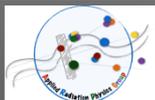




Radio-Guided-Surgery: status and perspectives

R. Faccini

University "La Sapienza" and INFN Rome
Incontro Nazionale Fisica Nucleare 16/11/2016



Chirone → Chir2



<http://arpg-serv.ing2.uniroma1.it/arpg-site/index.php>

Overview

- Radio-Guided Surgery(RGS): basic concepts
- γ probes – briefly
- β^+ probes
- Novel development: β^- RGS

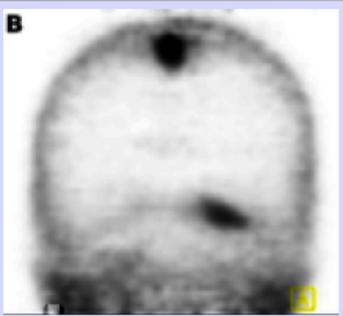


Radioguided surgery

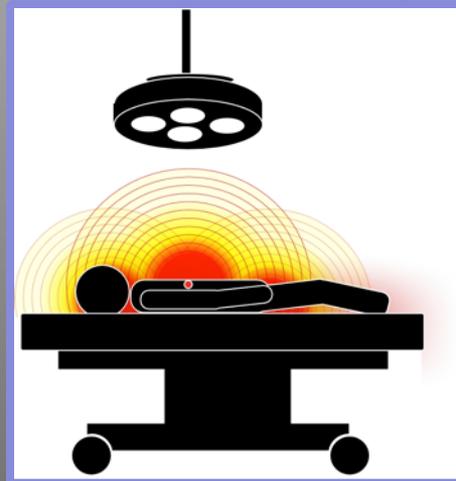
Radio Guided Surgery

PET/SPECT scan
to estimate
receptivity and
background

Each tumor requires its
own tracer



Administration
of radio-tracer



During surgery a probe
is used to detect
residuals/lymphnodes

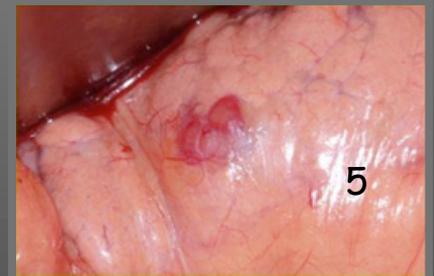
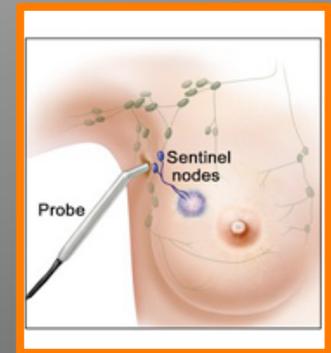
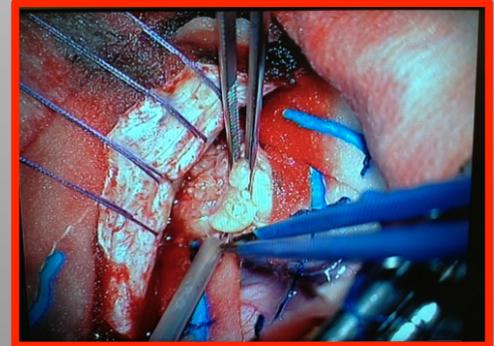


Probe adjustable
to needs



Intra-operative probes

- Needed when
 - Complete Tumor resection is mandatory
 - example: **brain**, pediatric tumors
 - Identification of **lymph-node** is needed
 - Example: breast tumor, melanoma
 - Tumor identification can reduce invasiveness
 - Example: parathyroid adenoma, insulinoma,...



Critical Aspects

1. Identification of clinical applications
2. Choice of the radio-nuclide
3. Identification of tracer and its match with the radio-nuclide
4. Probe design
5. Tests



Possible radio-nuclides

- Already tested nuclides include

| Radionuclide | Principali particelle emesse | $T_{1/2}$ | Radiofarmaci |
|-------------------|------------------------------|-----------|---|
| ^{99m}Tc | γ | 6.01 h | ^{99m}Tc -MDP ^{99m}Tc -MIBI |
| ^{18}F | β^+ | 110 min | ^{18}F -FDG |
| ^{111}In | γ | 67.4 h | ^{111}In -Octreotide |
| ^{86}Y | β^+ | 14.7 h | ^{86}Y -DOTATOC |
| ^{68}Ga | β^+ | 68 min | ^{68}Ga -DOTATOC |
| ^{90}Y | β^- | 64.1 h | ^{90}Y -DOTATOC |
| ^{177}Lu | β^- , γ | 6.73 d | ^{177}Lu -DOTATATE |
| ^{131}I | β^- , γ | 8.1 d | ^{131}I -MIBG |

SPECT

PET

Molecular RT

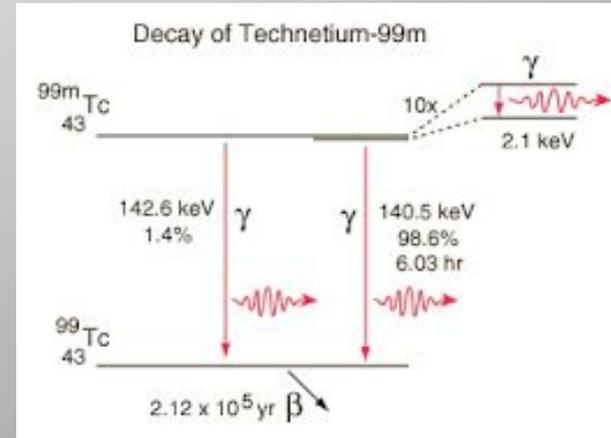


Radioguided surgery: γ probes

Existing: gamma probes

1. Choice of radio-nuclide: **gamma emitting, in particular ^{99m}Tc**

- well known detectors (camera or probes)
- used for SPECT: large number of known radio-tracers



2. Applications of interest:

- Search for tumor residuals (colon cancer, parathyroid adenoma, osteoid osteoma)
- Complete **sentinel-node mapping** (malignant melanoma and breast cancer)



Gamma probes applications

Local non-specific tracers

Systemic administration

| TARGET | TUMOR | UTILITY |
|---|--|---------|
| Sentinel lymph node by intra- or peritumoral administration of ^{99m} Tc-colloids | Breast cancer | ++ |
| | Melanoma | + |
| | Skin cancer | ++ |
| | Penile/vulvar cancer | ++ |
| | Colon cancer | ± |
| | Lung cancer | ± |
| | Head and neck cancer | ± |
| Tumor deposits by tumor-seeking agents (monoclonal antibodies, ^{99m} Tc-sestamibi) | Colon cancer | ± |
| | Ovarian cancer | - |
| | Breast cancer | - |
| | Medullary thyroid cancer | + |
| | Melanoma | - |
| | Neuroblastoma | ± |
| Bone abnormalities by ^{99m} Tc-diphosphonate | Parathyroid adenoma | ++ |
| | Osteoid osteoma | ++ |
| | Bone lesions suspected for bone metastasis | ++ |
| Occult tumors by intratumoral administration of an isotope tracer | Occult breast cancer | ++ |

Legend:

- ++ = proven clinical value
- + = may be of clinical value
- ± = clinical relevance insufficiently evaluated
- = proven not to be of clinical value

Mariani, Giuliano, Strauss 2004



LIMITS OF γ -RGS

140 keV photons
→ attenuation in body ~8cm

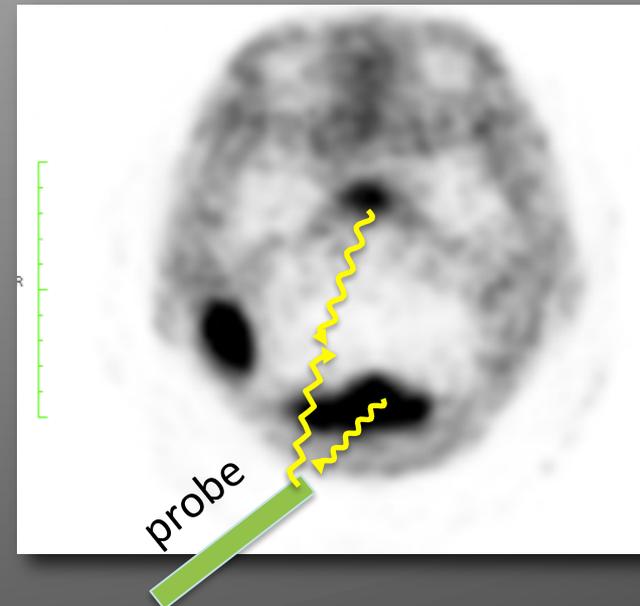
Long range of gamma's involve:

- exposure of medical personnel
- Background from healthy organs



Difficult to apply in:

- Brain tumors
- Abdominal tumors
- Pediatric tumors



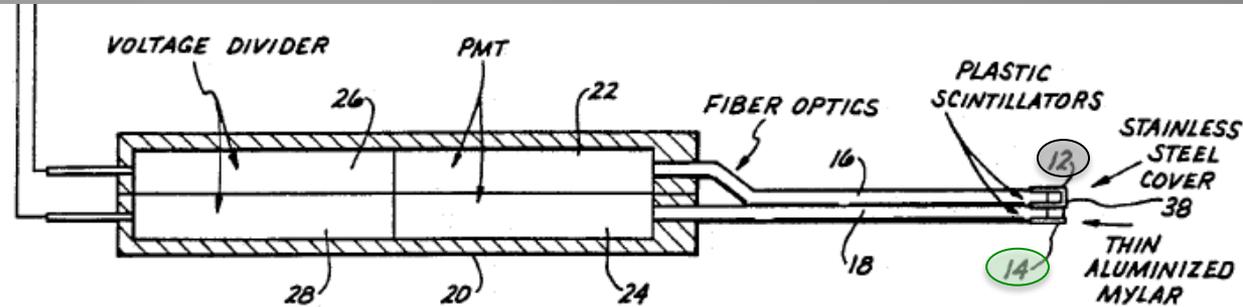
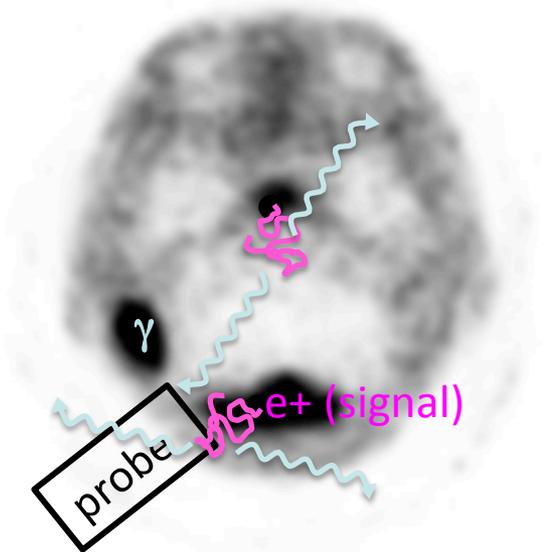
Radioguided surgery: β^+ probes

Daghighial et al 1994
Raylman et al 2001

β^+ RGS

- Use of β^+ decaying isotopes (same as PET) → detect positron (little penetration)
- Dual detectors for gamma background subtraction

WL: 2375 WW: 4751
From: 0% (0.00) to: 30% (4751.94)
K: 98 px Y: 127 px Value: 25.03
K: -80.81 mm Y: -0.46 mm Z: -153.40 mm



Two channels:

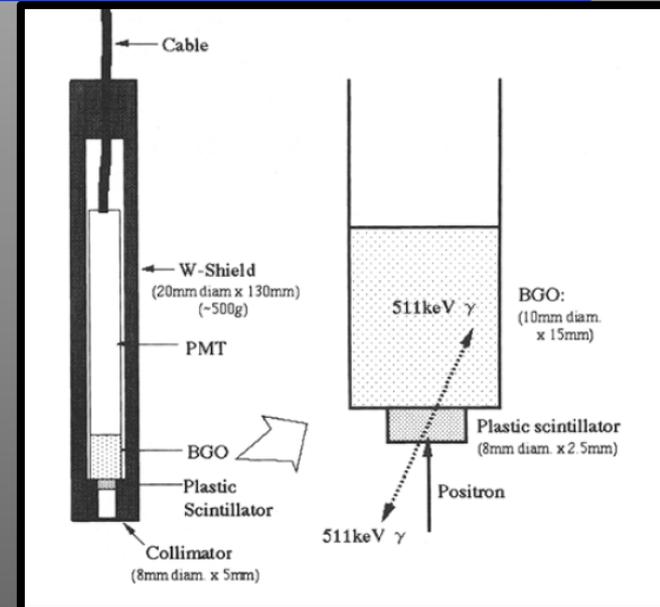
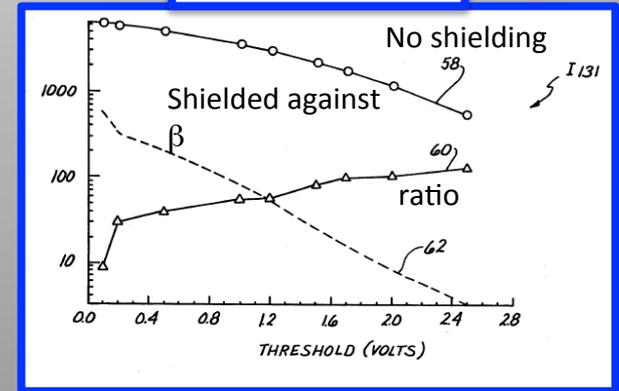
- one sensitive to both positrons and gamma (14) ($N1=P+G$)
- one sensitive only to gamma (12) ($N2=G$)

$$\text{signal} = N1 - N2$$

β^+ RGS: developments

- 1994 Daghighian: two different detectors for beta and γ
- 2001 Raylman: integrated dual-detector with semiconductor devices
- 2005 Yamamoto: plastic+BGO phoswitch

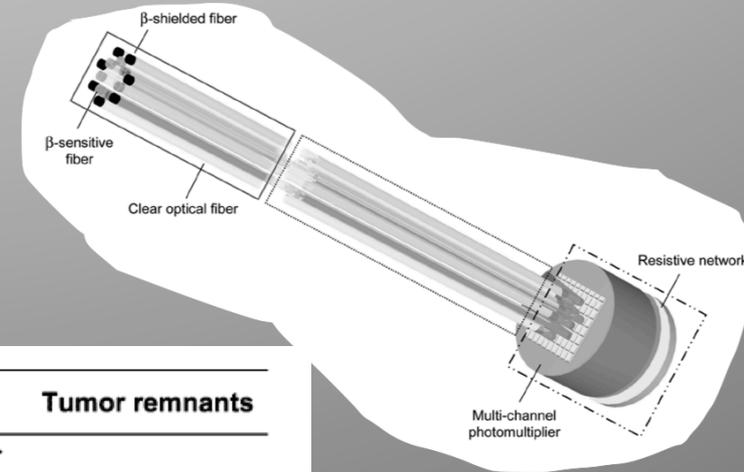
Tests with point-like source



β^+ RGS: clinical applications

Brain tumors: difficult use of pre-operative information

- 2007 Bonzom et al :
 - attach it to the surgical device
 - Different tracers considered to carry ^{18}F



| Activity ($\mu\text{Ci/ml}$) | Normal tissues | | Tumor remnants |
|-----------------------------------|----------------|-------------|----------------|
| | White matter | Gray matter | |
| FDG | 0.32 | 0.57 | 0.59 |
| FET | 0.075 | 0.104 | 0.29 |
| Choline | 0.019 | 0.017 | 0.170 |

- 2009 Bogalhas et al:
 - Test on phantom

Conclusions

This phantom also demonstrated the ability of the probe to detect tumour discs as small as 5 mm in diameter (20 mg) for tumour-to-background ratios higher than 3:1 and with an acquisition time around 4 s at each scanning step. These results indicate that our detector could be a useful complement to existing techniques for the accurate excision of brain tumour tissue and more generally to improve the efficiency of radio-guided cancer surgery.



β^+ RGS

- Use of β^+ tracers(positrons): pros
 - Detect positron that travels ~ 100 times less
 - PET tracers can be used
- Use of β^+ tracers: cons
 - Large irradiation of medical personnel ($\sim 20 \mu\text{Sv/hr}$)
 - Positrons annihilate and produce photons \rightarrow background \rightarrow need to subtract background
 - » Longer time to have a response
 - » More encumbrant detector

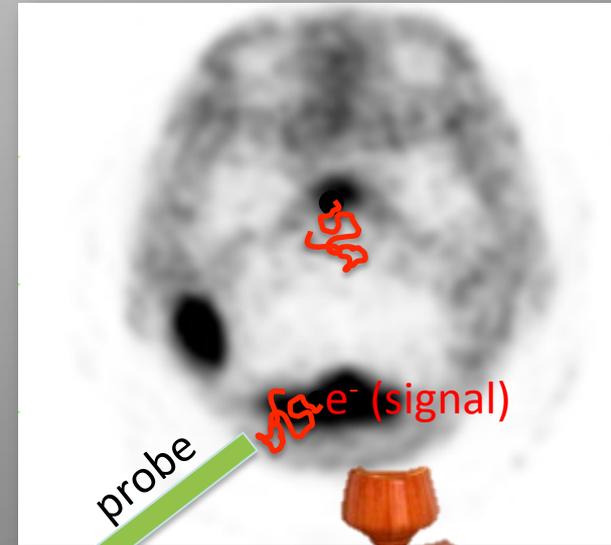


Radioguided surgery: β^- probes

A CHANGE IN PARADIGM

- Use of β^- tracers (electrons): pros
 - Detect electrons that travel ~ 100 times less than γ
 - Tracers with ^{90}Y can be used (already used for Molecular RT)
 - No background from gamma
 - Shorter time to have a response
 - » Smaller administered activity
 - Smaller and more versatile detector
 - Very reduced effect of nearby healthy tissues
 - Reduced dose to medical staff

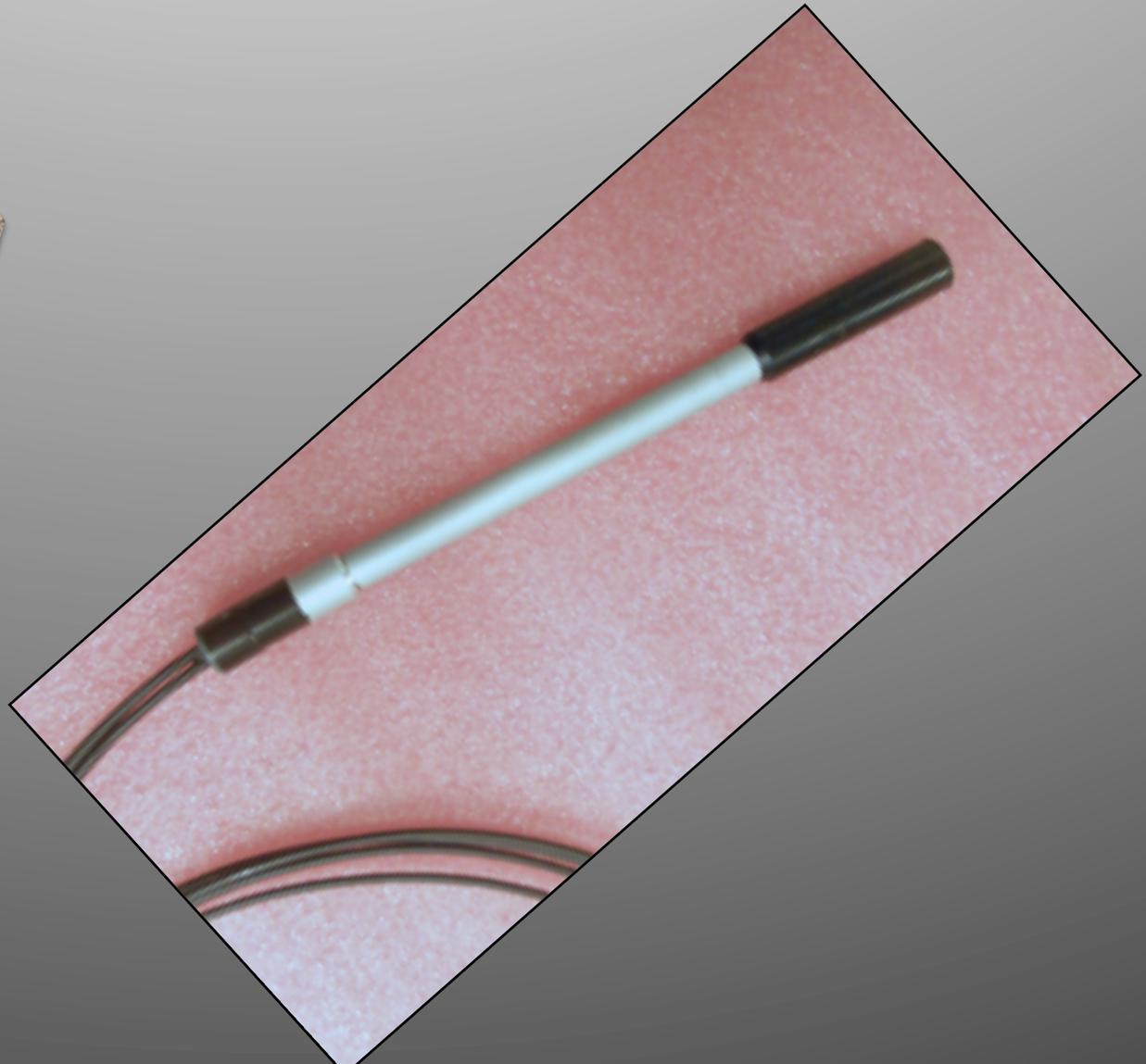
E. Solfaroli Camillocci et al, Sci. Repts. 4,4401 (2014)



EXTEND RGS TO MORE
CLINICAL CASES

RESEARCH PATH

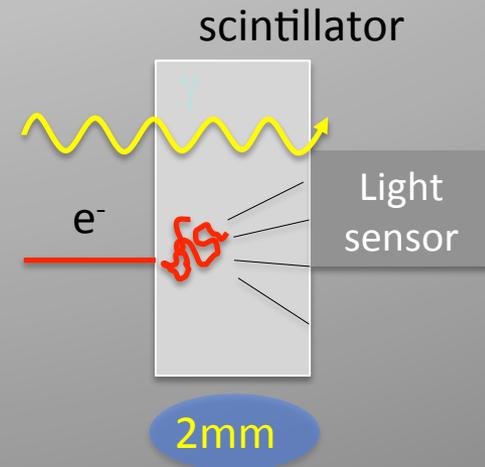
Probe
Prototypes



Low energy e- detector

p-terphenyl as scintillator

- High signal:
 - $LY(\text{pterf})=3LY(\text{Anthracene})$
- Low Z
 - Low sensitivity to photons
- Small attenuation length
 - $\lambda=(4.73 \pm 0.06) \text{ mm}$



Usually unused because signal attenuates if detector too thick

→ **Not for low energy electrons**

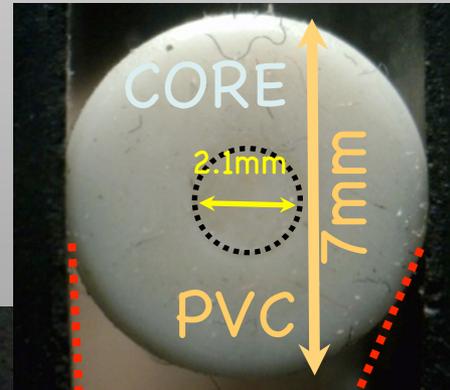
Note: also in case of pure β - emitters gamma rejection is important because of brehmsstrahlung

R. Faccini et al, **Properties of P-Terphenyl as detector for α , β , and γ radiation**, IEEE Trans. on Nucl. Sci. 2014; 61: 1483-7

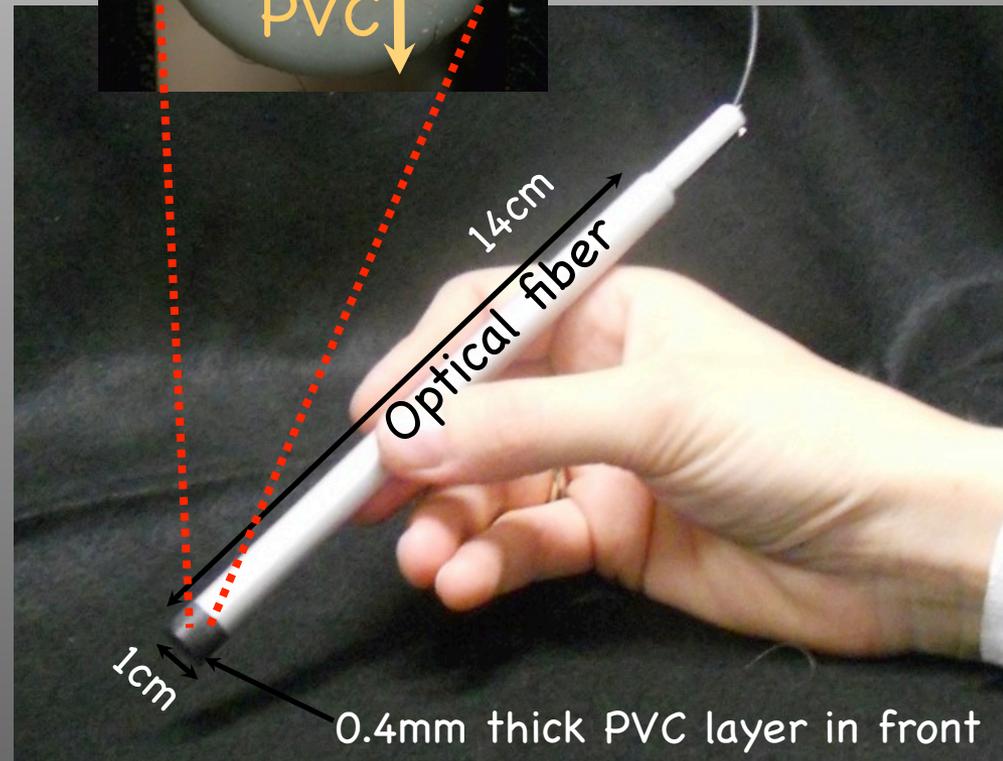


Prototypes

- **Core:** cylindrical scintillator of p-terphenyl $d=2.1\text{mm}$, $h=1.7\text{mm}$
- encapsulated into a **PVC ring** to shield it against radiation coming from the sides;
- inserted as a tip inside an easy **handling aluminum body**.
- A thin **black PVC cap** makes the enclosure light tight.
- Two options for light collection:
 - Scintillating fiber and PMT
 - SiPM (SensL B/C-series)



PMT



Constraints on medical devices apply

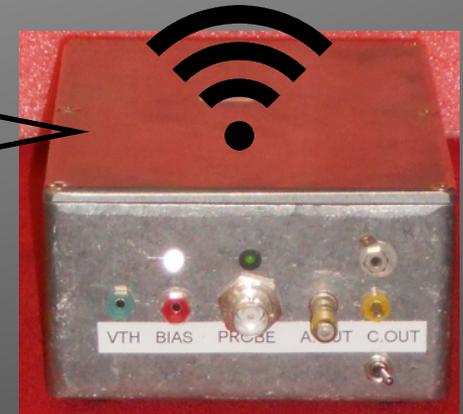
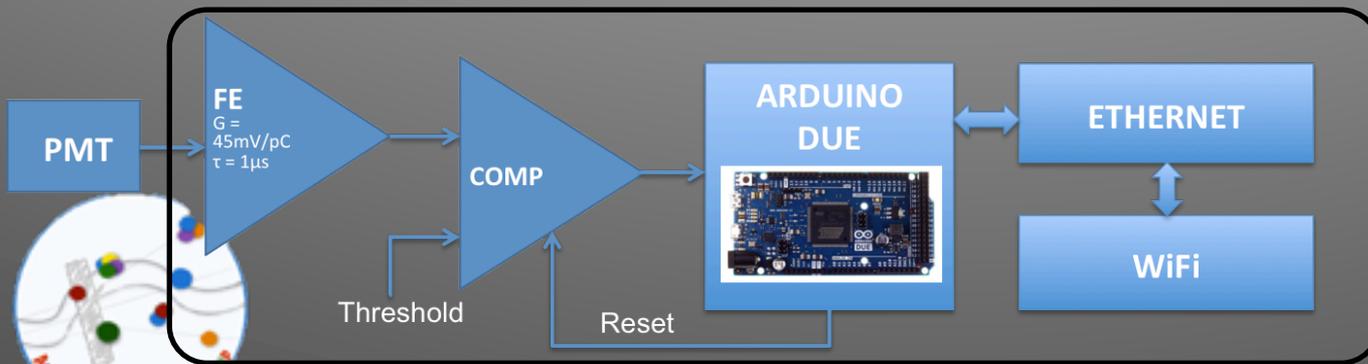
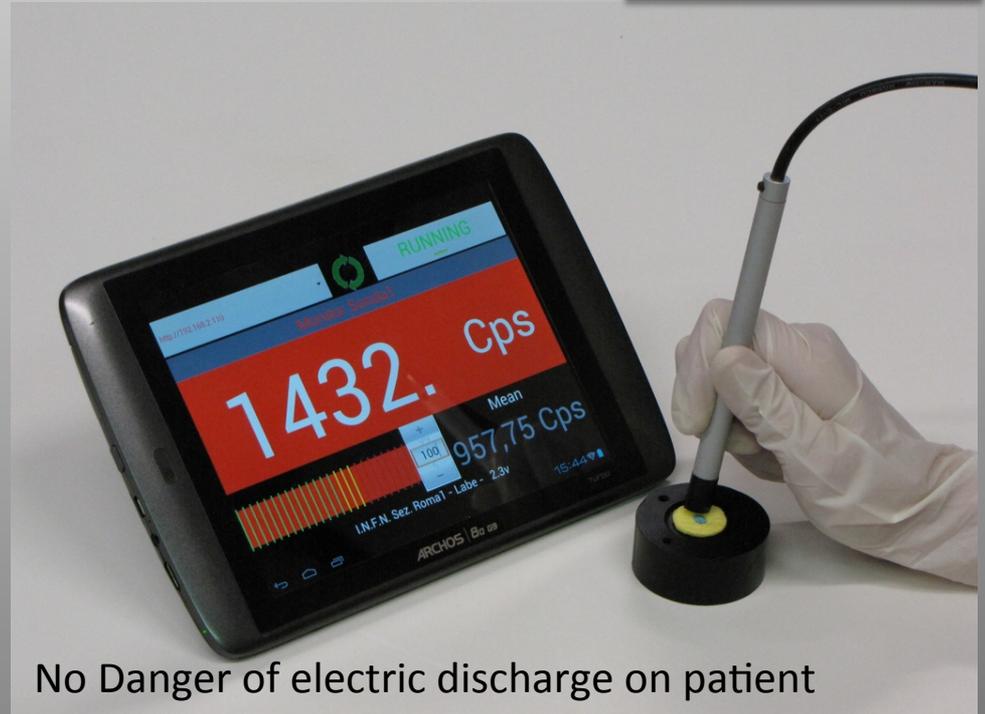


Electronics Read-out

ARDUSiPM
LABE-INFN RM1

Electronics read-out is portable and customized to match the surgeon needs

- acoustic and visual alarm;
- wireless data transfer;
- no connection with electrical line (batteries)
- user interface available both for PC or tablet.



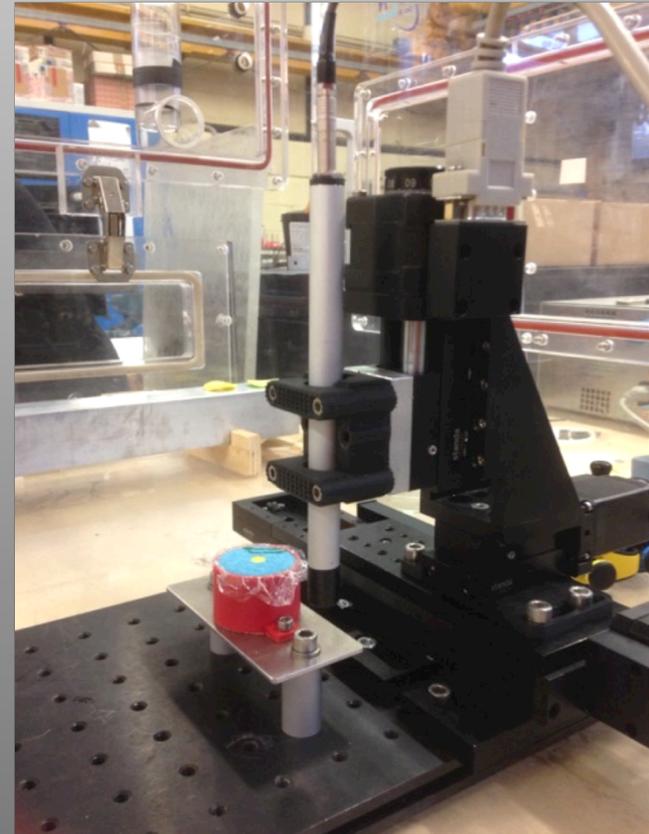
RESEARCH PATH

E. Solfaroli Camillocci et al, *J. Phys.:*
Conf. Ser. **620** 012009(2015)

Probe
Prototypes

Lab tests (phantom
factory)

- Measure spatial sensitivity
- Gamma rejection
- Estimate performances on phantoms
- Estimate dose on surgeon



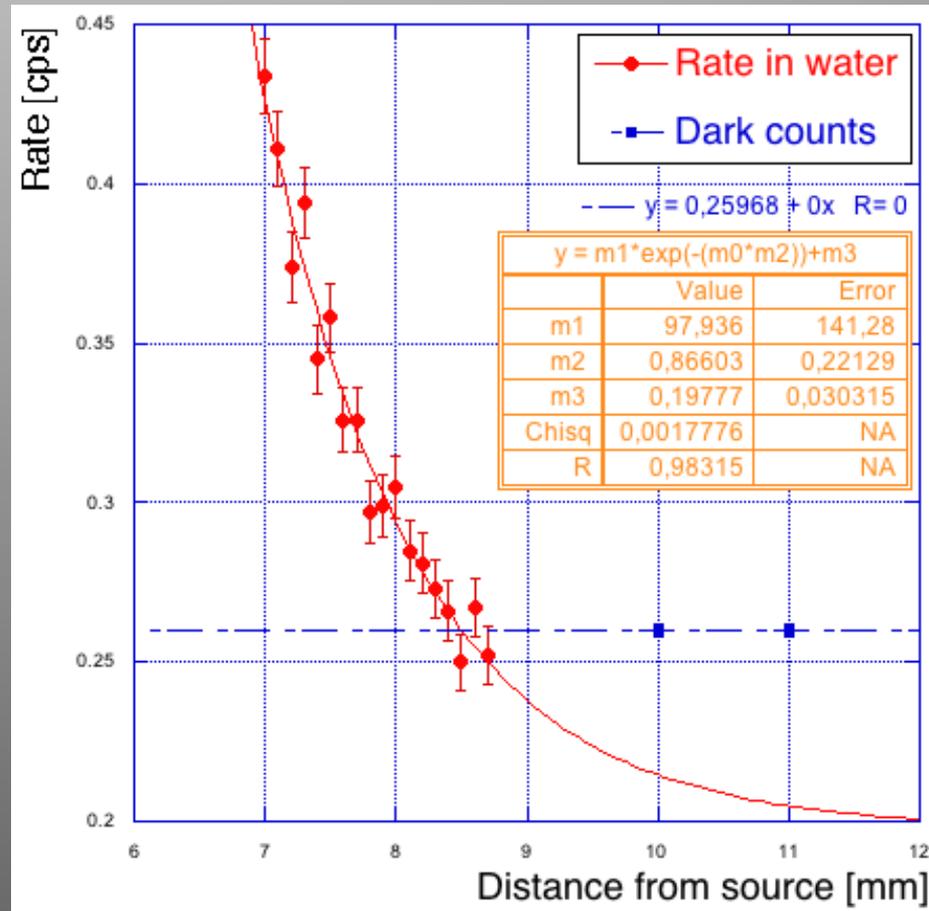
Estimated dose on surgeon administering 3MBq/kg:
 $1\mu\text{Sv/hr}$ on surgeon's hands
 $0.13\mu\text{Sv/hr}$ on medical personnel



Sensitivity to Electrons

Scan with different thicknesses of water

- Detection efficiency on ^{90}Sr point source
 - Rate $3.8 \cdot 10^5$ cps/MBq.
 - $\varepsilon_{\beta} = 40\%$
- Scan in water
 - $E_{\beta} > 500\text{keV}$.
 - Detection efficiency $\varepsilon_{\beta} > 80\%$ in the β^{-} ^{90}Y energy range.



Background Rejection

Background is mainly due to photons coming from Bremsstrahlung.

Sensitivity to photons

Bremsstrahlung E_γ spectrum

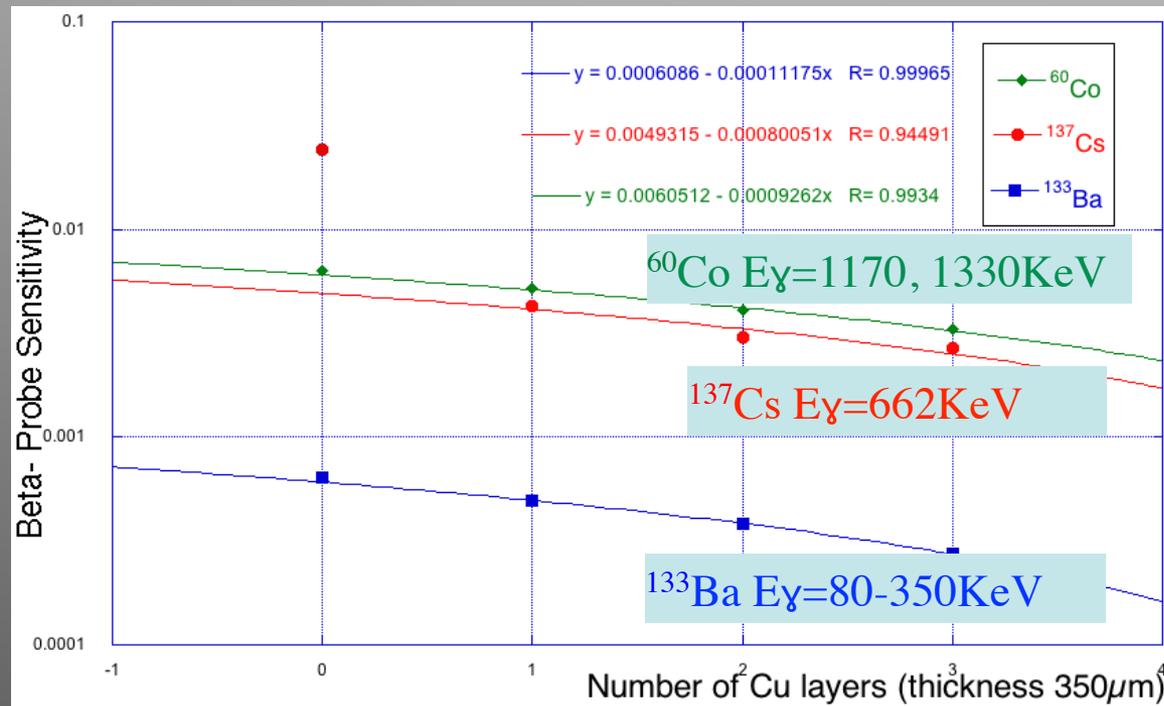
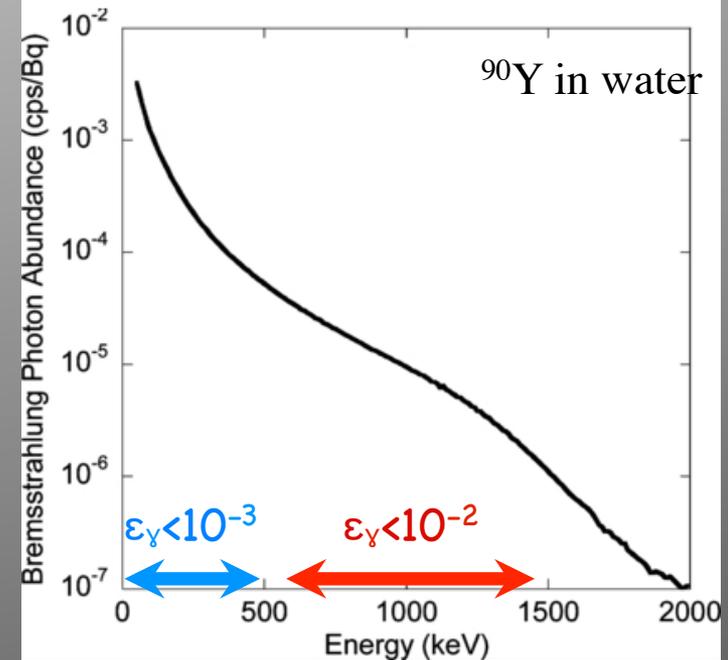


Figure 1 from Xing Rong et al 2012 Phys. Med. Biol. 57 3711



Almost transparent to Bremsstrahlung photons.

“Ad-hoc” Phantoms

To simulate tumor remnant embedded in healthy tissue.

Tumor residual
 $V=0.05\text{ml}$

embedded in
tissue with $A/10$

Motorized scans with S4-Probe

 The image cannot be displayed. Your computer may not have enough memory to open the image, or the image may have been corrupted. Restart your computer, and then open the file again. If the red x still appears, you may have to delete the image and then insert it again.

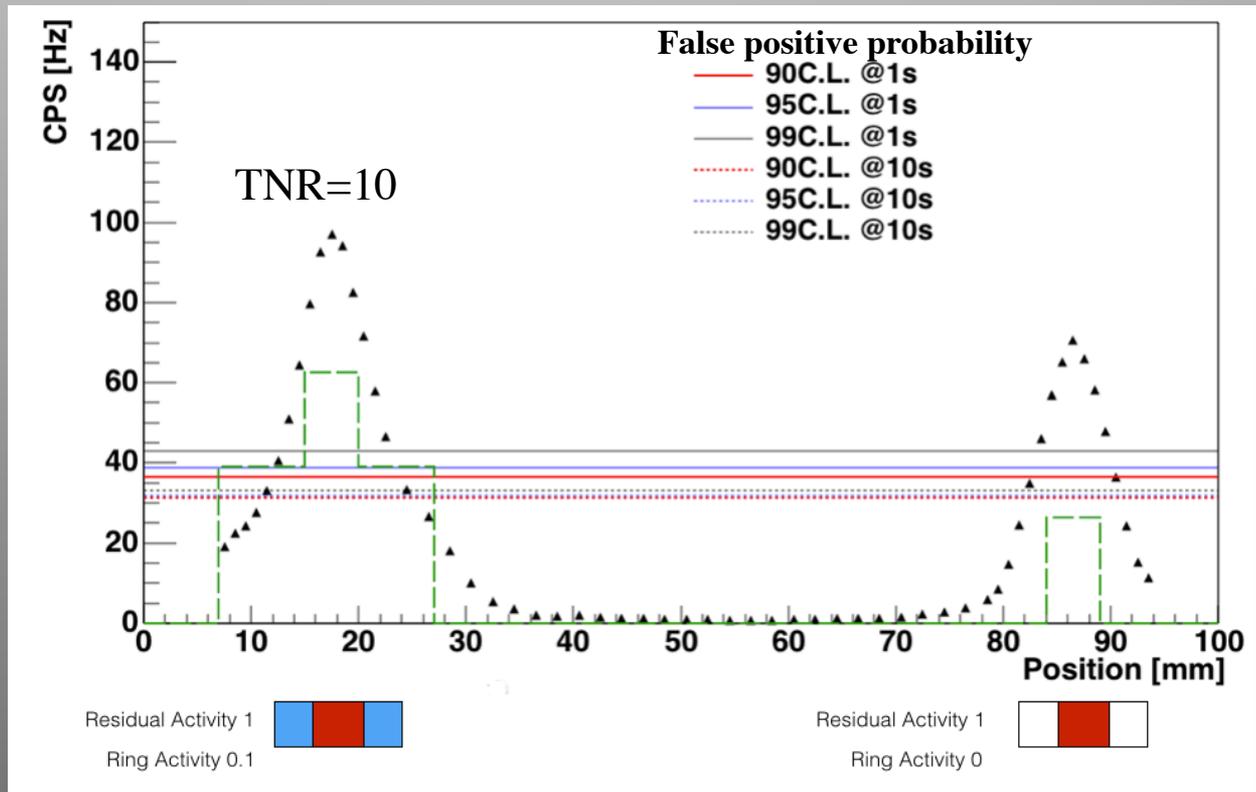
 The image cannot be displayed. Your computer may not have enough memory to open the image, or the image may have been corrupted. Restart your computer, and then open the file again. If the red x still appears, you may have to delete the image and then insert it again.



All the possible
configurations of
tumor residual
embedded in healthy
tissue.



Active Spot Identification



Human Factor

To include the human factor in the test colleagues were asked to simulate the surgeon:



Phantoms simulating tumor remnants embedded in healthy tissue with different TNRs

All “surgeons” required at least 4-5 seconds per position to take a decision.



RESEARCH PATH

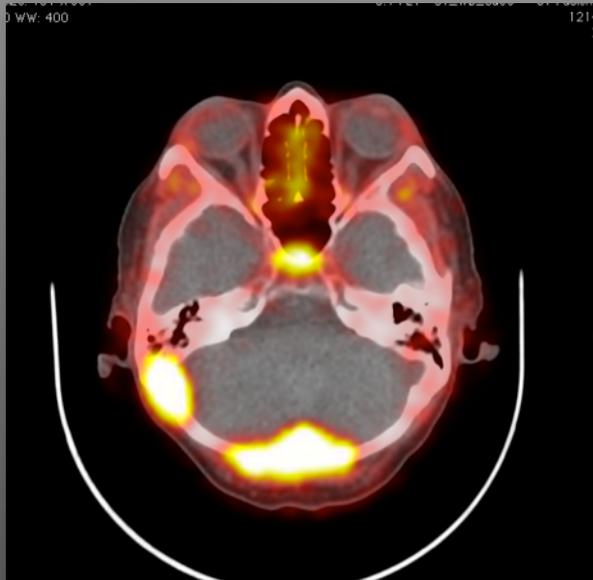
Probe
Prototypes

Lab tests
(phantoms)

Identification of proof of
principle

Start with existing radiotracers:
Somatostatine analogues marked ^{90}Y

Meningioma is avid of ^{90}Y -DOTATOC
→ Able to detect 0.1 ml residuals
administering only 1MBq/kg



RESEARCH PATH

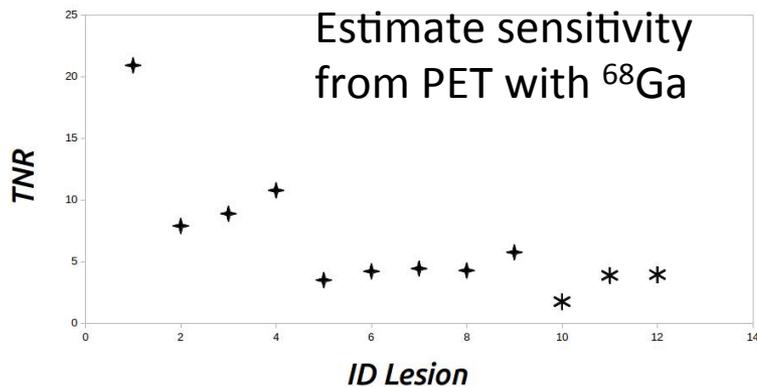
Probe
Prototypes

Lab tests
(phantoms)

Start with existing radiotracers:
Somatostatine analogues marked ^{90}Y

Identification of proof of
principle

Identification of first
clinical cases



First clinical cases:

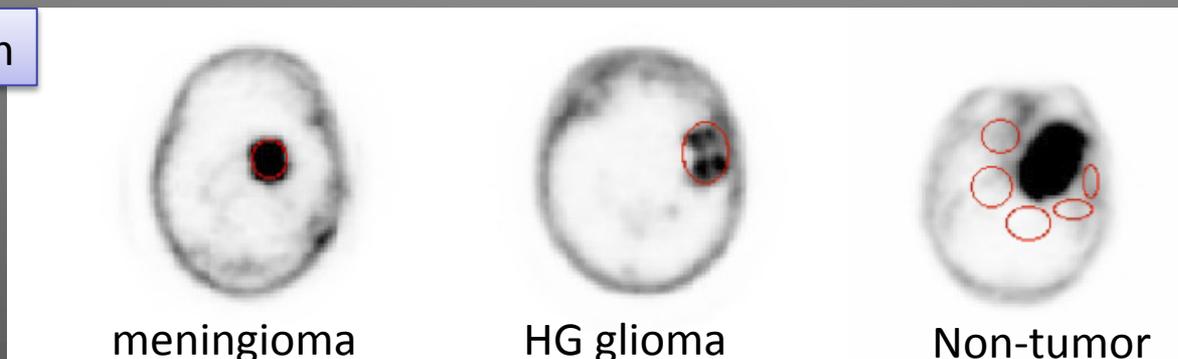
- Glioma (low and high grade)
- GEP-NET (start from small bowel)



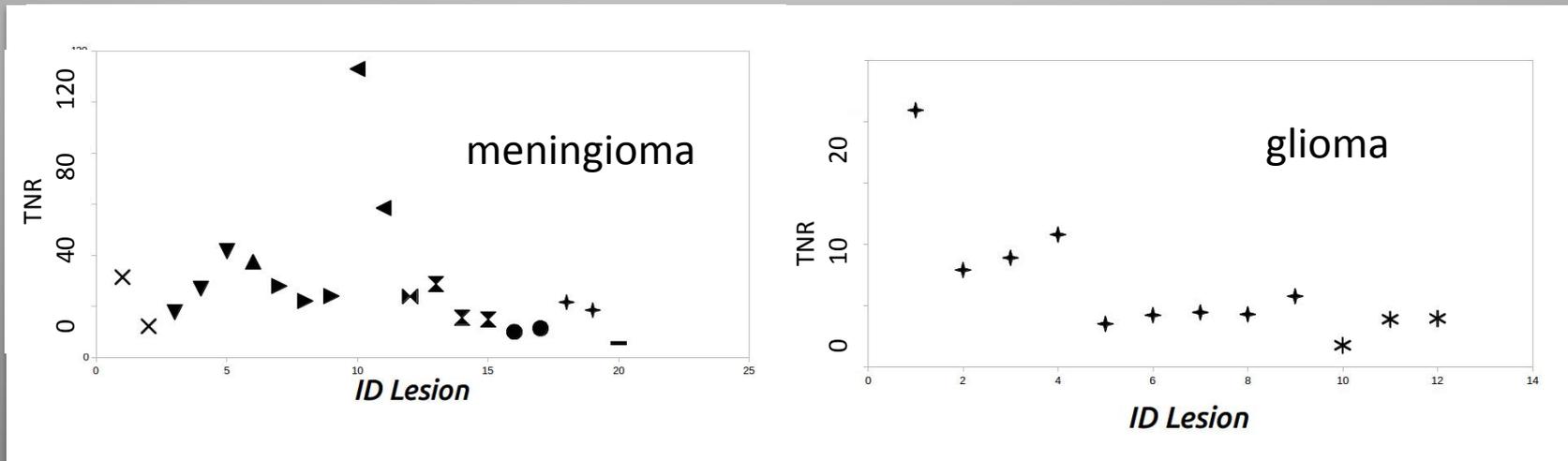
DOTATOC uptake in glioma

- DOTATOC is a somatostatin analog → known receptivity from NET .. but glioma?
- Even if TNR too low for therapy, can it be used for RGS?
- Use ^{68}Ga -DOTATOC PET scans to estimate signal and background

ROI definition



Glioma vs Meningioma



Meningioma has a definitely larger uptake, but is the glioma one acceptable?

Use FLUKA simulation to translate from activities to false positive (FP) and false negative (FN) rates

Consider a residual identified if $FP < 1\%$ and $FN < 5\%$



TNR of glioma is acceptable if probe can take $> \sim 6s$ to give answer



RGS for meningioma

| Patient ID | $N_{les.}$ | W (kg) | A_{adm} (MBq) | v (Hz) | v_{NT} (Hz) | t_{prob}^{min} * | A_{1s}^{min} ** (MBq/kg) | Diagnosis | Previous Treatment |
|------------|------------|--------|-----------------|----------|---------------|--------------------|----------------------------|-----------------|--------------------|
| M01 | 1 | 63 | 220 | 32.2 | 1.9 | 0.2 | 0.7 | atypical | S |
| M02 | 1 | 80 | 160 | 17.6 | 2.6 | 0.6 | 1.9 | atypical | S/RT/PRRT |
| M03 | 3 | 95 | 305 | 33.7 | 3.5 | 0.3 | 0.9 | likely atypical | S/RT |
| | | | | 50.3 | 3.5 | 0.3 | 0.5 | | |
| | | | | 76.8 | 3.5 | 0.1 | 0.3 | | |
| M04 | 1 | 48 | 200 | 89.4 | 4.5 | 0.1 | 0.2 | atypical | S/RT/CT |
| M05 | 3 | 57 | 130 | 66.7 | 4.4 | 0.2 | 0.3 | relapse | S/RT/CT/PRRT |
| | | | | 53.2 | 4.4 | 0.2 | 0.5 | | |
| | | | | 57.6 | 4.4 | 0.2 | 0.4 | | |
| M06 | 2 | 90 | 145 | 107.6 | 1.8 | 0.1 | 0.1 | unknown | PRRT |
| | | | | 56.1 | 1.8 | 0.2 | 0.4 | | |
| M07 | 1 | 74 | 237 | 50.2 | 3.9 | 0.2 | 0.5 | anaplastic | S/RT |
| M08 | 3 | 105 | 223 | 55.7 | 3.6 | 0.2 | 0.5 | atypical | S/RT |
| | | | | 31.2 | 3.6 | 0.2 | 0.9 | | |
| | | | | 29.6 | 3.6 | 0.4 | 0.9 | | |
| M09 | 2 | 48 | 145 | 13.4 | 2.4 | 0.9 | 2.7 | atypical | S/RT |
| | | | | 15.1 | 2.4 | 0.7 | 2.5 | | |
| M10 | 1 | 70 | 240 | 14.6 | 1.2 | 0.6 | 1.8 | atypical | S/RT |
| | | | | 12.6 | 1.2 | 0.8 | 1.9 | | |
| M11 | 1 | 75 | 220 | 12.7 | 3.8 | 1.6 | 5.0 | atypical | unknown |

- Very large uptake
- Can inject as low as 0.5 MBq/kg



* Time needed to detect 0.1 ml residual if 3MBq/kg are administered

** Activity that needs to be administered to achieve 1s response time

RGS for glioma

| Patient ID | W (kg) | A_{adm} (MBq) | v (Hz) | v_{NT} (Hz) | t_{probe}^{min} * (s) | A_{1s}^{min} ** (MBq/kg) | Diagnosis | Previous Treatment |
|------------|--------|-----------------|----------|---------------|-------------------------|----------------------------|-------------------|--------------------|
| G01 | 97 | 246 | 16.5 | 1.4 | 0.5 | 1.5 | HGG | S/RT/CT/PRRT |
| G02 | 68 | 223 | 5.2 | 1.1 | 2.6 | 8.5 | HGG | RT/CT/B |
| G03 | 80 | 152 | 9.6 | 1.9 | 1.4 | 4.3 | HGG | S/RT/CT |
| G04 | 93 | 198 | 22.4 | 3.7 | 0.6 | 1.8 | HGG | S/RT/CT/PRRT |
| G05 | 90 | 192 | 4.6 | 2.0 | 7.4 | 23.6 | HGG | S/RT/CT/PRRT |
| G06 | 60 | 185 | 4.4 | 1.6 | 5.8 | 20.0 | HGG | S/RT/CT |
| G07 | 63 | 194 | 4.8 | 1.7 | 5.1 | 17.6 | HGG | S/RT/CT |
| G08 | 70 | 266 | 2.1 | 0.8 | - | 40.0 | HGG | RT/CT |
| G09 | 85 | 255 | 3.7 | 1.1 | 5.3 | 17.6 | HGG | S/RT/CT |
| G10 | 80 | 224 | 2.2 | 1.6 | - | - | oligodendroglioma | S/RT/CT/I |
| G11 | 70 | 234 | 5.1 | 2.0 | 5.5 | 18.8 | HGG | RT/CT |
| G12 | 15 | 38 | 5.0 | 2.0 | 5.9 | 18.8 | pontine glioma | RT/CT/PRRT |

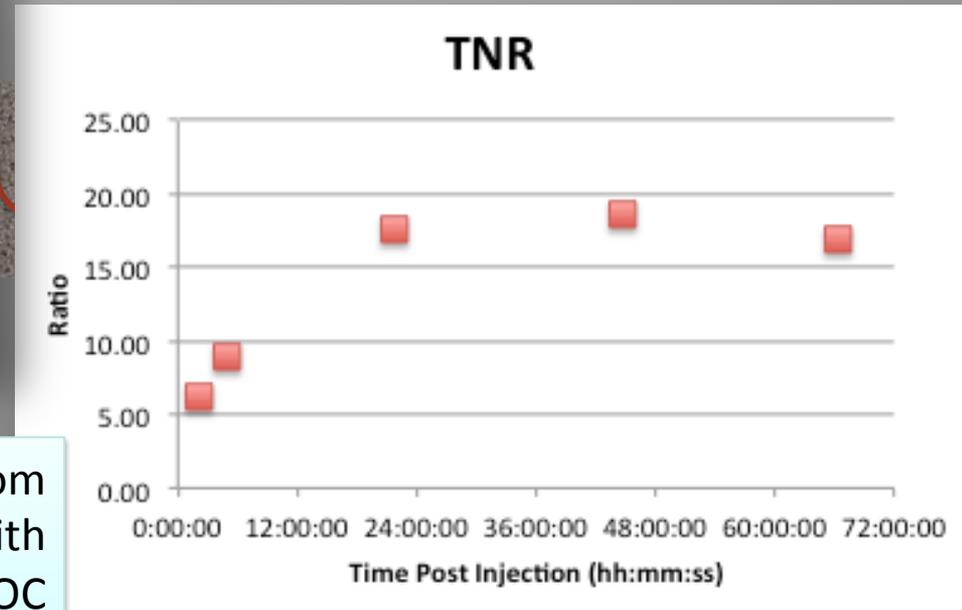
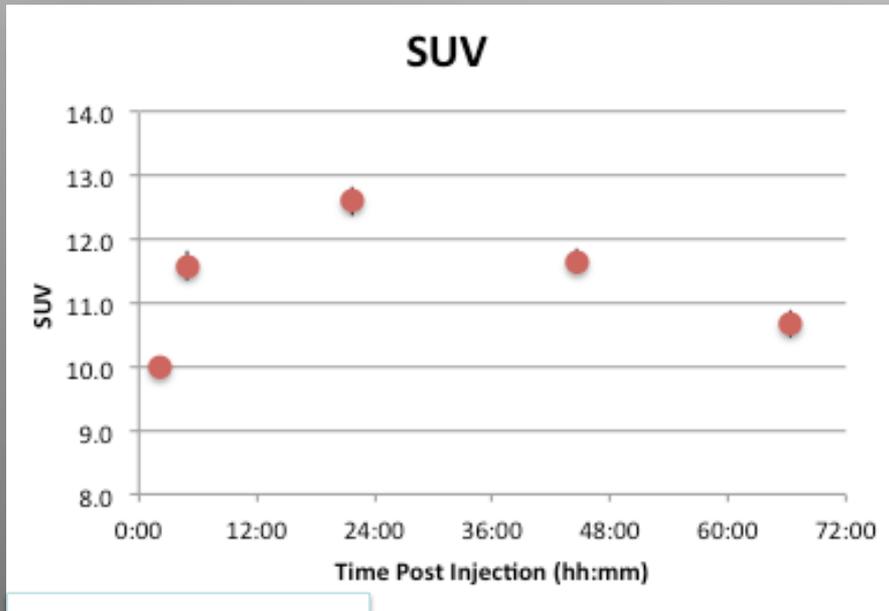
- Needs to wait for $\sim 6s$, but it works
- Margins to improve probe



* Time needed to detect 0.1 ml residual if 3MBq/kg are administered

** Activity that needs to be administered to achieve 1s response time

Time Evolution of uptake



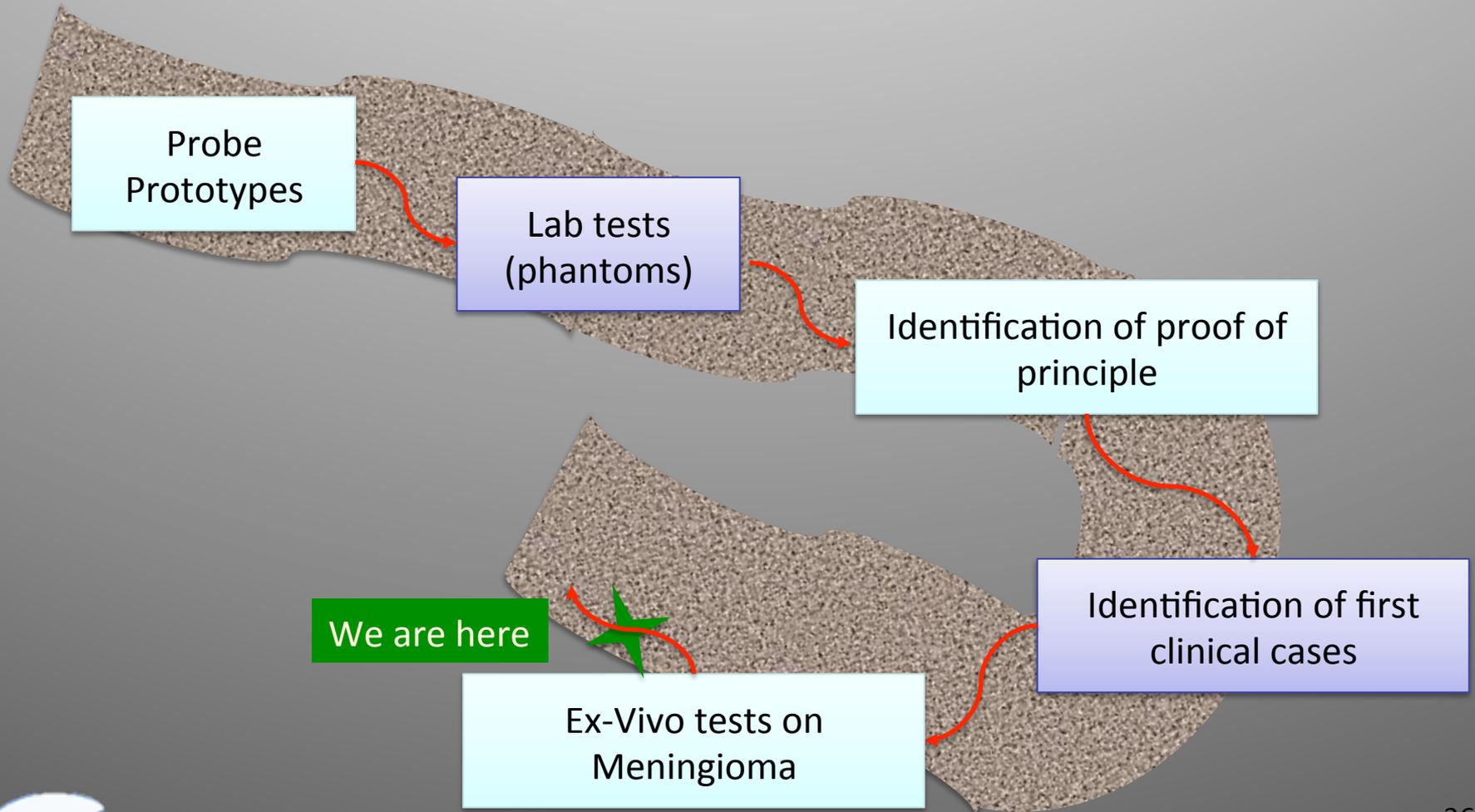
TNR for **liver**
NET vs time

Values estimated from
dosimetric SPECTs with
 ^{177}Lu -DOTATOC

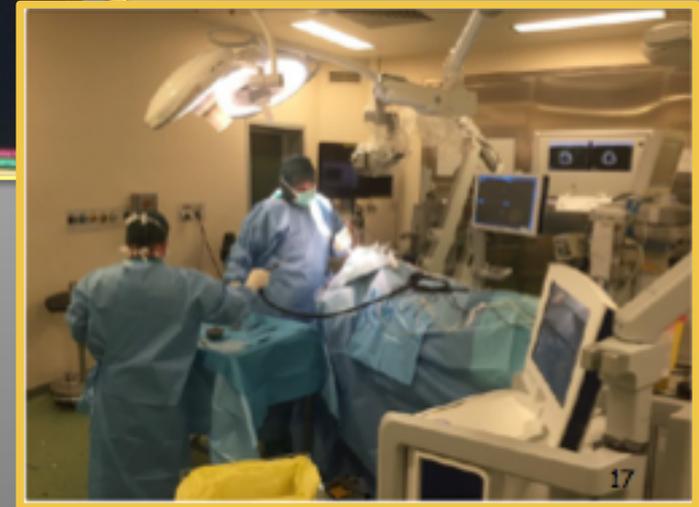
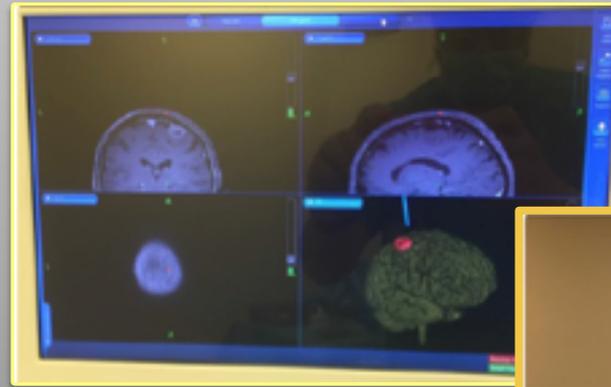
CONCLUSIONS:

- GEP-NETs (small bowel, insulinoma, ...) are a good candidate and similar among each other
- the best SUV and TNR are achieved if surgery is 24hrs after injection

RESEARCH PATH



Ex-vivo test on meningioma



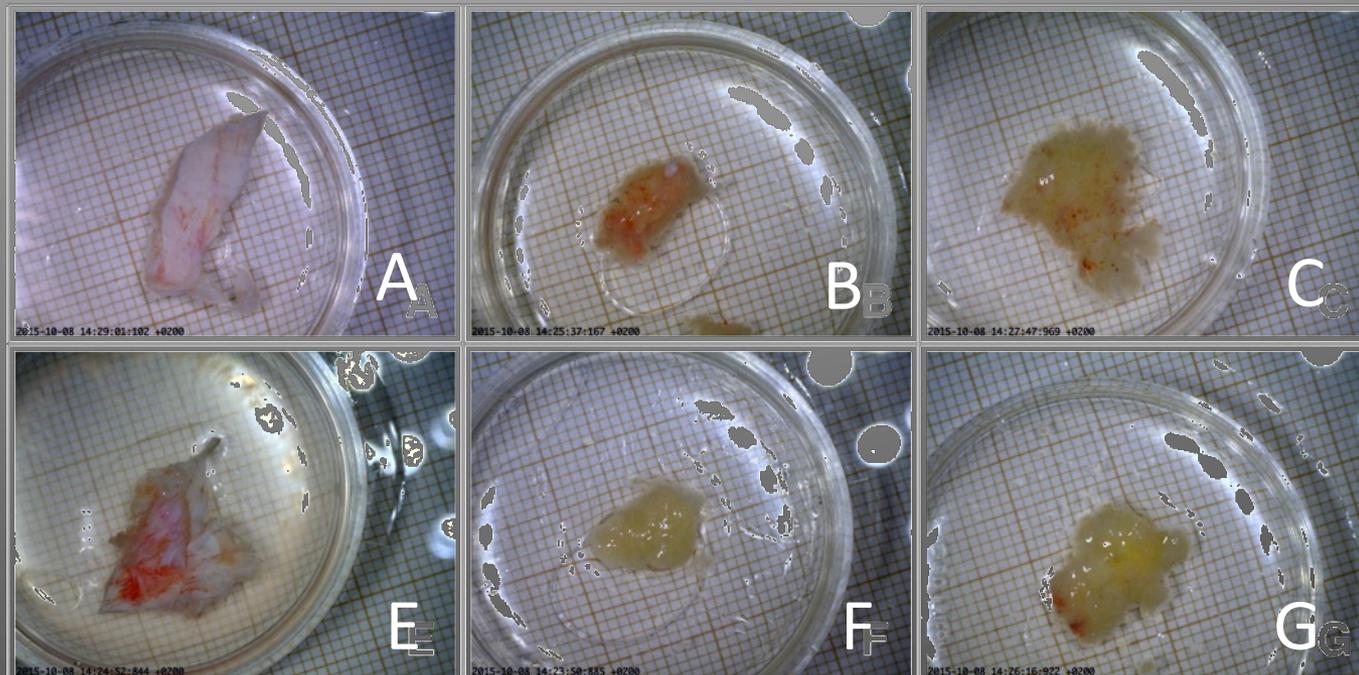
- PET with Ga68 on Sep 14th
 - Tumor SUV \sim 2g/ml (relatively low, but enough)
 - TNR \sim 14 (good)

- 8mCi Y90—DOTATOC on Oct 9th
- Surgery on Oct 10th

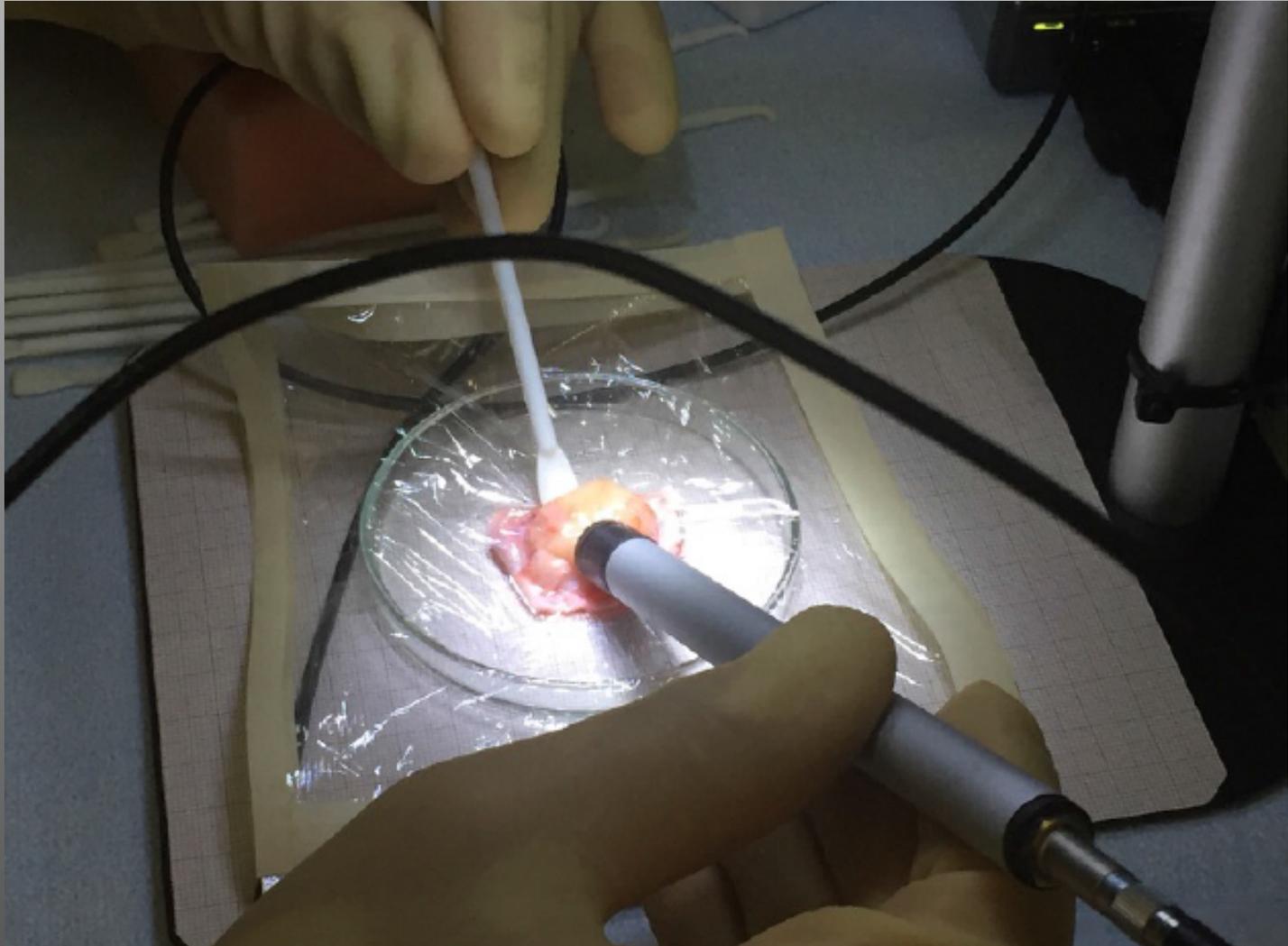


| Sample | "Diagnosis" |
|--------|----------------------|
| A | non-infiletered dura |
| B | Tumor upper margin |
| C | Tumor lower margin |
| D | Tumor Bulk |
| E | Medial dural border |
| F | Tumor center |
| G | Tumor center |

The Samples



Evaluating the samples rate

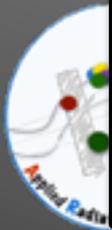


Results

- Residuals as small as 0.2ml are visible
- Predictions with simulation are reliable (115 cps predicted, 105 observed)
- Healthy brain ~ 1 cps (simulation)
infiltrated dure can be identified

+ Confirmed very low exposure of medical personell

| Sample | V(ml) | R(cps) | histology |
|--------|-------|--------|--|
| A | 0.38 | 5.0 | Dural tissue infiltrated by meningioma |
| B | 0.23 | 51.5 | Transitional meningioma |
| C | 0.72 | 45.0 | Transitional meningioma |
| D | 4.84 | 105.0 | Transitional meningioma |
| E | 0.88 | 3.5 | Dural tissue infiltrated by meningioma |
| F | 0.21 | 27.7 | Transitional meningioma |
| G | 0.39 | 39.3 | Transitional meningioma with micronecrosis and occasional mitosis |

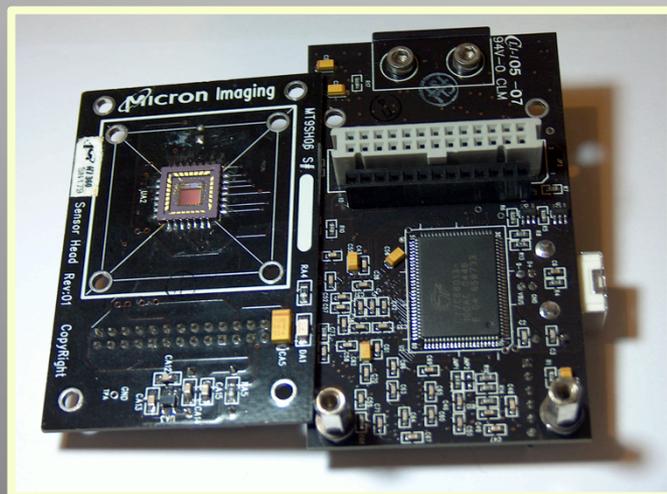


IRRADIATION MEASUREMENTS



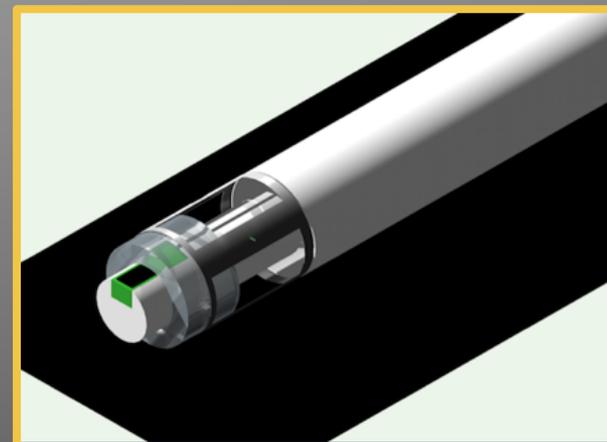
0 counts even
on surgical
instruments!

Probe developments



- Use CMOS technology to lower energy threshold (with INFN & Uni PG) → allow use of other isotopes
 - Matrix design for basic “imaging”

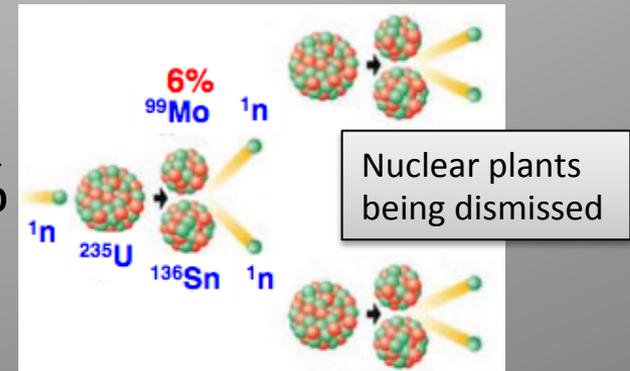
- Develop prototype for endoscopic (laparoscopy/Da Vinci ...) use
 - Multichannel design with p-terphenil



Radiotracers for Radioguided surgery

γ -RGS: the Tc crisis

- ^{99m}Tc is produced from ^{99}Mo decays
- Current production method
 - Canada 50%, Netherland 40%
 - + ...



- Need alternative methods

- $^{100}\text{Mo}(p,2n)^{99m}\text{Tc}$ [direct ^{99m}Tc production] \rightarrow Canada
 - $^{100}\text{Mo}(\gamma,n)^{99}\text{Mo}$, $^{238}\text{U}(\gamma,f)^{99}\text{Mo}$ \rightarrow USA, Canada
 - $^{98}\text{Mo}(n,\gamma)^{99}\text{Mo}$ \rightarrow testing
 - $^{100}\text{Mo}(n,2n)^{99}\text{Mo}$ \rightarrow testing
- } parent ^{99}Mo production
(easier to implement)



Developments in accelerator physics required

β^+ RGS: different isotopes

- ^{18}F not the only tracer
- Mean β^+ energy critical parameter
- Each tracer has different clinical applications

| <i>Isotope</i> | <i>Half-life</i> | <i>β^+ Energy (MeV)</i> |
|----------------|------------------|--|
| C-11 | 20.4 m | 0.385 (99.8%) |
| N-13 | 9.97 m | 0.492 (99.8%) |
| O-15 | 122 s | 0.735 (99.9%) |
| F-18 | 110 m | 0.250 (100%) |
| K-38 | 7.64 m | 1.216 (99.3%) |
| Cu-62 | 9.74 m | 1.315 (97.6%) |
| Cu-64 | 12.7 h | 0.278 (17.9%) |
| Ga-68 | 68.1 h | 0.836 (87.9%), 0.352 (1.12%) |
| Rb-82 | 75 s | 1.523 (83.3%), 1.157 (10.2%) |
| I-124 | 4.18 d | 0.686 (11.3%), 0.974 (11.3%) |



β^- probe on β^+ isotopes

- Positron/ γ separation with copper layers
- Results scaled to 10kBq/ml

| 10 kBq/ml | ^{18}F | ^{68}Ga |
|------------------------------------|-----------------|------------------|
| Counts no shield (e+ γ) | 11.9 \pm 0.3 | 51.2 \pm 0.8 |
| Counts with Cu shield (γ) | 3.0 \pm 0.1 | 1.7 \pm 0.1 |
| Difference (e) | 8.9 \pm 0.3 | 49.5 \pm 0.8 |



β^- - RGS: Other isotopes (I)

- used in Nucl. Med.
- Isotopes of those used in Nucl. Med.
- Same chem family of those used in Nucl. Med.

C. Mancini-Terracciano et al., arXiv:1610.09246

| Isotope | $T_{1/2}(h)$ | $E_g(keV)$ | $I_g(\%)$ | $EP_b(keV)$ | $I_b(\%)$ | Use |
|------------|--------------|------------|-----------|-------------|-----------|----------------------------------|
| ^{18}F | 1.8 | 511 | 200 | 633.5 | 97 | FDG, most tumors |
| ^{21}Si | 2.6 | | | 1491 | 100 | Same family as C (used in PET) |
| ^{32}P | 343 | | | 1710 | 100 | Brain tumors [1] |
| ^{67}Cu | 62 | 93/184 | 16/48 | 377/468/561 | 22/20/99 | Cu-64 in immuno-PET[3] |
| ^{83}Br | 2.4 | | | 935 | 99 | Same family as F |
| ^{90}Y | 64 | | | 2280 | 100 | NET & Brain tumors[1] |
| ^{97}Zr | 17 | 743 | 93 | 759 | 88 | ^{89}Zr used in immuno-PET [2] |
| ^{131}I | 192 | 365/637 | 82/7 | 334/696 | 7/90 | Thyroid[1] |
| ^{133}I | 20.8 | 530 | 87 | 1227 | 83.4 | Thyroid |
| ^{153}Sm | 46 | 103 | 29 | 635/704/808 | 31/49/18 | Bone Cancer[1] |
| ^{177}Lu | 160 | 112/208 | 6/10 | 500 | 79 | NET & Brain tumors[1] |
| ^{188}Re | 17 | 155 | 15 | 1962/ 2118 | 25/72 | Bone & Liver [2] Cancer |

- [1] Review in Yeong C.H. et al. J. Zhejiang Univ. SCIENCE B Vol.15 No.10 P.845-863 (2014)
 [2] van de Watering F.C. et al. Biomed Res Int. 2014;2014:203601.
 [3] Asabella A.N. et al. BioMed Res. Intl. 786463 (2014)



β - RGS: Other isotopes (I)

* Time needed to detect a 0.1 ml residual with FN<5% FP<1% if 3MBq/kg are administered and SUV=4, TNR=8

| Isotope | E_g (keV) | I_g (%) | EP_b (keV) | I_b (%) | T^*_{min} (s) |
|------------|-------------|-----------|--------------|-----------|-----------------|
| ^{18}F | 511 | 200 | 633.5 | 97 | >25 |
| ^{21}Si | | | 1491 | 100 | 0.4 |
| ^{32}P | | | 1710 | 100 | 0.3 |
| ^{67}Cu | 93/184 | 16/48 | 377/468/561 | 22/20/99 | >25 |
| ^{83}Br | | | 935 | 99 | 0.9 |
| ^{90}Y | | | 2280 | 100 | 0.5 |
| ^{97}Zr | 743 | 93 | 759 | 88 | 0.8 |
| ^{131}I | 365/637 | 82/7 | 334/696 | 7/90 | >25 |
| ^{133}I | 530 | 87 | 1227 | 83.4 | 2.8 |
| ^{153}Sm | 103 | 29 | 635/704/808 | 31/49/18 | 3.1 |
| ^{177}Lu | 112/208 | 6/10 | 500 | 79 | >25 |
| ^{188}Re | 155 | 15 | 1962/ 2118 | 25/72 | 0.4 |

 OK with current probe

 High SUV and TNR required: improvements in γ rejection and energy threshold useful

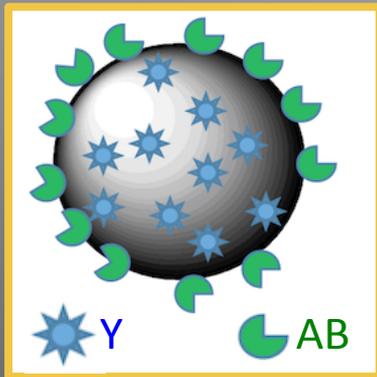
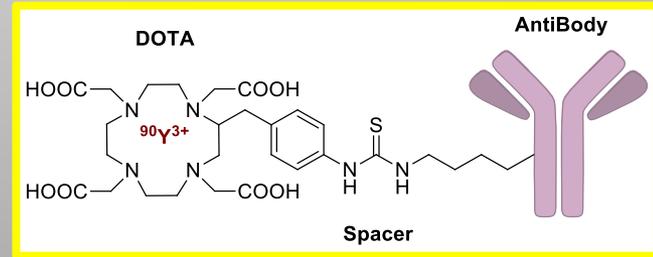
 Significant improvements in γ rejection and energy threshold required



β - RGS: alternative tracers with ^{90}Y

Synthesis of **new radio-tradiotracers** (with ^{90}Y)

- Monoclonal antibodies
(NIMOTUZUMAB) for EGFR receptors
- MIBG



Development of **nano-scale carriers** composed of polymers, antibody and ittrium



Nuclear
Physics

Oncology

Radio-
Chemistry

Nuclear Medicine

Radio-Guided-Surgery

Radiation
detection

Particle
accelerators



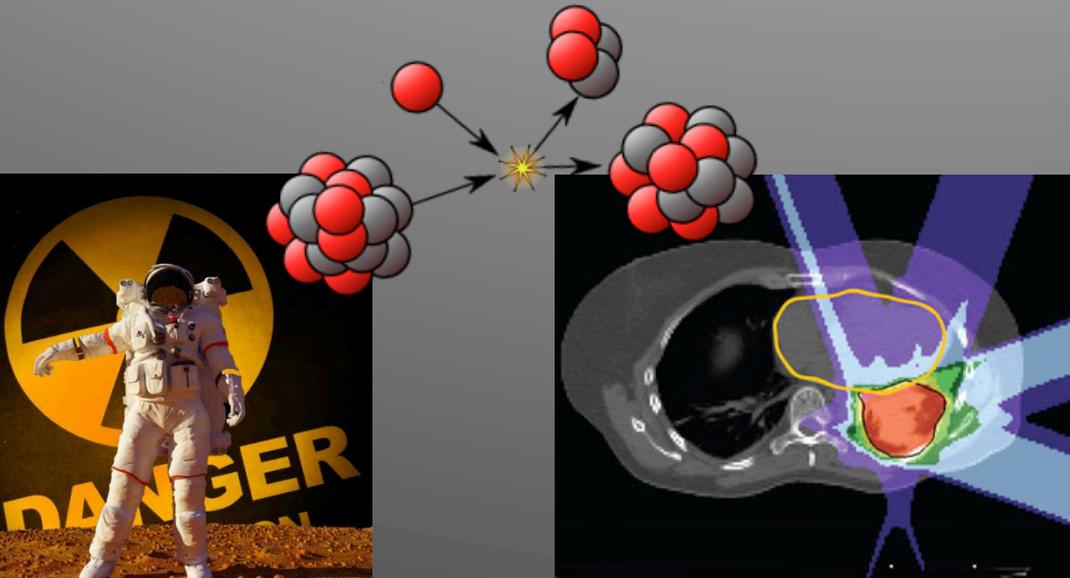
BACKUP

FOOT in pills

Sections/Labs: Bologna, Frascati, Milano, Napoli, Perugia, (Pavia), Pisa, Roma1, Roma2, Torino, Trento

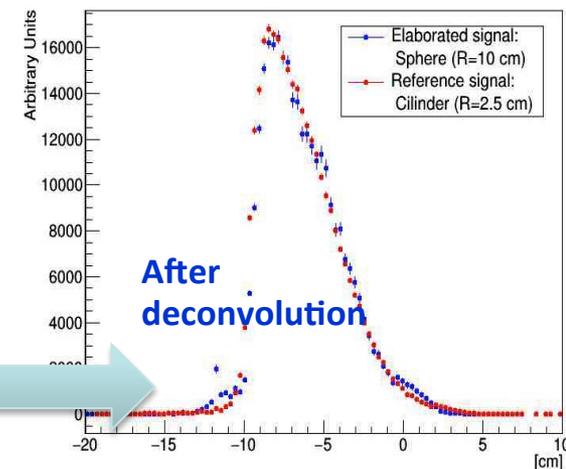
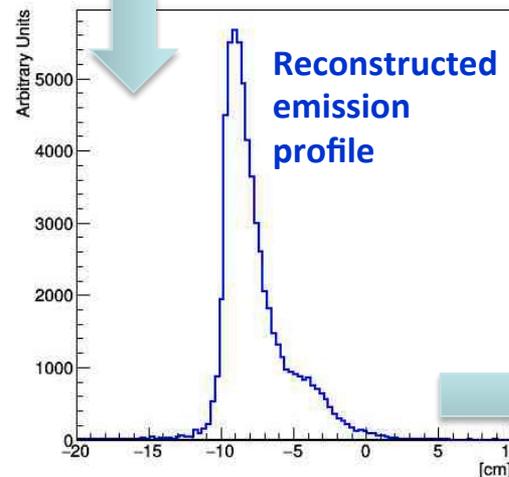
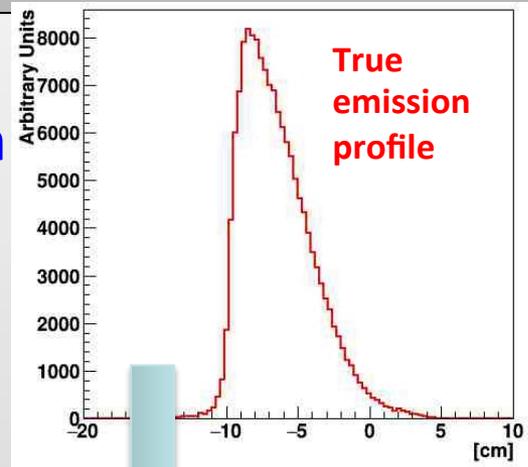
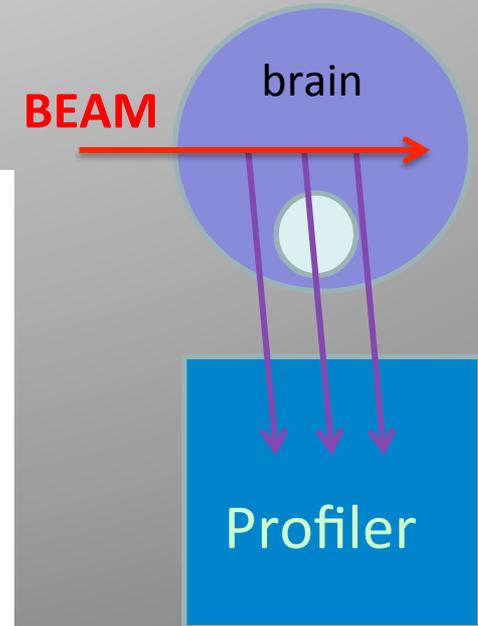
People: ~50 researcher, ~24 FTE

DATA taking foreseen @ CNAO, TIFPA, LNS, BTF



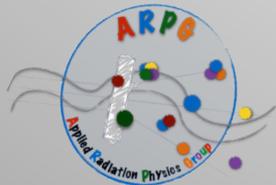
Experiment with translational approach: focus on nuclear physics, physics applied to medicine and radioprotection in space

Dosimetric imaging



□ Generation of calibration database for deconvolution of material absorption using FLUKA MC trained with experimental data.

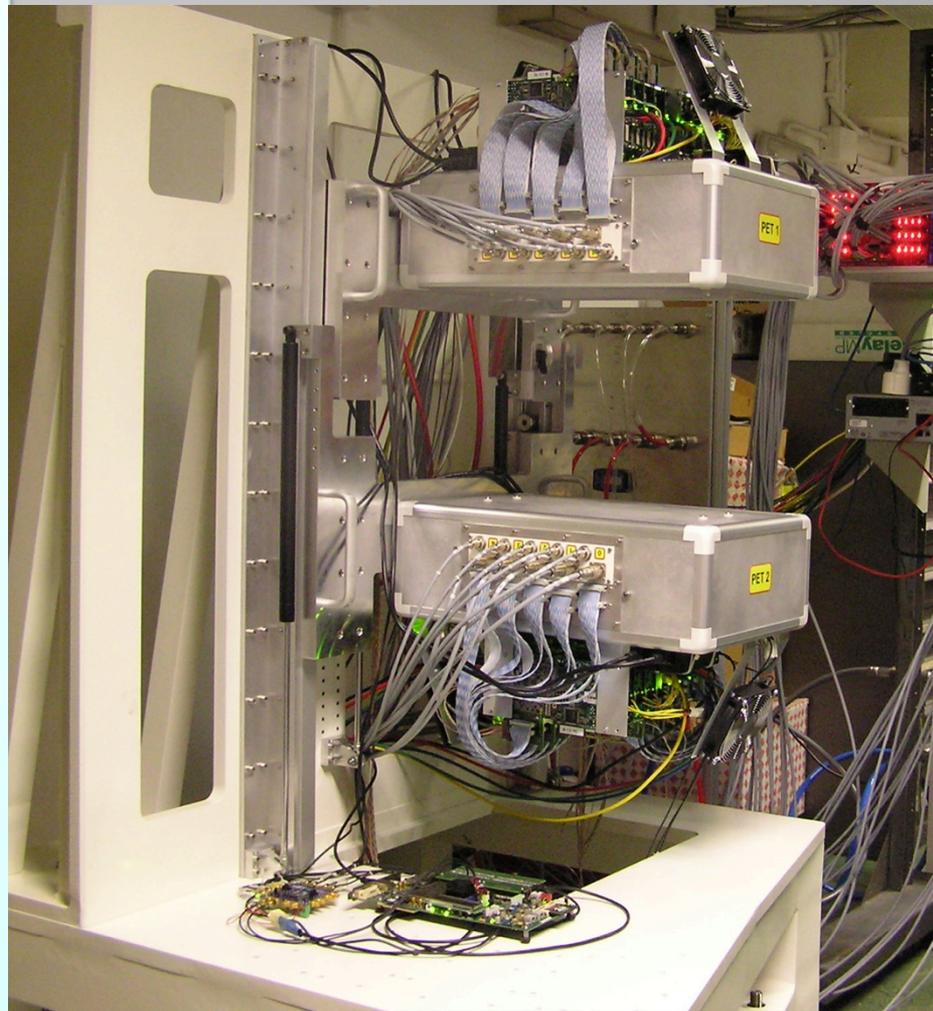
□ Development of lookup table to connect the emission point distribution of the secondary charged particle with the BP, in different, non homogeneous material



The INSIDE PET system

Inside

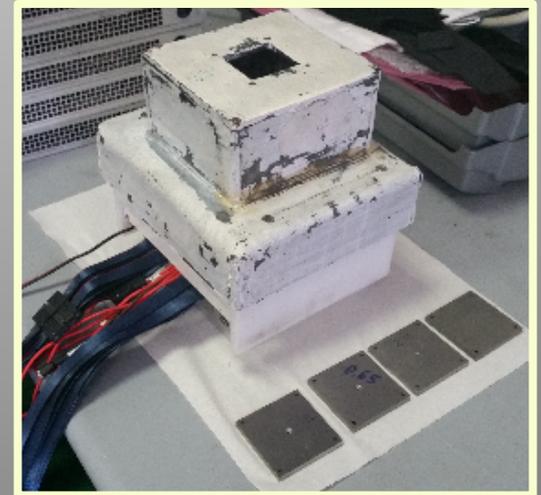
- DAQ sustains annihilation and prompt photon rates during the beam irradiation
- Two planar panels each 10 cm x 20 cm wide. Each panel will be made by 2 x 4 detection modules
- Each module is composed of a pixelated LYSO scintillator matrix 16 x 16 pixels, 3x3 mm² crystals, 3.1 mm pitch, for a total sensitive area of 5x5 cm²
- One SiPM array (16x16 pixels) is coupled to each LYSO matrix. 200 ps FWHM TOF capability



Current Efforts (II)

Setup the whole chain for radio-tracer development:

- cold synthesis
 - hot synthesis
 - in vitro tests
 - animal tests
- equip a facility for
animal tests with radioactivity



→ Need imaging capable to measure biodistribution of β -emitting tracers → **SPECT with Brehmsstrahlung**



Nucl . Medicine and Chemistry



Chemistry and CTF