

Geant4 applications in MRI-guided x-ray and proton beam therapy

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IV Geant4 International User Conference, Naples, Oct 24-26th 2022



- MRI guided Radiotherapy was first seriously envisaged around 2004
 - 6MV Linac + MRI scanner
 - Geant4 was used to examine the possible dose changes
 - 6MV x-ray beam in a 1.5 T magnetic field

Integrating a MRI scanner with a 6 MV radiotherapy accelerator: dose deposition in a transverse magnetic field

B W Raaymakers¹, A J E Raaijmakers¹, A N T J Kotte¹, D Jette^{2,3}
and J J W Lagendijk¹

Integrated MRI accelerator: dose deposition in a magnetic field

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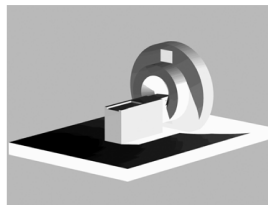
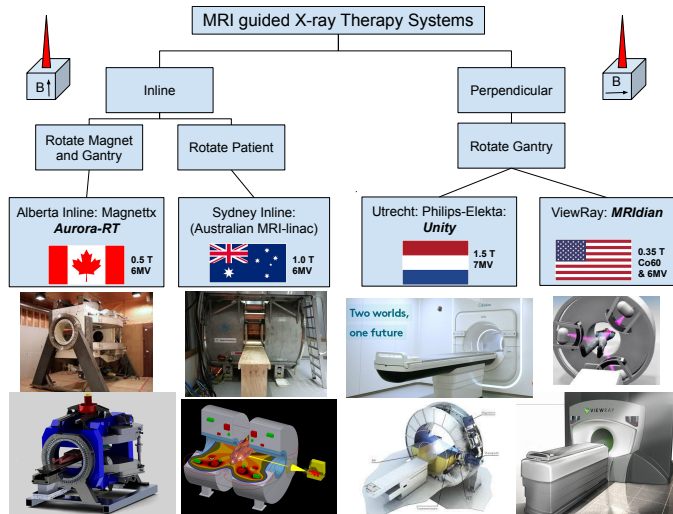


Figure 1. Artistic impression of an integrated MRI accelerator.

Fast forward to now...

- This is a major direction in modern radiotherapy
- There have been a few dosimetry surprises along the way
- Monte Carlo methods have been basically the only option for accurate dose calculations



- MRI guided proton therapy: 2008
 - Proton + MRI scanner
 - Geant4 was used to examine the possible dose changes
 - Proton beam in 0–3 T magnetic field

Feasibility of MRI guided proton therapy: magnetic field dose effects

B W Raaymakers, A J E Raaijmakers and J J W Lagendijk

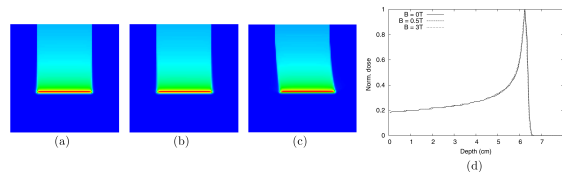
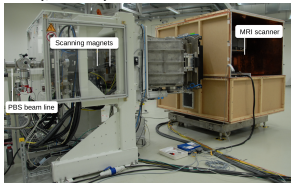


Figure 3. The dose distribution in a homogeneous water phantom for $B = 0$ T (a), 0.5 T (b) and 3.0 T (c) and the central depth dose profiles through the dose distributions (d). Note that there are actually three overlapping lines in (d).

MRPT prototypes and research hardware

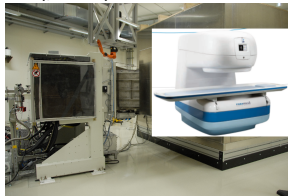
1. Dresden (OncoRay):
0.22 T MRI + horizontal PBS beam line (protons)



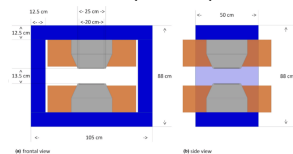
2. Heidelberg (HIT):
0.25 T MRI + horizontal PBS beam line (multi-ions)



3. Dresden (OncoRay):
0.33 T MRI + horizontal PBS beam line (protons)



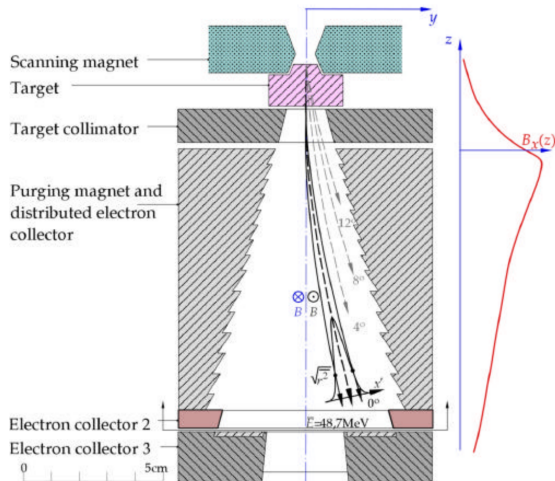
4. Vienna (MedAustron):
small 1 T research dipole magnet +
PBS beam line (multi-ion)



- Much more complicated than MRI-linacs
- First patient treatment planned for OncoRay 2023-2024

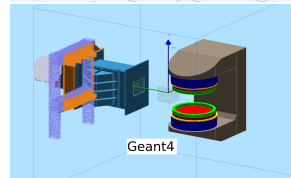
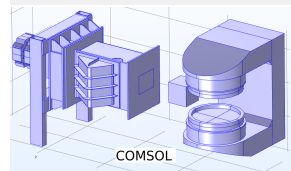
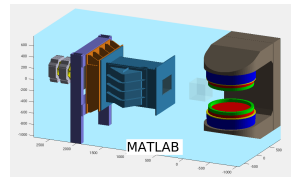
Geant4: Modelling MRI-guided radiotherapy

- Geant4 is a toolkit for radiation transport only
 - No complicated magnetic field modelling
 - Need to import 3D field maps
 - Generate 3D maps in finite element software
- **Purging Magnet** (Advanced Example) ideal for reading in 3D variable magnetic fields
- We are interested in dose changes, beam transport changes
 - SteppingAction class very useful



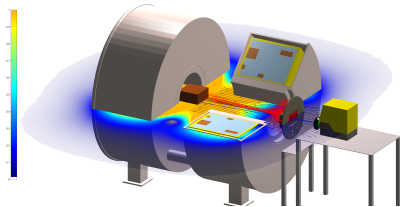
Modelling workflow

- Geometry registration (Matlab)
 - pdf files, some CAD files
 - mostly manually recreated with in-house definitions
 - fundamental boolean solids
- Magnetic Fields (COMSOL)
 - Non-linear solver
 - B-H or magnetization curves
 - electric current sources
 - steels and coil currents important
- Radiation transport (Geant4)
 - geometry location and composition important
 - magnetic field data from COMSOL
 - tedious process linking static data between codes!



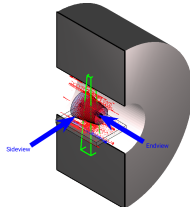
Part 1: MRI-Linac Modelling

- Australian MRI-Linac Program
 - 1 T split bore MRI
 - 6MV Linac
 - 120 Leaf MLC
- About 4 years part time to develop fully benchmarked model

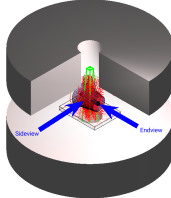


Magnetic field surrounding a phantom: 6 MV beam

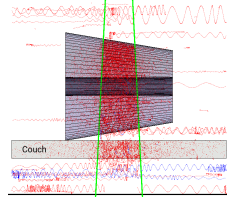
Cutaway: Generic Perpendicular MRI-linac



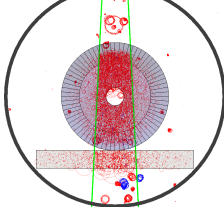
Cutaway: Generic Inline MRI-linac



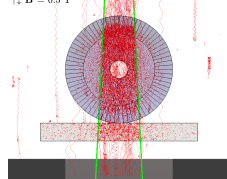
$\rightarrow \vec{B} = 0.5 \text{ T}$



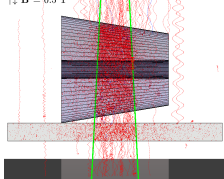
$\odot \vec{B} = 0.5 \text{ T}$



$\updownarrow \vec{B} = 0.5 \text{ T}$



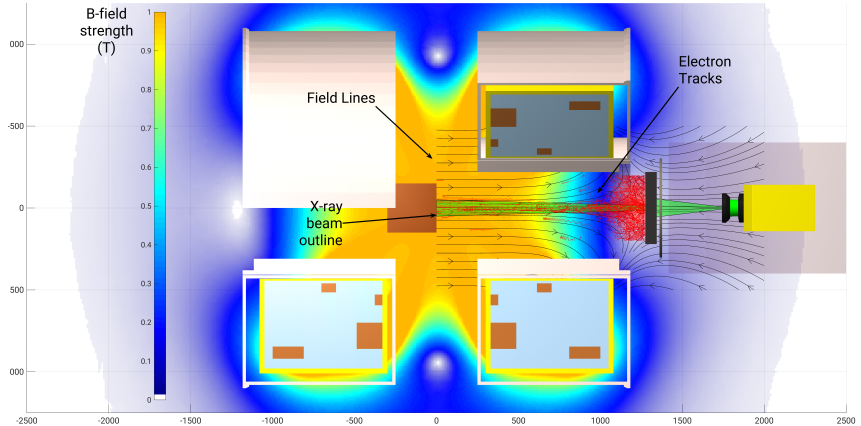
$\updownarrow \vec{B} = 0.5 \text{ T}$



Its all about the secondary electrons!

What about the full beam transport: inline orientation system

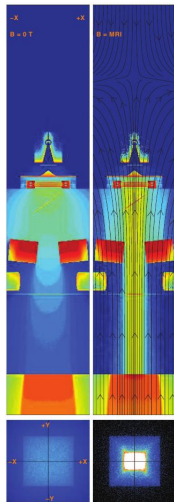
- The fringe field collects and focuses electron contamination
- This was an important discovery with major implications



Electron contamination: inline system

- Skin dose increases of 100-400%
- Various possible workarounds

Oborn *et al.*, Med. Phys. 41 (5), May 2014, 051708-1



Medical Physics

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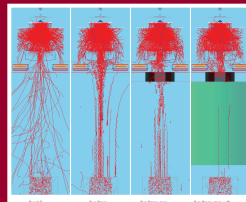


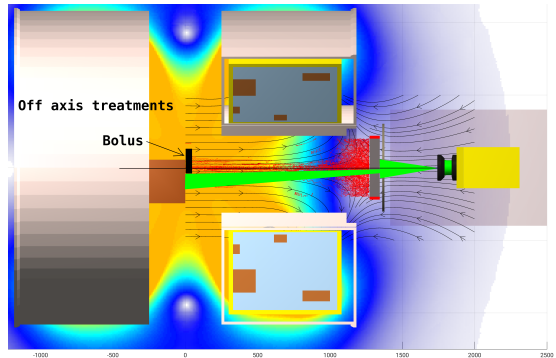
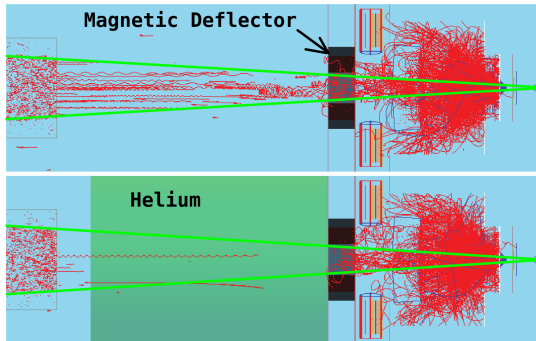
FIGURE 7
GIANT 4 Monte Carlo simulation of the impact of 1 T MRI magnetic field on contaminant electron surface dose for a fixed beam-line MRI-Linac combination. The central axis of the 6 MV photon beam is aligned with the cylindrical symmetry axis of the magnetic field with a source-to-skin distance of 100 cm. The tracks of 10,000 charged particles sampled from the phase space file at the base of flattening filter are shown for a 20x20 cm² field size. (a) B = 0 T magnetic field; (b) B = 1 T MRI with conventional air beam path; (c) B = 1 T with optimal electron contamination-deflector (ECD); (d) B = 1 T with optimal ECD and 71 cm thick helium gas reservoir (green rectangle). Clearly, the MRI field with unmodified beam path introduces a large surface-dose hotspot in the field center which is effectively mitigated by the ECD with helium gas reservoir.

[Figure 7 from Oborn, Kollig, Mercalli, Crozier, Litzberg, and Kroll, "Electron contamination modeling and reduction in a 1 T open bore inline MRI system," Med. Phys. 41, 051708 (15pp) (2014).]

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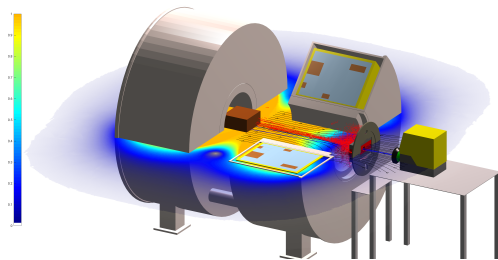
MRI-Linac: skin dose reduction simulations (PhD student projects)

- 1. Bolus above patient and Off-axis treatments
 - Elizabeth Patterson
- 2. Electron deflector and helium zone
 - Madiha Tai



Part 1: MRI-linac modelling - summary

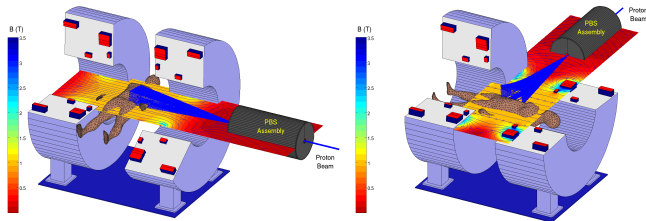
- Geant4 was the first code to be used to investigate the basics of dose changes due to magnetic fields in 2004
 - It has been used extensively at the CMRP over the last 14 years for studying various elements of MRI-Linac radiotherapy
 - It is helping guide the direction taken for the first patient treatments on the Australian MRI-linac system
 - Skin dose predictions very critical
 - Treatment plans will also be checked using Geant4



Part 2: MRI-proton modelling

Topic 1: Beam line transport

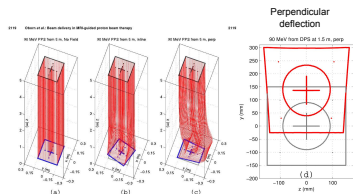
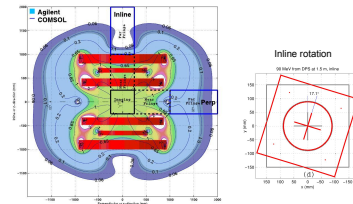
- Sydney MRI scanner
- First realistic look at beam transport through the MRI fringe field
- Implications: must use pencil beam scanning
- Proton beam deflections are important for treatment planning purposes



Proton beam deflection in MRI fields: Implications for MRI-guided proton therapy

B. M. Oborn¹

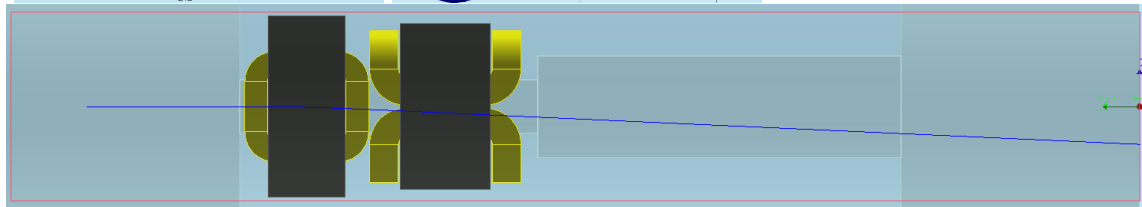
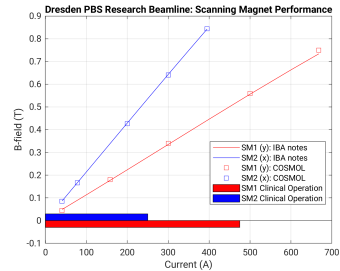
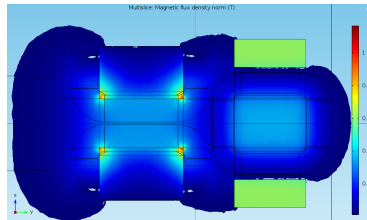
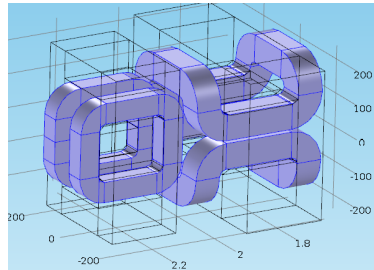
¹Illawarra Cancer Care Centre (ICCC), Wollongong, NSW 2500, Australia and Centre for Medical Radiation Physics (CMRP), University of Wollongong, Wollongong, NSW 2500, Australia



Oborn et al., Medical Physics, Vol. 42, No. 5,

Part 2: MRI-proton modelling

Topic 2: Scanning Magnet Modeling (Full modelling loop)



Inline Orientation Scanning Pattern

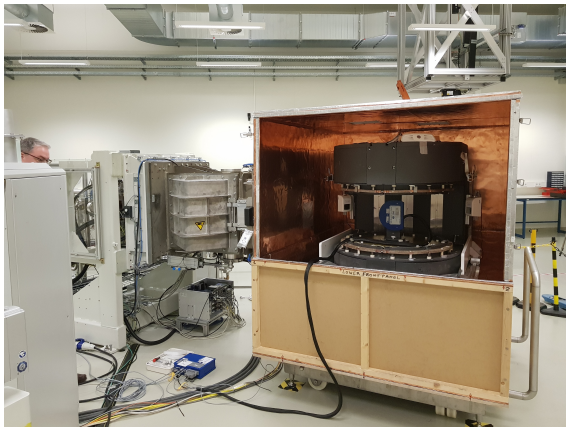
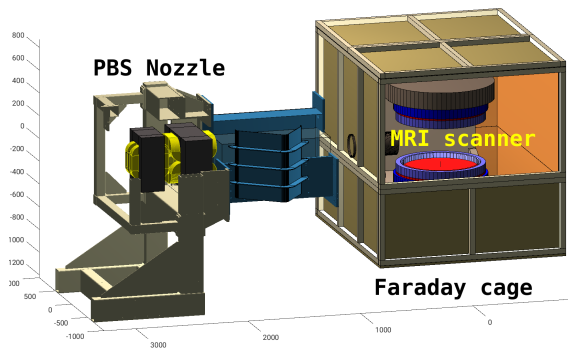
230 MeV pencil beam scanning, scanning magnets in clinical position: ([gif](#))

Perpendicular Orientation Scanning Pattern

230 MeV pencil beam scanning, scanning magnets in clinical position: [\(gif\)](#)

Part 2: MRI-proton modelling

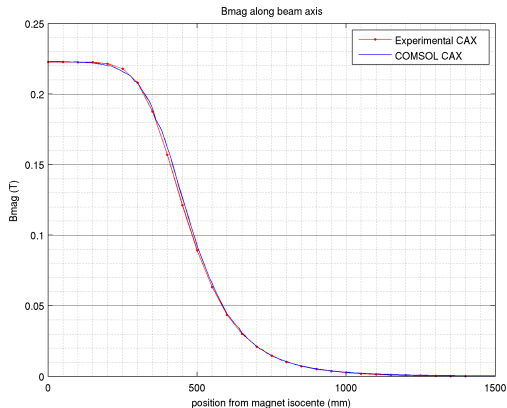
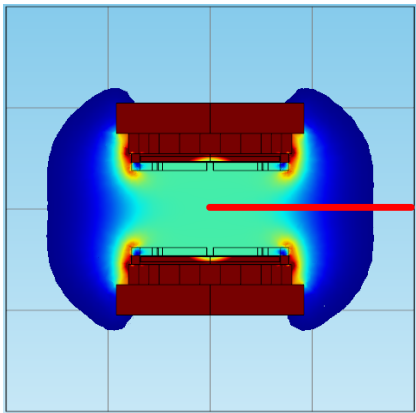
Topic 3: Modeling the OncoRay prototype: MRJ2200 + PBS:



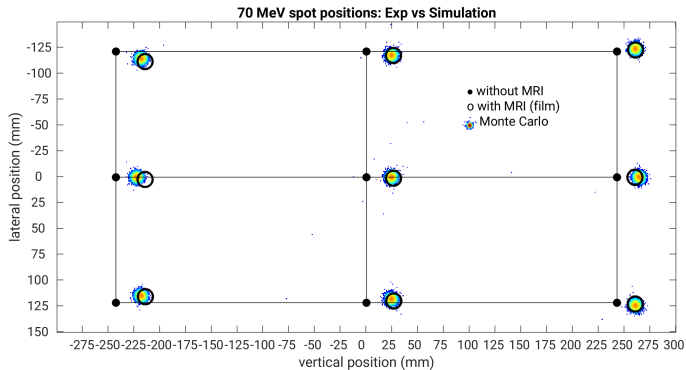
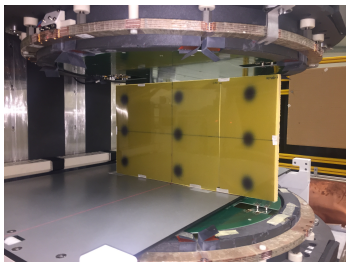
Part 2: MRI-proton modelling

COSMOL magnetic field map

- generally good agreement with experiments along the beamline
- small differences around the shoulder: 2%, 5 mm match



Results: PBS deflection - film vs Monte Carlo

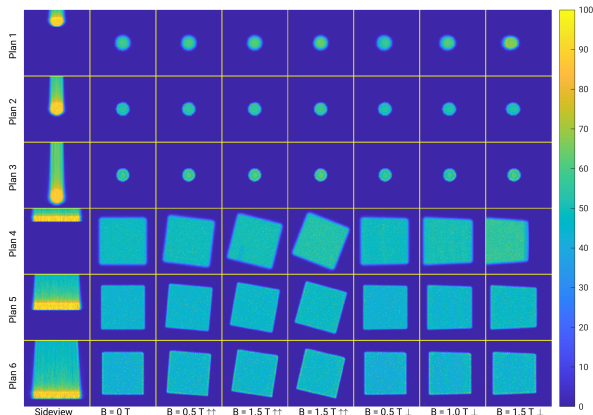


- The errors are related to small inaccuracies in the 3D magnetic field map
- Future work will use full benchmarked MRI models or experimental data for 3D field maps

Part 2: MRI-proton modelling

Topic 4: Electron contamination from proton beams (Entry skin dose)

- Sydney MRI with PBS plans (RayStation)
- 30x30x30 cm water phantom
- 5 cm spherical target
- 20x20x5 cm block target
- 70-213 MeV proton pencil beams
- < 5% dose increases only!
- So why no high skin dose??



Entry Skin doses at 70 μm depth

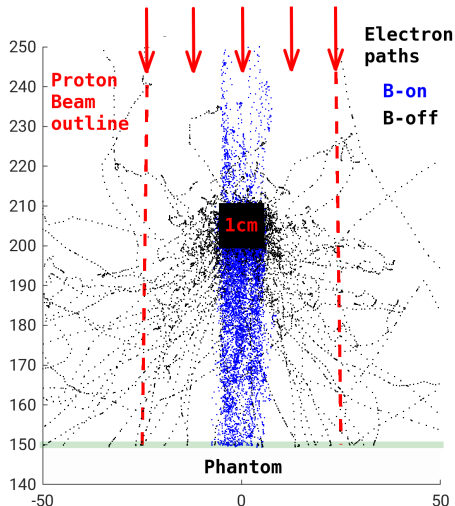
Electron contamination from proton beams: Entry skin dose

- Extract the electron properties starting from a 1 cm cube above the phantom
- Confirm how electrons travel along the field lines
- Examine their energy spectrum

```
void g4qsmSteppingAction::UserSteppingAction(const G4Step * theStep)
{
    ...
    G4Track * theTrack = theStep->GetTrack();
    G4ThreeVector cv = theTrack->GetVertexPosition();
    G4ParticleDefinition* particleType = theTrack->GetDefinition();
    G4String theParticleName = particleType->GetParticleName();

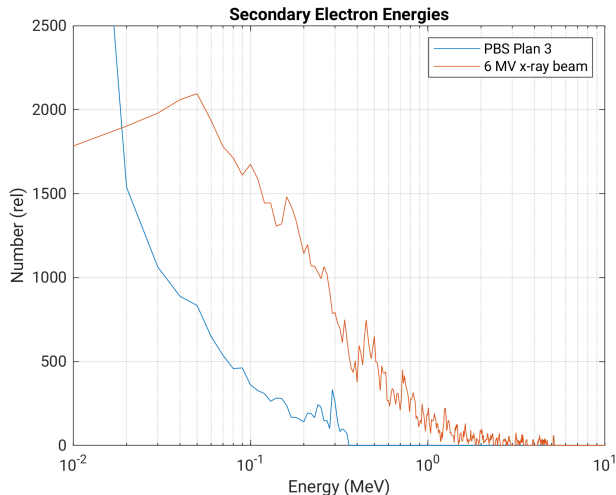
    if (particleType == G4Electron::ElectronDefinition())
    {
        && (cv.x() < 0.5*cm)
        && (cv.x() > -0.5*cm)
        && (cv.y() < 21*cm)
        && (cv.y() > 20*cm)
        && (cv.z() < 0.5*cm)
        && (cv.z() > -0.5*cm)
    }

    { then print the info to a text file...
      //- step locations
      //- energy
    }
}
```



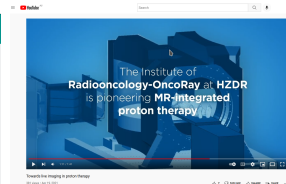
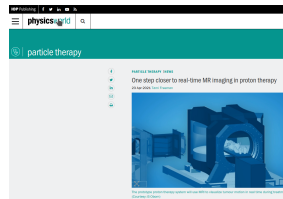
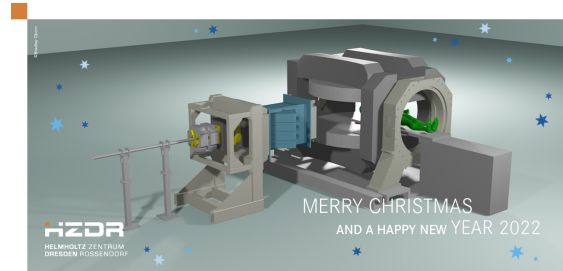
Electron contamination from proton beams: Entry skin dose

- But what about the electron energies?
- Much lower than those produced by x-ray beams!
- **Conclusion:** the secondary electrons simply don't have enough energy to travel long distances in air; no cascade effect towards the surface



Part 2: MRI-proton therapy modelling - summary

- Geant4 was the first code to be used to investigate the basics of dose changes due to magnetic fields in 2008
 - I have used it extensively at the CMRP over the last 8 years for studying various elements of MRI-Linac radiotherapy
 - It is helping guide the prototype development at OncoRay, Dresden
- Future work includes modelling of the next generation 0.5 T MRI system at Dresden



- Geant4 has been used for >15 years to model MRI-guided radiotherapy systems and dosimetry changes
 - Skin dose changes accurately predicted in x-ray therapy
 - Methods to lower skin dose increases modelled, under development at Sydney
 - Important beam transport modelling for MRPT
 - Ongoing modelling with Dresden MRPT development
- Acknowledgements:
 - Geant4 community (and Conference Organizers)
 - Australian MRI-Linac Program and University of Wollongong
 - OncoRay, Dresden
 - IBA, Belgium

Conclusions

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Thanks for your attention!