

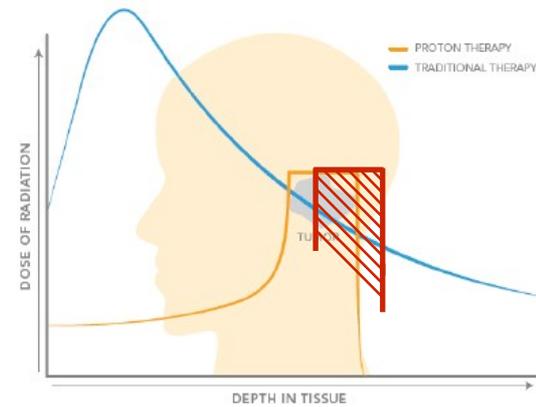
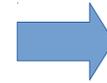
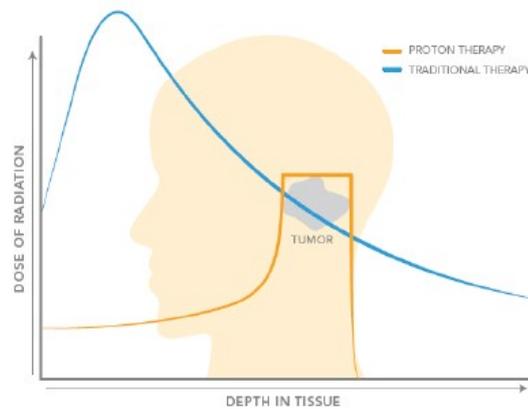
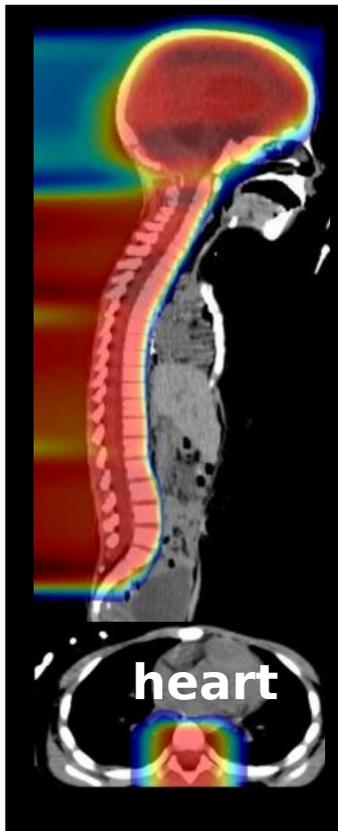
An introduction to PET activity simulations and detector study

FLUKA Advanced Course and Workshop
18-22 November, NEA, Paris

vferrero@to.infn.it

Why PET activity?

Proton treatment



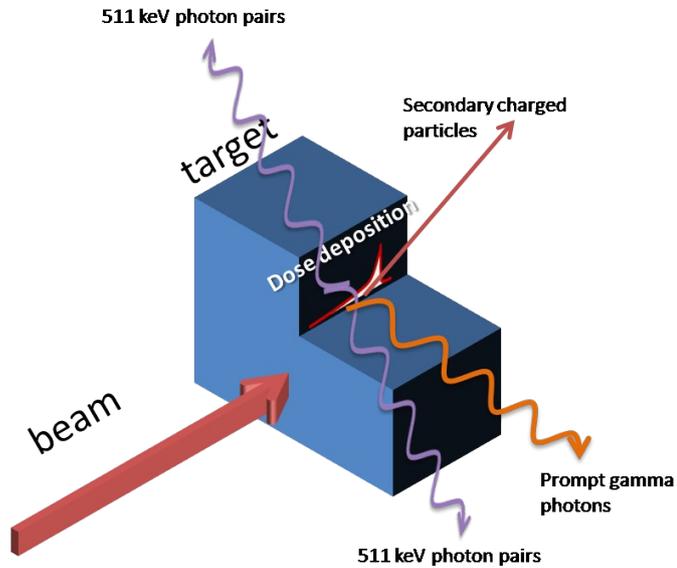
$$-\frac{dE}{dx} = 4\pi N_A r_e^2 m_e c^2 \rho \frac{Z_t Z_p^2}{A_t \beta^2} \left[\ln\left(\frac{2m_e c^2 \beta^2 \gamma^2}{I}\right) - \beta^2 - \frac{\delta}{2} - \frac{C}{Z_t} \right]$$

Dose uncertainties:

- Patient setup
- Anatomical changes
- Dose calculation

→ need of **particle range verification**

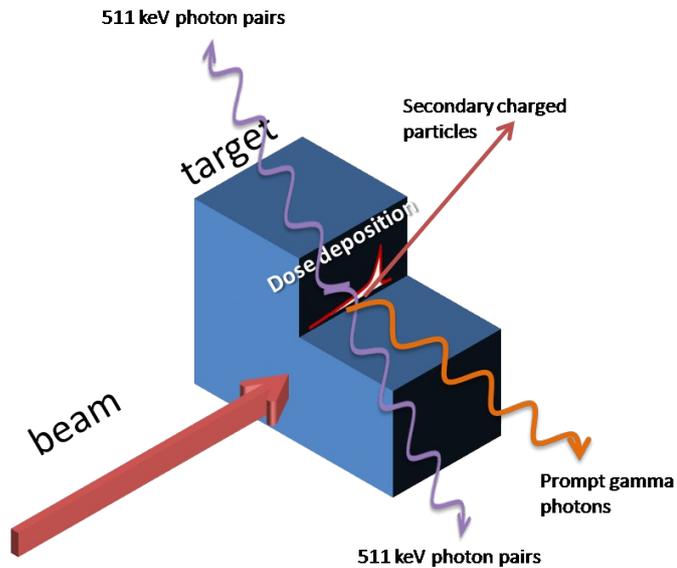
Why PET activity?



Particle range verification:

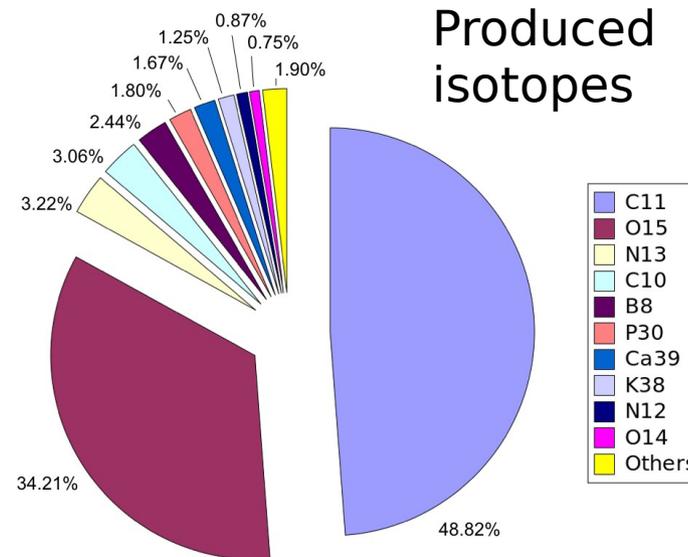
- Nuclear de-excitation → Gamma prompt
- Fragmentation → Charged particles
- β^+ isotopes → 511 keV annihilation photons

Why PET activity?



Particle range verification:

- Nuclear de-excitation → Gamma prompt
- Fragmentation → Charged particles
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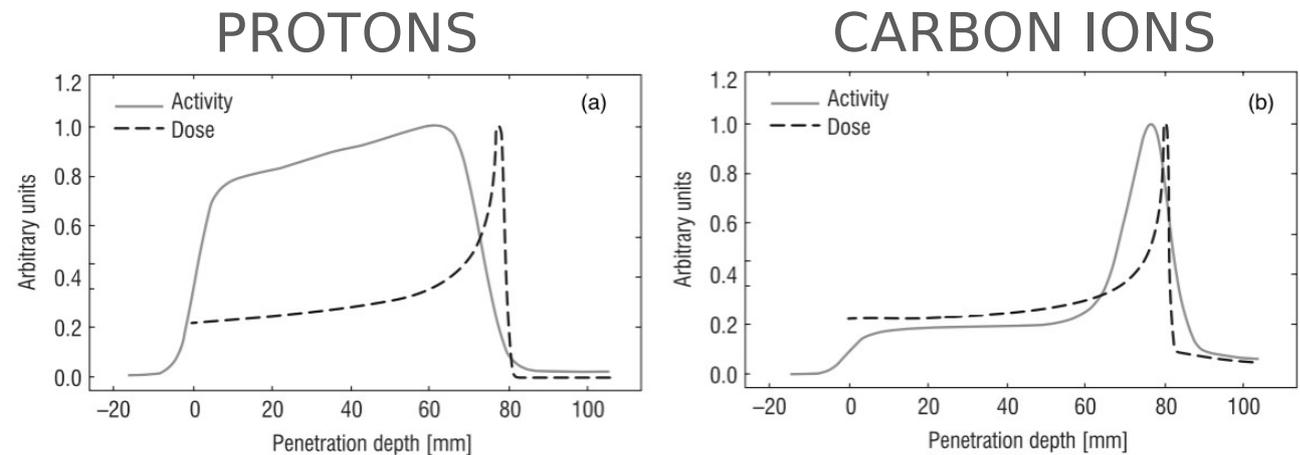


Isotope	$t_{1/2}$
^{10}C	19.3 s
^{11}C	20.28 min
^{14}O	70.59 ms
^{15}O	2.03 min
^{12}N	11.0 ms
^{13}N	9.96 min
^8B	770 ms
^{38}K	7.63 min
^{30}P	2.49 min
^{39}Ca	859 ms

The INSIDE project



Short decay time: **online measurement** to minimize loss of signal and distribution washout (in-beam PET)



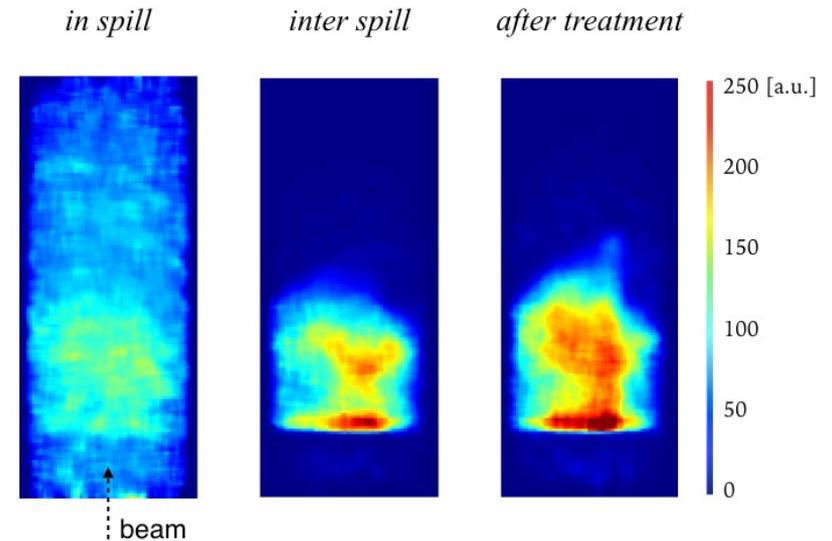
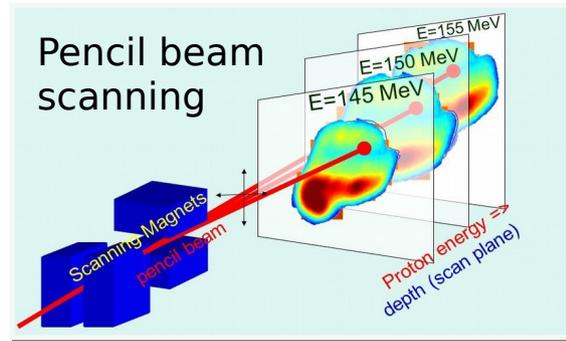
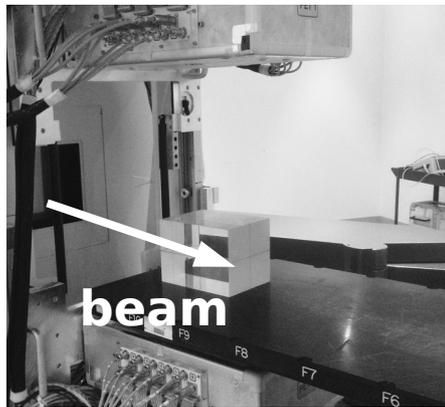
Enghardt W. et al. Radiother Oncol. 2014, 73.2:S96-98

We measure the activity, not the dose (indirect comparison) → **need of an activity simulation**

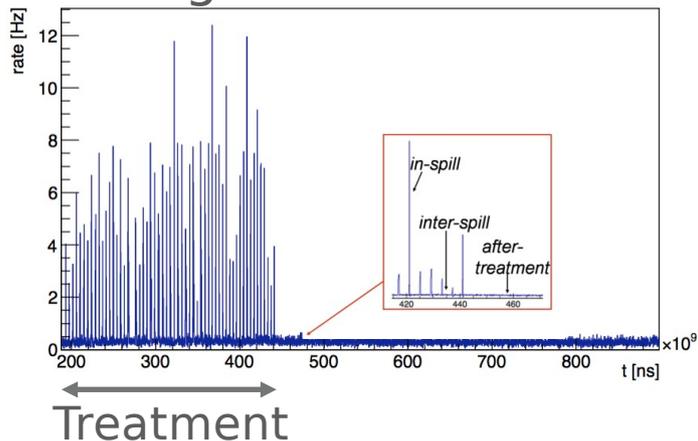
PET distribution: basic concepts

eg. treatment plan delivered on a PMMA phantom

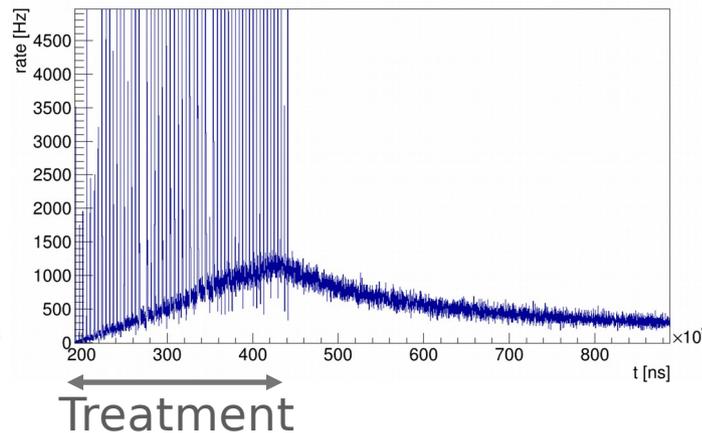
$E=83-150$ MeV, protons



Single event rate



Coincidence event rate

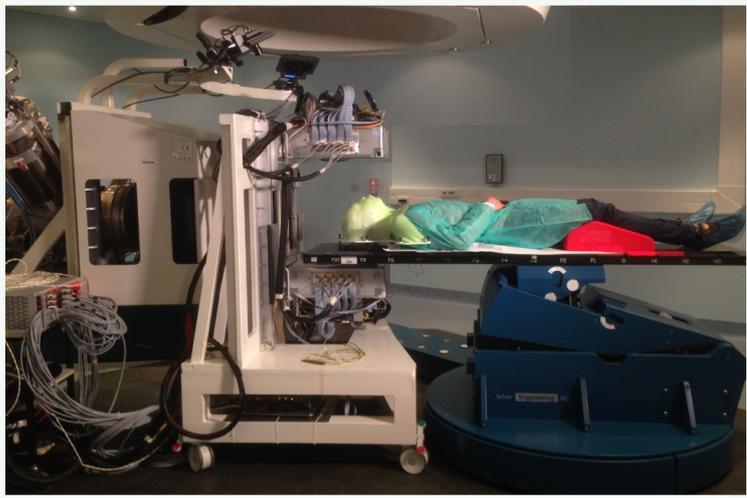


Phantoms studies published in: V. Ferrero JINST 12(3), 2017; V. Ferrero et al, TRPMS 2(6), 2018; F. Pennazio et al., PMB 63, 2018.

The INSIDE PET simulation

Scanner geometry
 Target model
 Beam line characteristics
 Treatment plan information
 β^+ isotopes characteristics

Two-step simulation

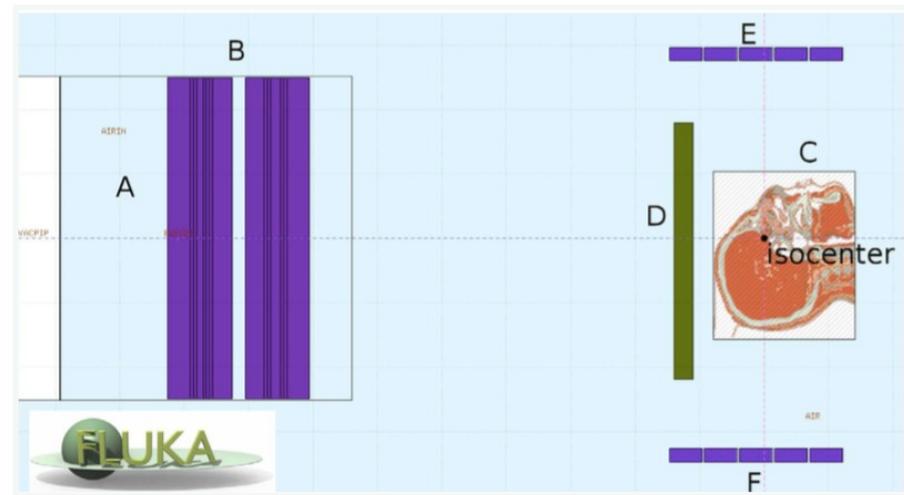


<i>STEP 1 beam simulation</i>	<i>Time-tagged activity scoring</i>	<i>STEP 2 PET simulation</i>	<i>Image reconstruction</i>
A fraction of primary hadrons is simulated (e.g. 1/100)	Isotope production map	All positrons are simulated (x100)	Same analysis chain as real data



The temporal and spatial structure of the beam are simulated

Isotopes decay is simulated



The INSIDE PET simulation: step1

CNAO/INSIDE user ROUTINES (MGDRAW, SOURCE)

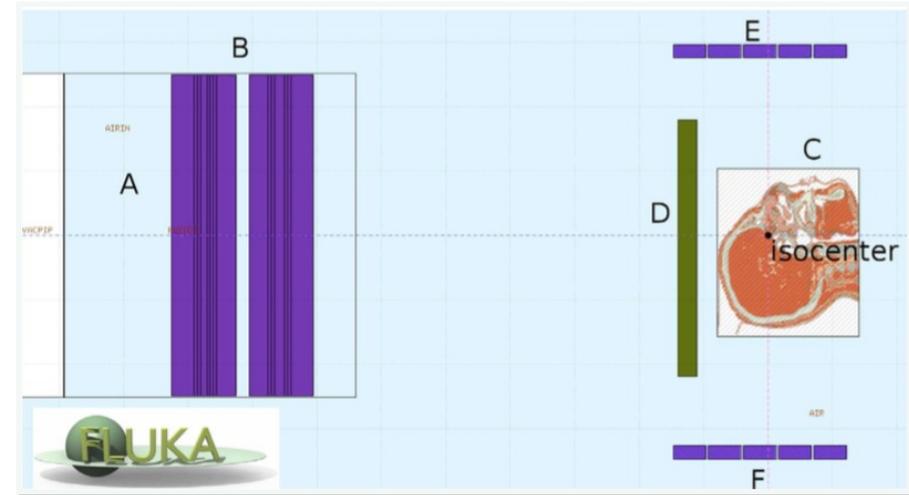
- Description of the **CNAO beam line** (particle, beam size)
- Description of the **treatment** (number of slices, energy, total particles/treatment, particle/spot, spot coordinates, delivery time)

The treatment information are directly passed through the user ROUTINES

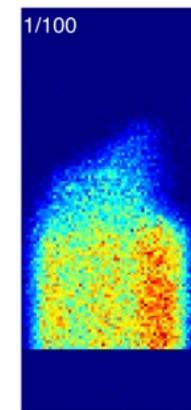
1/100 wrt total primaries is simulated for computational time issues (→ simulation is biased)

OUTPUT: fragmentation processes that result in the production of β^+ isotopes are scored in the target (spatial and time coord)

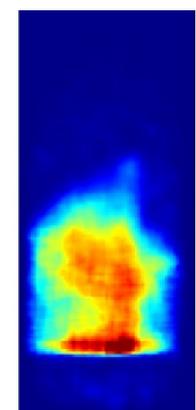
Other process (neutron, prompt photons, charged fragments) are not taken into account



*MC truth
(step1 sim)*



Exp data

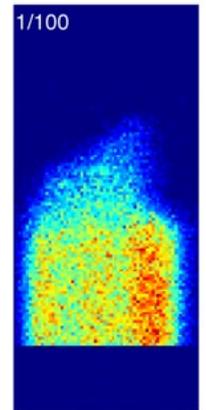


The INSIDE PET simulation: step2

CNAO/INSIDE user ROUTINES (MGDRAW, SOURCE, USRINI)

- **Step1 output** (i.e., isotope map distribution) as generator
- **All initial statistics** is accounted for (step1 output is read 100 times if 1/100 statistics was run in step1)
- Extraction of **decay events** over characteristics isotopes curve
- Simulation of **annihilation events** and scoring of 511 keV photons on the detector elements

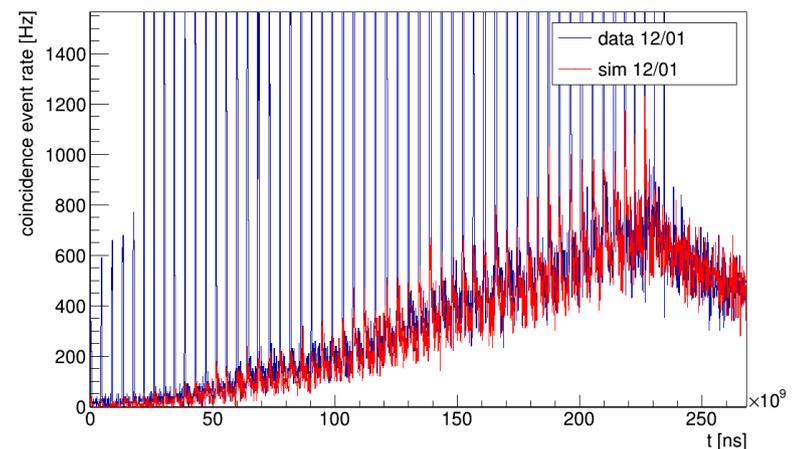
*MC truth
(step1 sim)*



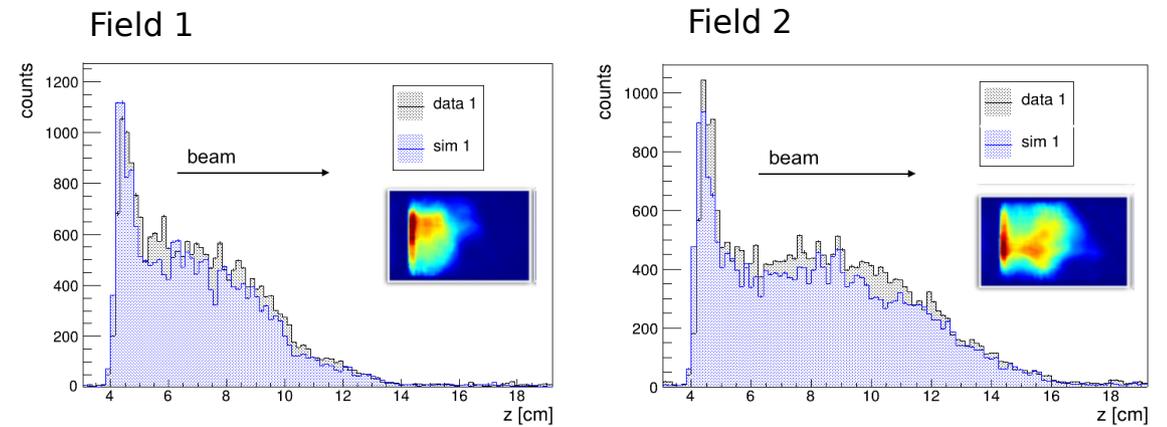
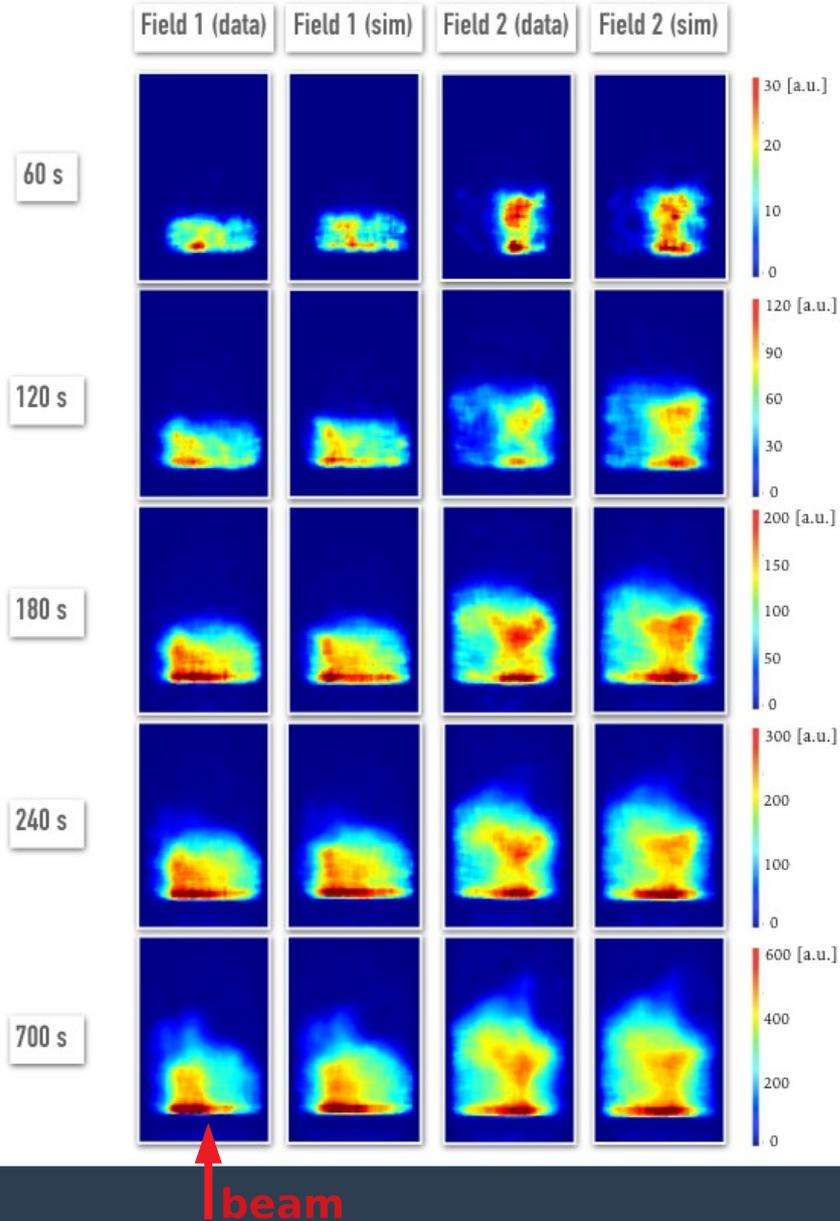
OUTPUT: file with single detected events

Simulated data is post-processed considering the detector experimental performances and a coincidence data filtering algorithm is applied

Coincidence event rate



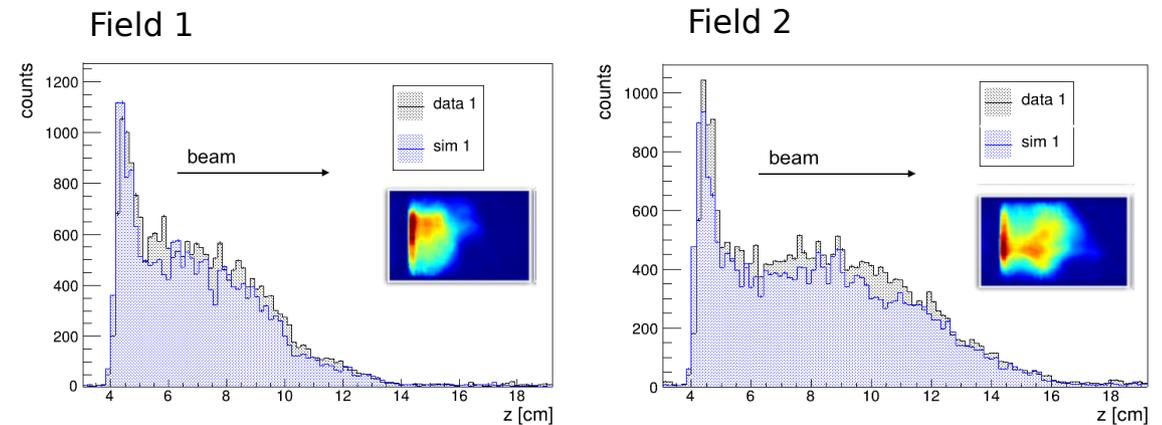
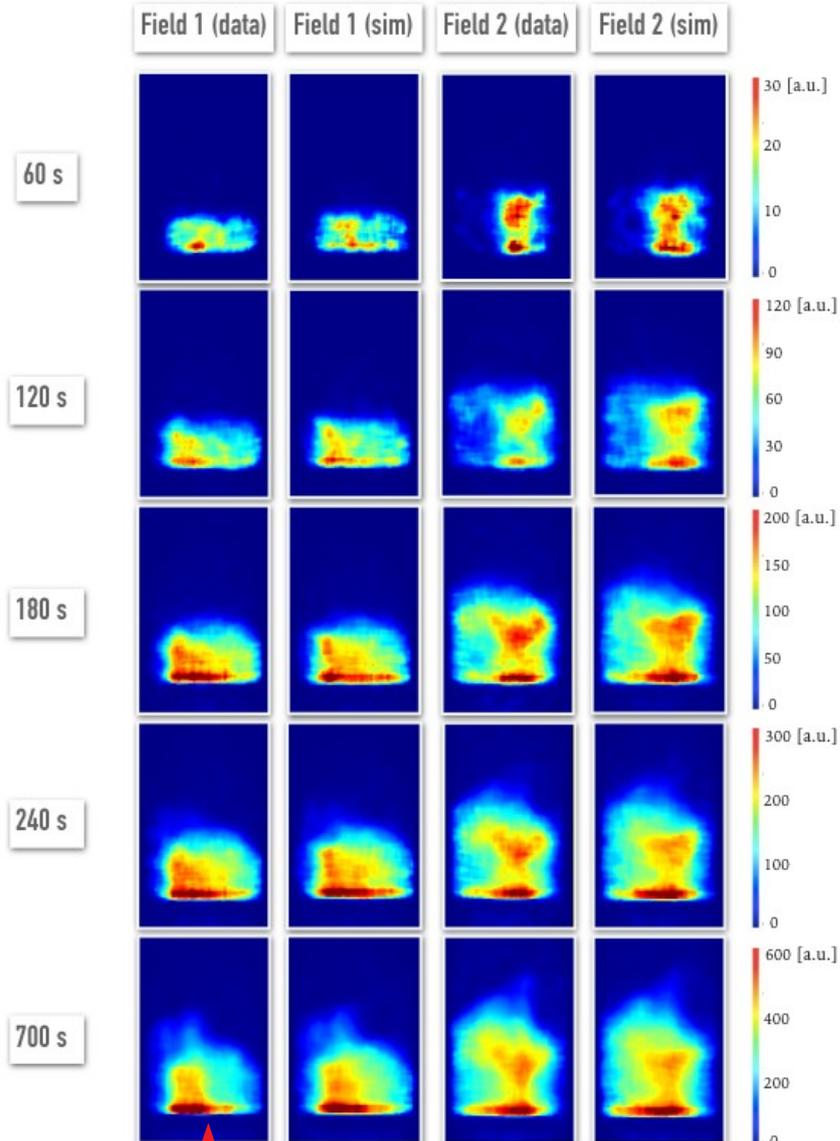
PET activity simulation



Field 1				
	data 1	sim 1	data 2	sim 2
Rising edge (mm)	44.5 ± 0.8	43.9 ± 0.6	44.5 ± 0.9	43.9 ± 0.6
Falling edge (mm)	97.2 ± 0.9	96.6 ± 0.9	97.7 ± 0.9	96.8 ± 0.9
Range (mm)	52.7 ± 1.2	52.7 ± 1.1	53.2 ± 1.3	52.9 ± 1.1

Field 2				
	data 1	sim 1	data 2	sim 2
Rising edge (mm)	44.5 ± 0.9	43.9 ± 0.6	44.4 ± 0.9	43.9 ± 0.6
Falling edge (mm)	128.8 ± 0.8	123.4 ± 0.9	123.3 ± 0.9	123.9 ± 0.9
Range (mm)	79.3 ± 1.2	79.5 ± 1.1	78.9 ± 1.3	80.0 ± 1.1

PET activity simulation



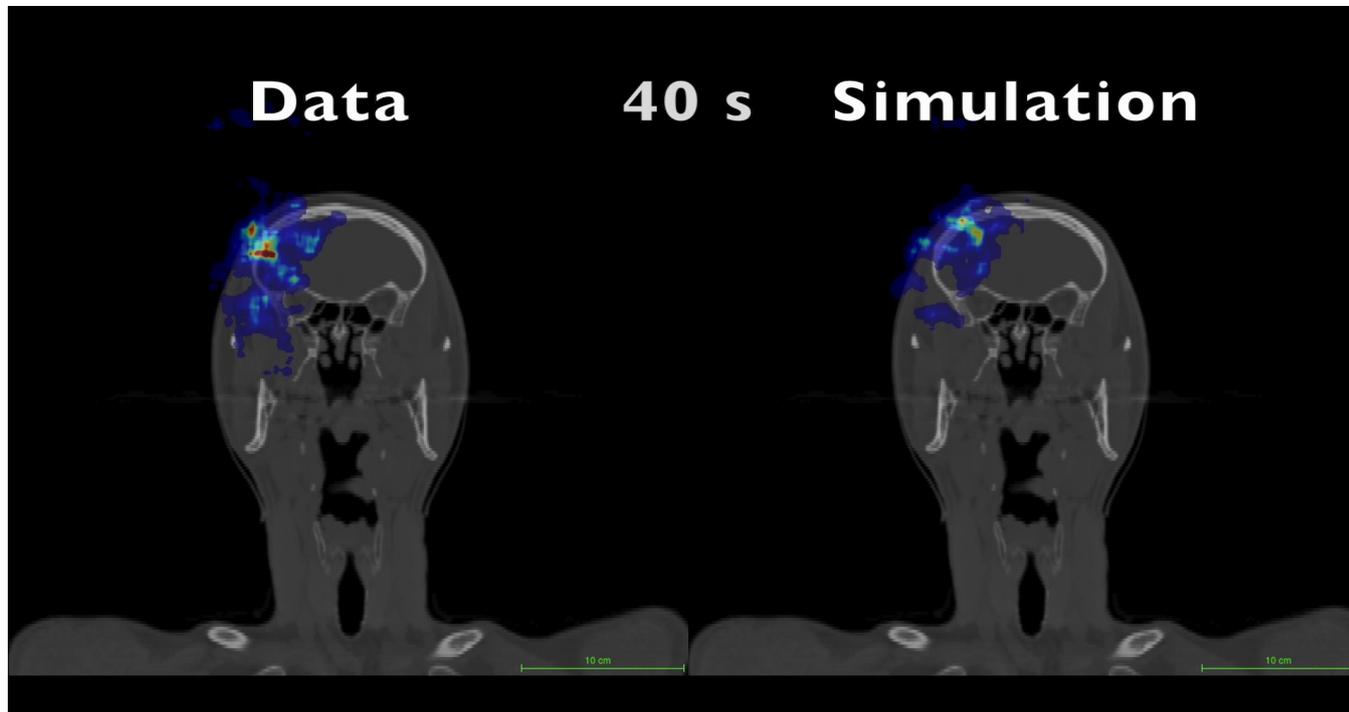
Field 1				
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Range (mm)	52.7 ± 1.2	52.7 ± 1.1	53.2 ± 1.3	52.9 ± 1.1

Agreement:

- within **0.5 mm** between **experimental measurements**
- within **1 mm** between **experimental and simulated data**

The first in-vivo monitoring

The first in-vivo acquisition on Dec. 2015 showed the feasibility of using the INSIDE in-beam PET for range verification



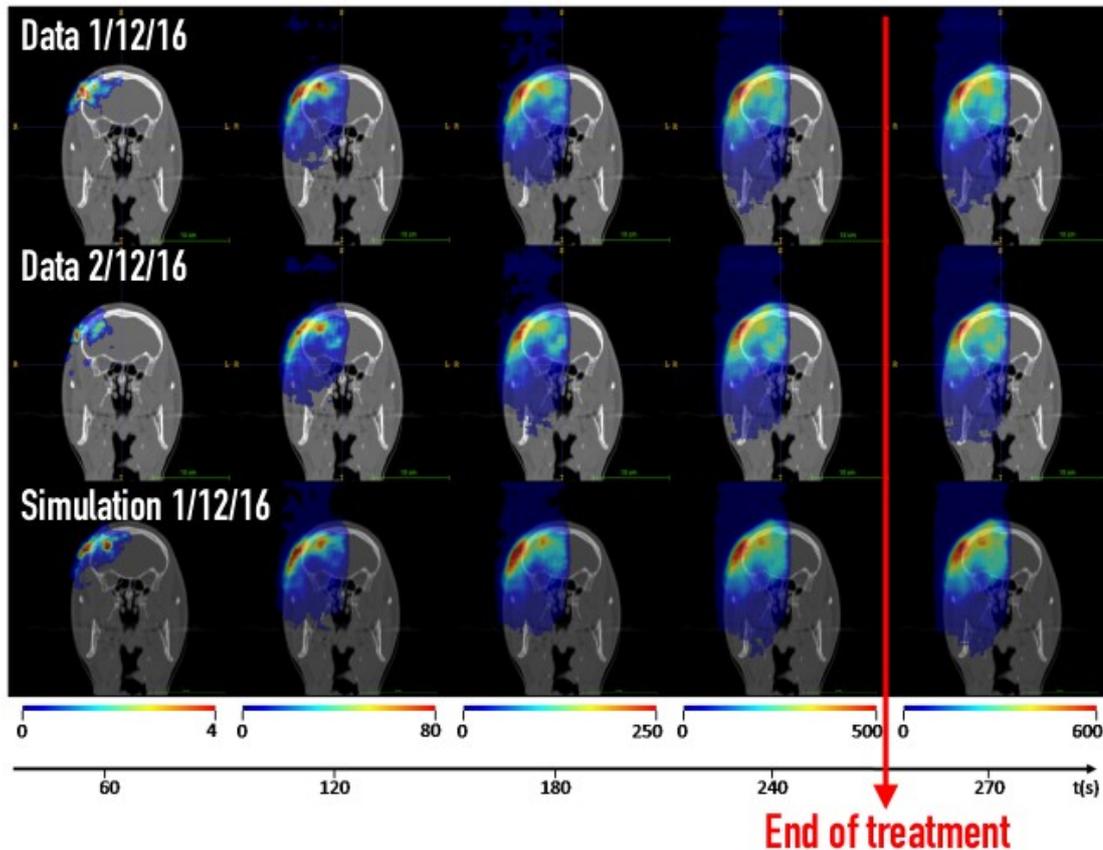
Carcinoma of the lacrimal gland
3.7 10^{10} protons
[66.3, 144.4] MeV/u
30 fractions, 2.2 GyE
Treatment time: 240 s

In-beam PET: no washout model is included

Results published in: V. Ferrero et al., Sci Rep 8.1, 2018;
E.Fiorina, V. Ferrero, et al. Phys Med 51, 2018.

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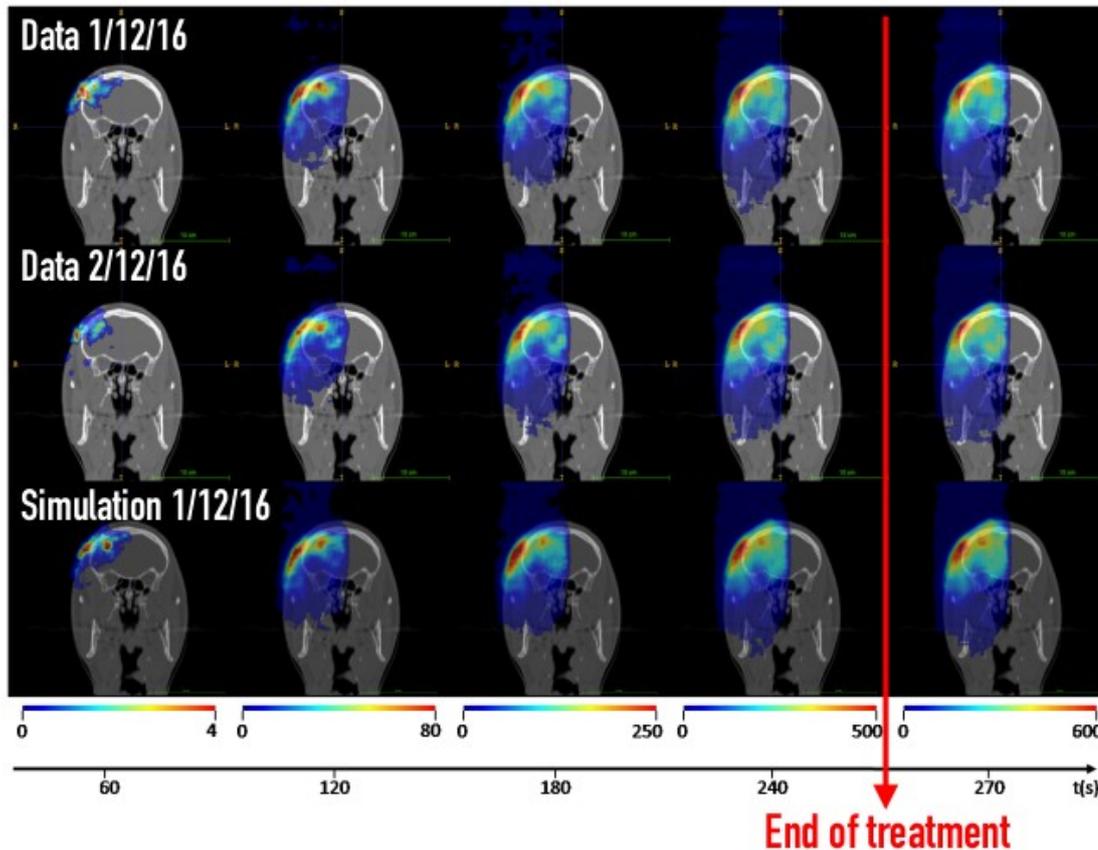
Carcinoma of the lacrimal gland
3.7 10^{10} protons
[66.3, 144.4] MeV/u
30 fractions, 2.2 GyE
Treatment time: 240 s

Agreement within **3 mm** before the treatment end, **FWHM \leq 17.6 mm (data vs sim), 12.8 mm (data vs data)**

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↓
How significant are these values?

Results published in: V. Ferrero et al., Sci Rep 8.1, 2018;
E.Fiorina, V. Ferrero, et al. Phys Med 51, 2018.

The INSIDE clinical trial



Currently installed @ CNAO, Italy

The INSIDE clinical trial

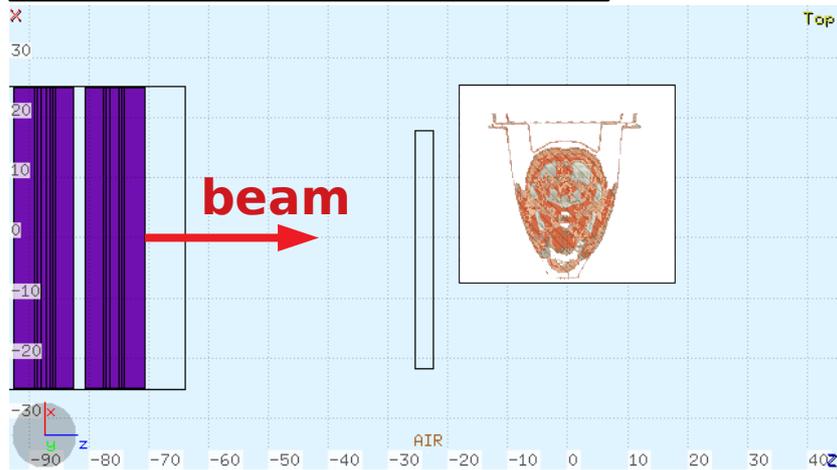
- Cohort of 20+20 patients
- Proton and carbon ion beams
- Different pathologies
- Study and optimize the INSIDE performances
- Find the clinically relevant tolerances
- Evaluate the benefits of the INSIDE system wrt the clinical routine

The INSIDE clinical trial started on Jul 19. Patients treated with both proton and carbon ion beams are being monitored

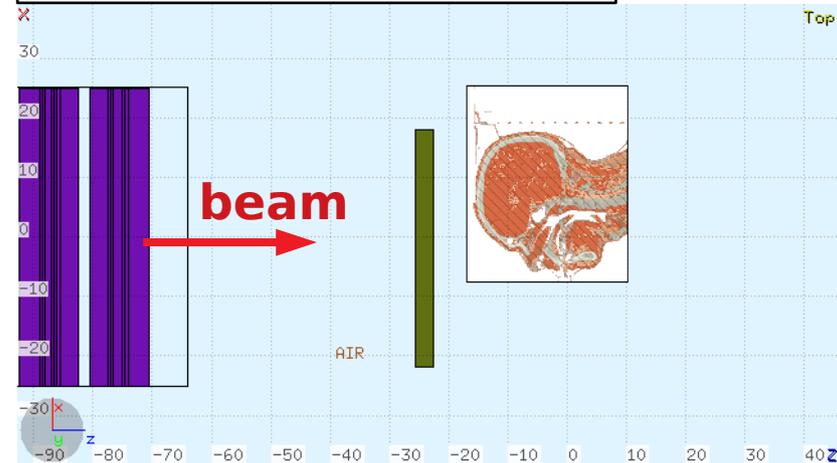
ClinicalTrials.gov ID: NCT03662373

The INSIDE clinical trial

Field 1: 0° IEC, no RS



Field 2: 270° IEC, RS

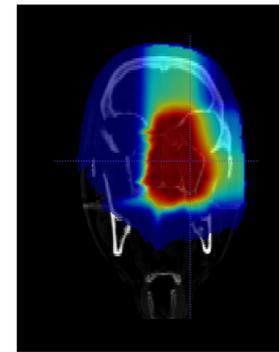


Squamocellular rhinopharynx carcinoma

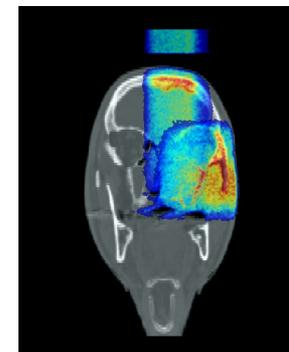
Patient treated with 2 fields (0° and 270° IEC)

27 sessions, $D_{\text{tot}}=54$ Gy

Planned dose

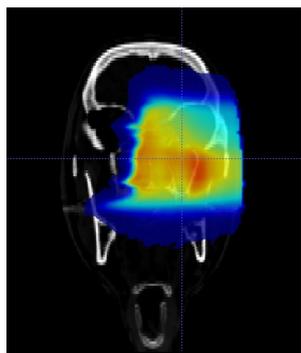


MC truth

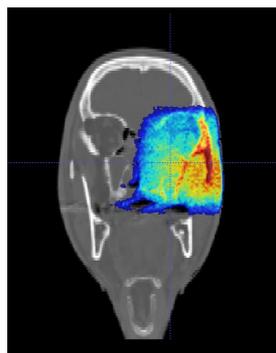


The INSIDE clinical trial

Planned dose

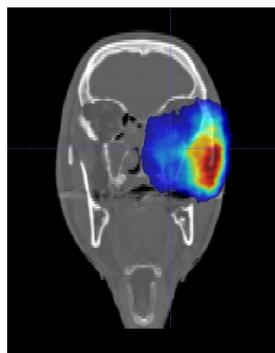


MC truth



step1

MC, reconstructed



step2

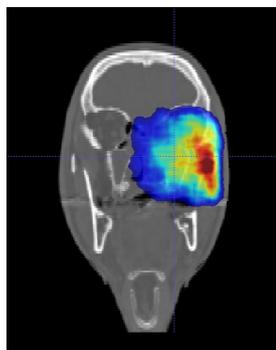
Squamouscellular rhinopharynx carcinoma

Patient treated with 2 fields
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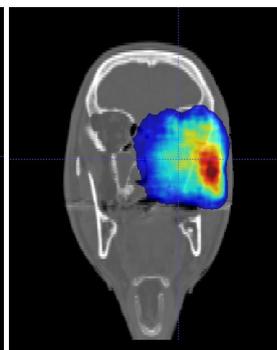
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Field 1: 0° IEC, no RS

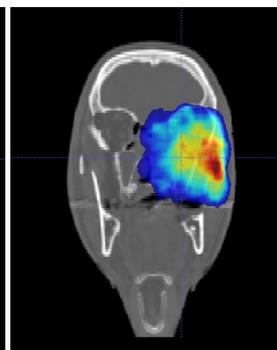
frac 16



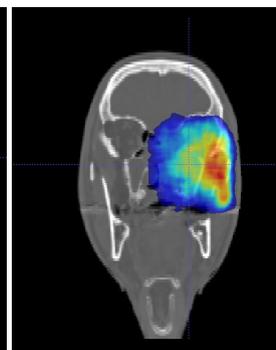
frac 17



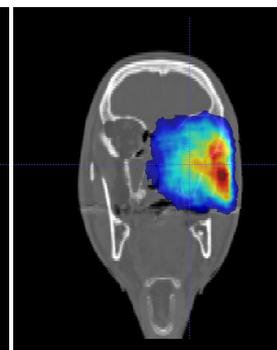
frac 22



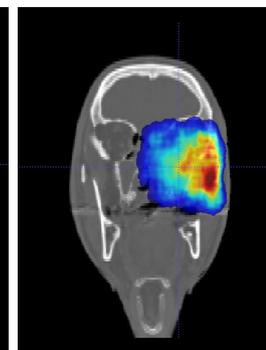
frac 23



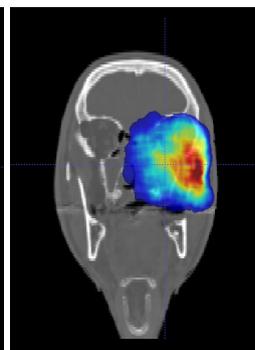
frac 24



frac 25



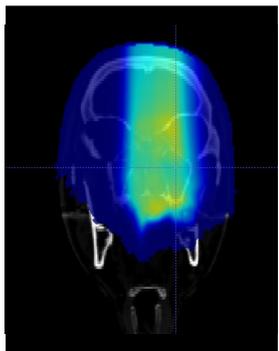
frac 27



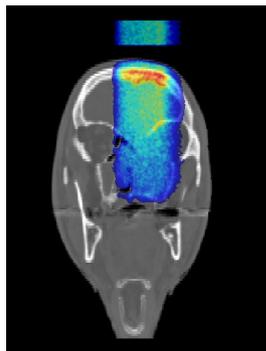
ClinicalTrials.gov ID: NCT03662373

The INSIDE clinical trial

Planned dose

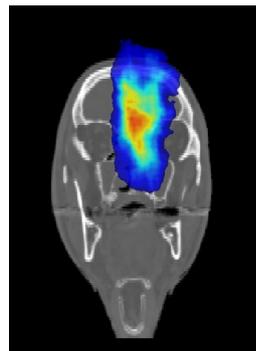


MC truth



step1

MC, reconstructed



step2

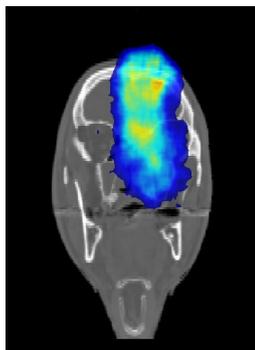
Squamouscellular rhinopharynx carcinoma

Patient treated with 2 fields
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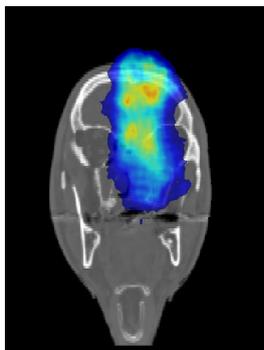
27 sessions, $D_{\text{tot}}=54$ Gy

Field 2: 270° IEC, RS

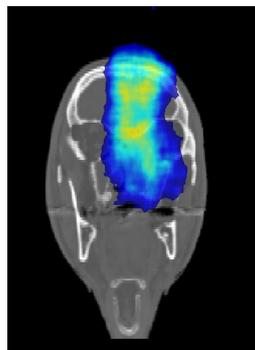
frac 16



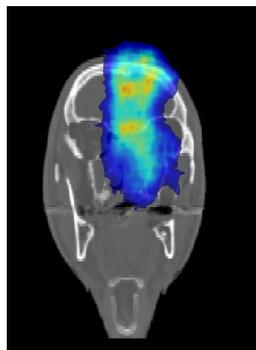
frac 17



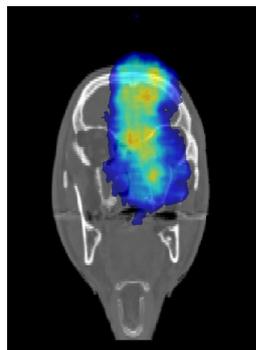
frac 22



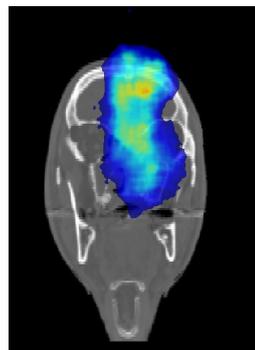
frac 23



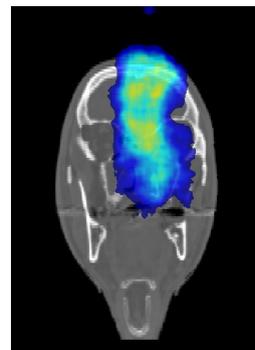
frac 24



frac 25



frac 27



Exp data

ClinicalTrials.gov ID: NCT03662373

The INSIDE clinical trial

Field 1: 0° IEC, no RS

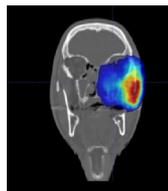
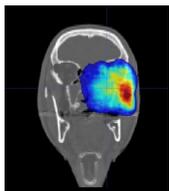
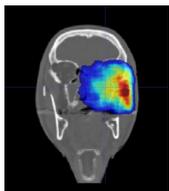
Image comparison	Range difference	Range difference FWHM	Pearson correlation coefficient
frac 16 vs 17	-0.68 mm	8.0 mm	0.96
frac 16 vs 22	0.83 mm	8.0 mm	0.95
frac 16 vs 23	-2 mm	9.6 mm	0.96
frac 16 vs 24	0.05 mm	11.2 mm	0.96
frac 16 vs 25	-0.62 mm	8.0 mm	0.95
frac 16 vs 27	-0.75 mm	8.0 mm	0.95

Image comparison	Range difference	Range difference FWHM	Pearson correlation coefficient
sim vs 16	-0.94 mm	6.4 mm	0.83
sim vs 17	-0.88 mm	8.0 mm	0.83
sim vs 22	-1.45 mm	9.6 mm	0.77
sim vs 23	-0.99 mm	6.4 mm	0.79
sim vs 24	-0.92 mm	9.6 mm	0.80
sim vs 25	-1.26 mm	4.8 mm	0.82
sim vs 27	-1.49 mm	11.2 mm	0.82

frac 16

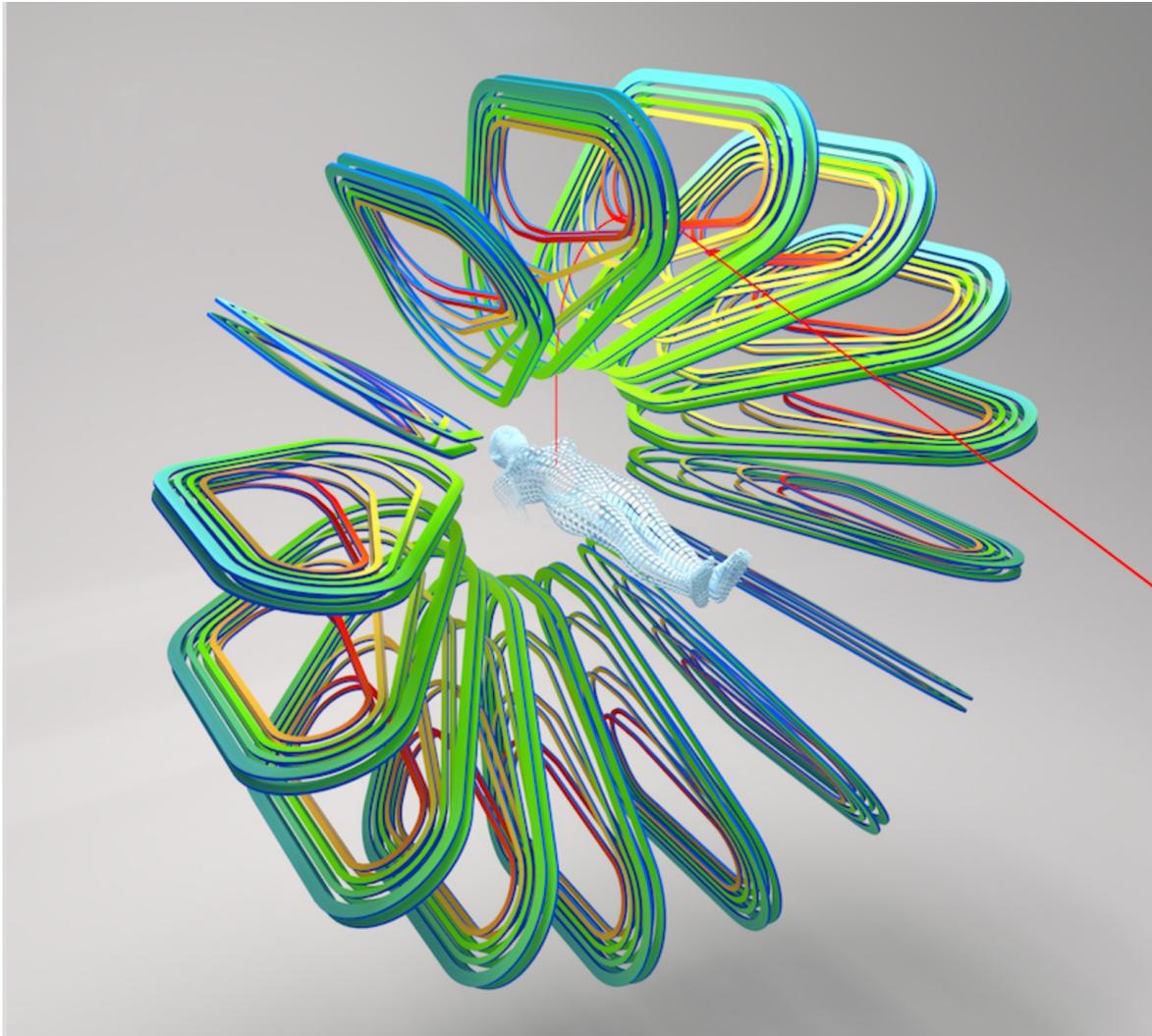
frac 17

sim



Analysis described in: V. Ferrero et al. TRMPS 2(6), 2018; E.Fiorina, V. Ferrero, et al. Phys Med 51, 2018.

GaToroid: an idea for an integrated design

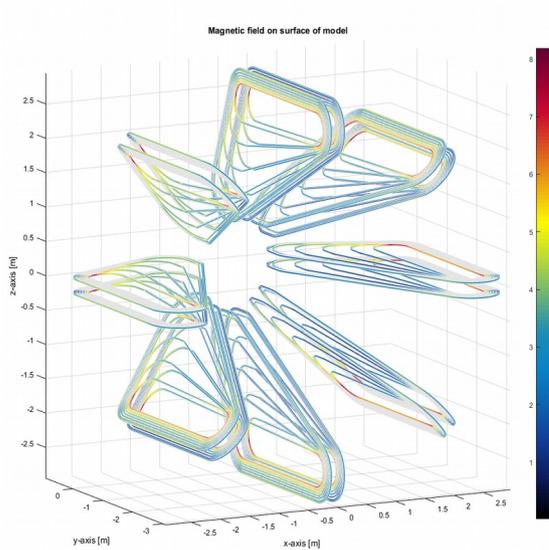


A Gantry and Apparatus for Focusing Beams of Charged Particles.

L. Bottura, European Patent Application EP 18173426.0, May 2018

Static gantry: beam delivery at discrete angles without magnet rotation → steady-state configuration, superconducting magnets → reduction of size, weight and costs

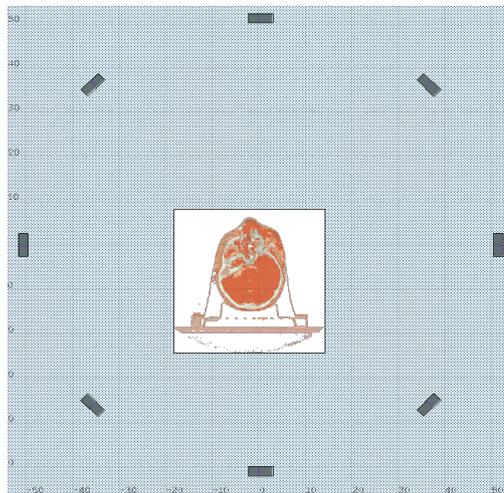
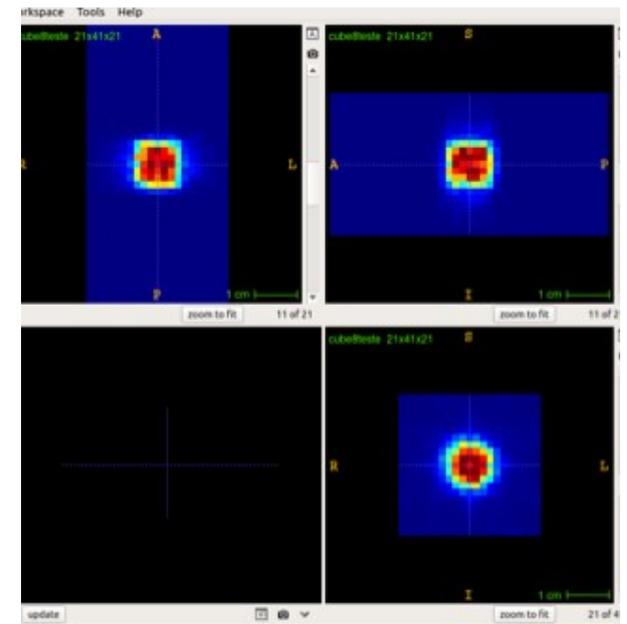
GaToroid: an idea for an integrated design



Test geometry:

- 8 coils
- 100 cm bore

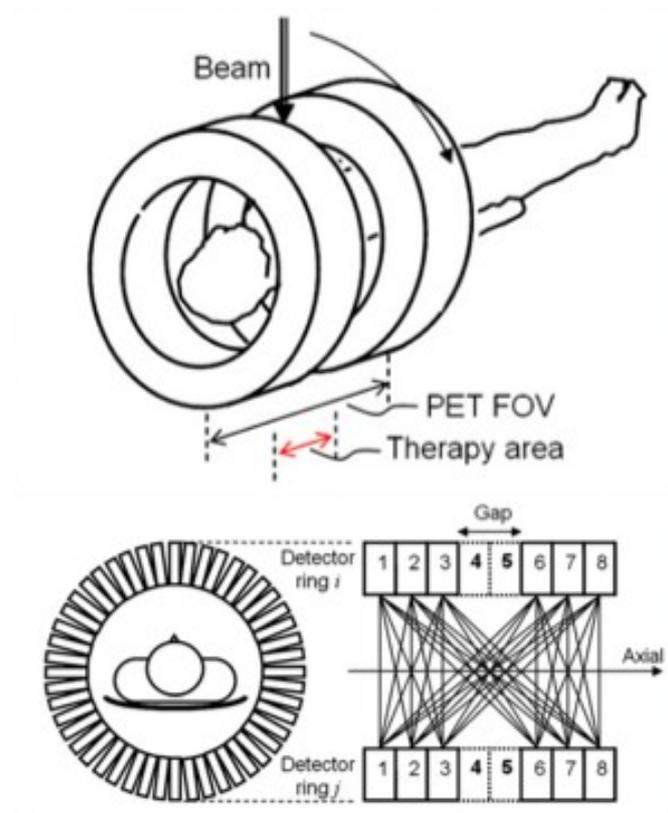
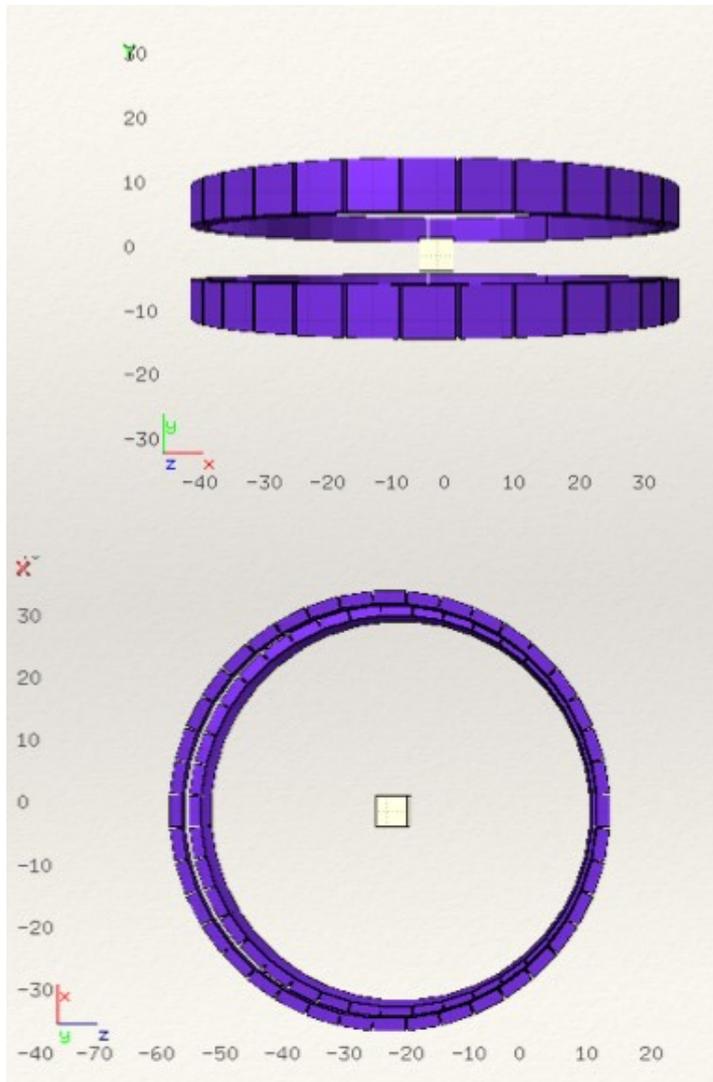
FLUKA simulation:
1 cm³ activity cube



Test geometry:

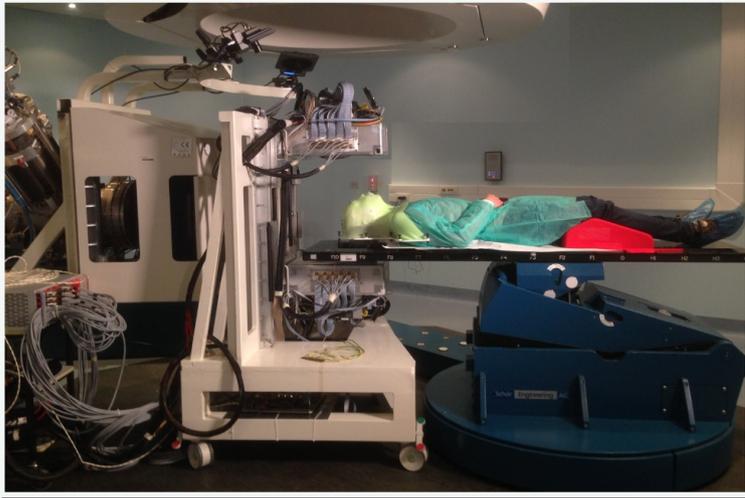
- 8 PET detector blocks
- 3 modules for each block (5x15 cm²)
- 16x16 crystals (3.2 mm pitch) for each module

GaToroid: an idea for an integrated design

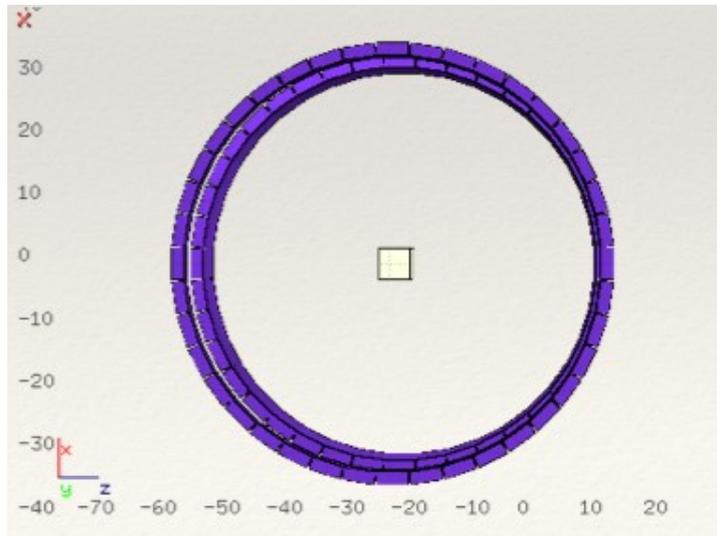


Repetition of the same detector block: LATTICE, ROT-DEFI

Conclusions



The INSIDE clinical trial: understand detector limits, sensitivity, impact on physicians
...with the aid of FLUKA



GaToroid: study and optimization for an integrated gantry geometry
...with the aid of FLUKA