

Quantification and processing of NMR imaging data through Deep Learning techniques

AIM Kick-off meeting, Pisa, 30 Gennaio 2019

Marco Barbieri

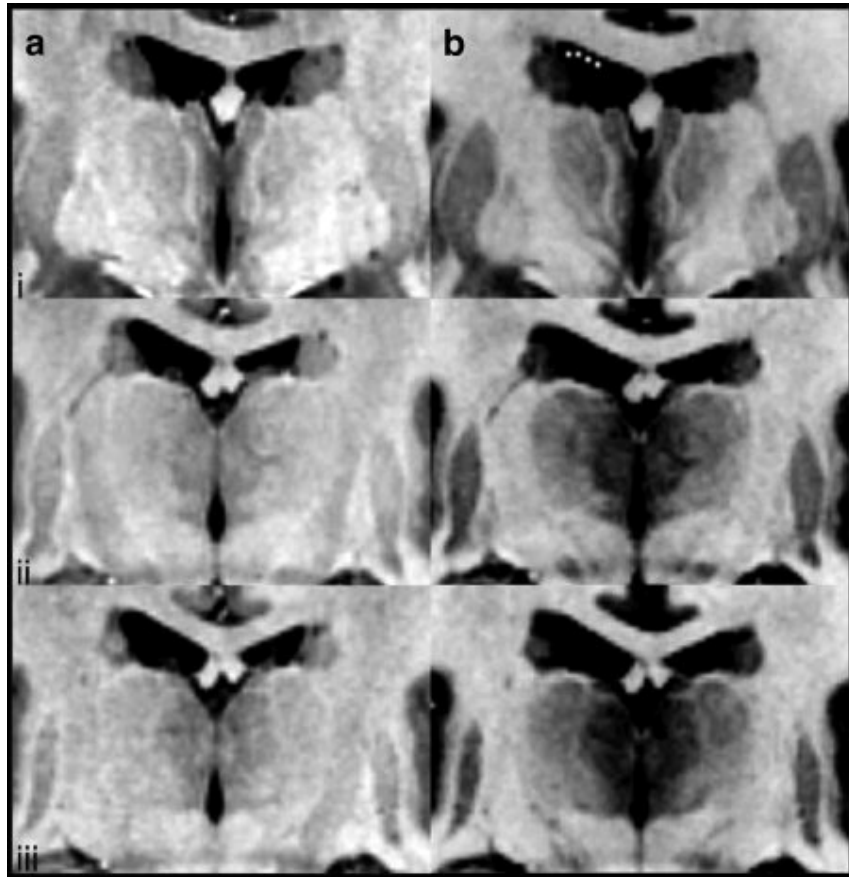


Overview

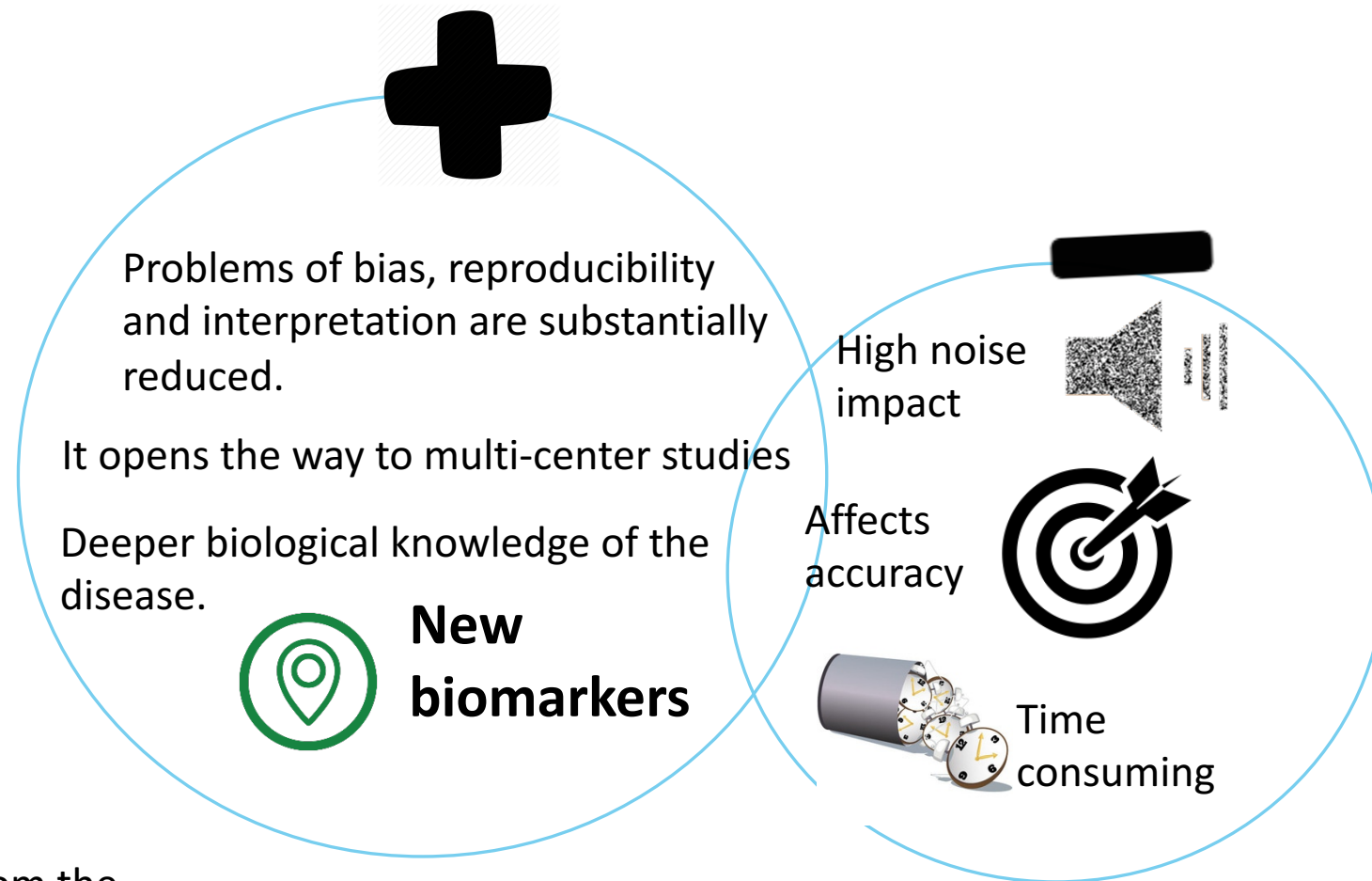
1. MR Imaging: from qualitative to quantitative imaging.
2. Deep Learning for Magnetic Resonance Fingerprinting
 1. Brief introduction to Magnetic Resonance Fingerprinting.
 2. Change of paradigm in quantitative NMR mapping.
 3. Curse of Dimensionality in Magnetic Resonance Fingerprinting
 4. Deep Learning as a solution.
3. Quantitative Susceptibility Mapping: a deep learning approach
 1. Ill-posed problem in QS Mapping.
 2. Deep Learning to solve QSM preserving accuracy while shortening acquisition time.



Shift of paradigm: from qualitative to quantitative MRI



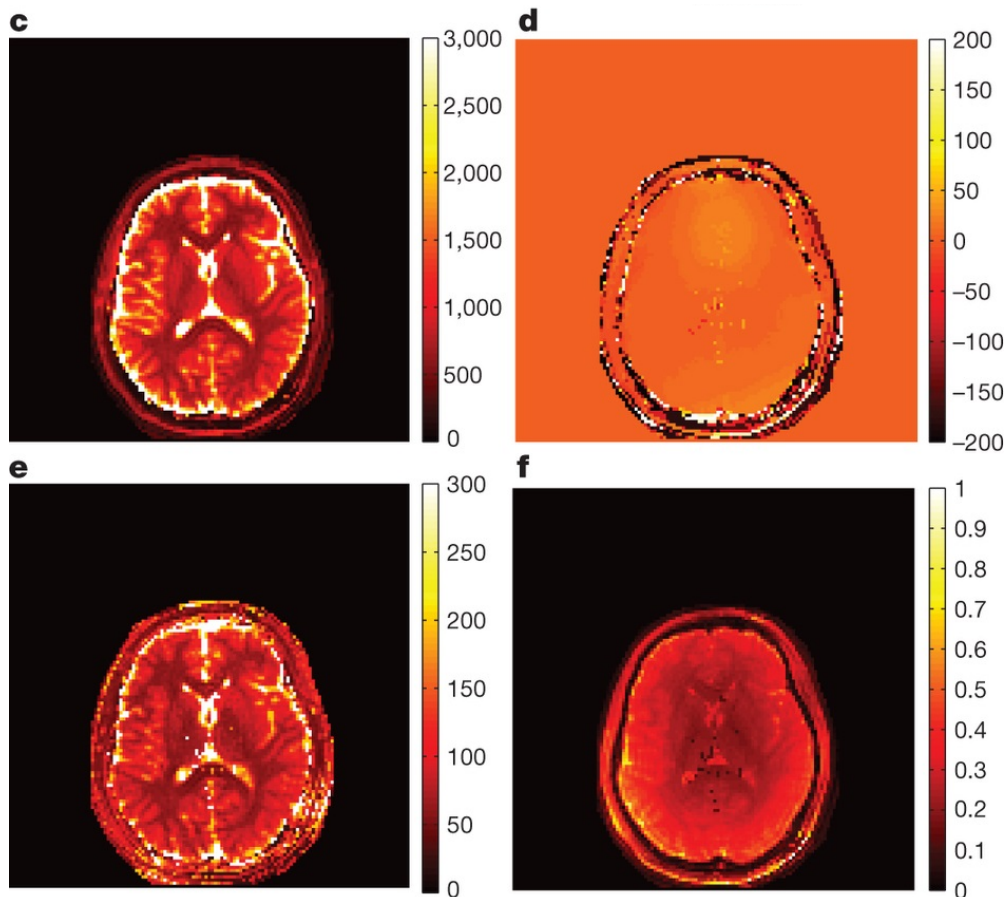
Comparison of coronal slices through the thalamus from the (a) 10× averaged deep brain T_1 -weighted image and (b) the 10× averaged deep brain T_1 map. Acquisition time: 17 min each [1]



Nowadays, qMRI is not part of routine clinical evaluation.

Magnetic Resonance Fingerprinting (MRF)

A new approach to quantitative MRI



(c) T1 map (ms), (d) Off-resonance frequency (Hz),
(e) T2 map (ms), (f) Proton density (M_0) normalized scale.

Magnetic resonance fingerprinting

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qMRI multi-parametric acquisition.

T1, T2, PD, Off resonance frequency.

Time saving!

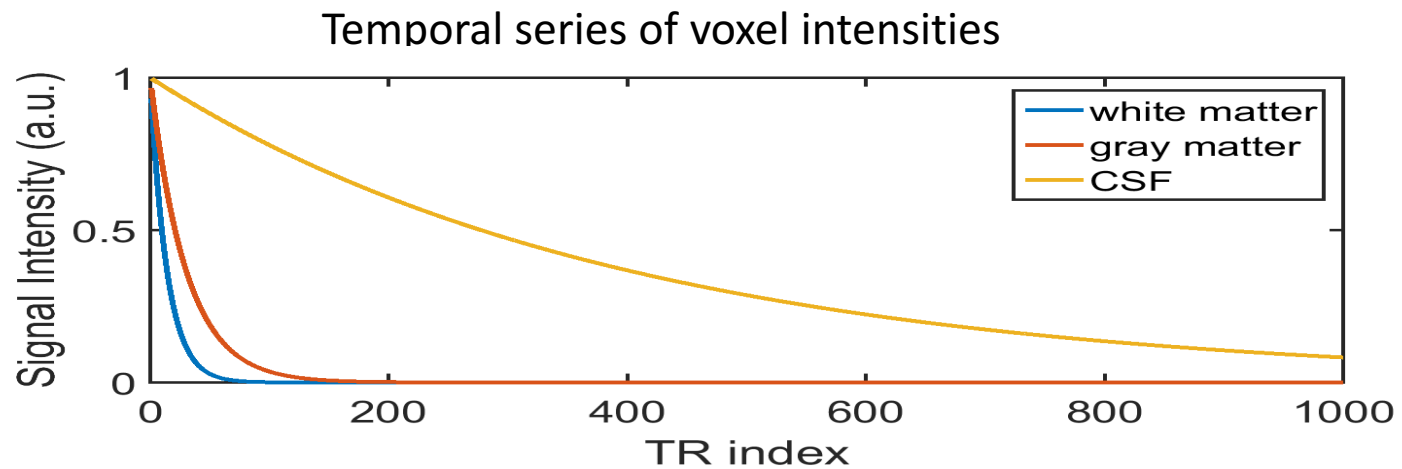
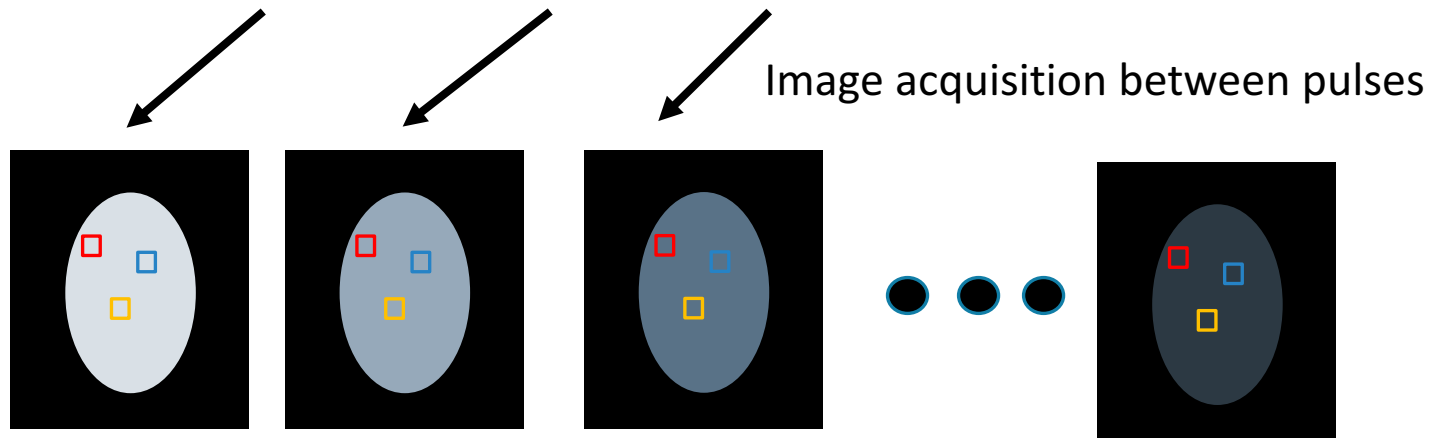
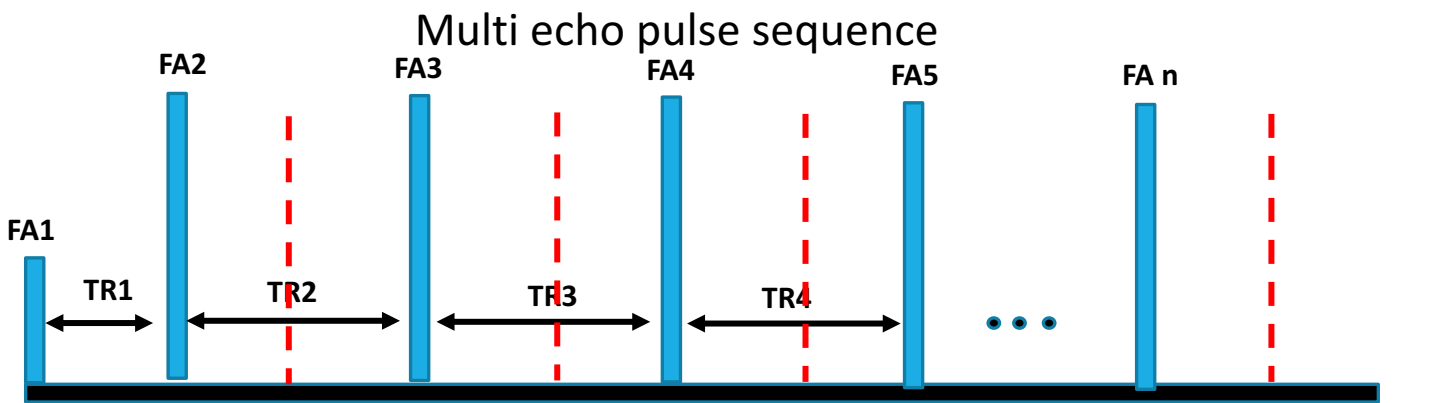
These data required 12.3 s to acquire.



designed by freepik.com



Conventional approach to MR parameter mapping

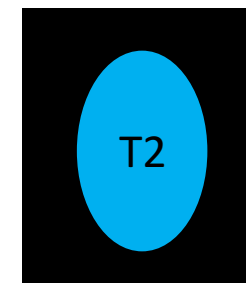


T2 parameter map estimation

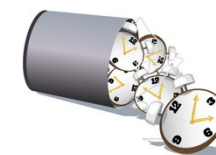
Known analytical model for multi echo sequences in function of T2 MR parameter

$$S(t) = S_0 \exp\left(-\frac{t}{T_2}\right)$$

Model fitting per each voxel



Using different pulse sequence to obtain different parameter maps



Time consuming

MRF approach to MR parameter mapping

MRF pulse sequence

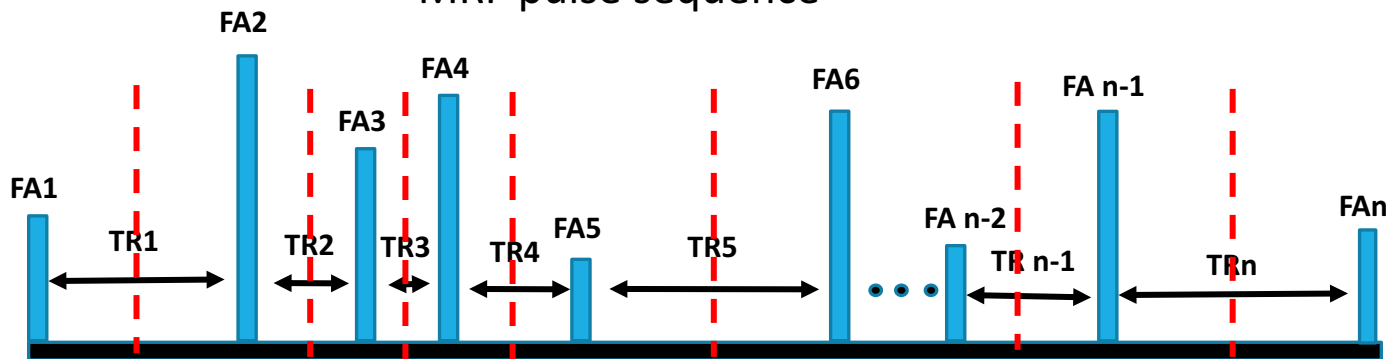
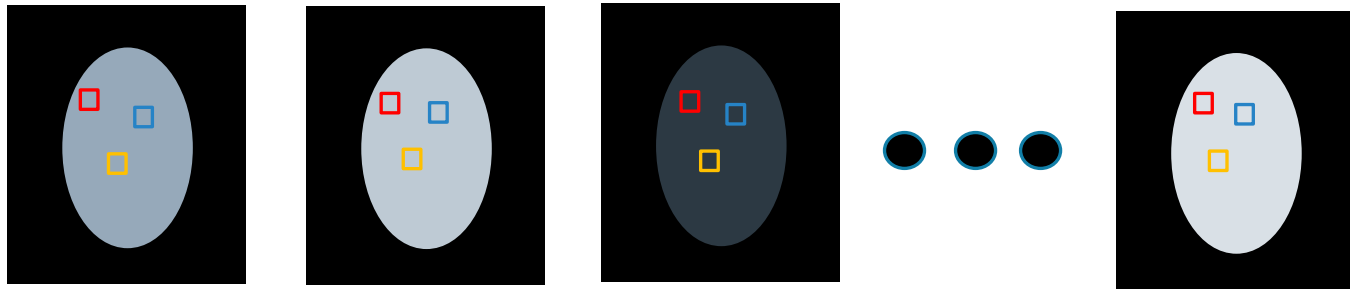
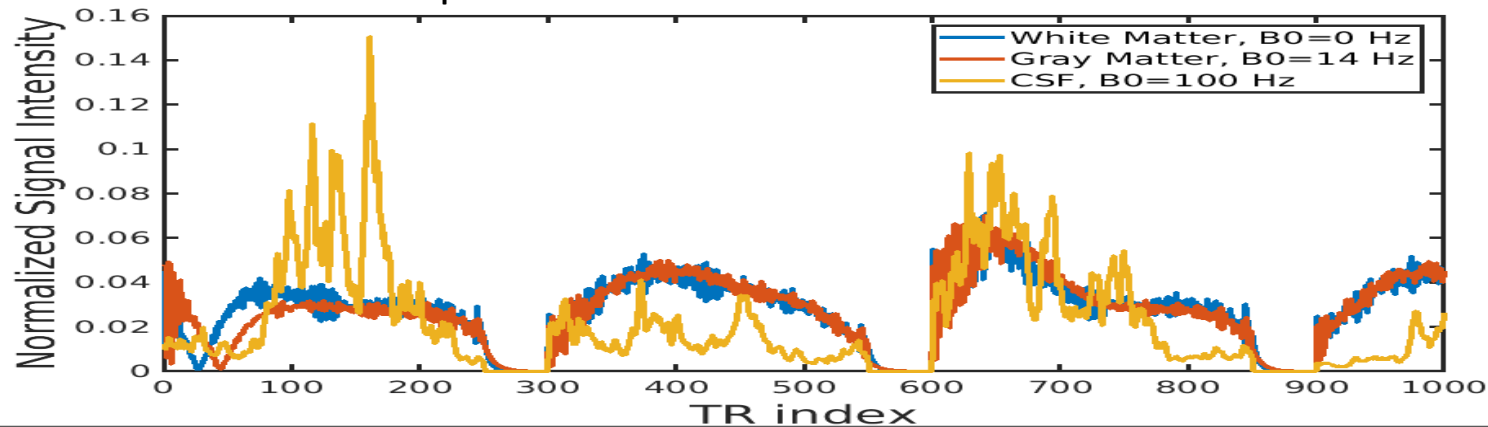


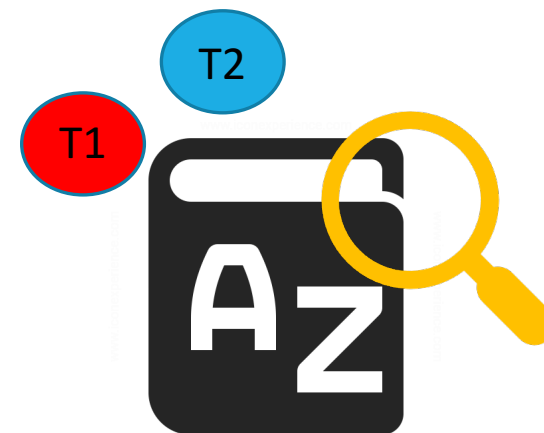
Image acquisition between pulses



Temporal series of voxel intensities

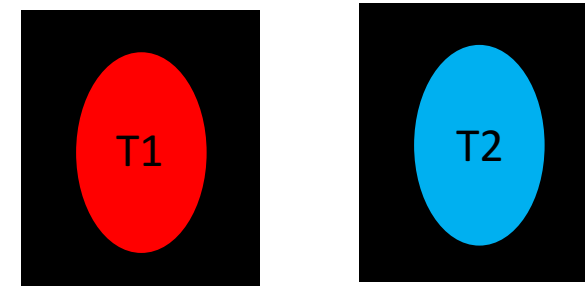


Parameter maps estimation

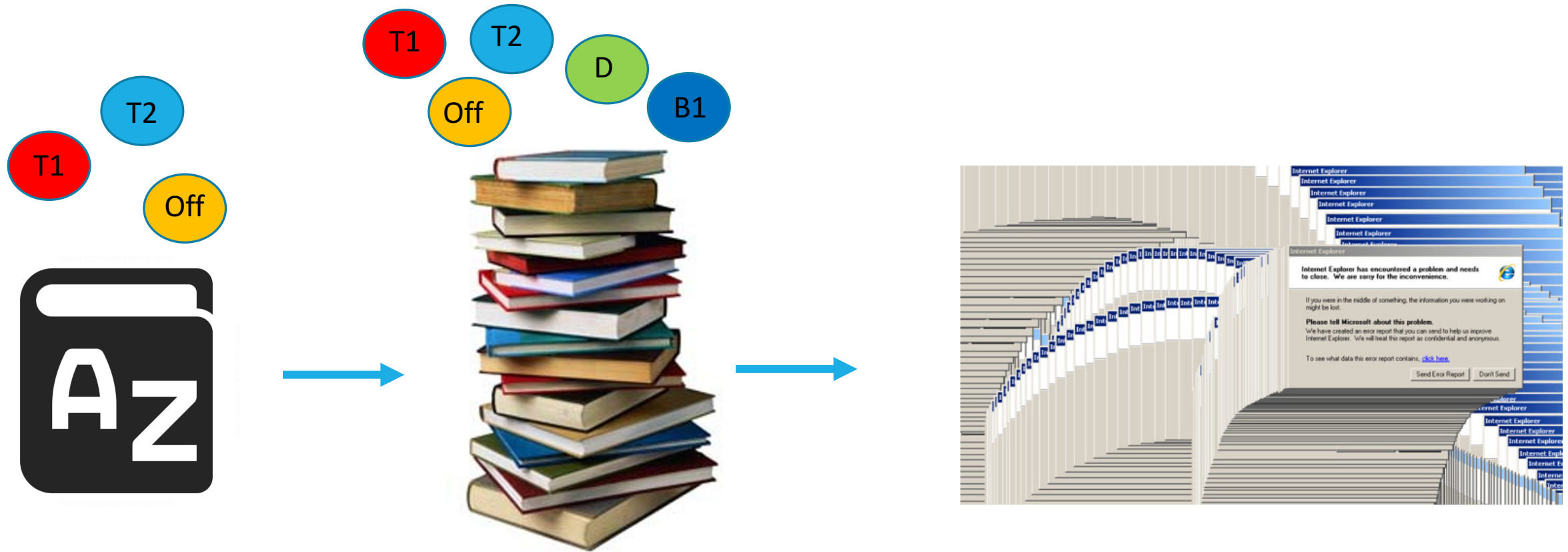


Simulating a dictionary with possible evolutions given a set of NMR parameters

Per each experimental voxel signal performing Nearest Neighbour matching



The Curse of Dimensionality in Dictionary-based MR Fingerprinting



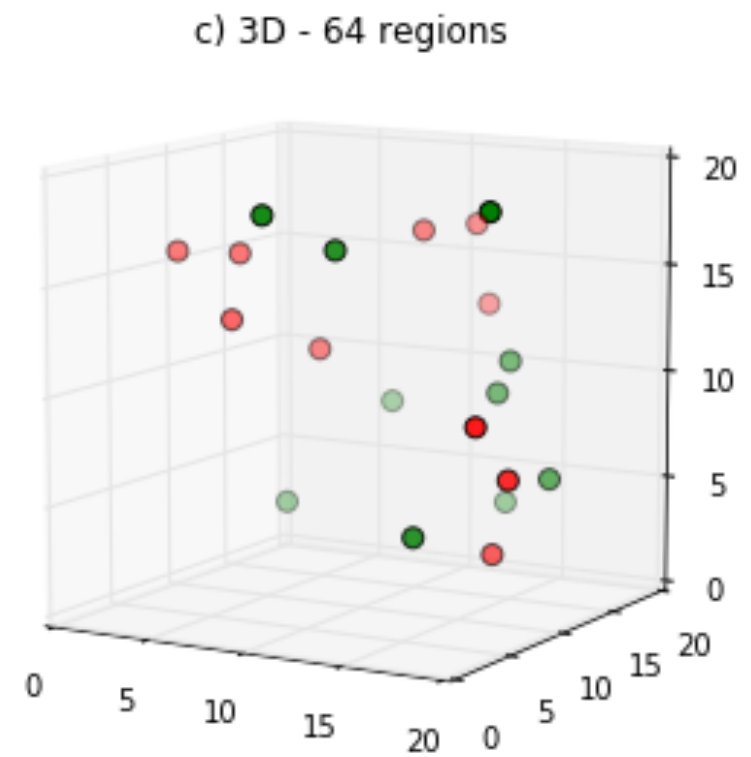
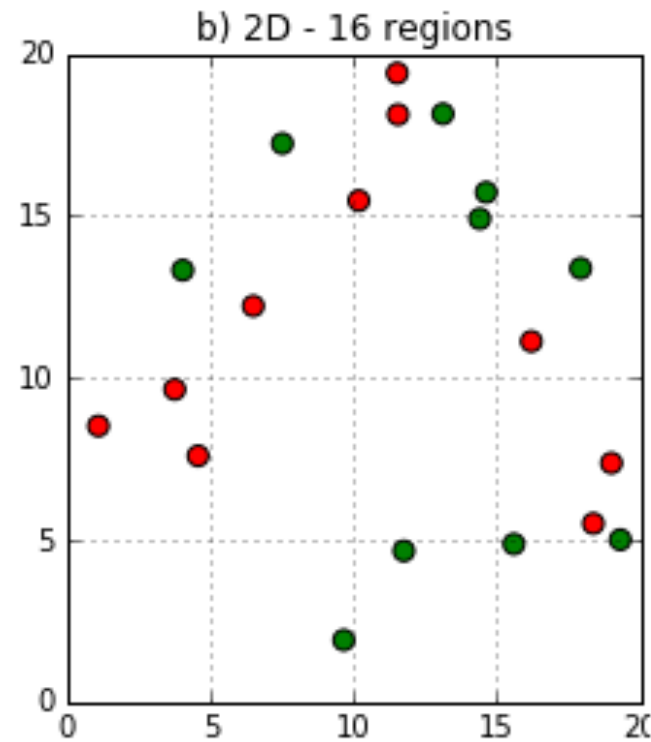
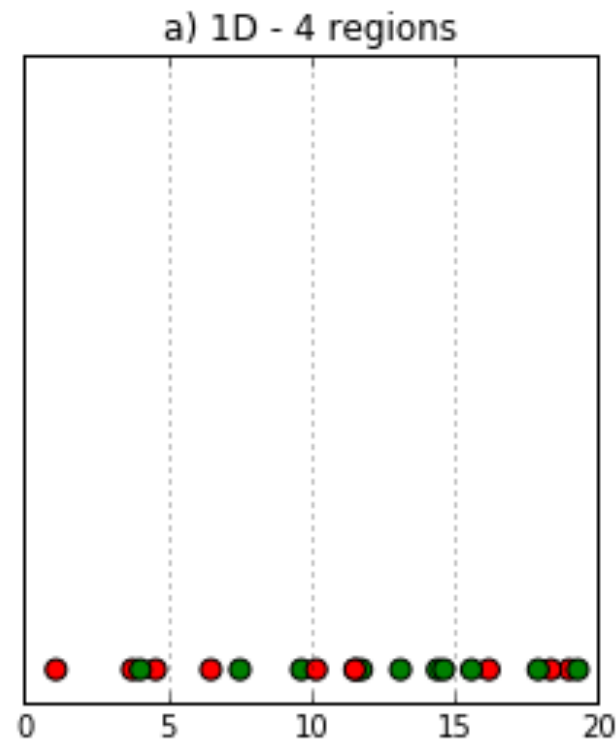
The more parameters the bigger the dictionary, if no drops in accuracy is wanted.

Memory usage inefficiency

Exhaustive search can be computationally inefficient.

The Curse of Dimensionality in Dictionary-based MR Fingerprinting

Adding a new dimension to the problem leads to an **exponential growth** in the number of entries to be insert into the box if no degradation in resolution are wanted [1]

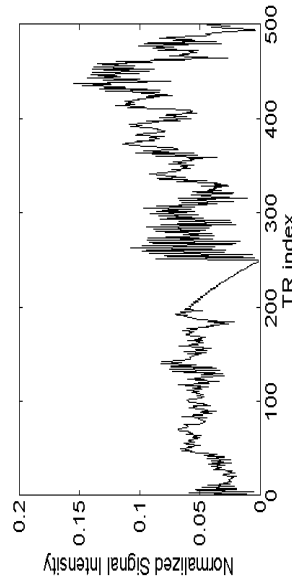


This introduce sparsity, which can produce high biases in nearest-neighbour algorithms [2]

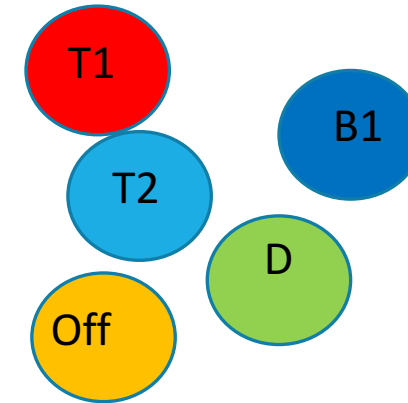
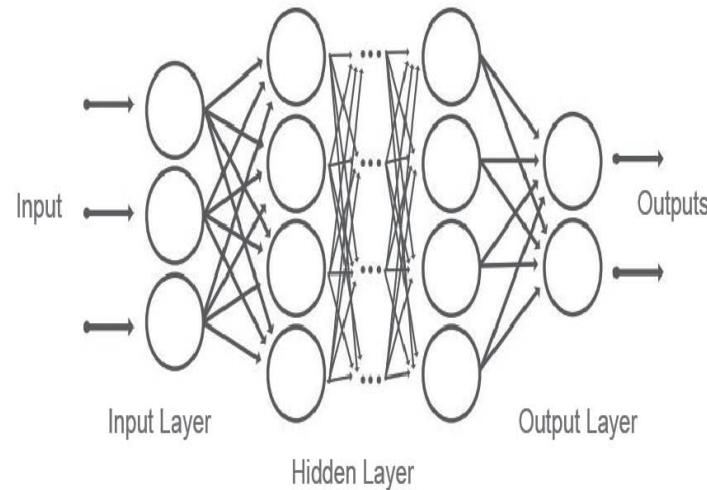
[1] R. Bellman, Adaptive control processes: a guided tour, Princeton University Press, 1961.

[2] J. H. Friedman, On bias, variance, 0/1-loss, and the curse-of-dimensionality, Data Mining and Knowledge Discovery 1 (1) (1997)

Circumventing the Curse of Dimensionality through a Deep Learning Approach



Examples from the signal space



MR parameters that generated the input signal

Learning the Inverse Transfer Function

Once trained, the Neural Network Model allows dictionary free MRF, because the model approximates the inverse transfer function.

Deep Learning for MRF

Our activity

Numerical simulations using different MRF pulse sequences: <https://arxiv.org/abs/1811.11477>

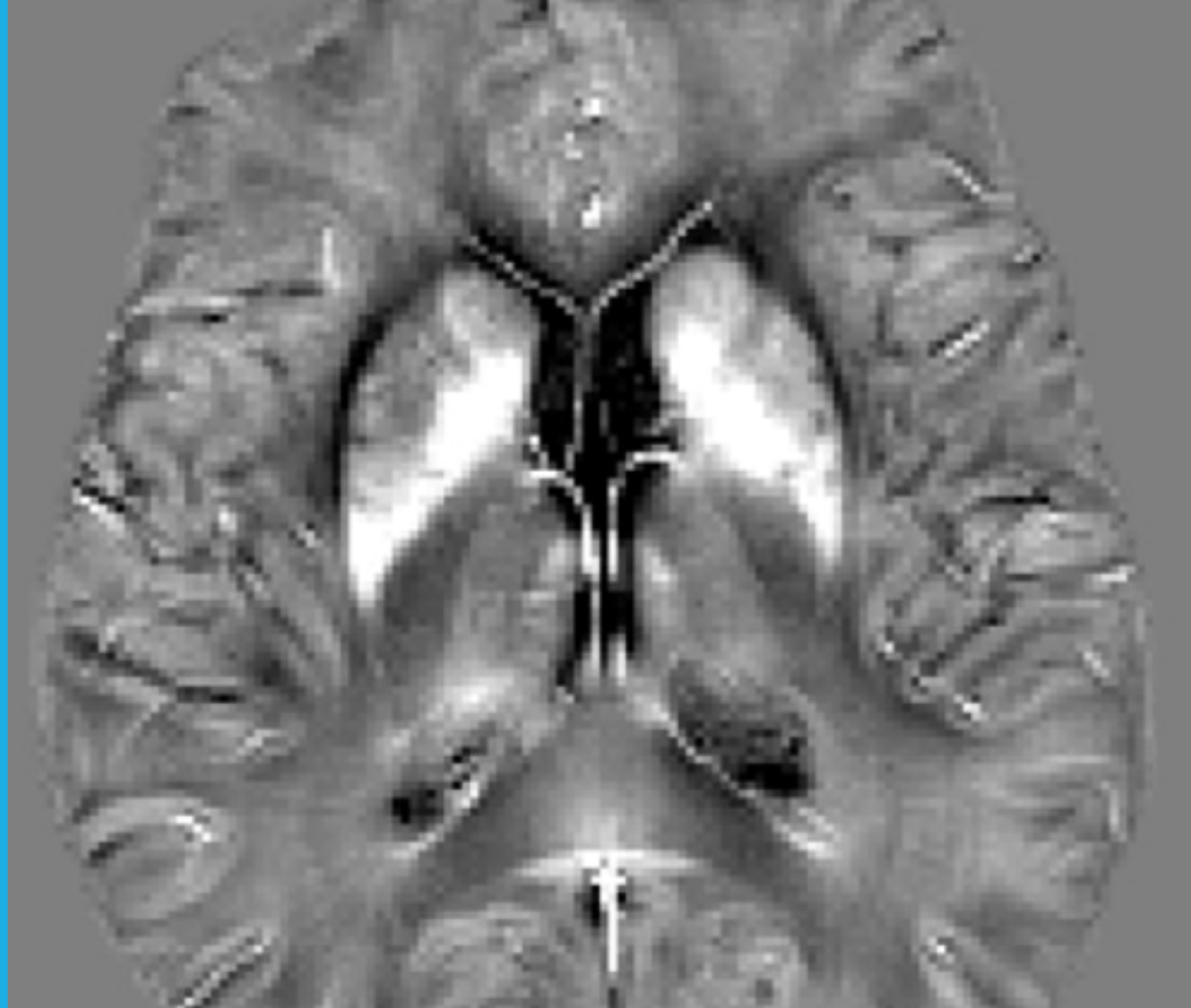
Deep Learning approach scales really well with number of MR parameters, while dictionary matching approach scales poorly.



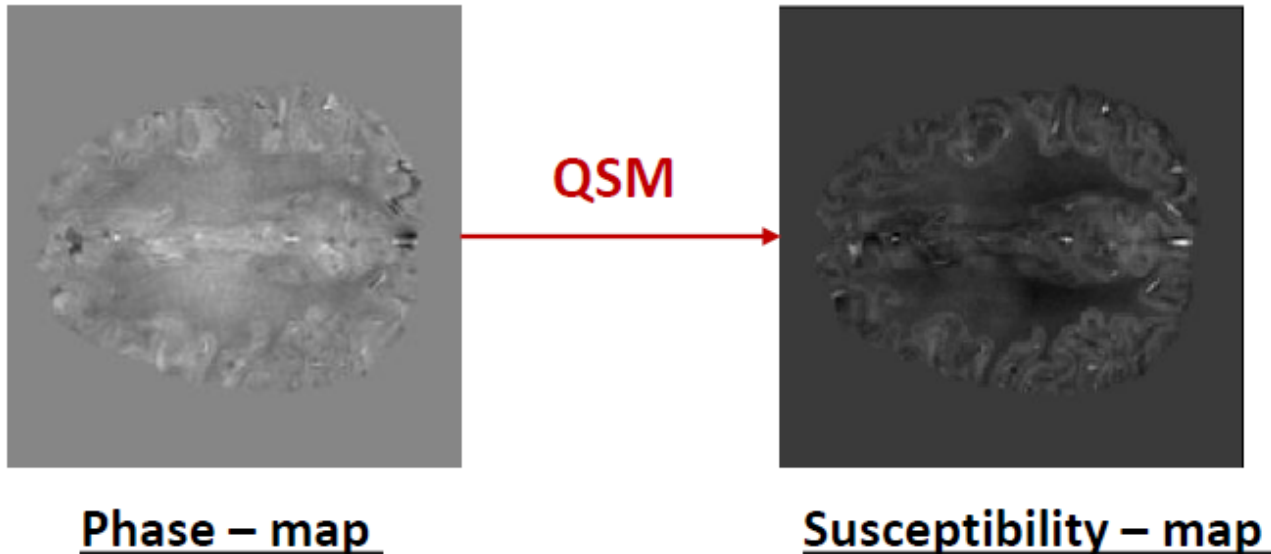
Quantitative Susceptibility Mapping

Deep Learning approach

Collaboration with
"Sir Peter Mansfield
Institute" Nottingham UK



Quantitative Susceptibility Mapping: using the phase of the signal to retrieve tissue properties



Susceptibility map: tissue contrasts in MRI

- 1980s, diseases characterization
- Response to an external magnetic field
- *In vivo*: water, myelin, iron and calcium

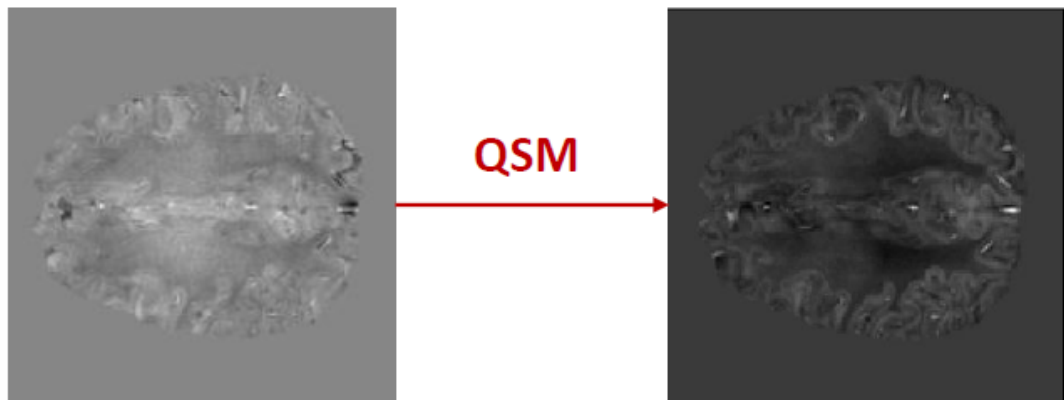
Applications

- Anatomical imaging of human brain
- Lesion classification
- TBI (Traumatic Brain Injury)
- Brain tumours
- Neurodegenerative diseases
- DBS (Deep Brain Stimulation)
- Blood oxygen saturation
- Short relaxation times

$$\vec{M} = \chi \vec{H}$$

Dimensionless proportionality constant indicating the degree of magnetization of a material in response to an applied magnetic field.

Quantitative Susceptibility Mapping: an ill-posed problem



$$\chi(k) = \Delta B(k) / \left(\frac{1}{3} - (\hat{\mathbf{k}} \cdot \hat{\mathbf{z}})^2 \right) = \Delta B(k) / D(k)$$

Noise and errors amplification

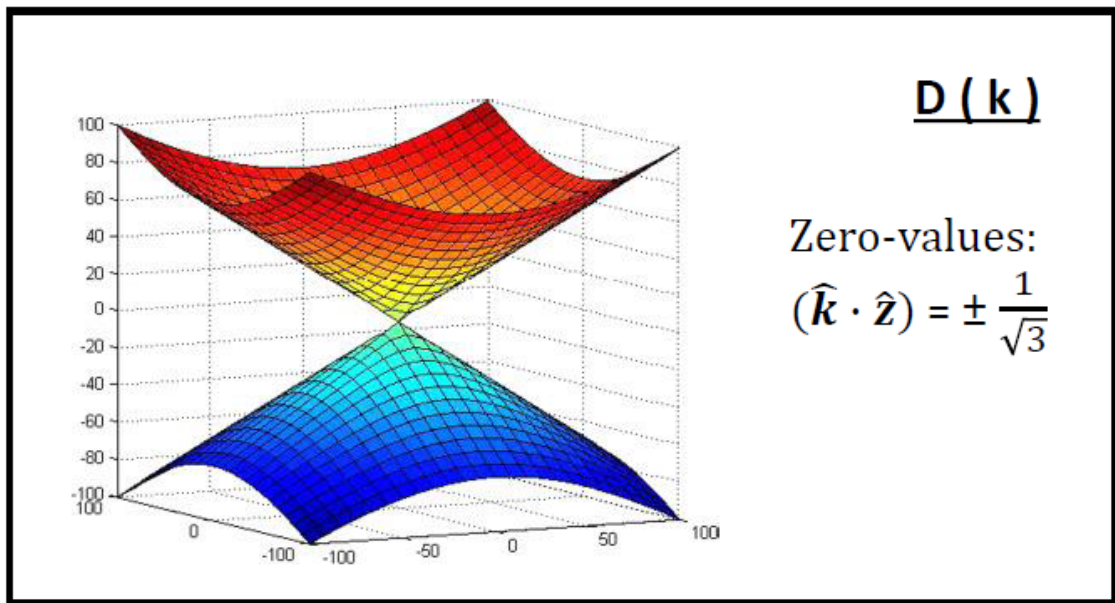
Inverse Problem: $\varphi(r) \rightarrow \chi(r)$

Ill-posed problem: $D(k) = 0$ in k-space

- Different object orientations
- Numerical strategies

Phase – map

Susceptibility – map



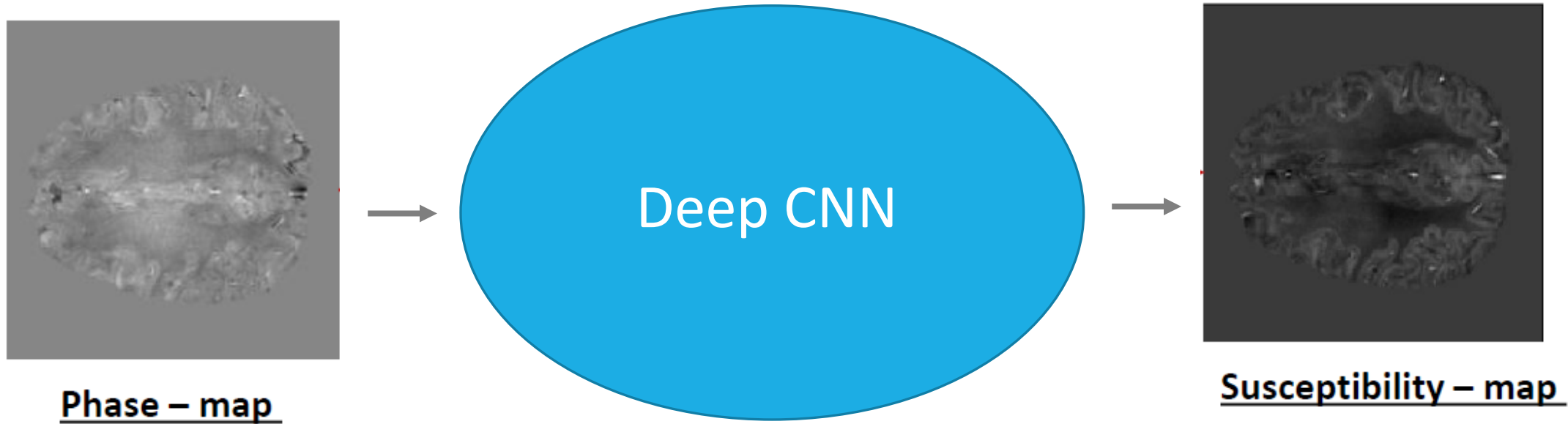
TKD:
(Truncated K-space Division)
Faster
Noise and artifacts

COSMOS:
(Calculation Of Susceptibility through Multiple Orientation Sampling)

Long acquisition time
More accuracy



Quantitative Susceptibility Mapping: Deep Learning approach (*in progress*)



Train a Deep CNN to retrieve COSMOS output with only one phase map

- Time efficiency without drops in accuracy;
- Feasible in clinical protocols.