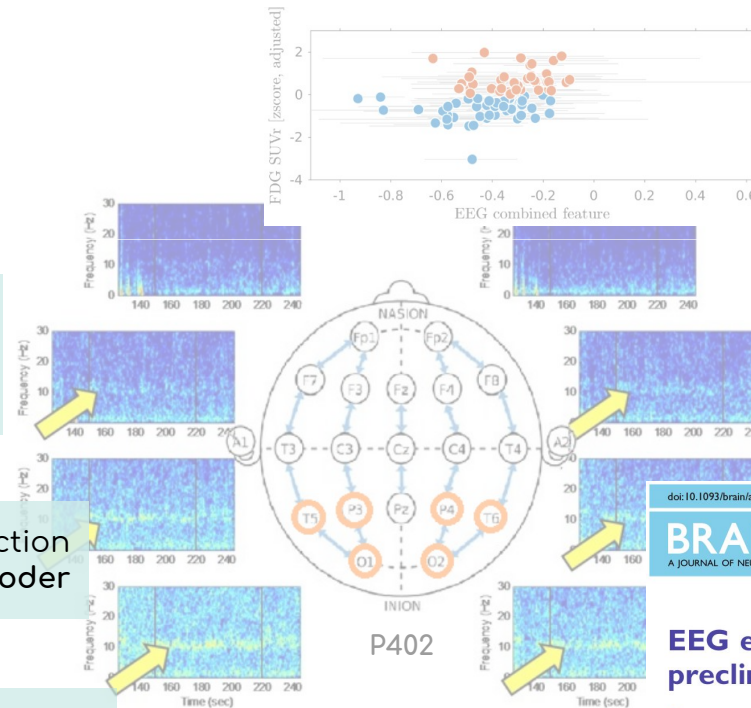
# from EEG to amyloid

89 cases  
symptomatic outpatients  
age [50 - 82]

1 amyloid PET  
1 FDG PET  
low-density EEG  
per patient

EEG features selection  
with deep autoencoder

EEG features are corrected  
for neurodegeneration



Investigate possible relation  
between  $A\beta$  and EEG signal

doi:10.1093/brain/awz150

BRAIN 2019; Page 1 of 17 | 1

**BRAIN**  
A JOURNAL OF NEUROLOGY

**EEG evidence of compensatory mechanisms in preclinical Alzheimer's disease**

① Sinead Gaubert,<sup>1,2,3,8</sup> Federico Raimondo,<sup>1,4,5,6,8</sup> Marion H. ...  
② Marie-Constance Corsi,<sup>1,2</sup> Lionel Naccache,<sup>1,9</sup> ...  
③ Bertrand Hermann,<sup>1</sup> Delphine Oudiette,<sup>10</sup> ...

positive subjects, either following a U-shape curve for delta power or an inverted U-shape curve for the other bands, meaning that EEG patterns are modulated differently depending on the degree of amyloid burden. This finding suggests initial compensatory mechanisms that are overwhelmed for the highest amyloid load. Together, these results indicate that EEG metrics are useful biomarkers for the preclinical stage of Alzheimer's disease.

game changer for screening?



Flavio Nobili, Matteo Pardini, Silvia Morbelli, Dario Arnaldi, Matteo Bauckneht, Matteo Grazzini

The group

Thank you!

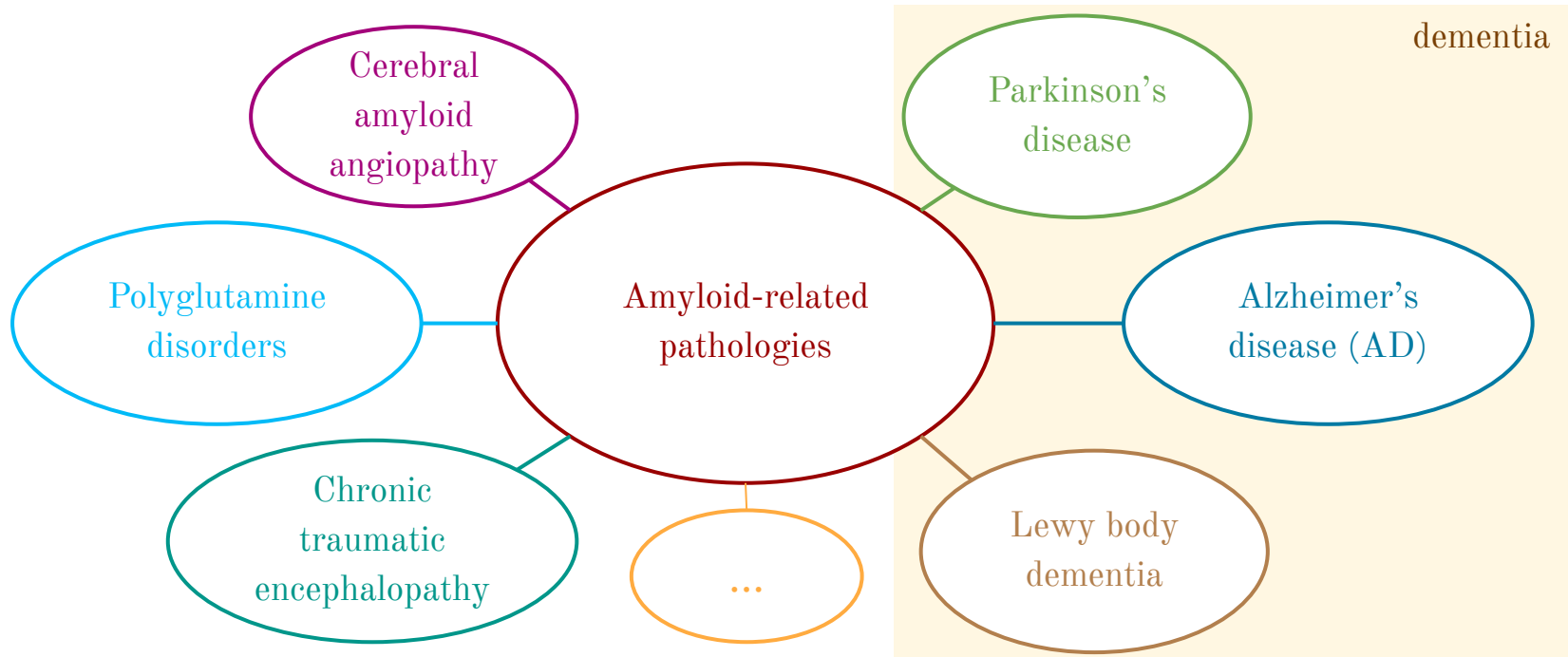


Andrea Chincarini, Francesco Sensi, Enrico Peira, Nicola Alchera, Gloria Pedemonte

special thanks to Ugo Paolo Guerra

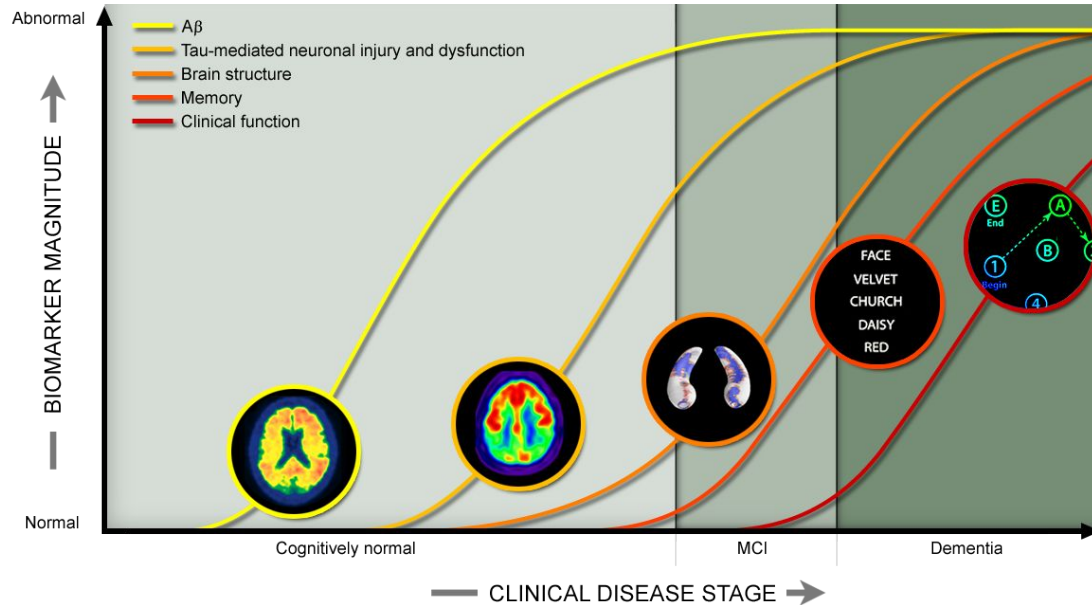
# Brain amyloidosis

- Amyloidosis is a general term that describes a **wide spectrum of diseases** characterized by a **deposit** of a neurotoxic peptides ( $\beta$ -Amyloid, **A $\beta$** ) in different organs
- A $\beta$  deposit in the central nervous system represents the most frequent form of amyloidosis in humans



# Amyloid: why?

The **increase of  $A\beta$**  is a key event in **AD**: its aggregation **precedes clinical symptoms** by many years (Jack 2010)



The **in-vivo** assessment of cerebral amyloid is taking a leading role in the **early differential diagnosis** becoming a biomarker of prime importance for **AD**

# Amyloid: a watershed in the AD diagnosis

## IWG-2 criteria for asymptomatic at risk for AD (A plus B)

*Lancet Neurol* 2014; 13: 614–29

### Advancing research diagnostic criteria for Alzheimer's disease: the IWG-2 criteria

Bruno Dubois, Howard H Feldman,  
Dennis Selkoe, Randall Bateman, S  
Marie-Odile Habert, Gregory A Jich  
Marie Sarazin, Stéphane Epelbaum  
Jeffrey L Cummings

*Alzheimers Dement.* 2018 April ; 14(4): 535–562. doi:10.1016/j.jalz.2018.02.018.

### NIA-AA Research Framework: Toward a biological definition of Alzheimer's disease

Clifford R. Jack Jr.<sup>a,\*</sup>, David A. Bennett<sup>b</sup>, Kaj Blennow<sup>c</sup>, Maria C. Carrillo<sup>d</sup>, Billy Dunn<sup>e</sup>,  
Samantha Budd Haeberlein<sup>f</sup>, David M. Holtzman<sup>g</sup>, William Jagust<sup>h</sup>, Frank Jessen<sup>i</sup>, Jason  
Karlawish<sup>j</sup>, Enchi Liu<sup>k</sup>, Jose Luis Molinuevo<sup>l</sup>, Thomas Montine<sup>m</sup>, Creighton Phelps<sup>n</sup>,  
Katherine P. Rankin<sup>o</sup>, Christopher C. Rowe<sup>p</sup>, Philip Scheltens<sup>q</sup>, Eric Siemers<sup>r</sup>, Heather M.  
Snyder<sup>d</sup>, and Reisa Sperling<sup>s</sup>

## B In-vivo evidence of Alzheimer's pathology (one of the following)

- Decreased A $\beta_{1-42}$  together with increased T-tau or P-tau in CSF
- Increased tracer retention on amyloid PET
- AD autosomal dominant mutation present (in PSEN1, PSEN2, or APP)

A $\beta$  negativity excludes the AD !

AT(N) profiles	Biomarker category	
A-T-(N)-	Normal AD biomarkers	
A+T-(N)-	Alzheimer's pathologic change	Alzheimer's continuum
A+T+(N)-	Alzheimer's disease	
A+T+(N)+	Alzheimer's disease	
A+T-(N)+	Alzheimer's and concomitant suspected non Alzheimer's pathologic change	
A-T+(N)-	Non-AD pathologic change	
A-T-(N)+	Non-AD pathologic change	
A-T+(N)+	Non-AD pathologic change	

# In-vivo amyloid assessment

## PET

### cons

radiation dose to patient, a-specific sites (WM), ...

### pro

routine technique, reliable, easier quantification, tracer availability, ...

## CSF

### cons

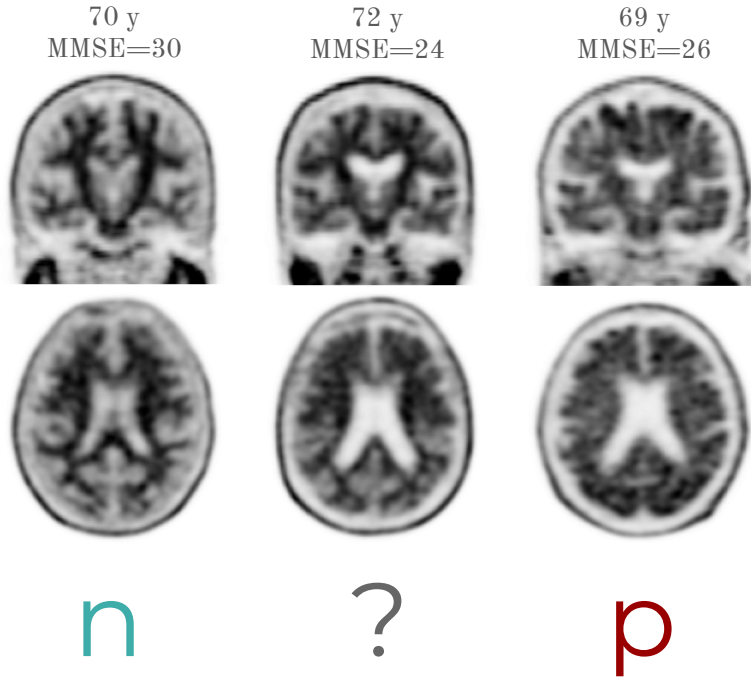
lumbar puncture: invasive, results sensitive to procedure, ...

### pro

$A\beta_{40}/A\beta_{42}$ , phosph- $\tau$  / tot- $\tau$ , higher clinical content, ...

With the hopefully near introduction of disease-modifying drugs, we expect a **paradigm shift** in the current **diagnostic pathway** with an unprecedented surge in the request of exams and detailed analysis

# Amyloid PET: binary classification



## binary reading rules of thumb

- visually inspect image for quality and artifacts
- review ligand-specific criteria for positivity (e.g: positive if contrast reduction at least in two lobes)
- inspect and evaluate on all cross-sections

## Recommendations from the Italian Interdisciplinary Working Group (AIMN, AIP, SINDEM) for the utilization of amyloid imaging in clinical practice

Ugo Paolo Guerra · Flavio Mariano Nobili · Alessandro Padovani ·  
Daniela Perani · Alberto  
Marco Trabucchi

It is common wisdom that a dichotomous classification (positive/negative exam) is inadequate for a thorough interpretation and reporting procedure. The amyloid accumulation period can last for up to 15 years and during this positivity level gradually increases [22, 23].

Therefore, a quantification or semi-quantification of the PET exam providing information about the level of positivity is advisable and should be strongly encouraged.



# TDr validation - Data & Study Design

## Cross-sectional data

- **Symptomatic outpatient**
- **143** patients (age [54-87])
- **Clinical suspicion:** FTD, AD, MCI, MCIAD, Dep, SMC, VCI, CBS, MSA, SNAP
- **Amyloid PET**, 2 acquisitions per patient
  - **early** (0-5 min. after injection)
  - **late** (50-70 min. after injection)
- **<sup>18</sup>F-florbetapir**
- **4 centers**
  - IRCCS Maugeri (Pavia)
  - IRCCS S.Martino (Genoa)
  - Fondazione Poliambulanza (Brescia)
  - HUG (Geneva)

## Late scans:

1. **Visually inspected & labeled**  
(blind & open visual assessment session)



70 negatives / 73 positive

+ 5 yr scan reporting (NM)

2. Processed with **SUV<sub>r</sub>** & **ELBA** (Chincarini 2016)

## Early and late scans:

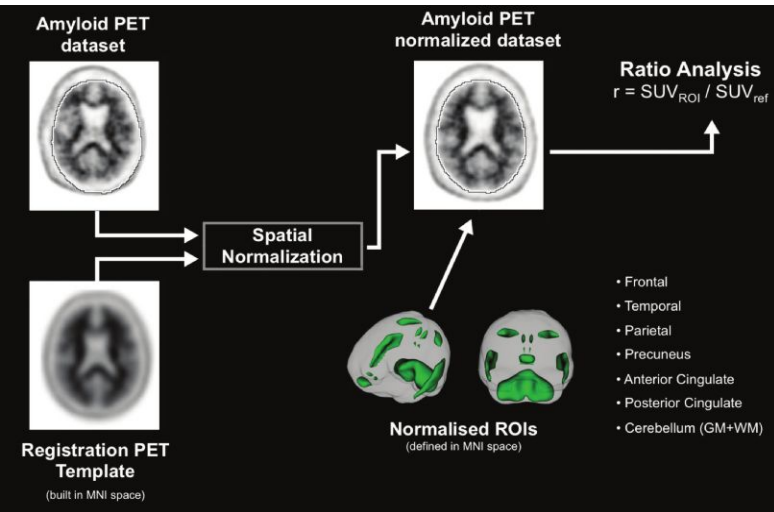
- **TDr** calculation

## Comparison:

- TDr vs. visual assessment
- TDr vs. SUV<sub>r</sub> & ELBA

# SUV<sub>r</sub> [Standardized Uptake Value ratio]

- register on a reference spatial frame (i.e. MNI)
- select reference (cerebellum, brain stem, ...) & target ROI (cortical)
- average counts (single/all ROI) and take the ratio

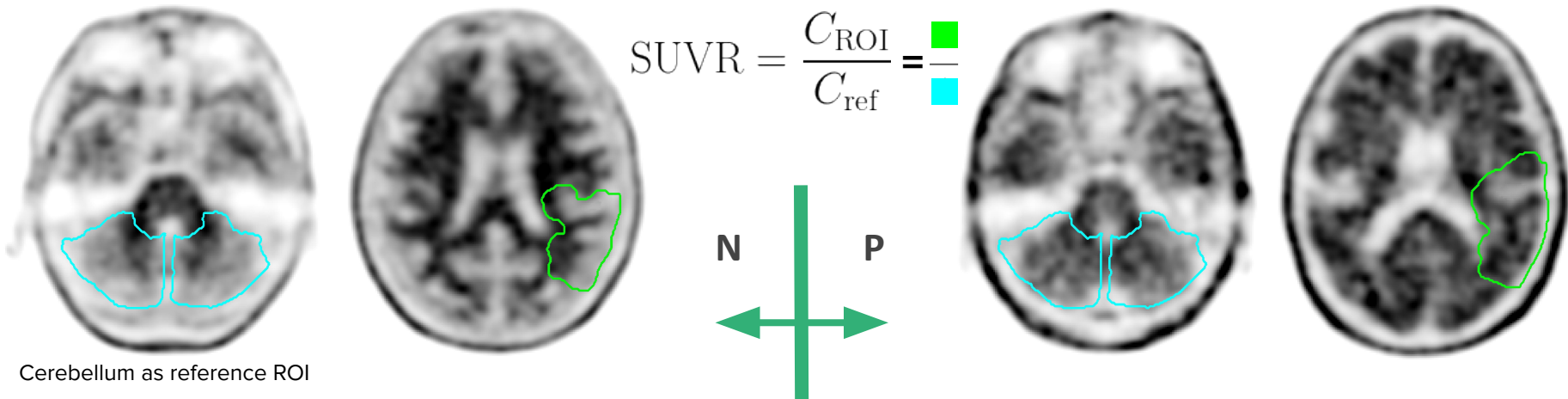


ratio of raw (mean) intensities  
*segmentation dependence*  
*fixed target ROI*  
*fixed reference ROI*

very common quantification approach (Kinahan 2010)

automatic analysis software available

SUV<sub>r</sub> values/outcome critically depend on ROI definitions and positioning



## SUVR method

- Acquisition noise
  - Poor image quality, arbitrariness in acq. parameters
- Physiological noise
  - To some extent canceled by the pathology
  - Issues with severe atrophy (e.g., ventricles enlargement)
- Gold-standard noise
  - Expert reader evaluated images
  - “Weak” gold standard (P/N)
- Data processing noise
  - Implement two other methodologies..

## noises & assumptions

- Additivity
  - Pathologic  $A\beta$  deposit adds to aging-related (incidental) effect
- Linearity
  - Common & significant contribution in all the affected subjects
- Isolation
  - Slow time-scale
- Derivative
  - Smooth transition between N/P

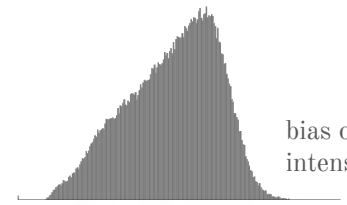
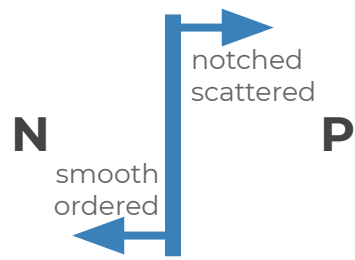
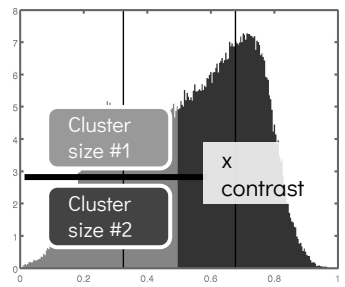
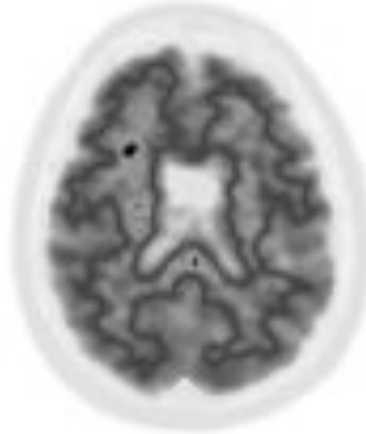
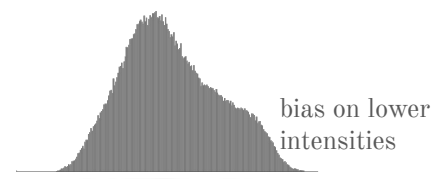
equal mix of geometric properties  
(sphericity) of iso-intensity surfaces &  
intensity statistics

no need for ROIs, no  
need for reference  
uptake!



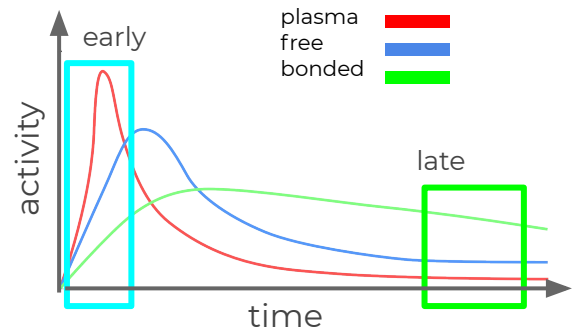
[1] *SUVr-independent evaluation of brain amyloidosis*, Journal of Alzheimer's Disease, Vol. 54-4 (2016)

[2] *Approaches to semi-quantification: beyond SUVr in amyloid imaging*, European Conference on Clinical Neuroimaging, Roma (2016)



# TDr [Time-Delayed ratio]

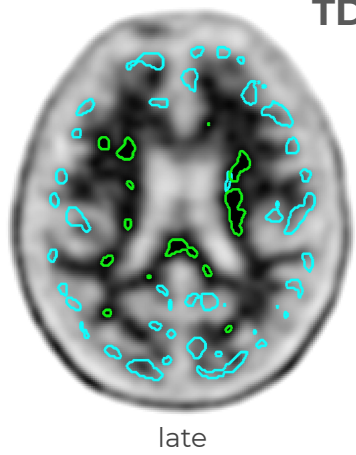
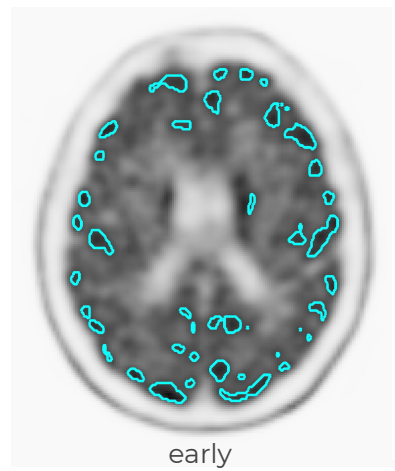
**REQUIREMENT:** early acquisition, proxy of brain blood perfusion (Contractor 2012)



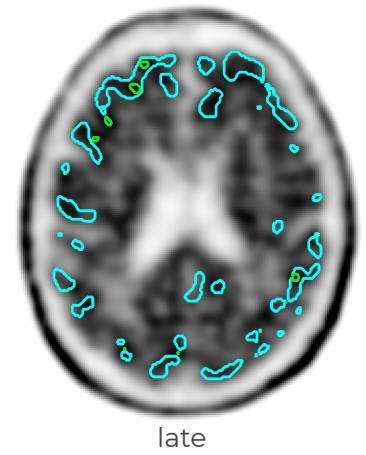
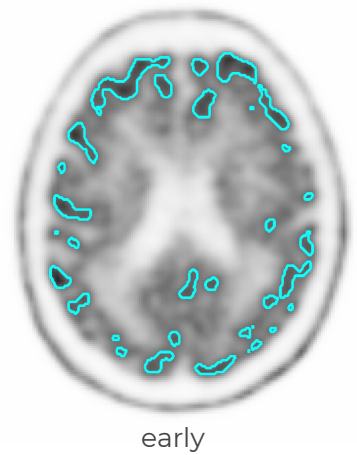
Target	Reference
highest uptake in the <b>early</b> scan (CBF)	highest uptake in the <b>late</b> scan (hot spot)
(Osch 2009)	(Fleisher 2017)

ratio of raw (mean) intensities  
*no segmentation*  
*subject-dependent uptake ROI*  
*subject-dependent reference ROI*

$$\text{TDr} = \frac{\langle I_{\text{late}} \rangle_{\text{Target}}}{\langle I_{\text{late}} \rangle_{\text{Reference}}} = \frac{\text{cyan}}{\text{green}}$$



< N | > P

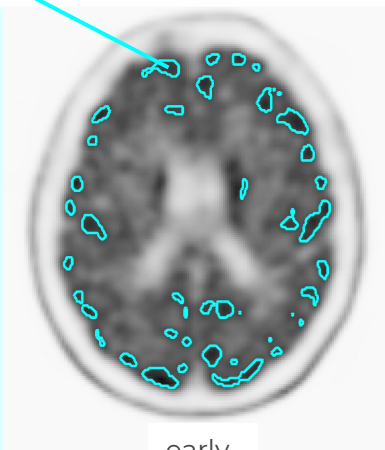


# ROI definition

**Target region ( $D_E$ )**

$$D_E = (v \in E | I_v \geq I_0^E) \quad I_0^E = 0.85$$

percentile on **early** ( $I_0^E$ ) and **late** ( $I_0^L$ ) scan intensity distribution



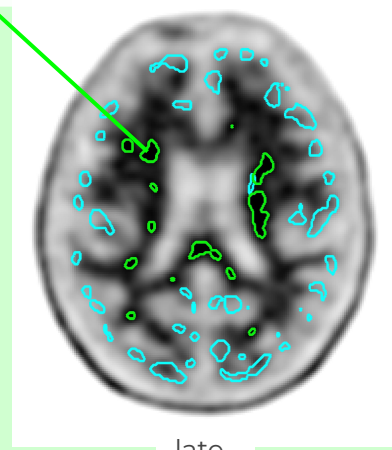
early

average target

ROI thickness  $\mu = 3.1 \pm 1.4$  mm, **comparable** to the cortical GM thickness (Hutton 2008, Lerch 2004)

**Reference region ( $D_L$ )**

$$D_L = (v \in L | I_v \geq I_0^L) \quad I_0^L = 0.99$$



late

**hot spot** on the late scan  
(non negligible volume,  $\mu = 13.47 \pm 1.2$  ml)

# Concordance with visual assessment

Site	TDr	SUV <sub>r</sub>	ELBA
Brescia	1.00	0.99	1.00
Geneva	1.00	0.95	1.00
Genoa	0.99	0.76	0.99
Pavia	1.00	0.94	0.98
Whole set	0.99	0.92	0.99

- AUC (Area Under ROC curve)

- TDr: **discriminating** power (single site, overall)

- Leave-10-out **cross validation**

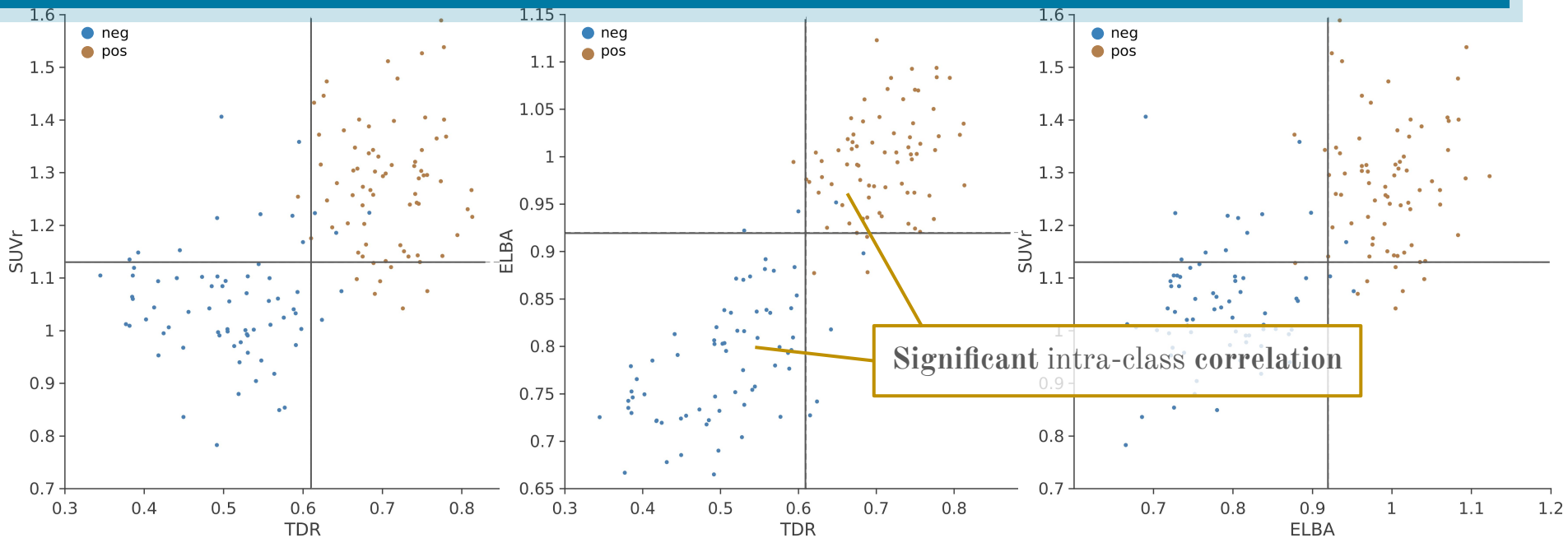
- **500** repetition

- cut-off ( $c_{TDr} = 0.611$ )

- TDr: **excellent performances**

	Accuracy	Specificity	Sensitivity
	[95% CI]		
TDr	0.945 [0.937 0.951]	0.933 [0.931 0.934]	0.957 [0.928 0.970]
SUV <sub>r</sub>	0.862 [0.853 0.874]	0.836 [0.831 0.848]	0.893 [0.864 0.906]
ELBA	0.955 [0.944 0.958]	0.958 [0.958 0.959]	0.953 [0.930 0.957]

# TDr versus SUVr and ELBA



	Methods	whole set	negative	positive
<b>Correlation</b> Pearson $r$	TDr/SUVr	0.61 ( $<10^{-3}$ )	0.08 ( $<0.517$ )	0.002 ( $<0.980$ )
	TDr/ELBA	0.86 ( $<10^{-3}$ )	0.57 ( $<10^{-3}$ )	0.314 ( $<0.006$ )
	SUVr/ELBA	0.66 ( $<10^{-3}$ )	0.21 ( $<0.082$ )	0.03 ( $<0.801$ )

**TDr significantly correlates with SUVr & ELBA**



# Quantification and grading - Data & Study Design

## Cross-sectional data

- **Symptomatic outpatient**
- **175** patients (age [62-88])
- **Clinical suspicion:** MCIAD, possAD, probAD, probFTD, possDLB, probVaD, pseudoDD, aMCI, naMCI, SCI
- **6 centers**
  - HUG (Geneva)
  - IRCCS S.Martino (Genoa)
  - Fondazione Poliambulanza (Brescia)
  - Institute of Mental Health (Mannheim)
  - University of Paris Diderot (Paris)
  - University of Antwerp (Antwerpen)
- **No shared acquisition protocol**

## Late scans:

1. **Visually inspected & labeled** (5 readers, 2 scales)  
(no consensus reached)



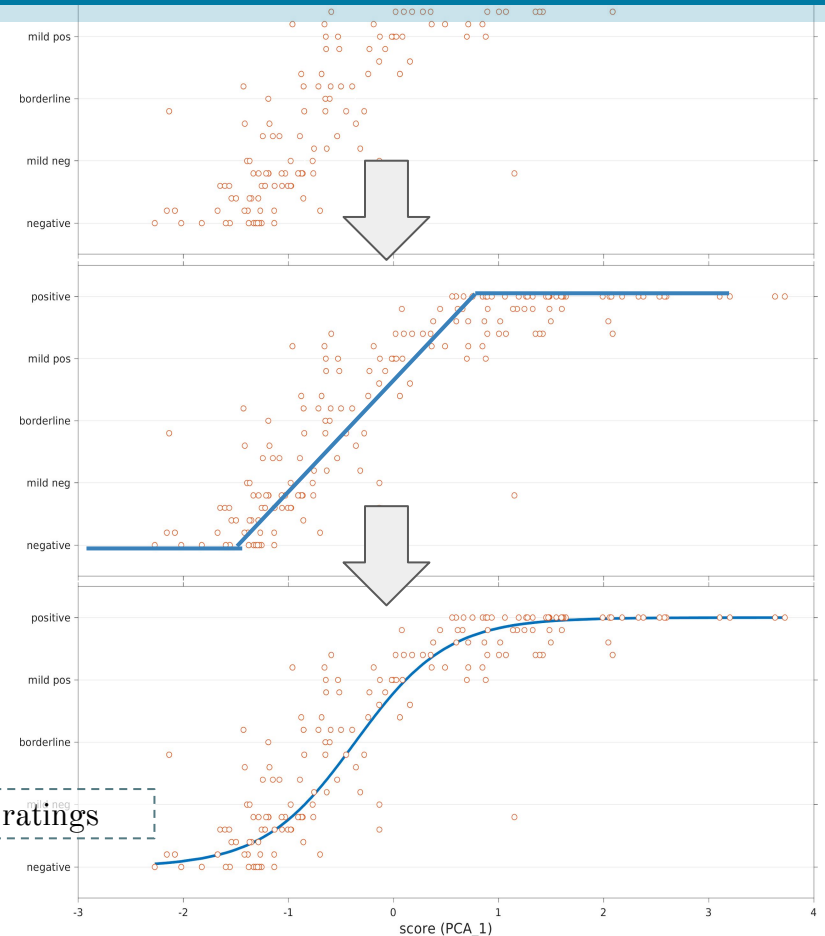
+ 5 yr scan reporting (NM)

2. Processed with **SUVr** & **ELBA** (Chincarini 2016)
3. Investigate link between quantification and 5-step scale
4. Study the “latitude”: the discrepancies of 5-step classification among evaluators

# Quantification and grading - Link with quantification

The *natural* function to link semi-quantification to grading is the **sigmoid**.

It follows from the floor/ceiling effect on the visual reading and the necessity of a [smooth] transition (accumulation is gradual)



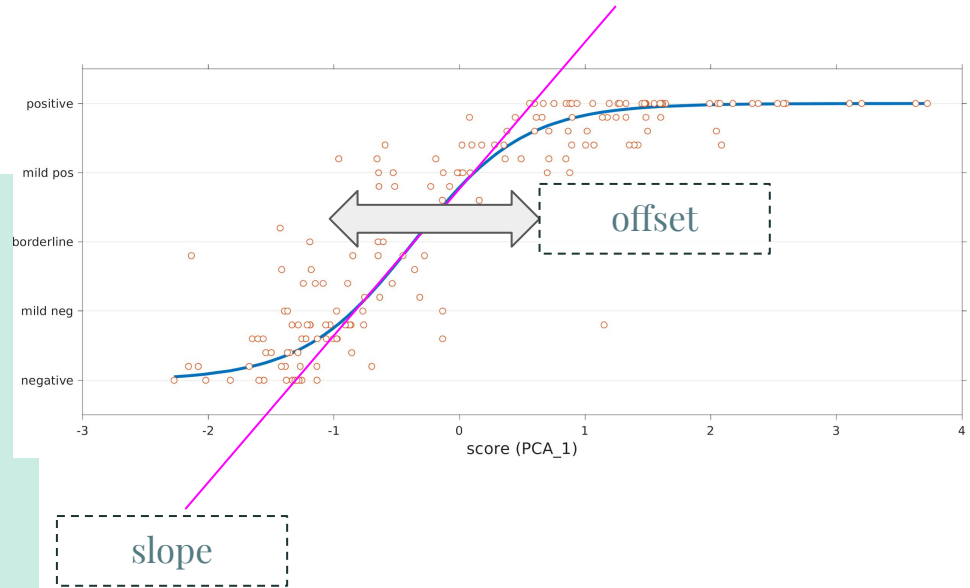
# Quantification and grading - Free parameters

$$Gr(n, p, s, o) = p - \frac{p - n}{1 + e^{-s(q-o)}}$$

$p$  &  $n$  values are set by limiting conditions

Only the slope  $s$  and the offset  $o$  are free parameters.

Only 2 d.o.f. to fit ~60 data points



# Quantification and grading - What can we measure?

the model can be used to study:

## Contrast on tracers

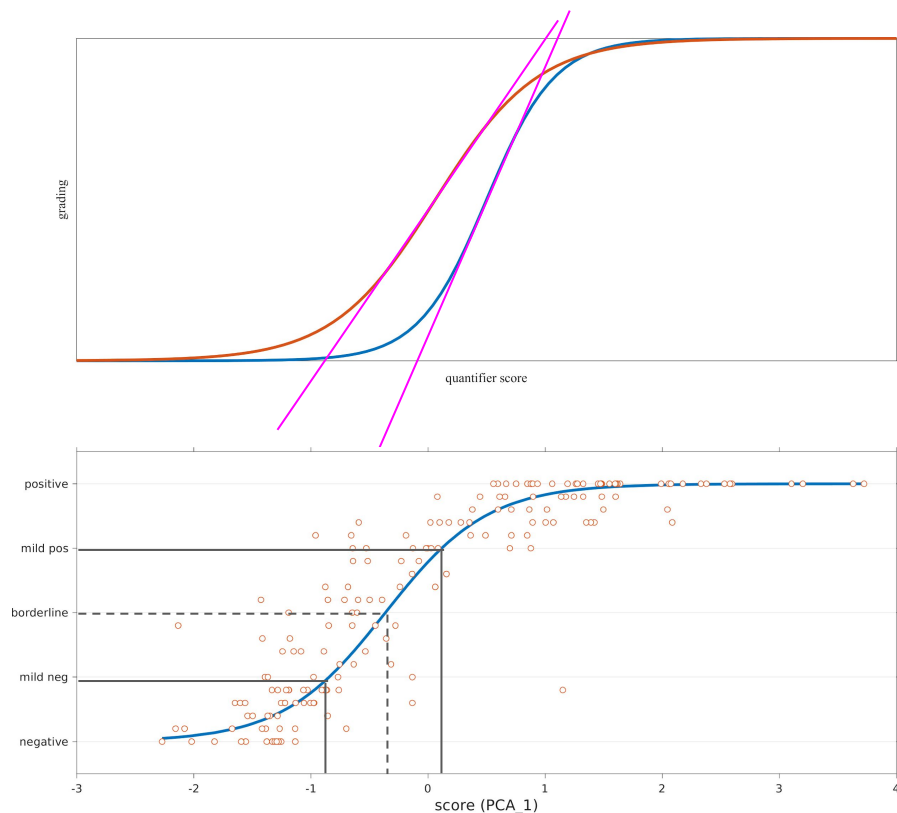
- Different slopes on different quantifiers hint to the degree of neg/pos discrimination of the tracer

## Equivalence of quantifiers

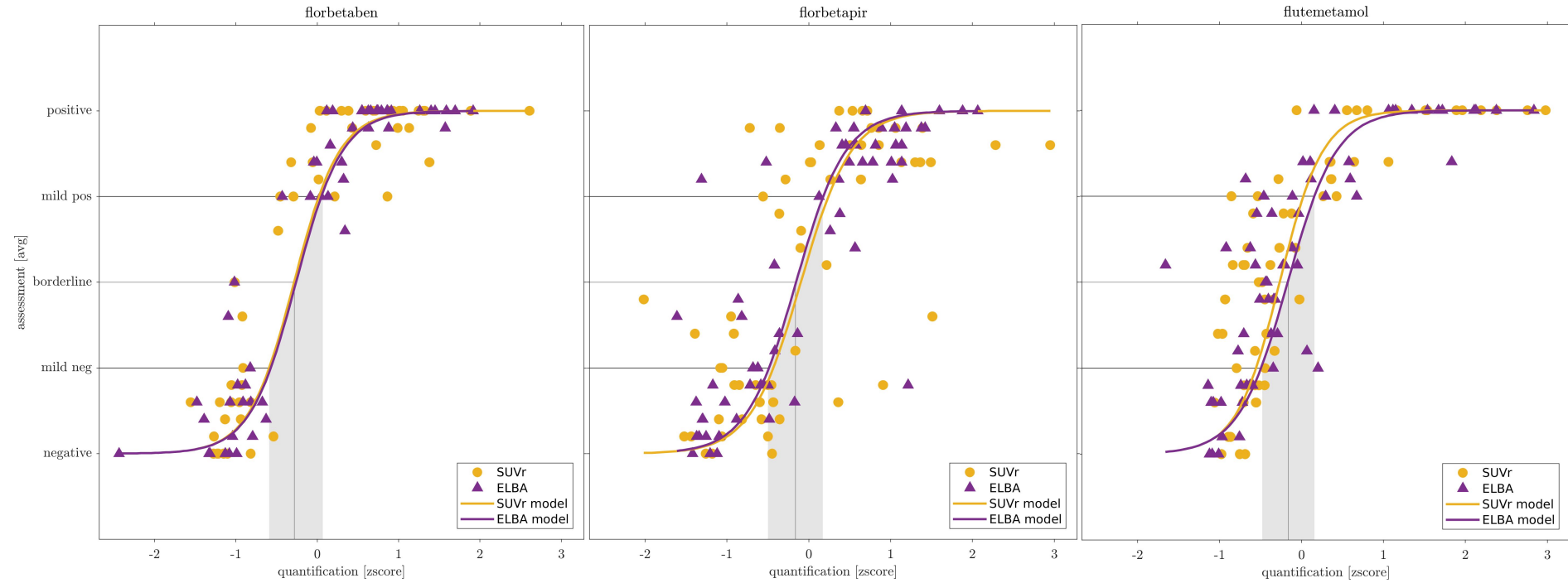
- Similarity of slope and offset for different quantifiers show equal ability to match the visual rating

## Cutoff & Transition region

- model-driven cutoff allow a [almost] population-independent value



# Quantification and grading - Sigmoid models by tracer



# Quantification and grading - Latitude

