Medical Physics Research Laboratory


# Geant4 Medical Physics applications at University of Naples Federico II

sarno@na.infn.it

Istituto Nazionale di Fisica Nucleare

# “Siehe Neapel und Stirb” J. W. Goethe

# “Siehe Neapel und Stirb” J. W. Goethe

# “Siehe Neapel und Stirb” J. W. Goethe

# “Siehe Neapel und Stirb” J. W. Goethe

# The team at Medical Physics Research Lab today

**Paolo Russo**
**Professor**
Univ Naples Federico II
INFN Napoli

**Giovanni Mettivier, Phd**
**Associate professor**
Univ Naples Federico II
INFN Napoli

**Antonio Sarno, Phd, Ing**
**Reasearch Associate**
Univ Naples Federico II
INFN Napoli

**Daniele Esposito, Phd, Ing**
**Post-doc researcher**
INFN Napoli

**Laura Cerbone**
**PhD Student**
Scuola Superiore Meridionale, Napoli
INFN Napoli

# Monte Carlo simulation research started in Naples in 1990 (A. Del Guerra and P. Russo)

*Improvements/Enhancements* *Physics Modeling*

**KAND L-SHELL FLUORESCENCE**

- Standard-EGS4 does not create/transport fluorescent photons
- Substitute sampling routine SUBROUTINE PHOTO allows for generation of $K_{\alpha_1}$ and $K_{\beta_1}$ fluorescent photons.
  - Originally developed by Nelson and Jenkins in 1985.
  - Now used as standard in UNIX and PC distributions.
  - Switch (IEDGFL) turns on fluorescence by geometry region.
  - Requires auxiliary subroutine EDGSET (extended by K. Weaver (UCSF) to include all 100 elements).
- Del Guerra *et al.* (1991)[11] have developed K and L-edge sampling scheme for compounds.

11. A. Del Guerra, W. R. Nelson and P. Russo, "A simple method to introduce K-edge sampling for compounds in the code EGS4 for X-ray element analysis", Nucl. Instr. Meth. A306 (1991) 378.

SLAC-PUB-6625
18 August 1994
(N)

DISCLAIMER

This report was prepared as an account of work sponsored by an agency of the United States Government. Neither the United States Government nor any agency thereof, nor any of their employees, makes any warranty, express or implied, or assumes any legal liability or responsibility for the accuracy, completeness, or usefulness of any information, apparatus, product, or process disclosed, or represents that its use would not infringe privately owned rights. Reference herein to any specific commercial product, process, or service by trade name, trademark, manufacturer, or otherwise does not necessarily constitute or imply its endorsement, recommendation, or favoring by the United States Government or any agency thereof. The views and opinions of authors expressed herein do not necessarily state or reflect those of the United States Government or any agency thereof.

*EGS4 in '94*

*A Decade of Enhancements**


W. R. NELSON
*Radiation Physics Department*
*Stanford Linear Accelerator Center*
*Stanford University, Stanford, California 94309, USA*

A. F. BIELAJEW AND D. W. O. ROGERS
*Institute for National Measurement Standards*
*National Research Council of Canada*
*Ottawa, K1A 0R6, Canada*

H. HIRAYAMA
*National Laboratory for High Energy Physics*
*1-1 Oho, Tsukuba-shi, Ibaraki-ken, 305, Japan*

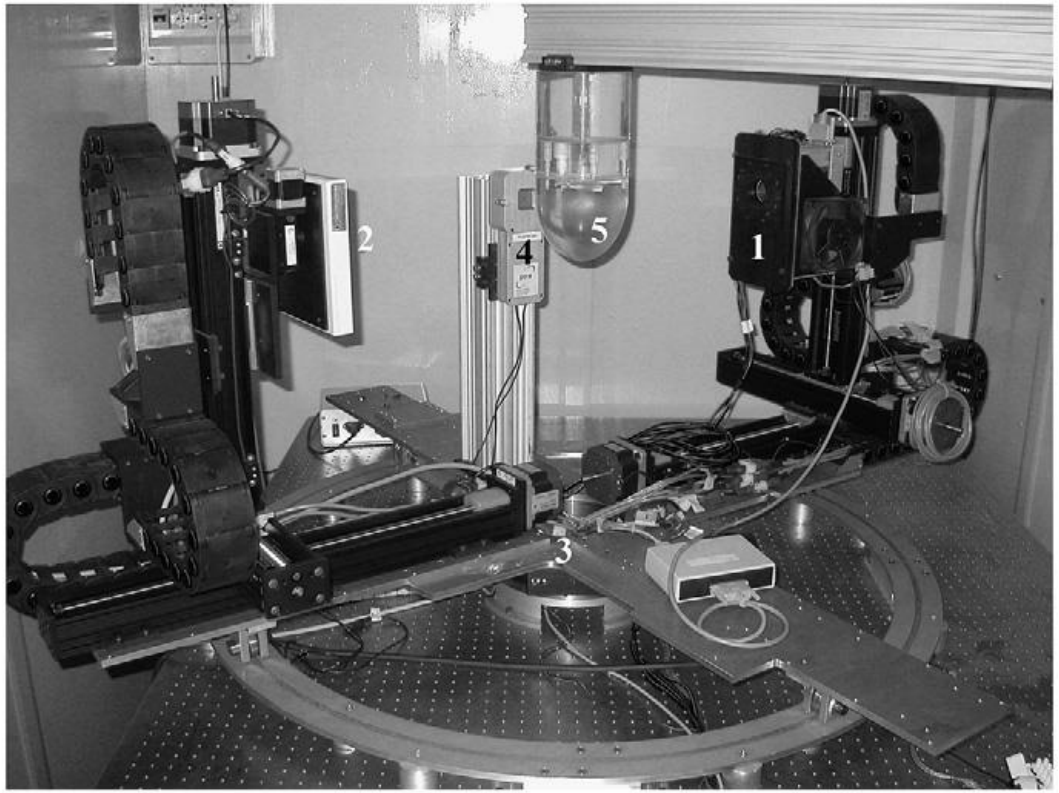


Presented at the World Congress on Medical Physics and Biomedical Engineering
21–26 August 1994, Rio de Janeiro, Brazil


**1994: EGS4 Course held in Capri (fist time outside North America)**

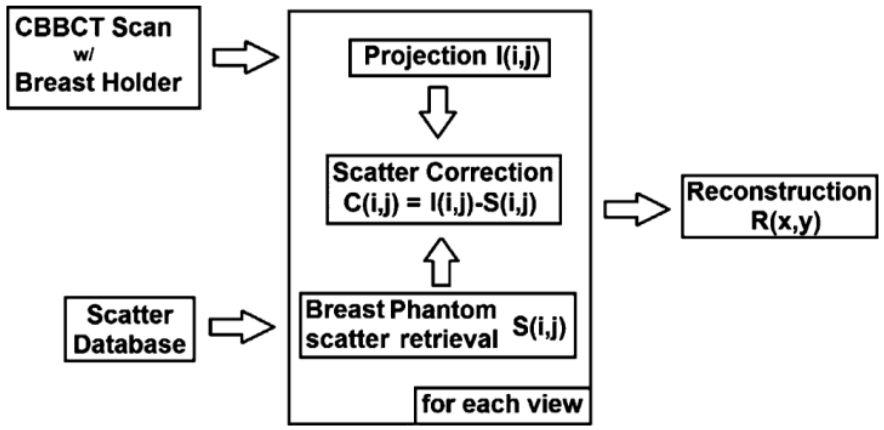
# Recent genesis: 3D breast CT - first prototype in Europe in 2008

Prof. John Boone inaugurates the new BCT prototype in Sep 2009




8 degrees of freedom step-motor drives
Microfocus X-ray tube (80 kV, 0.5 mA)
Breast dedicated CT and SPECT imaging

# Geant4 for scatter correction in breast CT



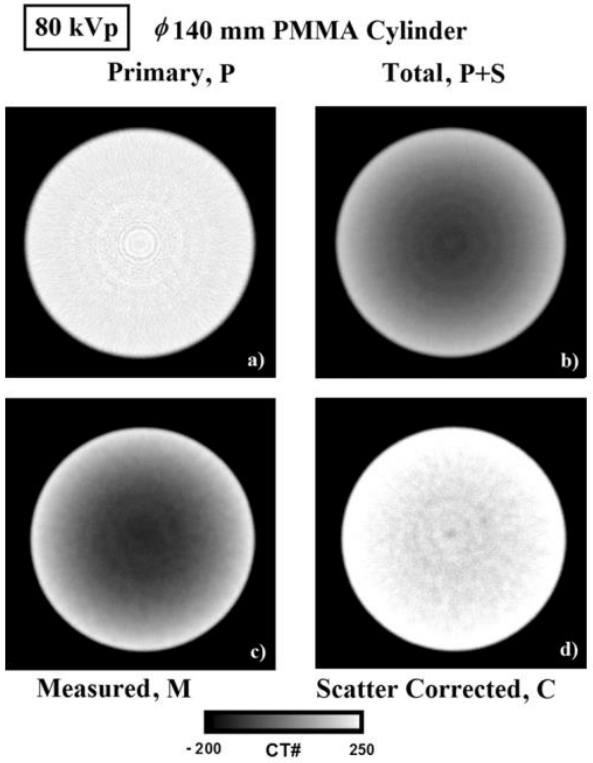




Fig. 8. Simulated primary (a), simulated total (b), measured (c) and scatter-corrected (d) reconstructed axial slices (at 80 kVp) of the 140-mm PMMA cylindrical phantom.

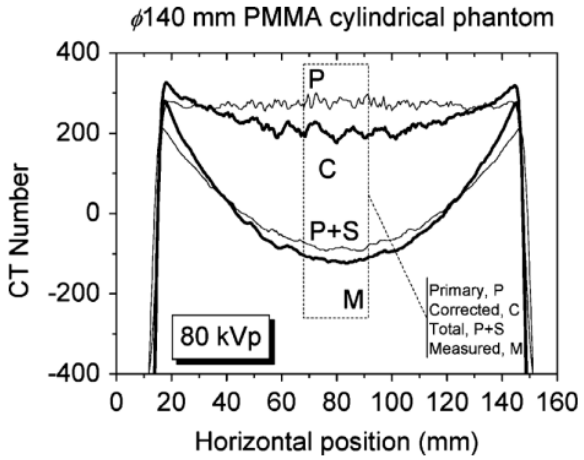



Fig. 9. Line profiles along the diameter of a 140-mm diameter PMMA cylinder on a reconstructed axial slice, at 80 kVp, obtained from simulated primary components only, from simulated total signal (primary plus scatter), from measurements and from measured data corrected for scatter.


Mettivier, G., Russo, P., Lanconelli, N., & Meo, S. L. (2010). Evaluation of scattering in cone-beam breast computed tomography: a Monte Carlo and experimental phantom study. IEEE Transactions on Nuclear Science, 57(5), 2510-2517.

Mettivier G, Lanconelli N, Meo SL & Russo, P. (2012). Scatter correction in cone-beam breast computed tomography: simulations and experiments. *IEEE Transactions on Nuclear Science*, *59*(5), 2008-2019.

# Geant4 for dose distribution assessment in x-ray breast imaging

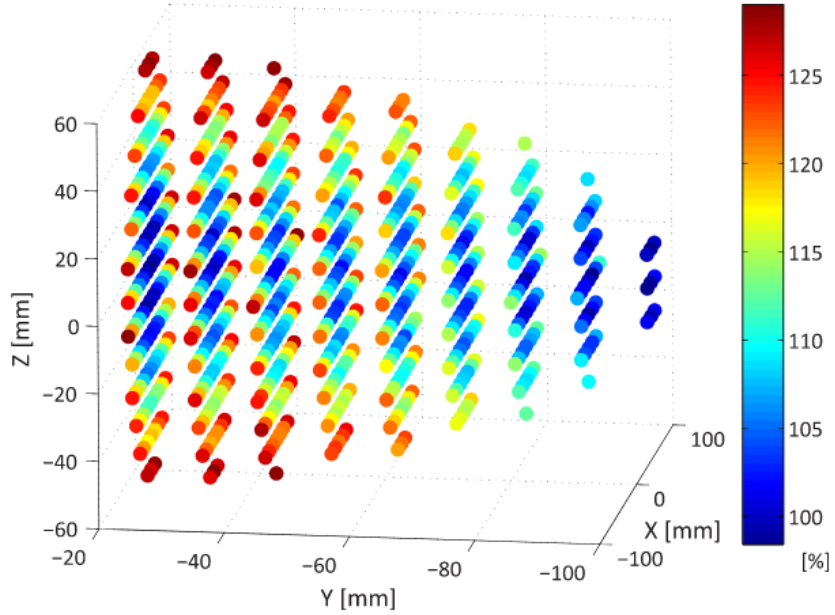



**Figure 4** 3D dose distribution of the PMMA breast phantom irradiated with the 80 kVp beam. The 3D position (*x*,*y*,*z*) of the different voxels is represented along the 3 coordinate axes, whereas their dose values are shown with a color map. Data are normalized to the minimum value registered. The *y*-axis is directed along the scanner rotation axis, with chest wall at left and nipple at right.

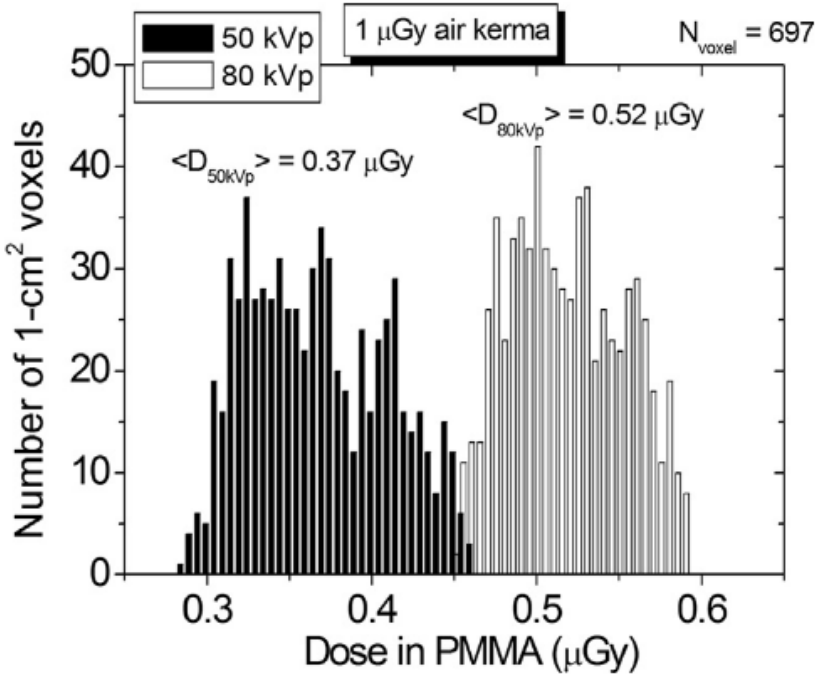
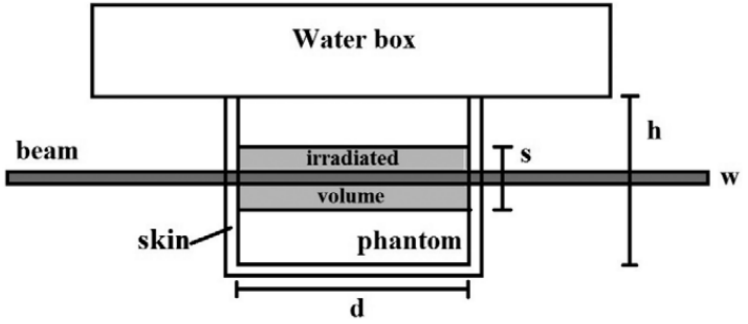



**Figure 6** Histogram of the dose in PMMA breast phantom for two different beams: 50 kVp (black), and 80 kVp (white). The free-in-air air kerma at isocenter was fixed at 1 μGy.

Lanconelli N, Mettivier G, Meo SL & Russo, P. (2013). Investigation of the dose distribution for a cone beam CT system dedicated to breast imaging. *Physica Medica*, *29*(4), 379-387.

# New technologies requires new models: partial breast irradiation with a synchotron radiation beam

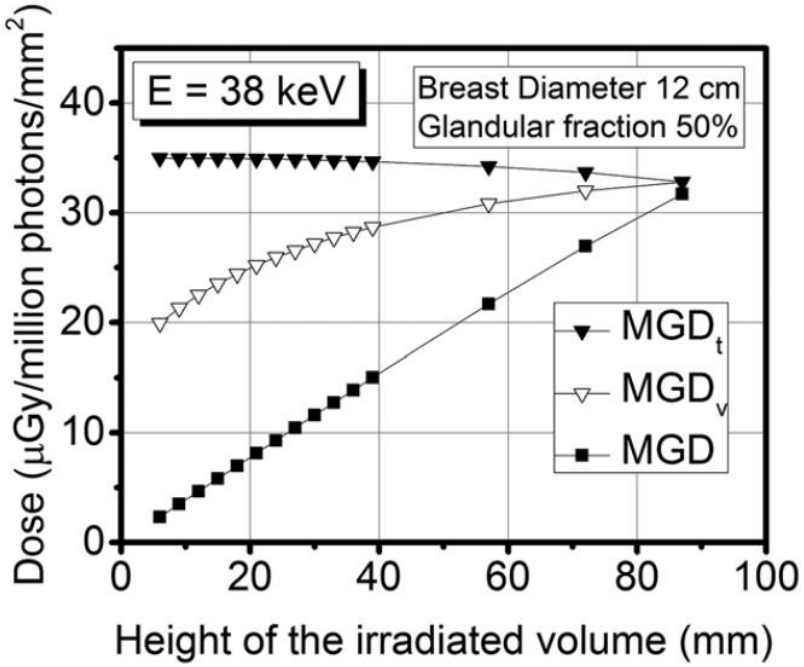
***SYRMA-CT/SYRMA3D INFN national project***


$$MGD = \frac{E_M}{M}$$

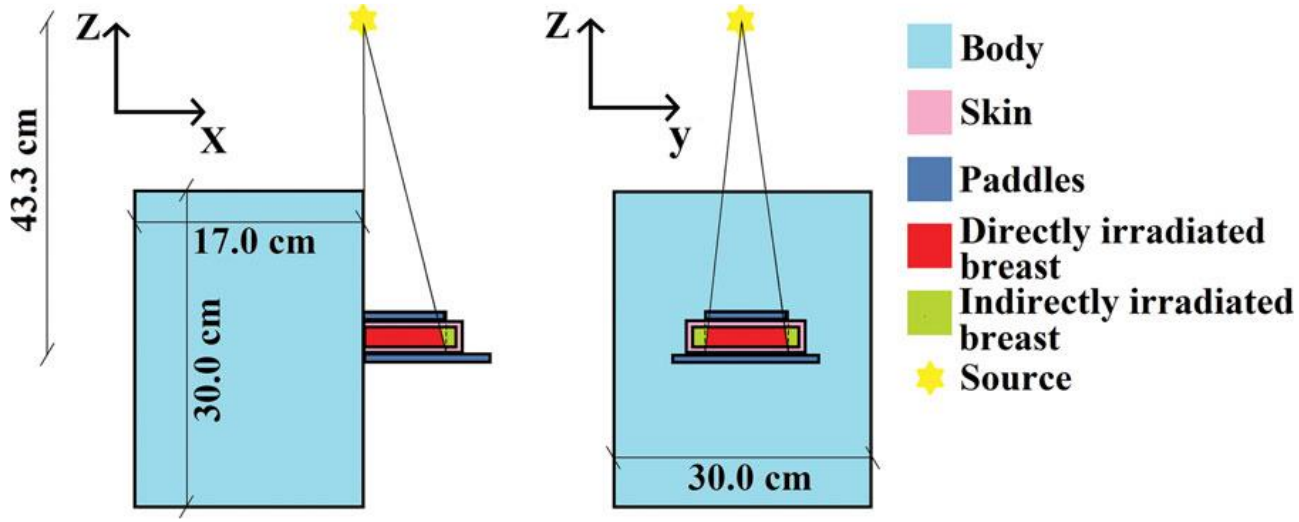
$$MGD_t = \frac{E_M}{m}$$

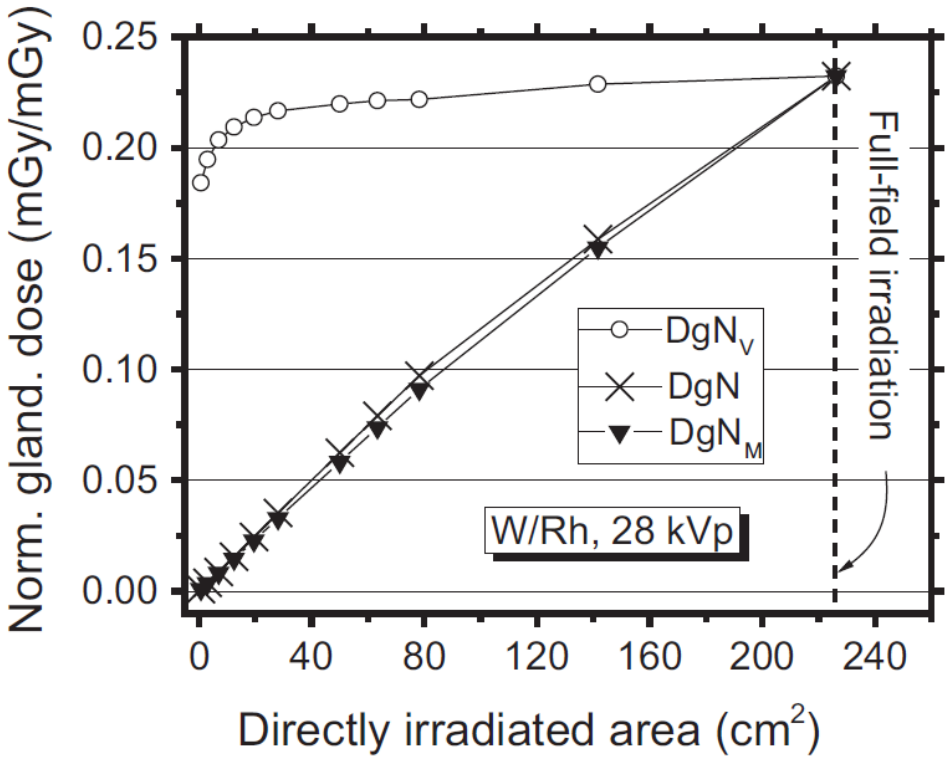
$$MGD_V = \frac{E_m}{m}$$




Mettivier, G., Fedon, C., Di Lillo, F., Longo, R., Sarno, A., Tromba, G., & Russo, P. (2015). Glandular dose in breast computed tomography with synchrotron radiation. *Physics in Medicine & Biology*, *61*(2), 569.

# The case of spot mammography dosimetry: a European collaboration

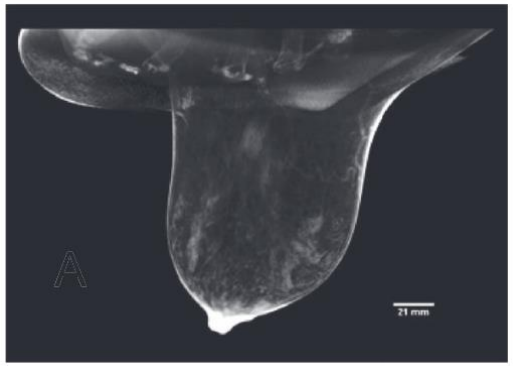



Sarno, A., Dance, D. R., Van Engen, R. E., Young, K. C., Russo, P., Di Lillo, F., ... & Sechopoulos, I. (2017). A Monte Carlo model for mean glandular dose evaluation in spot compression mammography. *Medical physics*, *44*(7), 3848-3860.

# Adoption of a new skin model for mammography dosimetry

**Breast CT for finer skin model: 1.45 mm thick instead of the supposed 4-5 mm**



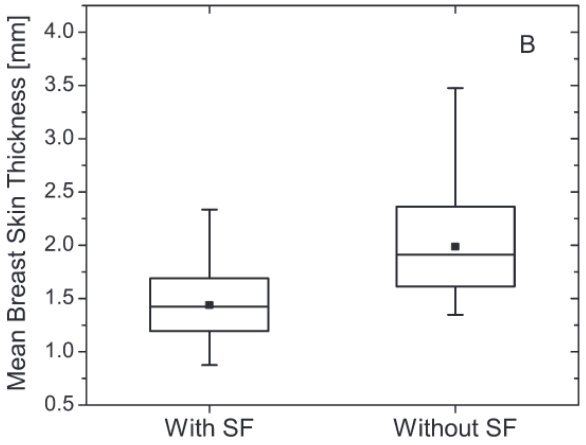
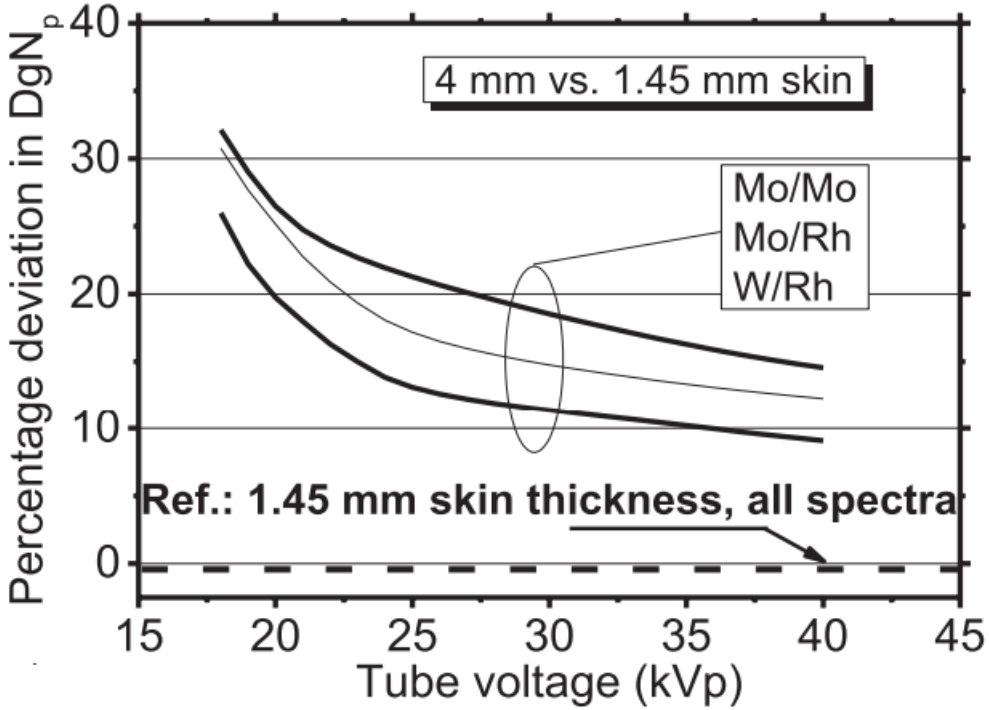




FIG. 1. Histogram (a) and box-plot (b) of the mean (location-averaged) breast skin thickness estimated with and without surface fitting (SF) the segmented skin layer. In the box-plot (b), the symbol within the box represents the mean, the horizontal line within the box represents the median, the box boundaries represent the ±1 SD, and the whiskers represent the minimum and maximum. Wilcoxon signed ranks test indicated that there was a significant difference at the 0.05 level between the two methods ($p = 3.2 \times 10^{-24}$).

Shi L et al. "Skin thickness measurements using high-resolution flat-panel cone-beam dedicated breast CT." *Med Phys* 40.3 (2013): 031913.
Huang S-Y et al. "The effect of skin thickness determined using breast CT on mammographic dosimetry." *Med Phys* 35.4 (2008): 1199-1206.




Sarno, A., Mettivier, G., Di Lillo, F., & Russo, P. (2016). A Monte Carlo study of monoenergetic and polyenergetic normalized glandular dose (DgN) coefficients in mammography. *Physics in Medicine & Biology*, *62*(1), 306.

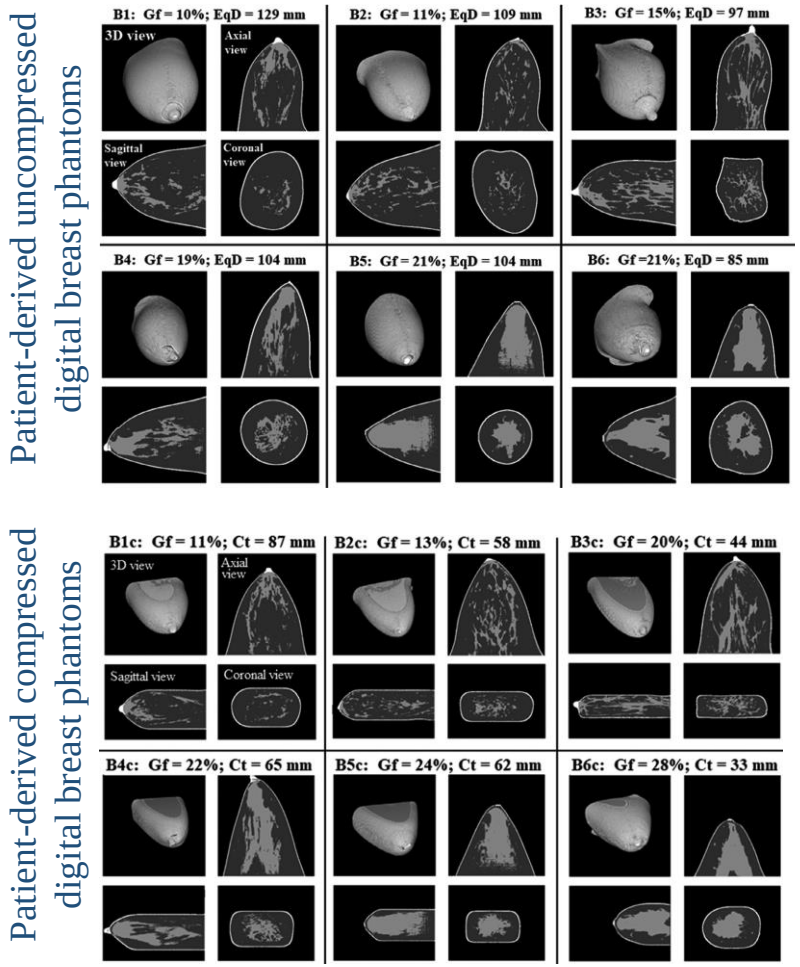
# Recalculation of dose conversion coefficients in DM and DBT

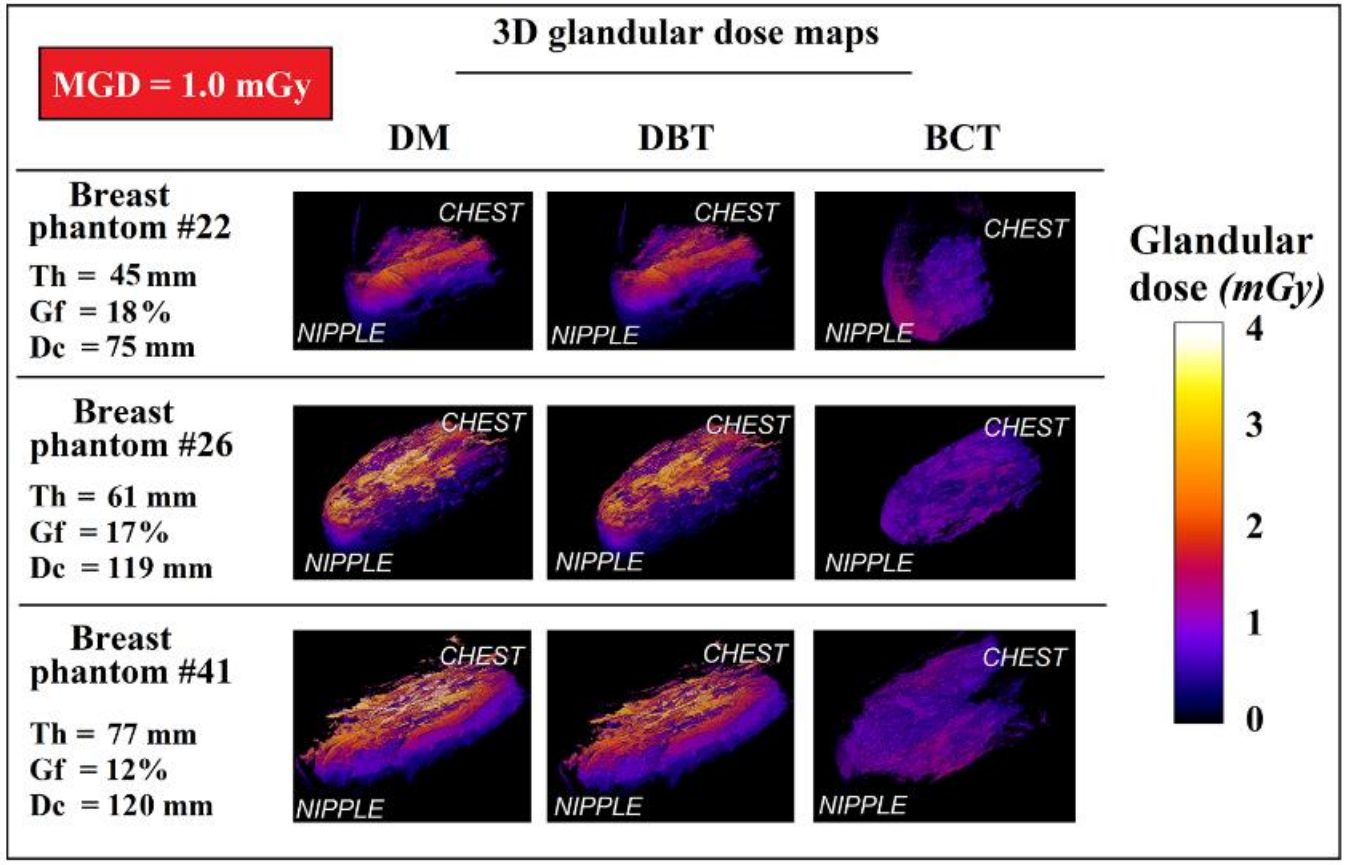
| | A | B | C | D |
|---|---|---|---|---|
| 1 | ***I_DgNdbt v.1.0*** | | | |
| 2 | | | | |
| 3 | **DBT system** | Siemens_Mammomat_Inspiration | | |
| 4 | | | | |
| 5 | **Breast thickness (20 - 90 mm)** | 88.0 | **Tube Voltage (kV)** | 32 |
| 6 | | | | |
| 7 | **HVL (mm Al)** | 0.522 | **Glandular fraction by mass (%) (1-100)** | 40.0 |
| 8 | | **Beam HVL** Type the 1st HVL in mm Al | | |
| 9 | **Interpolated DgN (mGy/mGy air kerma) CC view** | 0.160 | **Input validated** | |
| 10 | | | | |
| 11 | **Color legend:** | **Input data from the user** | **Result** | |


Sarno A et al. "Monte Carlo calculation of monoenergetic and polyenergetic DgN coefficients for mean glandular dose estimates in mammography using a homogeneous breast model." *Phys Med Biol* 64.12 (2019): 125012.

Sarno A et al. "Normalized glandular dose coefficients for digital breast tomosynthesis systems with a homogeneous breast model." *Phys Med Biol* 66.6 (2021): 065024.

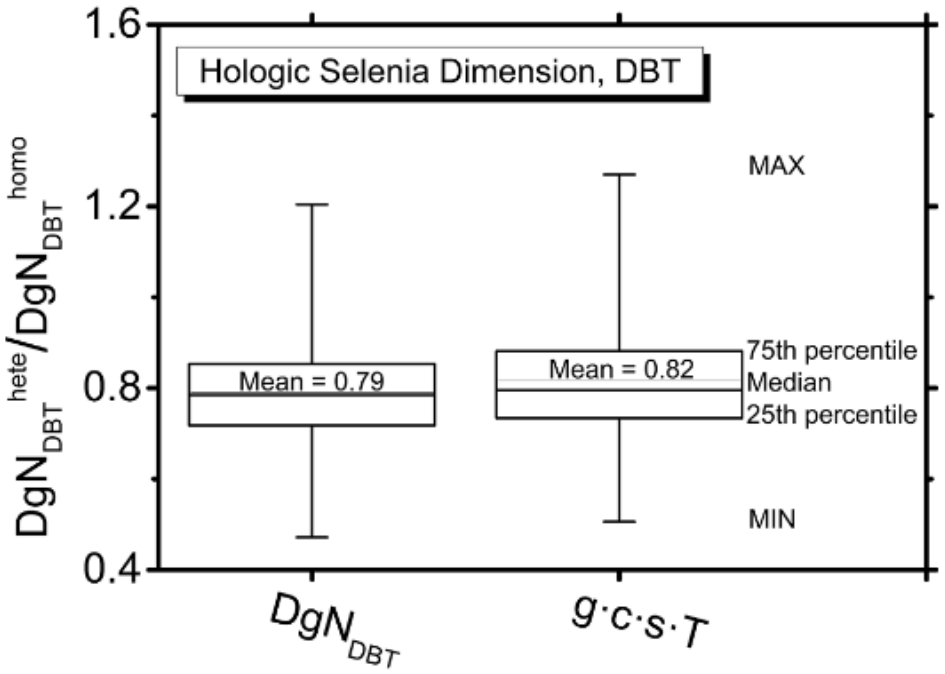
# Homogeneous vs. non-homogeneous models in x-ray breast imaging

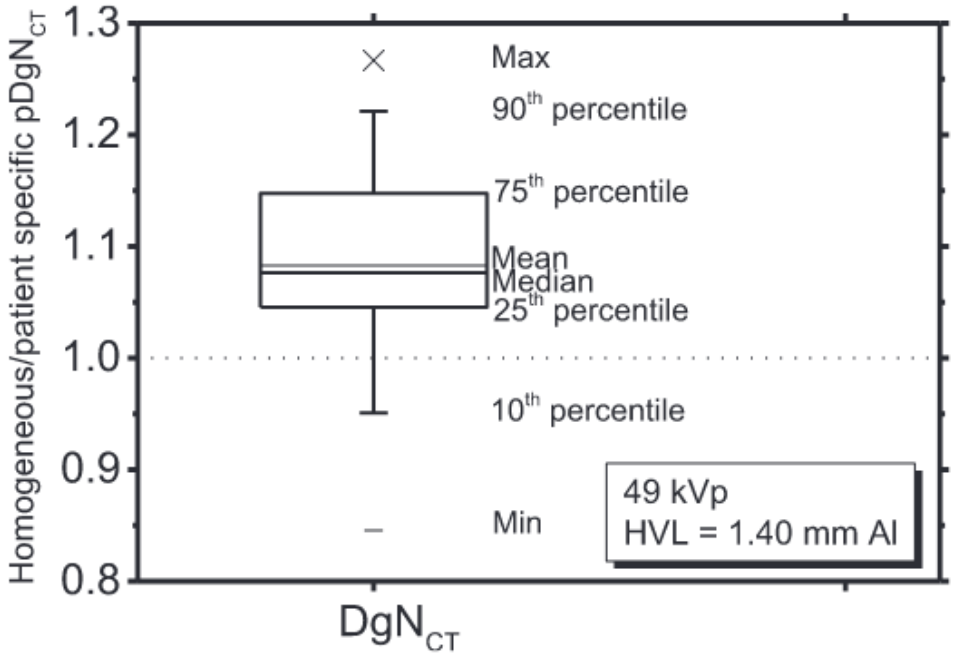



Sarno A et al. "Dataset of patient-derived digital breast phantoms for in silico studies in breast computed tomography, digital breast tomosynthesis, and digital mammography." Medical Physics 48.5 (2021): 2682-2693; Dataset available on zenodo.org, https://doi.org/10.5281/zenodo.4529852 and https://doi.org/10.5281/zenodo.4515360
Sarno A et al. "Comparisons of glandular breast dose between digital mammography, tomosynthesis and breast CT based on anthropomorphic patient-derived breast phantoms." Physica Medica 97 (2022): 50-58.

# Is a new paradigm necessary in x-ray breast imaging dosimetry?



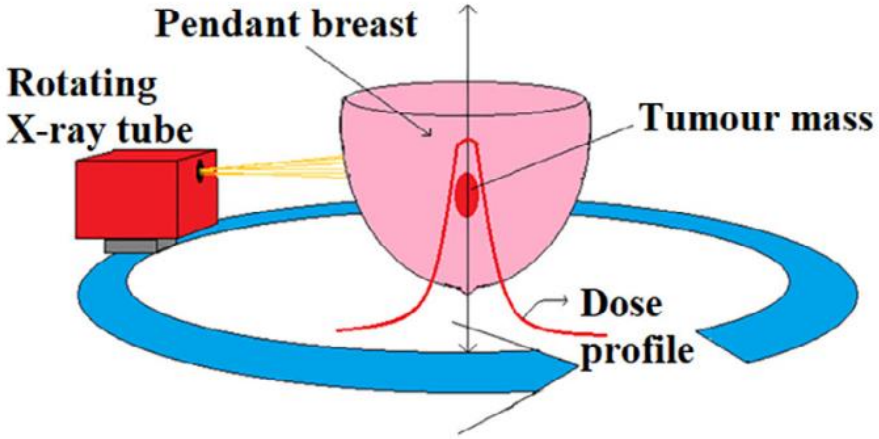


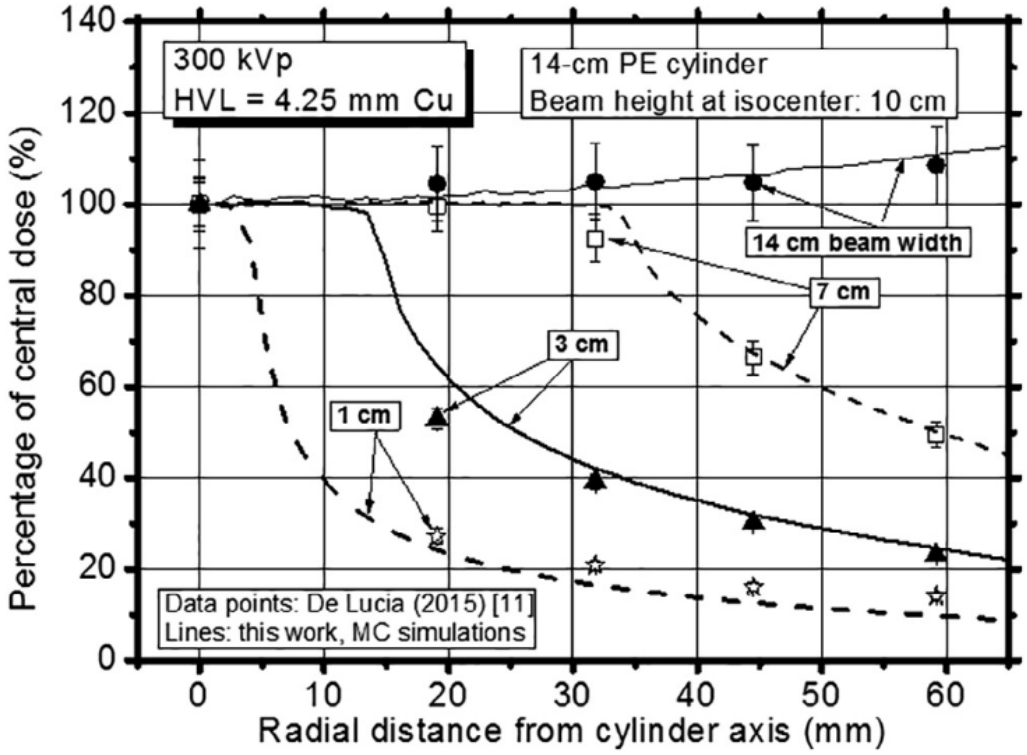
Sarno A et al. "Homogeneous vs. patient specific breast models for Monte Carlo evaluation of mean glandular dose in mammography." *Physica Medica* 51 (2018): 56-63.

Sarno A et al. "Comparisons of glandular breast dose between digital mammography, tomosynthesis and breast CT based on anthropomorphic patient-derived breast phantoms." Physica Medica 97 (2022): 50-58

Sarno A et al. "Monte Carlo evaluation of glandular dose in cone-beam X-ray computed tomography dedicated to the breast: Homogeneous and heterogeneous breast models." Physica Medica 51 (2018): 99-107.

# Kilovoltage rotational breast radiotherapy: innovative approach at low photon energy

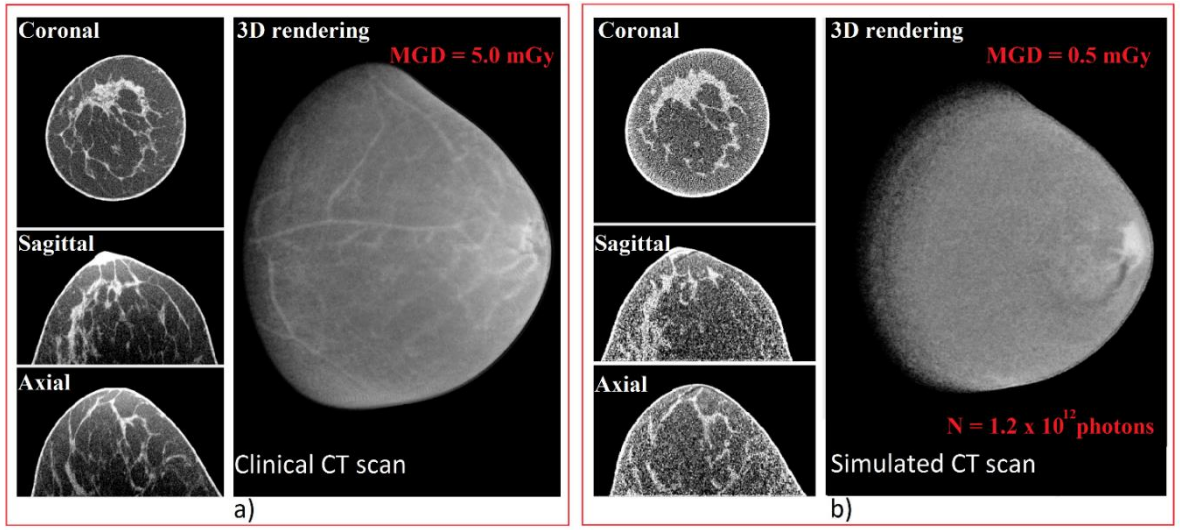


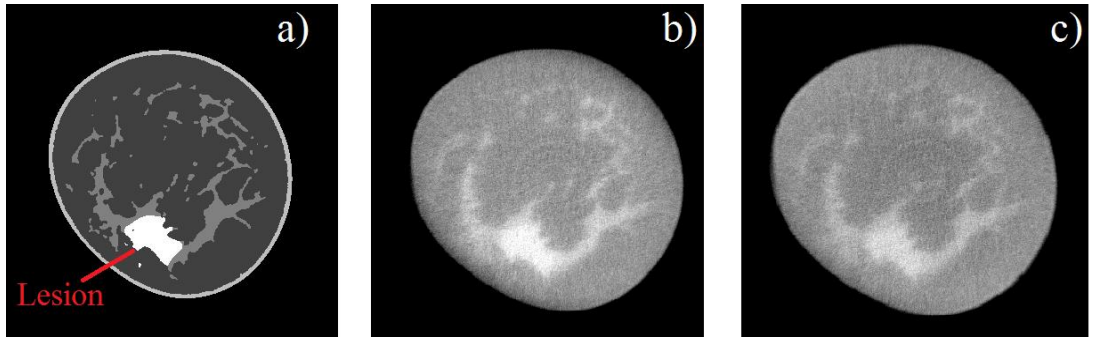




MC simulation and experimental validation at 300 kV of a technique initially proposed by J. Boone 2012

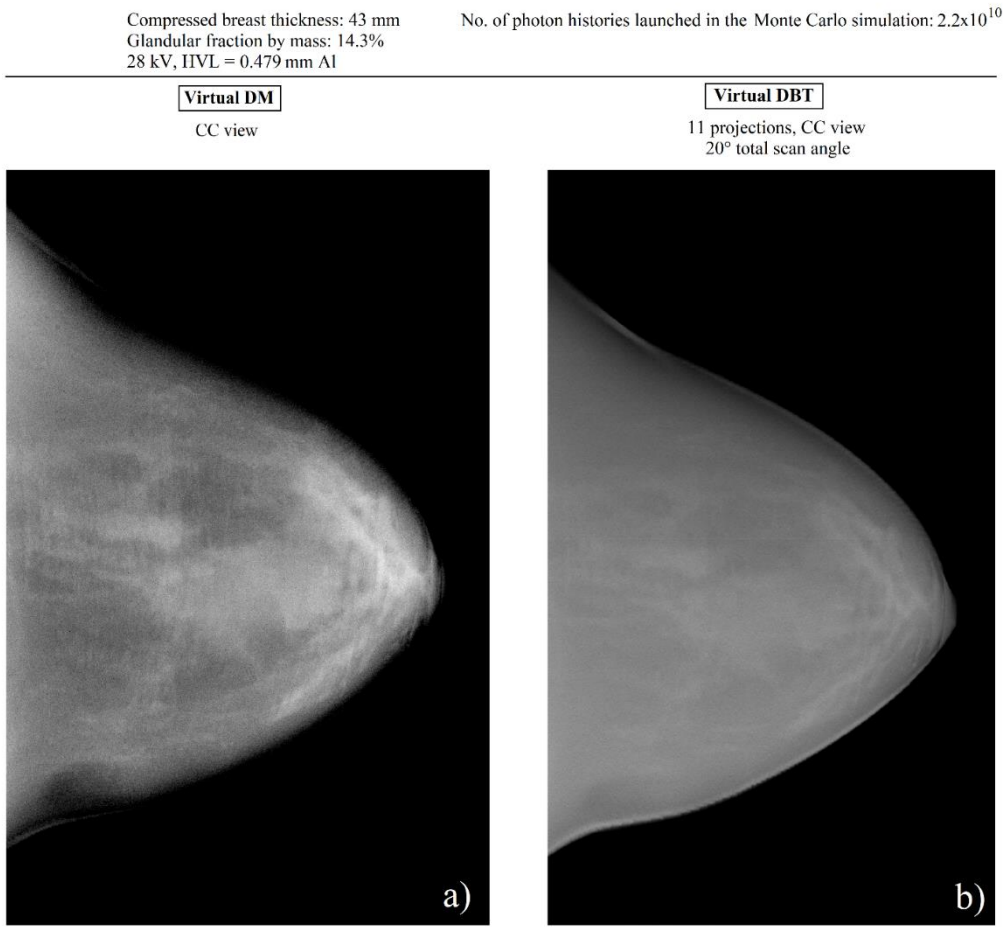
Buonanno F. et al. "Rotational radiotherapy of breast cancer with polyenergetic kilovoltage X-ray beams: An experimental and Monte Carlo phantom study." *Phys Med* 62 (2019): 63-72.

# Virtual clinical trials in x-ray breast imaging: the AGATA project




Digital phantom | Energy window: 1-80 keV | Energy window: 10-50 keV





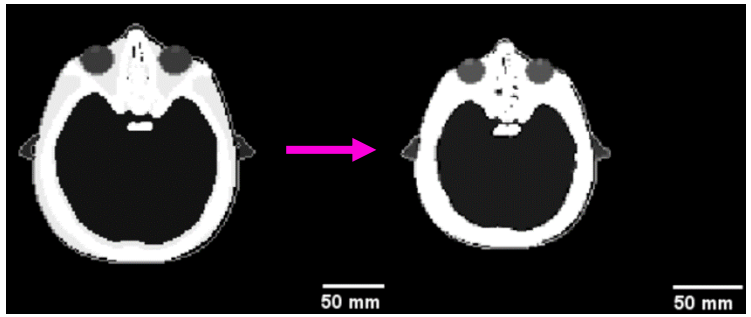
di Franco F et al (2020). GEANT4 Monte Carlo simulations for virtual clinical trials in breast X-ray imaging: Proof of concept. Physica Medica, 74, 133-142.

Sarno A et al. "Advanced Monte Carlo application for in-silico clinical trials in X-ray breast imaging." *IWBI2020*. Vol. 11513. SPIE, 2020.


*Further details in the presentation that will be taken by A. Sarno “Noise in accelerated in-silico x-ray breast images: impact on the breast anatomy and the detector”, Monday, Sess II

# New models for dosimetry in CT: 3D optical scanning for personalized dose estimates before the CT scan

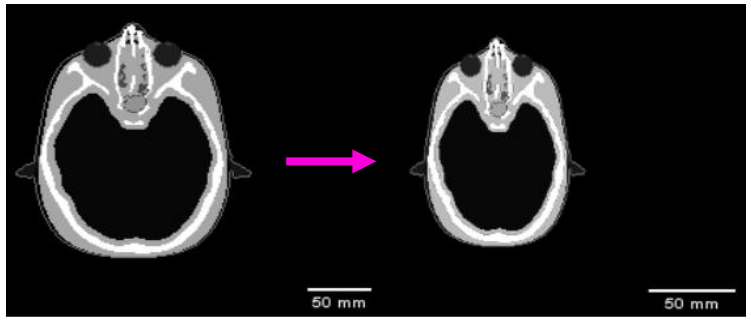
## *Male adult*




Relative discrepancies between standard and customized phantoms

| Tube spectrum | Brain | Eyeballs dose | Lens dose | Pituitary gland dose |
|---|---|---|---|---|
| **80 kV** | +0.8 | -7.4 | -10.2 | +4.9 |
| **100 kV** | -2.7 | -9.2 | -13.1 | -0.7 |
| **120 kV** | -4.5 | -10.0 | -12.2 | -4.1 |
| **135 kV** | -5.1 | -9.9 | -13.7 | -4.9 |

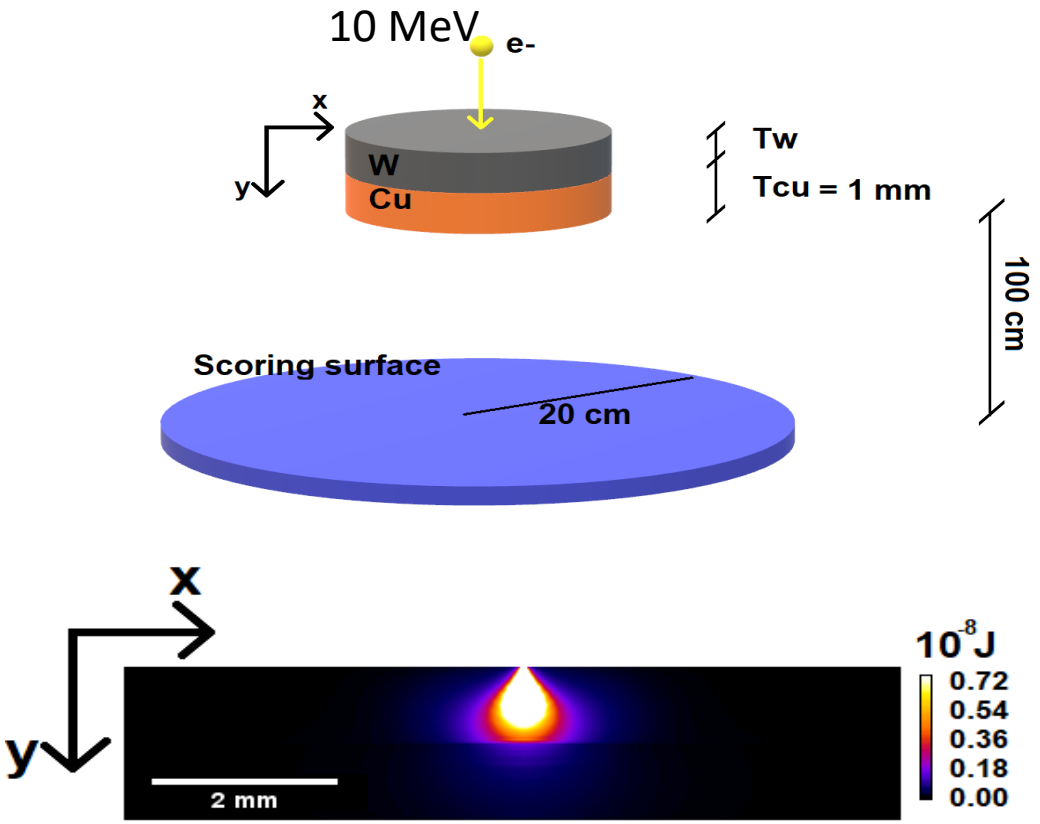
## *Female adult*



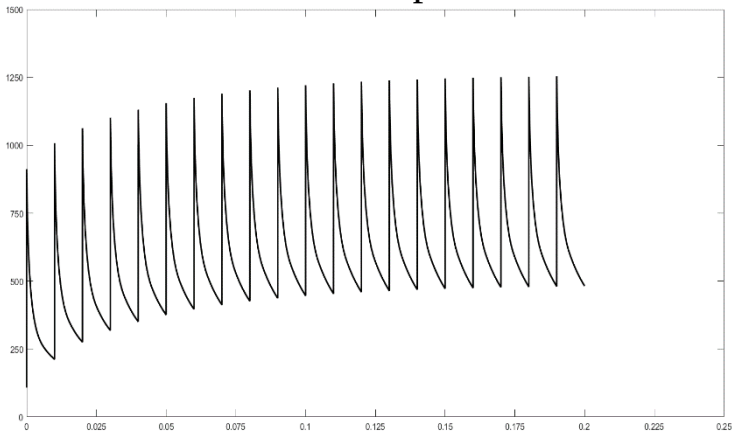

| Tube spectrum | Brain | Eyeballs dose | Lens dose | Pituitary gland dose |
|---|---|---|---|---|
| **80 kV** | +17.9 | +8.9 | +4.7 | +20.4 |
| **100 kV** | +36.3 | +30.8 | +28.2 | +38.0 |
| **120 kV** | +22.2 | +17.6 | +14.9 | +23.3 |
| **135 kV** | +24.4 | +16.8 | +3.0 | +6.6 |

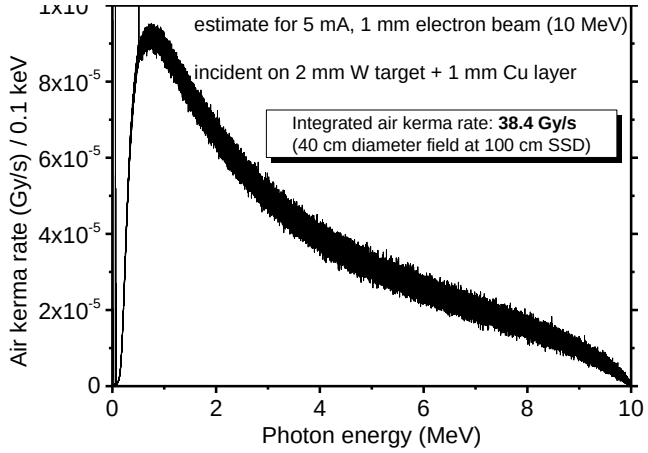
*Further details in the presentation that will be taken by F.S. Maddaloni "Geant4 Monte Carlo simulations for size specific organ dose estimates in CT based on patient silhouette and voxelilzed phantoms", Monday, Sess II

# X-ray flash radiotherapy: simulation of beam production for the new BriXSino high brilliance source




Temperature over the time: Max target temperature (1200 °C) for 10^9 electrons/pulse at 100 Hz






*Further details in the presentation "Monte Carlo optimization of the target configuration for bremsstrahlung x-ray production in flash radiotherapy", Tuesday, Sess IV


IV Geant4 International User Conference 2022, 24–26 October 2022, Napoli (Italy)

# Welcome in Napoli and have an amazing conference!!!

sarno@na.infn.it