



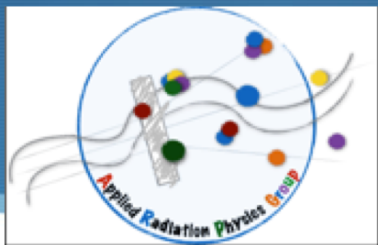
- 14:15 Introduction
Riccardo Faccini (*Sapienza e INFN Roma*)
- 14:35 Medical image processing and analysis
Alessandra Retico (*INFN Pisa*)
- 15:15 Artificial intelligence in MR image analysis
Carlo Mancini Terracciano (*INFN Roma*)
- 15:35 Break
- 15:55 Automatic classification of patients response to chemo-radiotherapy in rectal cancer
Cecilia Voena (*INFN ROMA*)
- 16:15 In vivo drugs monitoring by ^{19}F -MR imaging and ^{19}F -MR spectroscopy
Silvia Capuani (*CNR ISC UOS Roma Sapienza*)
- 16:35 Machine Learning applications to doctor-patient interactions
A. Ciardiello (*Univ. Sapienza-INFN Roma*)





SAPIENZA
UNIVERSITÀ DI ROMA

ARPG



NUCLEAR MEDICINE

CHIRONE

(Radio Guided Surgery)

DOSE PROFILER

(Particle Therapy dosimetry)

HADRON THERAPY

FOOT

(RBE in PT)

FRED

(TPS with GPU)

MONDO

(Fast Neutron Detection)

GENIALE

(Low Energy Nuclear Interactions)

ARTIFICIAL INTELLIGENCE IN MEDICINE

MARIANNE

(Imaging for stadiation)

NEPTUNE

(^{19}F -MRI)

FILOBLU

(Patient-Doctor interactions)

Collaborations

Activity driven by medical input, with involvement of SMEs



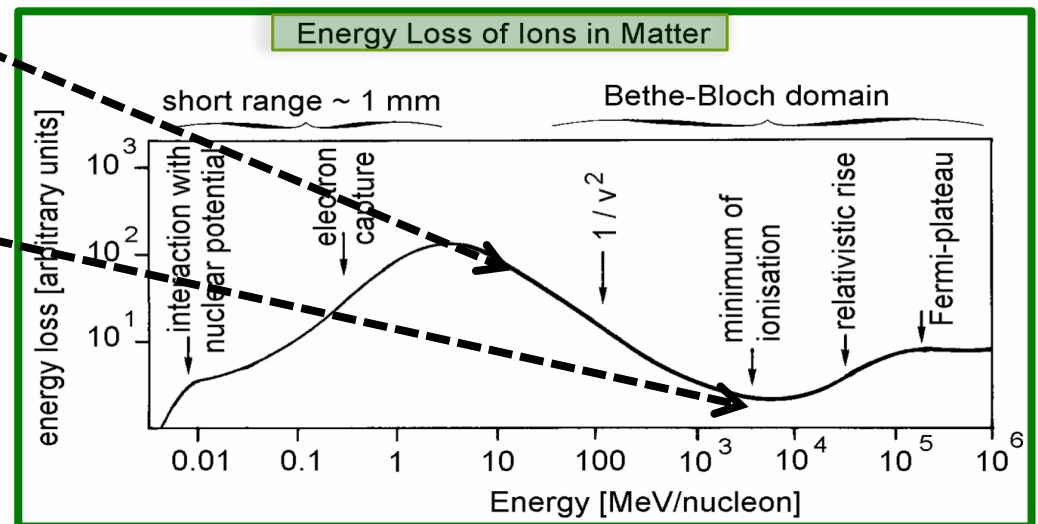
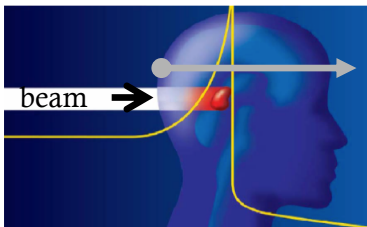
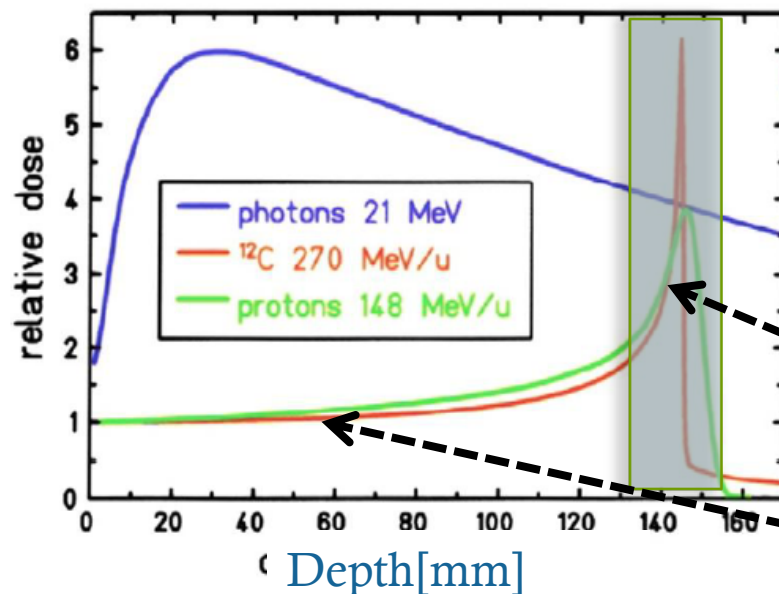
HADROTHERAPY



Hadrotherapy

Proton/ion beams on patient

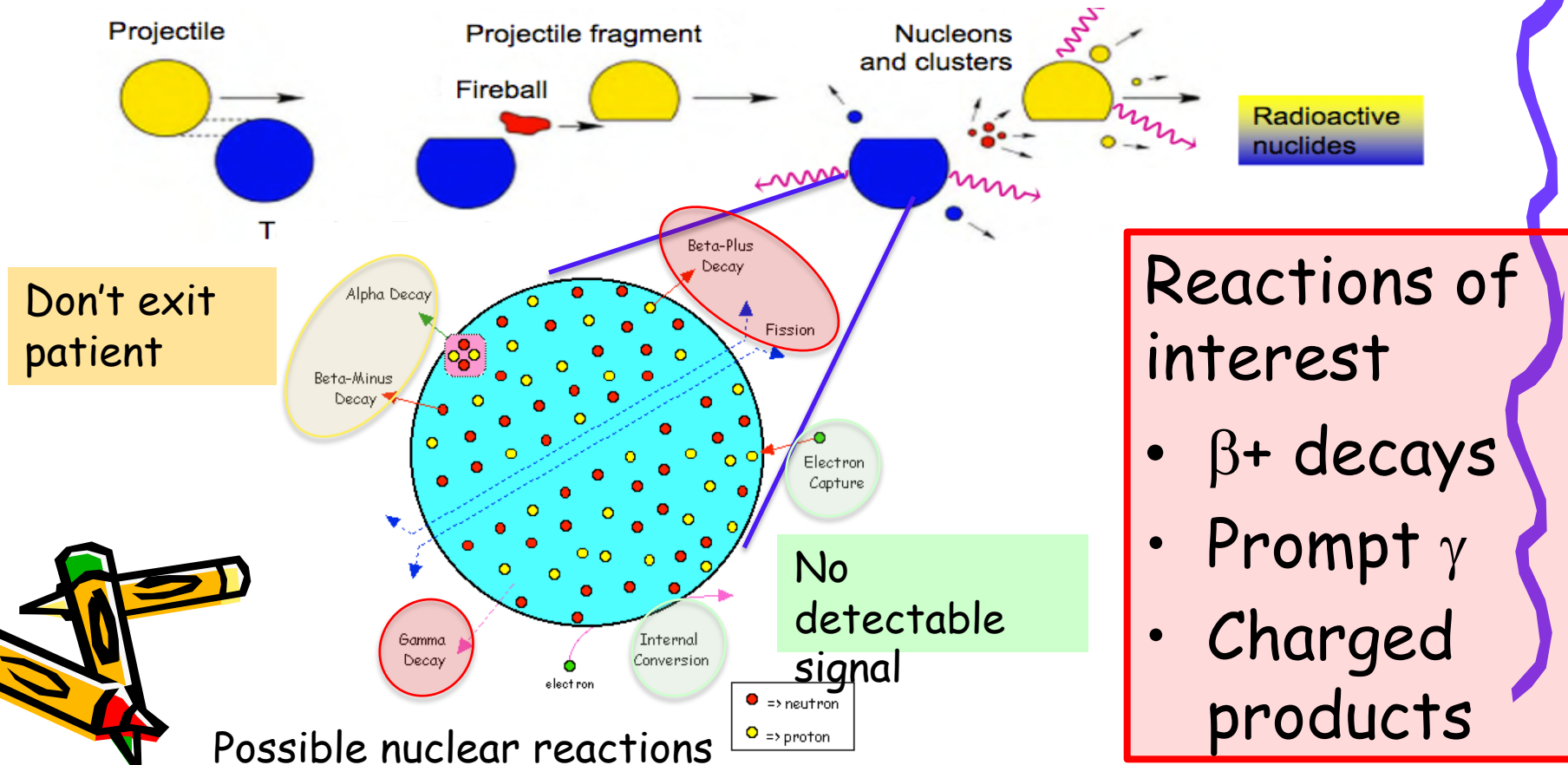
Concentrate release of energy inside **tumor** due to release of energy in ionization.



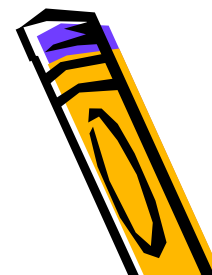
Measuring the dose

RF, V. Patera,
"Dose Monitoring in
Particle Therapy",
Mod. Phys. Lett. A

Based on nuclear reactions between
the projectile and the patient



Correlation between activity and dose

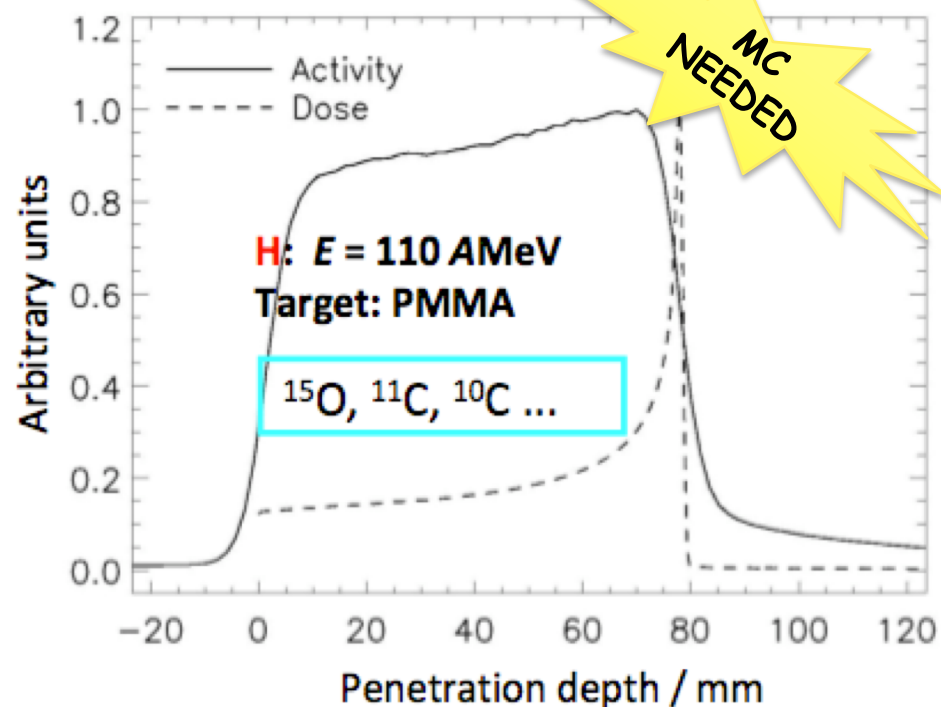
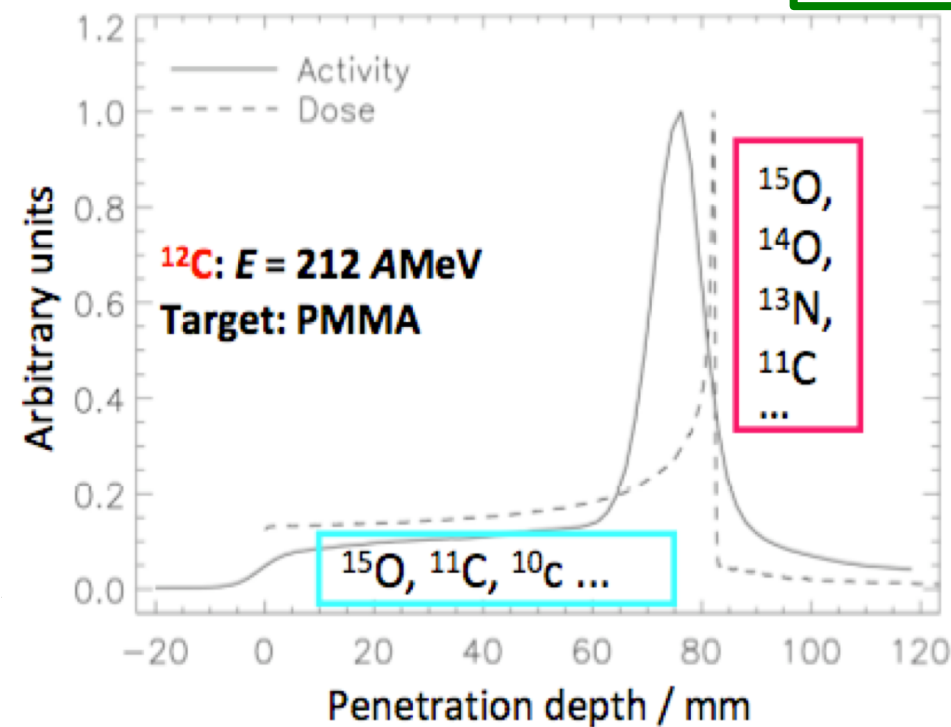


Therapy beam	^1H	^3He	^7Li	^{12}C	^{16}O	Nuclear medicine
Activity density / $\text{Bq cm}^{-3} \text{ Gy}^{-1}$	6600	5300	3060	1600	1030	$10^4 - 10^5 \text{ Bq cm}^{-3}$

Projectiles & target fragmentation

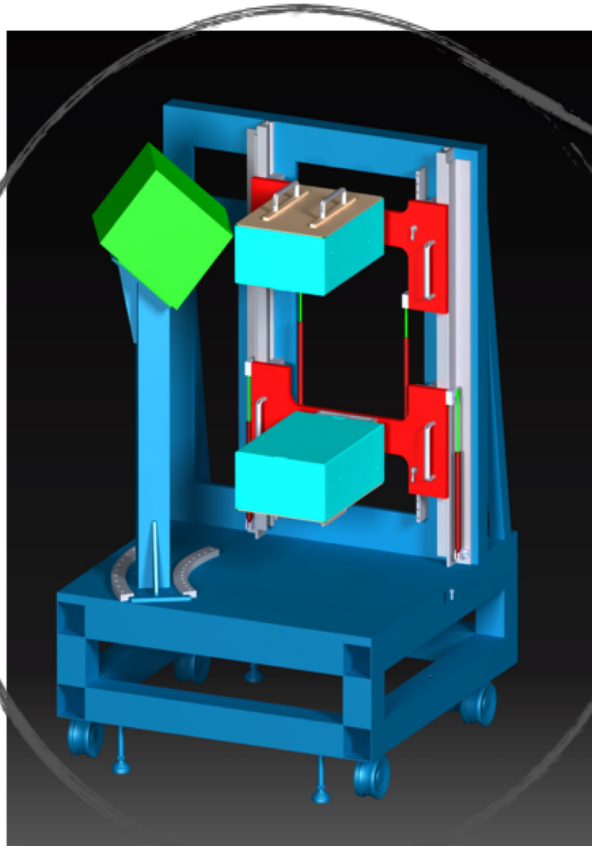
Target fragmentation

Example of β^+

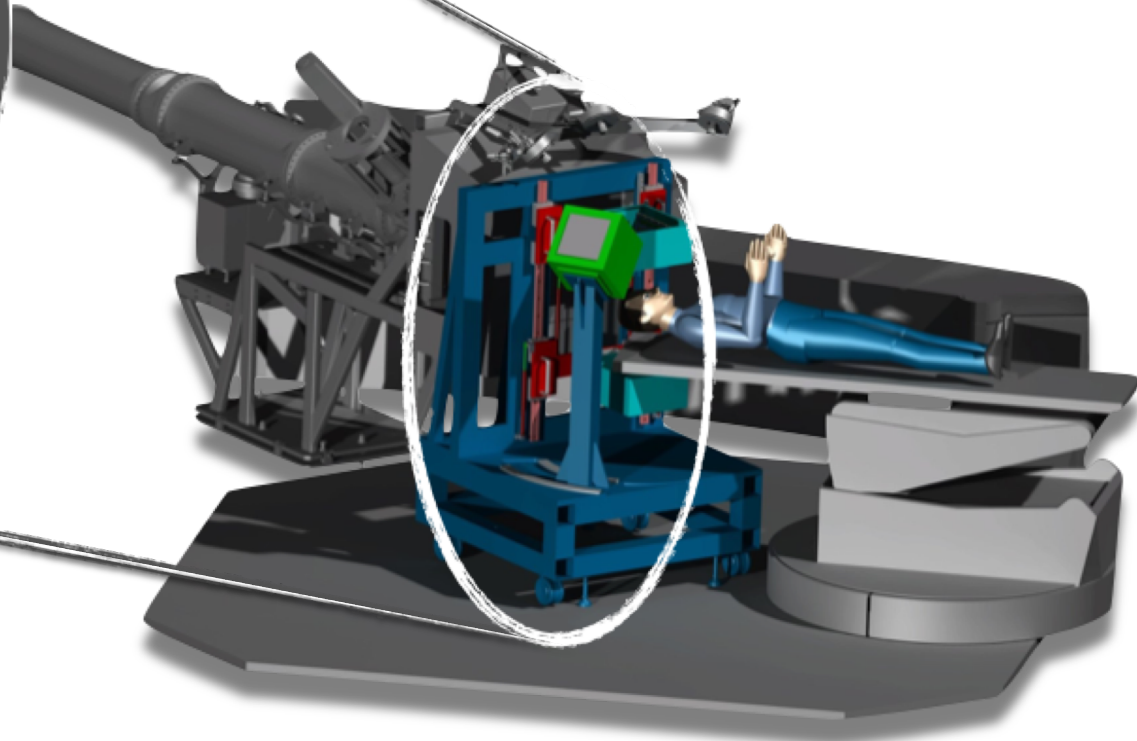


Range monitor applications

- ◆ To exploit the secondary particles detections as an online monitor, a **Dose Profiler** has been designed (within the INSIDE Italian project) to be deployed in the CNAO treatment center.



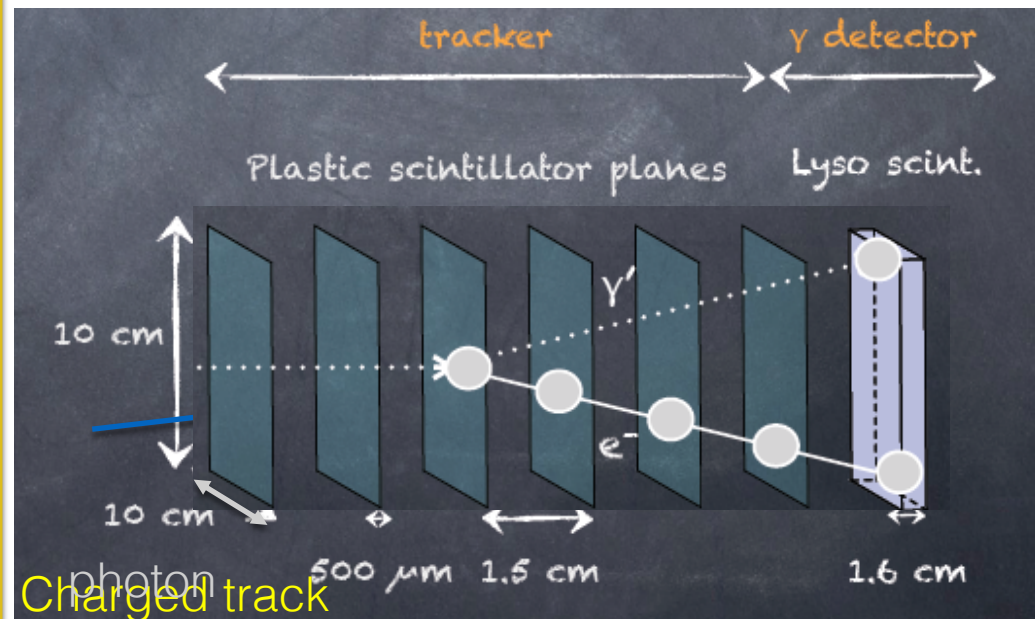
Project funded as a part of
INSIDE Prin, **INFN RDH**
and **Premiale C.F.**



Dose Profiler

Need a detector to simultaneously measure the rate of:

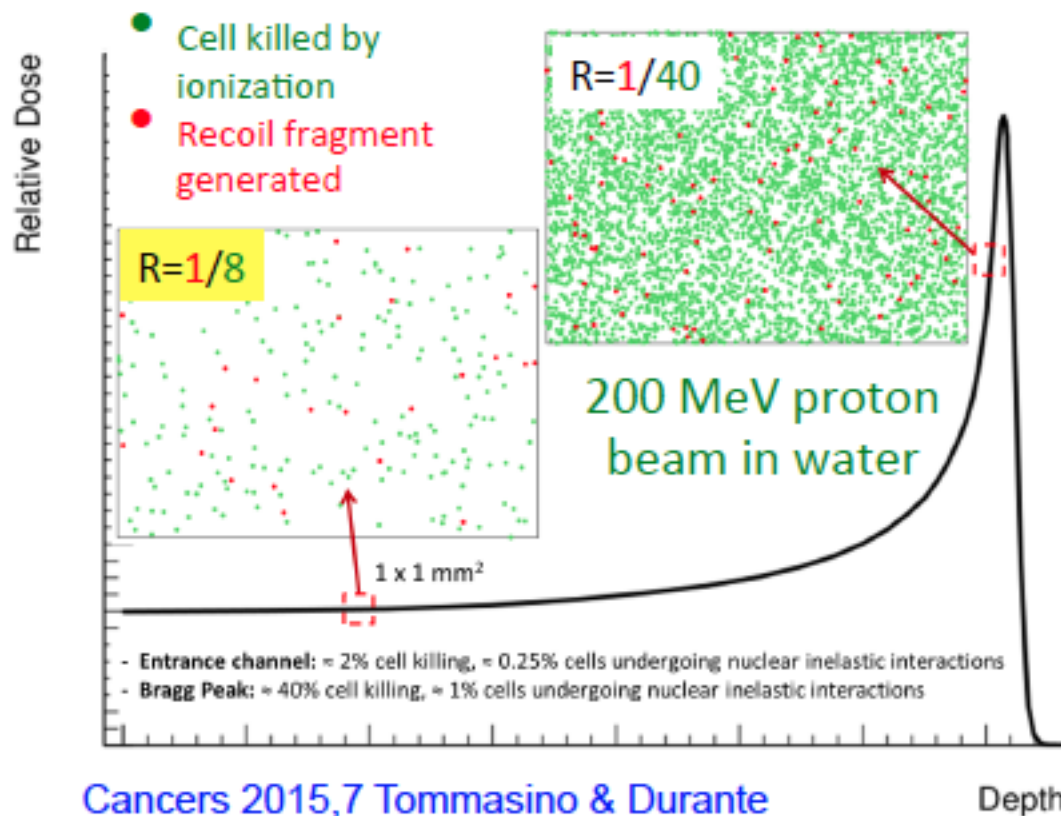
- charged particles with multilayer for track reconstruction
- single photons with compton camera





Target (patient) fragmentation & PT

Target fragmentation in proton therapy: gives contribution also outside the tumor region!



About 10% of biological effect in the entrance channel due to secondary fragments (Grun 2013)

Largest contributions of recoil fragments expected from

He, C, Be, O, N

In particular on
Normal Tissue

Complication Probability

See also :

- Paganetti 2002 PMB

- Grassberger 2011 PMB



p-> C, p->O scattering @200 MeV

The elastic interaction and the forward Z=1 fragment production (p,d,t) are quite well known. Large uncertainty on large angle Z=1,2 fragments.

Missing data on heavy fragments. Unreliable nuclear models

“Heavy” (A>4)
fragment yields
and emission
energy ~ unknown

Very low energy-
short range
fragments.

MCs confirm this
picture

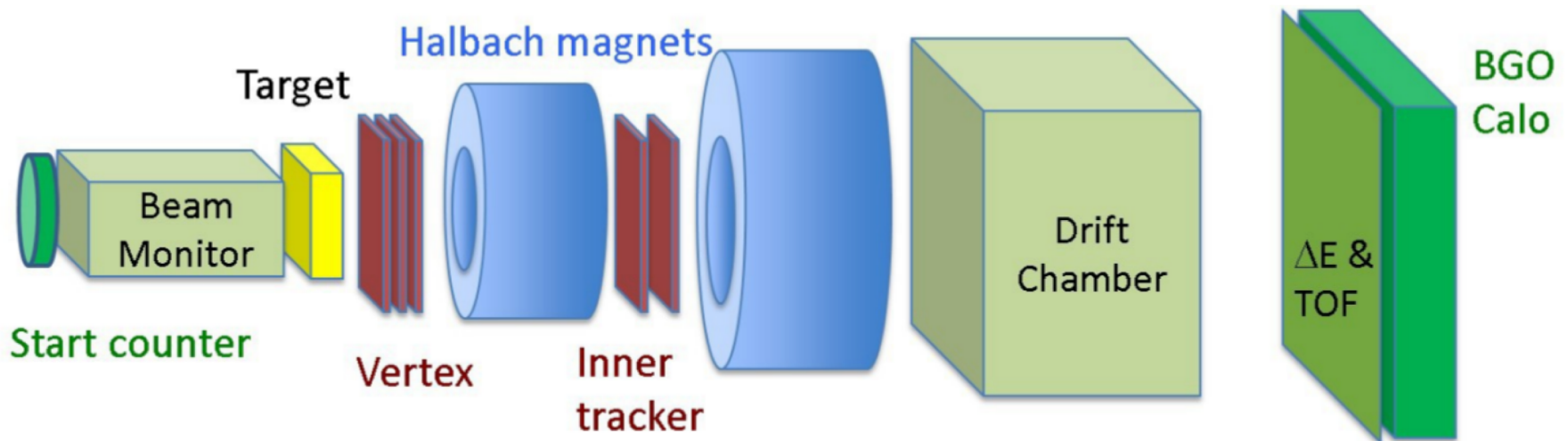
Nuclear model &
MC not reliable

Analitic model results on p->O @200 MeV

Fragment	E (MeV)	LET (keV/ μ m)	Range (μ m)
¹⁵ O	1.0	983	2.3
¹⁵ N	1.0	925	2.5
¹⁴ N	2.0	1137	3.6
¹³ C	3.0	951	5.4
¹² C	3.8	912	6.2
¹¹ C	4.6	878	7.0
¹⁰ B	5.4	643	9.9
⁸ Be	6.4	400	15.7
⁶ Li	6.8	215	26.7
⁴ He	6.0	77	48.5
³ He	4.7	89	38.8
² H	2.5	14	68.9

Cancers 2015,7 Tommasino & Durante

The FOOT Experimental setup

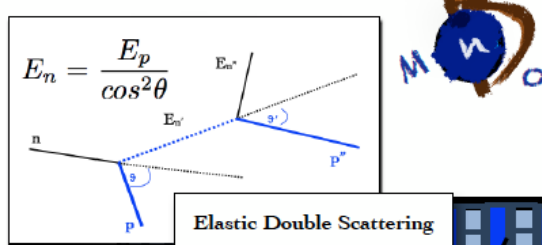


Expected performances:

- Resolution on fragment X-section < 5%
- Energy resolution < 1 MeV/u
- Measurements of Z with mistag < 3%
- Measurement of A with mistag < 5%

MONDO (Fast Neutron Detection)

High energy neutron detector



In a particle therapy treatment the beam interactions with patient produce many secondary particles. Monitoring methods using photons and charged particles have already been proposed, but no attempt has been made yet to use the abundant neutron component. The large penetrating power of neutrons produces nearly energy threshold free escape, providing a secondary particle sample that is higher in number with respect to photons and charged particles. Therefore, neutrons allow for a backtracking of the emission point that is not affected by multiple scattering.

Moreover The neutron induced complications are the main concerns in Particle Therapy administration and planning, in particular in pediatric treatments [1].

We want to measure and track the ultra-fast neutrons produced in Particle Therapy treatments developing a **tracking device** tailored for hadrontherapy dose monitoring applications!

[1] M.Durante W.D. Newhauser doi:10.1038/nrc3069

Plastic Scintillator

- 4 x 4 x 8 cm³;
- scintillating fibres 250 µm;
- x-y layer orientation;

Image Intensifier: Triple GEM detector

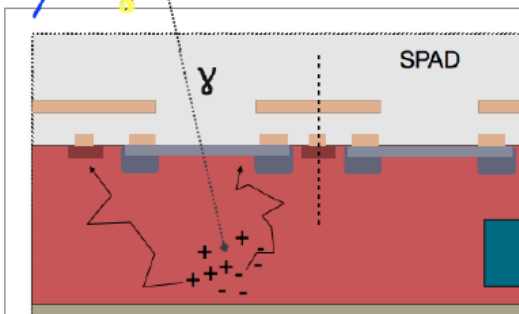
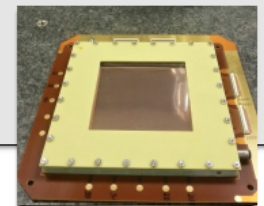
Gas Electron Multiplier

- 45 µm hole
- 70 µm hole distance
- triple GEM

We use GEM as photon intensifier instead of look for electron multiplication

Collaboration with
CERN

For GEM light
measurements => See
also D.Pinci
POSTER



- ✓ integrated TDC (resolution ~65 ps)
- ✓ self triggered sensor
- ✓ pixel 600 µm

Signals ReadOut: CMOS Single Photon Avalanche Diode (SPAD) array sensor



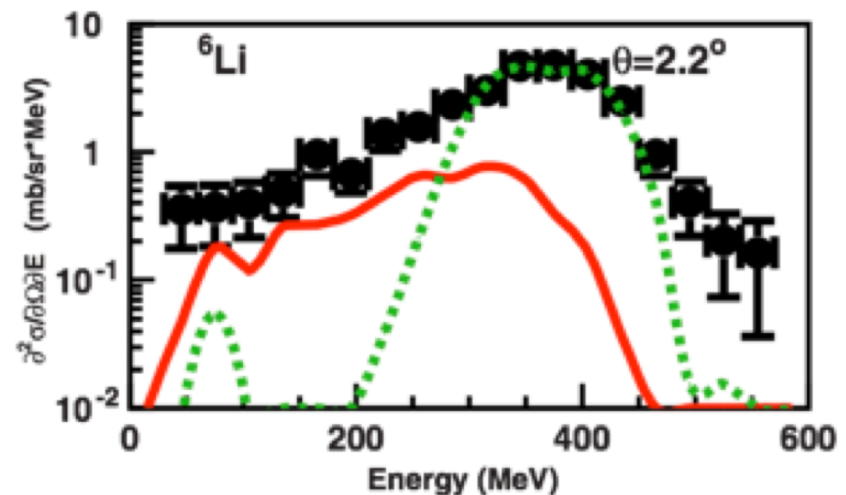
GENIALE

(Low Energy Nuclear Interactions)

- Despite the numerous and relevant application would use it, there is no dedicated model to nuclear interaction below 100 MeV/A in Geant4
- Many papers showed the difficulties of Geant4 in this energy domain:
 - Braunn et al. have shown discrepancies up to one order of magnitude in ^{12}C fragmentation at 95 MeV/A on thick PMMA target
 - De Napoli et al. showed discrepancy specially on angular distribution of the secondaries emitted in the interaction of 62 MeV/A ^{12}C on thin carbon target
 - Dudouet et al. found similar results with a 95 MeV/A ^{12}C beam on H, C, O, Al and Ti targets

- **Exp. data**
- **G4-BIC**
- **G4-QMD**

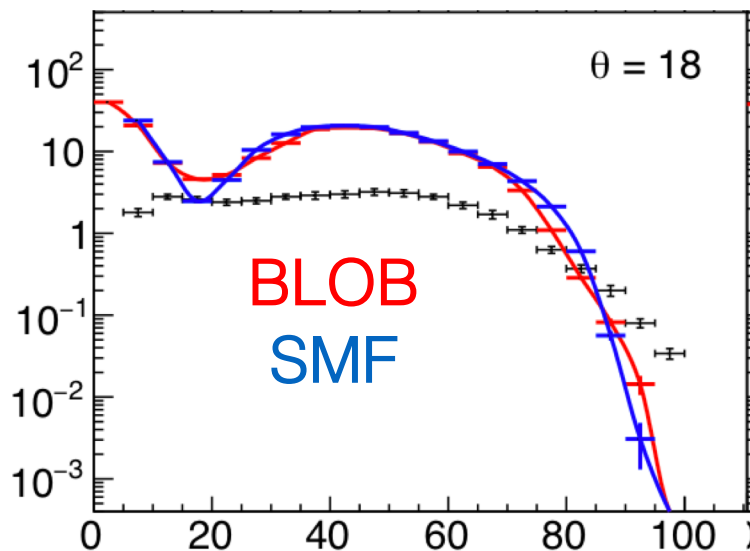
[Plot from De Napoli et al. Phys. Med. Biol., vol. 57, no. 22, pp. 7651–7671, Nov. 2012]



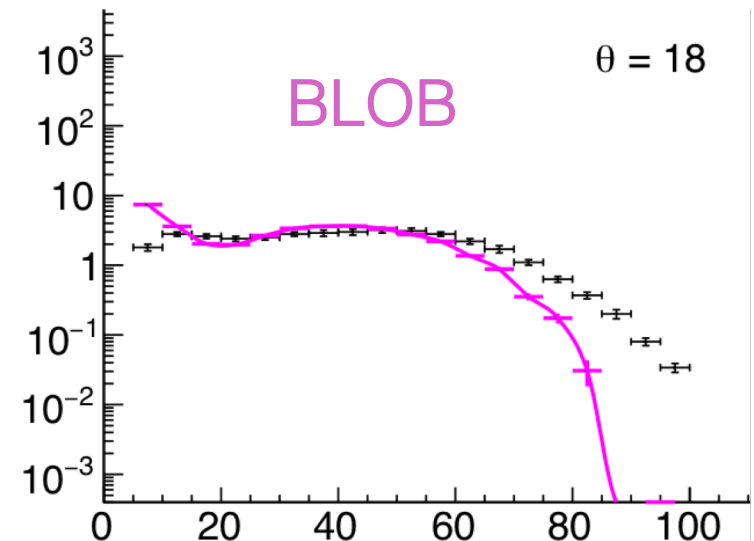
Cross section of the ^6Li production at 2.2 degree in a ^{12}C on ^{12}C reaction at 62 MeV/A.

GENIALE: results

Example: alpha production



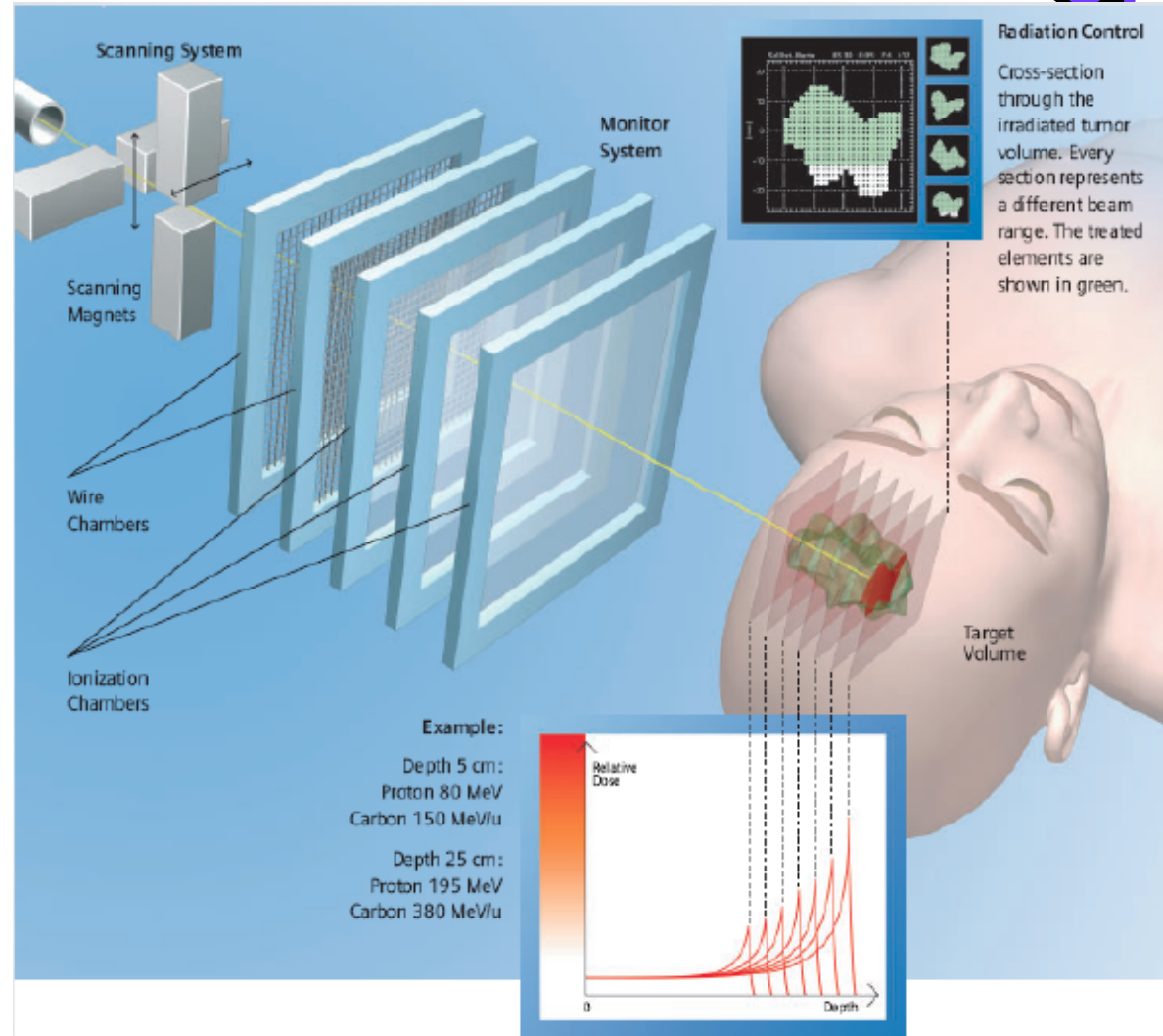
- COALESCENCE
- EXITATION ENERGY CORRECTION



FRED
(TPS with GPU)

Treatment Planning System

From the
tumor margin
to the beam
sequencing
("Raster
Scan")



Use of GPUs

Typical times:

- Full MC 72hr
- Analytical commercial sw: 1hr
- GPUs \rightarrow 1min



Algorithm 3.2.1 Original Dose Calculation

```
1: for  $i = 0$  to  $N_{beams}$  do
2:   for  $j = 0$  to  $N_{beamlets}[i]$  do
3:      $currentBeamlet \leftarrow j + ptr$ 
4:     calculate angle  $\theta$ 
5:     calculate radiological depth  $d$ 
6:     compute input and output body points and corrections  $W_1, W_2$ 
7:     for  $ivoxel = 0$  to  $N_{voxels}$  do
8:       calculate parameters to dose calculation
9:       compute  $F_x$ 
10:      calculate dose  $D(\vec{r})$ 
11:    end for
12:  end for
13:   $ptr \leftarrow ptr + N_{beamlets}[i]$ 
14: end for
```

Split algo to
parallelize

Algorithm 3.2.2 Loop 1

```
1: for  $i = 0$  to  $N_{beams}$  do
2:   for  $j = 0$  to  $N_{beamlets}[i]$  do
3:      $currentBeamlet \leftarrow j + ptr$ 
4:     calculate and store angle  $\theta$ 
5:     calculate and store radiological depth  $d$ 
6:     compute and store input and output body points
7:   end for
8:    $ptr \leftarrow ptr + N_{beamlets}[i]$ 
9: end for
```

Algorithm 3.2.4 Kernel Loop

```
1:  $threadIdx, blockIdx$ 
2: for  $i = 0$  to  $N_{beams}$  do
3:   for  $j = 0$  to  $N_{beamlets}[i]$  do
4:     calculate  $x$  and  $y$ 
5:     calculate parameters to dose calculation
6:     compute  $F_x$ 
7:     each thread calculates its dose contribution  $D(\vec{r})$ 
8:   end for
9:    $ptr \leftarrow ptr + N_{beamlets}[i]$ 
10: end for
```

Hardware and Performance

		Threads	primary/s	$\mu s/primary$
CPU ^a	full-MC *	1	0.75 k	1340
	FRED	1	15 k	68
	FRED	16	50 k	20
	FRED	32	80 k	12.5
GPU	FRED	1 GPU ¹	500 k	2
	FRED	2 GPU ²	2000 k	0.5
	FRED	4 GPU ³	20000 k	0.05

Table A1: Computing times for different hardware architectures.

^a motherboard with two Intel[®] Xeon E5-2687 8-Core CPU at 3,1GHz

¹ LAPTOP: Apple[®] MacBook Pro with one AMD[®] Radeon R9 M370X.

² DESKTOP: Apple[®] Mac Pro with two AMD[®] FirePro D300.

³ WORKSTATION: Linux box with four NVIDIA[®] GTX 980.

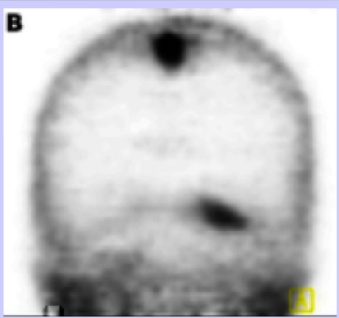
NUCLEAR MEDICINE



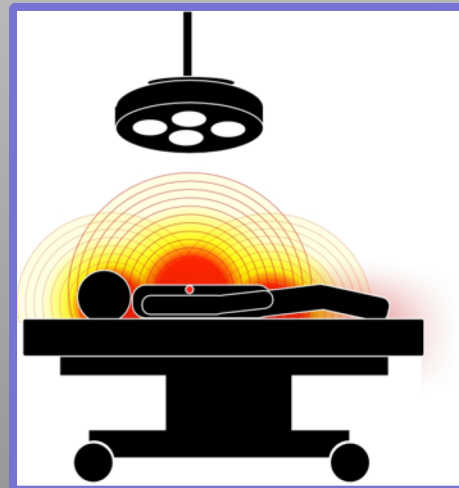
Radio Guided Surgery

PET/SPECT scan
to estimate
receptivity and
background

Each tumor requires its
own tracer



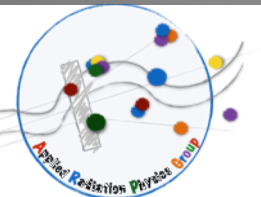
Administration
of radio-tracer



During surgery a probe
is used to detect
residuals/lymphnodes



Probe adjustable
to needs



LIMITS OF γ -RGS

140 keV photons
→ attenuation in body ~8cm

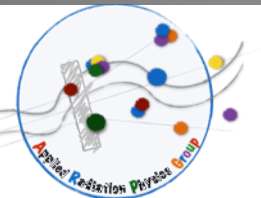
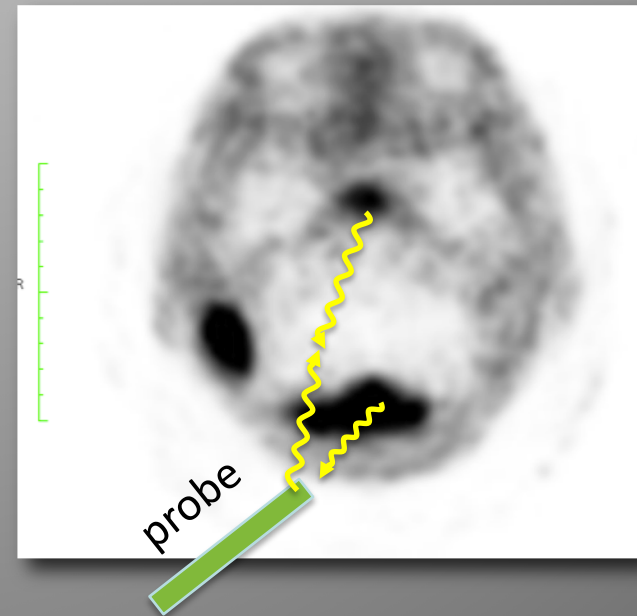
Long range of gamma's involve:

- exposure of medical personnel
- Background from healthy organs



Difficult to apply in:

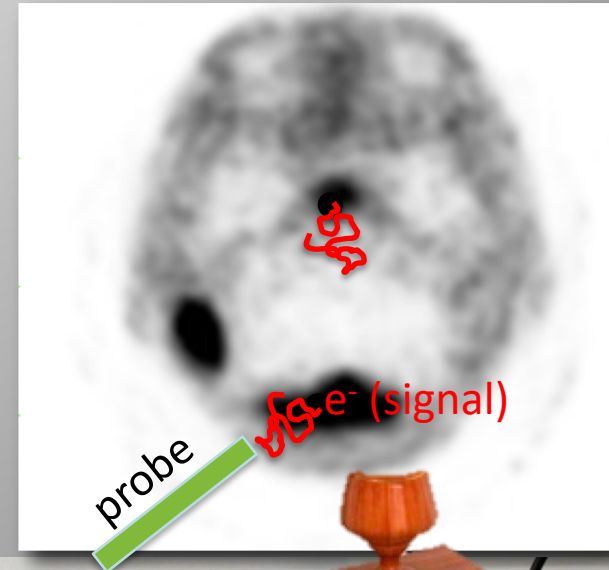
- Brain tumors
- Abdominal tumors
- Pediatric tumors



A CHANGE IN PARADIGM

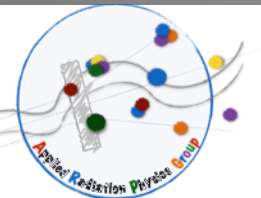
- Use of β^- tracers (electrons): pros
 - Detect electrons that travel ~ 100 times less than γ
 - Tracers with ^{90}Y can be used (already used for Molecular RT)
 - No background from gamma
 - Shorter time to have a response
 - » Smaller administered activity
 - Smaller and more versatile detector
 - reduced effect of nearby healthy tissues
 - Reduced dose to medical staff

E. Solfaroli Camillocci et al, Sci. Repts. 4,4401 (2014)



NOTE: only detection at contact is possible

EXTEND RGS TO MORE
CLINICAL CASES



The probe prototype

Compact, easy to handle,
local measurement

Simple technology:

- scintillating crystal
- Light sensor (SiPM)

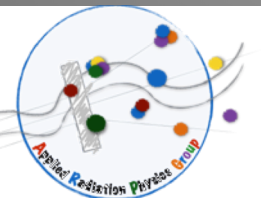
Most stringent constraints:

- Mechanics
- electrical safety
- sterilization

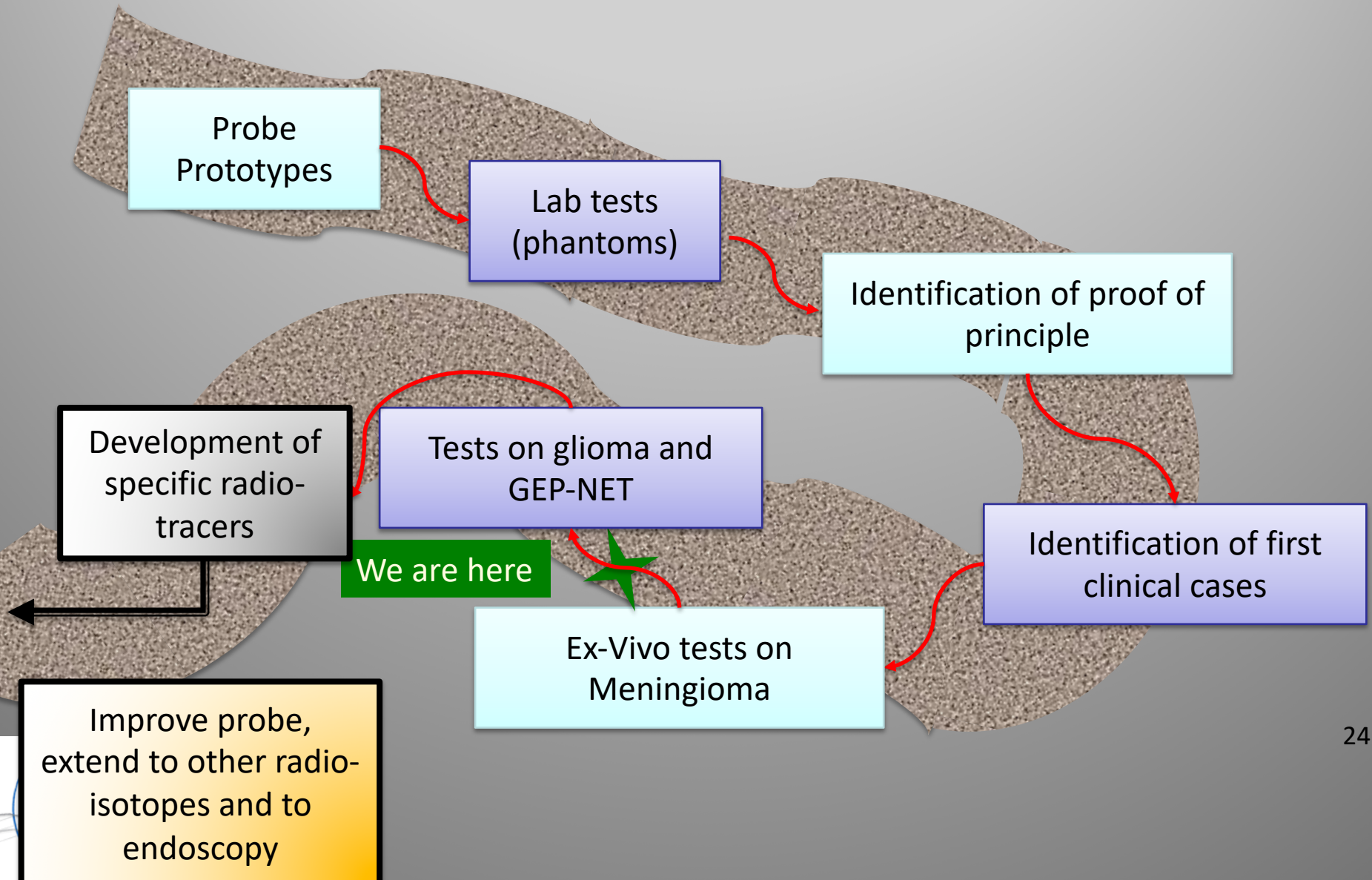
Ongoing R&D:

- Detector improvements to lower energy threshold
- Laparoscopic application (adjustment in size, multiple reading for information from the side)

Fig: Probe in ex-vivo tests on meningioma



RESEARCH PATH



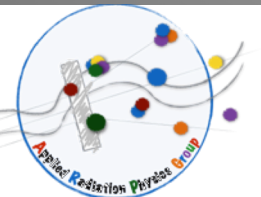
Perspectives

Application to other radio-tracers

- ^{68}Ga in prostate cancer
- Development of a CMOS sensor based device
 - Extend to more radionuclides → more tumors

Other applications of low energy electrons detection

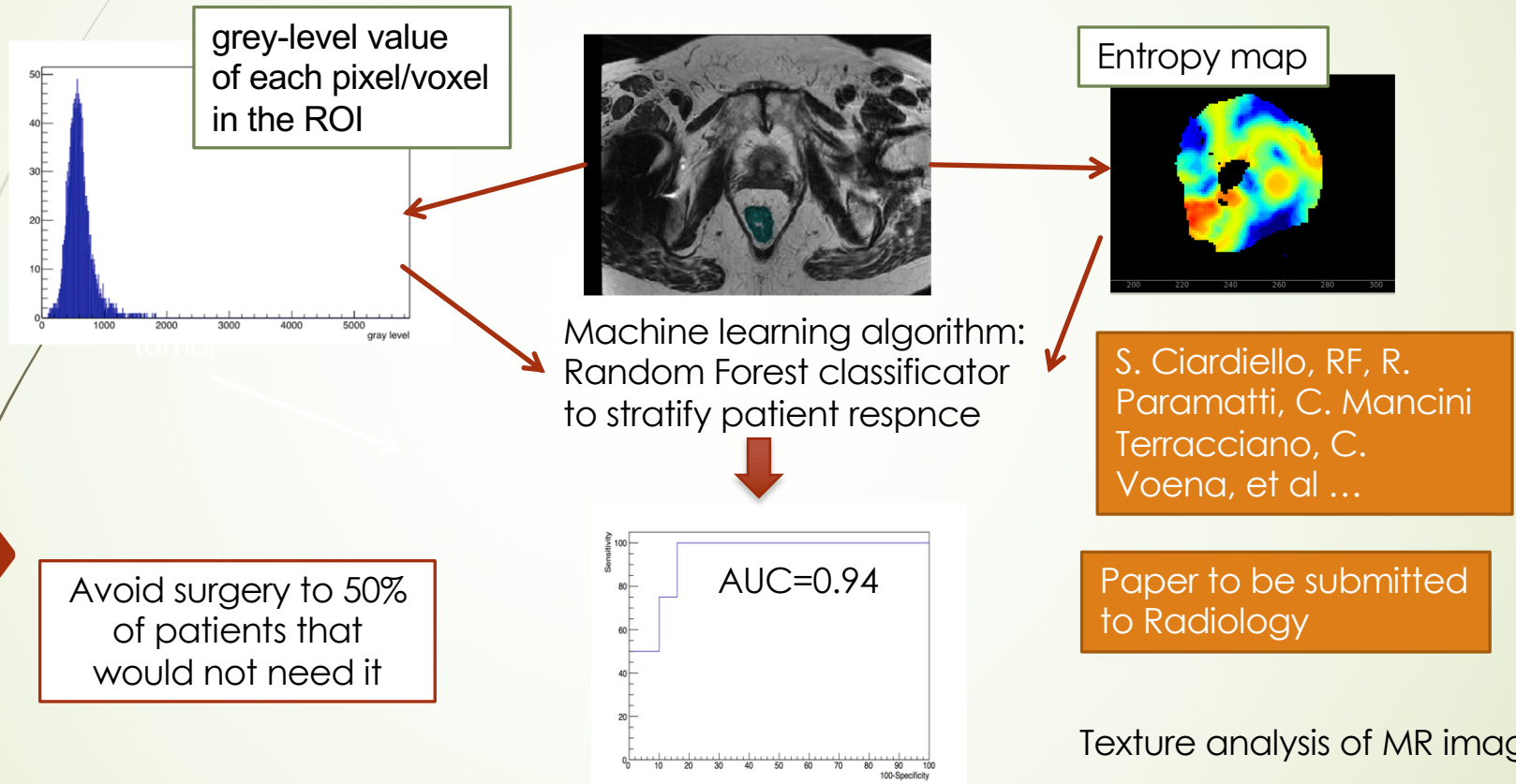
- dosimetry in **radio-metabolic therapy**
- use of cell-phones in **massive dose monitoring** during nuclear emergencies
- particulate density measurement in **pollution detectors**



ARTIFICIAL INTELLIGENCE IN MEDICINE



Automatic classification of response to chemoradiotherapy in rectal cancer using 3T T2-w MRI



Tomotherapy Quality assurance

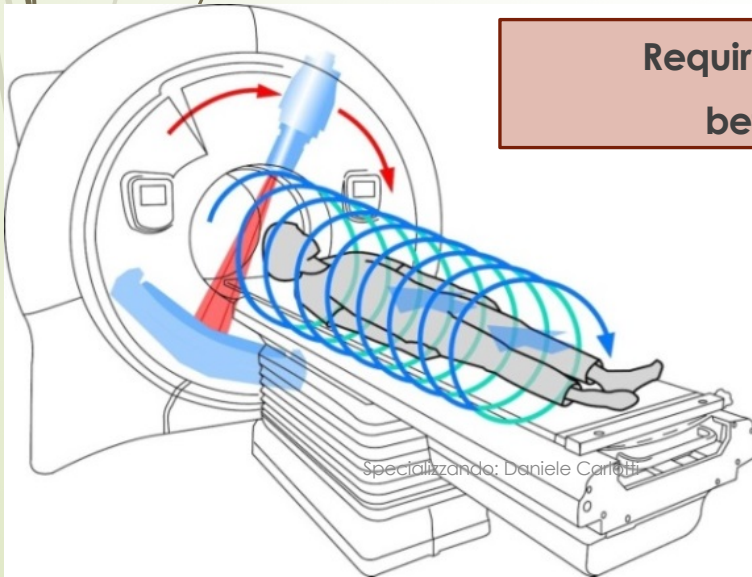
Tomotherapy (radiotherapy by slices) is a radiotherapy with very accurate dose profiling



Complex dose delivery



Requires accurate verification of correspondence between estimated and measured activity



Application of Machine Learning

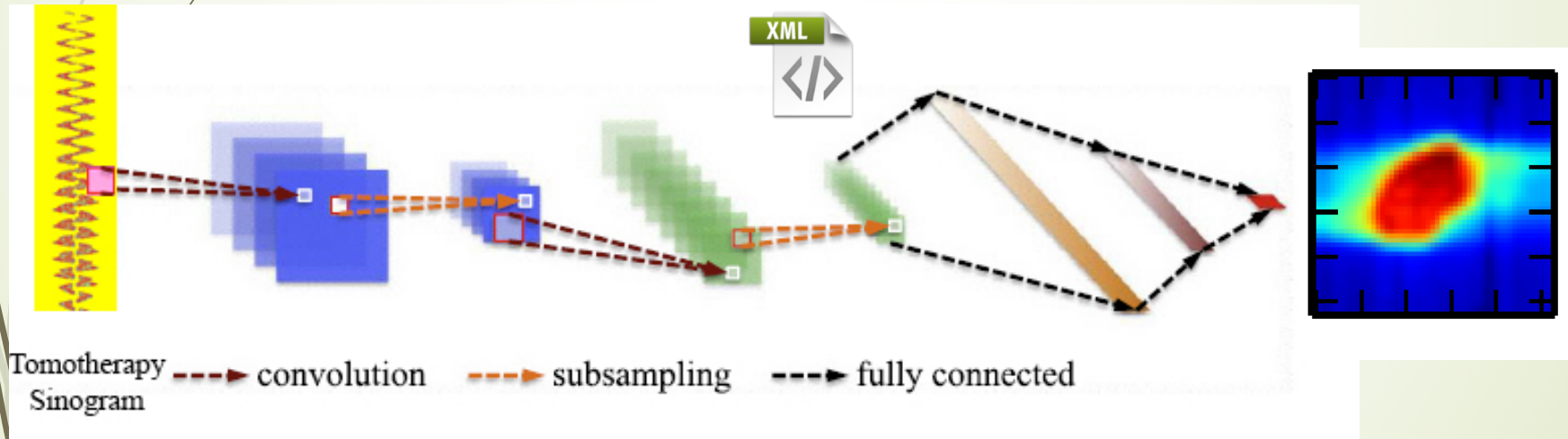
Aim of the study: develop an algorithm capable to estimate, patient by patient, the dose profile of TomoTherapy HiArt Delivery Quality Assurance (DQA)



Towards artificial QA

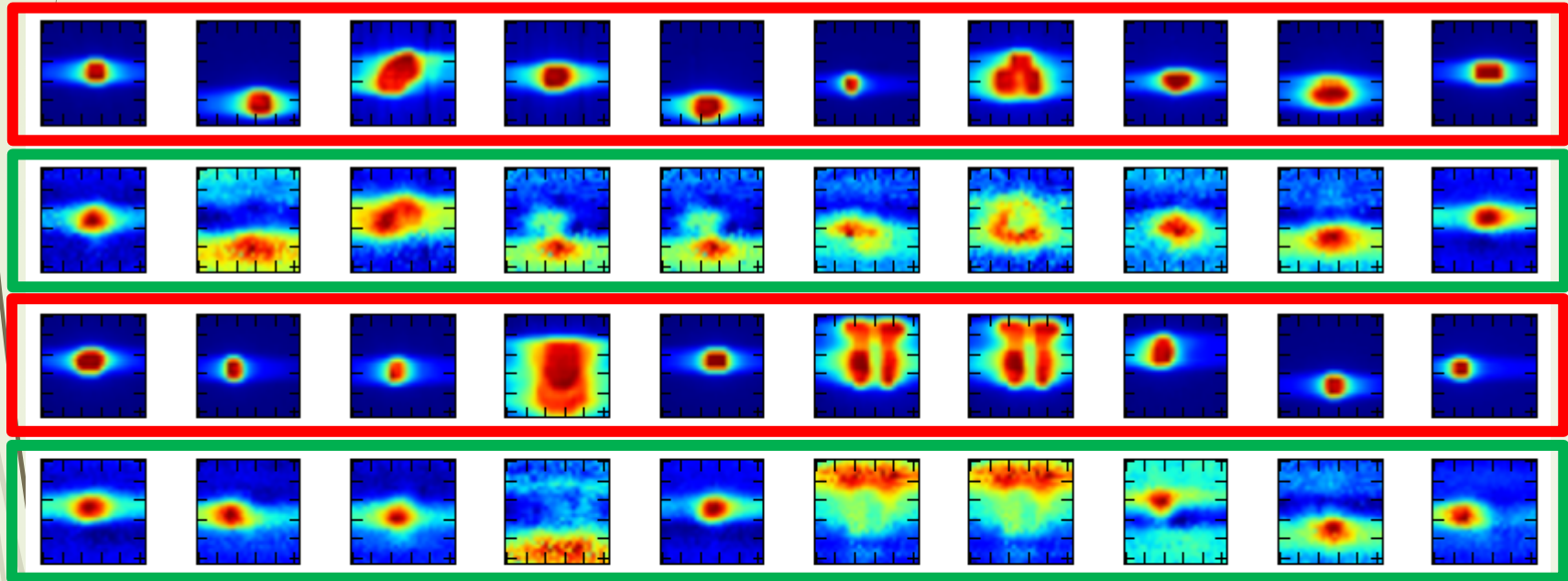
Raw Data

Dose profile



USE OF NNETS

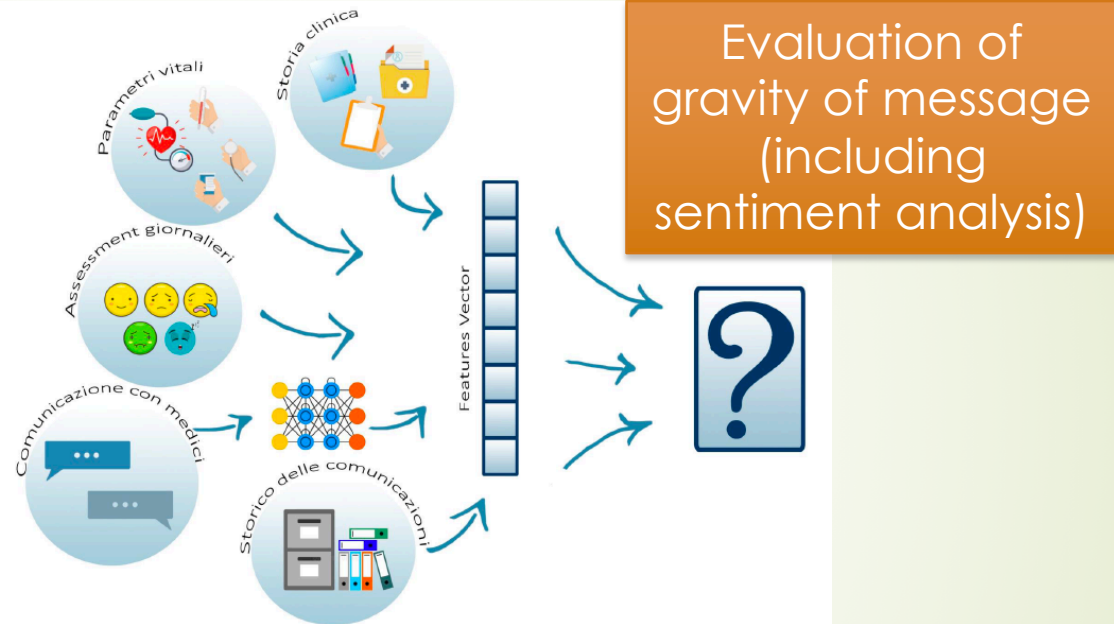
Virtual dose distribution



- In **red** measured images (sample of 729)
- In **green** images simulated with the developed neural network.

Machine learning for patient–doctor interactions

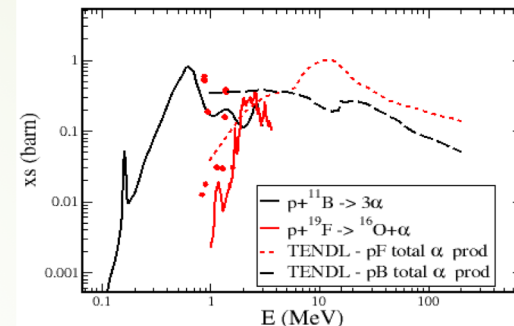
FILOBLU is an App to
deal with post-operation
follow-up @ home



- Machine Learning is required to
 - Automatic text analysis
 - Data Augmentation
 - Response classification



Titolo	Nuclear process-driven Enhancement of Proton Therapy UNravEled
Area di ricerca	multidisciplinare
Responsabile nazionale	G Cuttone (INFN-LNS)
Unità partecipanti	LNS, Napoli, Roma1, Roma3, LNL, Milano, Pavia, TIFPA



PROJECT GOAL

Evaluate impact of ^{19}F
and ^{11}B on particle
therapy

GOALS OF
WP2
(IMAGING)

RM1

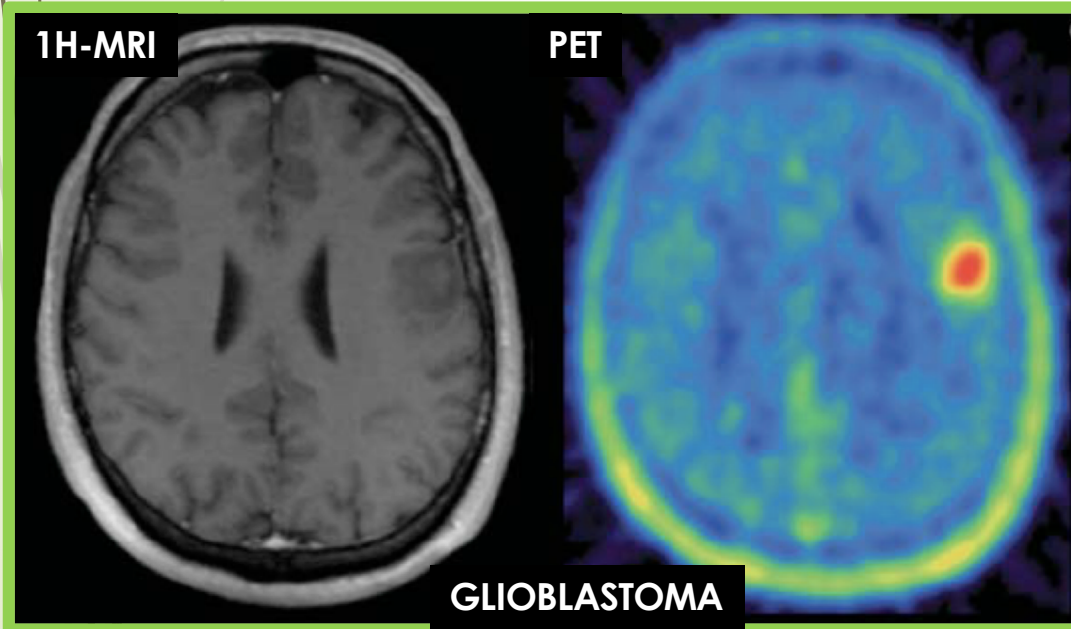
Evaluate bio-
distribution of
tracers

Evaluate
concentration of
samples

NA,P
V

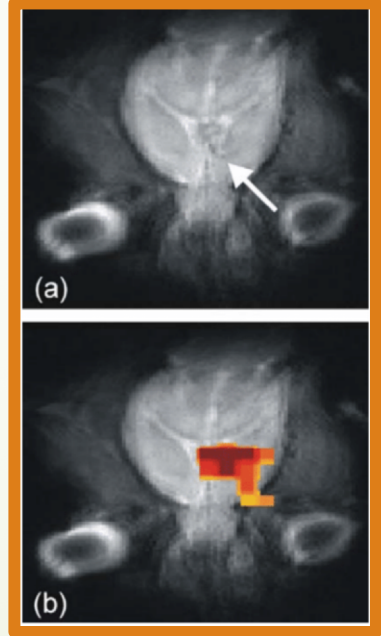
Available techniques: PET/MRI

PET has a worse resolution and tracers more difficult to synthesize/handle but ^1H -MRI does not show a signal ...



... but:

- gyromagnetic factor of ^{19}F is only 6% away from ^1H
- ^{19}F is not present in human body (no physical background)



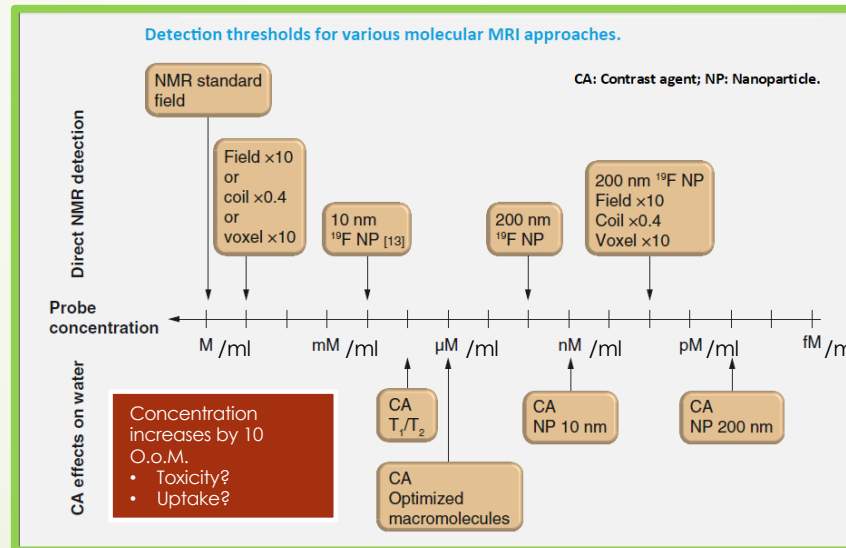
Concentrations and Performances

PET

- Typical PET activity concentrations:
 - Inject $\sim 200\text{MBq}$ FDG (i.e. $3 \cdot 10^{-12}$ moles), detect $\sim 10^{-16}$ moles/ml

Cell Lines: PANCREAS(PANC-1)
Tracers: BSH
phenylalanine

MRI



Concentrations required by Particle Therapy:

- 80 ppm
- 0.11 mg/ml
- 10 $\mu\text{M}/\text{ml}$

Evaluation of bio-distributions of tracers

THIS PROJECT

- A) Tests on animals to have samples with the correct concentration
- B) Setup a test stand to study and improve, with INFN competences, the signal/noise ratio



- C) Study co-registered ^{19}F and ^1H images to study the noise correlation and possible algorithms to enhance sensitivity to signal



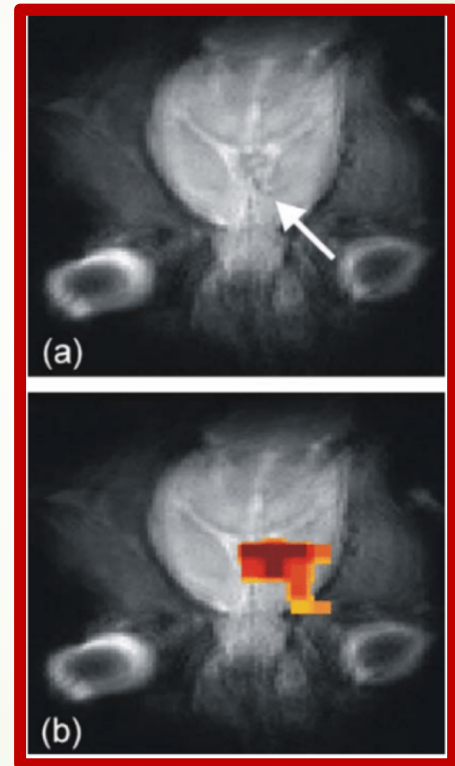
Study of co-registered 1H-19F analyses

Currently 1H and 19F images are only superimposed for visual comparison (combination is just product of signals)



Artificial Intelligence needed to:

- Align images
- Use autoencoders as de-noisers
- Segment 1H images
- Data augmentation



OUTLINE

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(Radio Guided Surgery)

DOSE PROFILER
(Particle Therapy dosimetry)

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ARTIFICIAL INTELLIGENCE IN MEDICINE

→ A. Retico

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(Imaging for stadiation)

NEPTUNE
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FILOBLU
(Patient-Doctor
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→ Carlo Mancini Terracciano
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