

Giornate Romane su “Particelle e Fisica Applicata”

Dipartimenti di Fisica e Matematica

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Development of a diagnostic system for
therapeutic proton beam and indirect monitoring
of patient released dose

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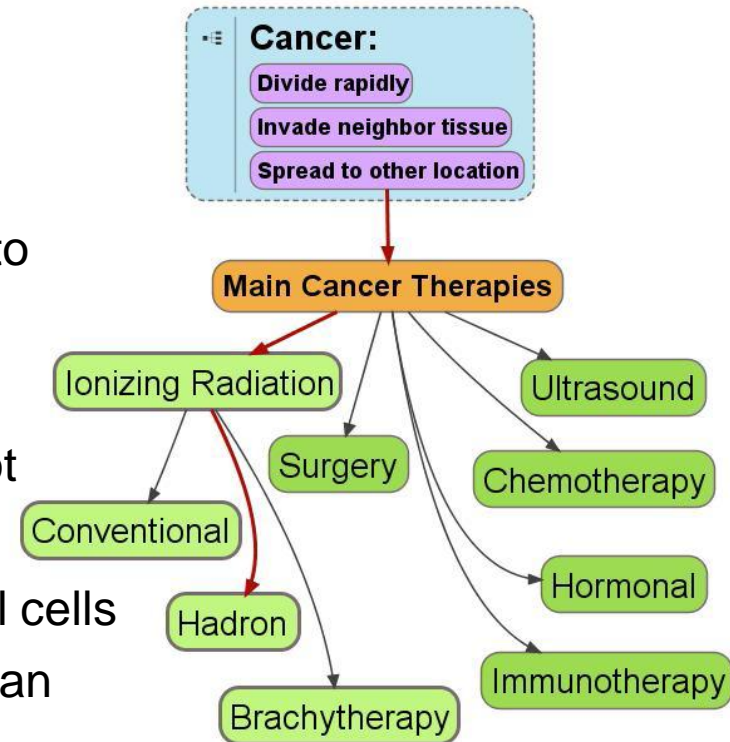
Cancer Relevance

Cancer affects 1/3 of people – first cause of death between 45 and 65 years

- ❑ Multiple Approaches: surgery, chemotherapy, immunotherapy, radiotherapy, hormonal.
- ❑ Approx. 1/4 patients owe their 5 years survival to radiotherapy

Radiotherapy plays a leading role. Radiation is not selective, but it is possible to achieve selectivity:

- ❑ Tumor cells are more radiosensitive than normal cells
- ❑ Reparability of malignant cells is less efficient than normal cells
- ❑ Dose delivered can be conformed to diseased tissue



Any additional progress can improve the number of the cured patients and the quality of live: the use of hadrons is presently on of the most promising way in specific cancers

Modern radiotherapy consists mainly of:

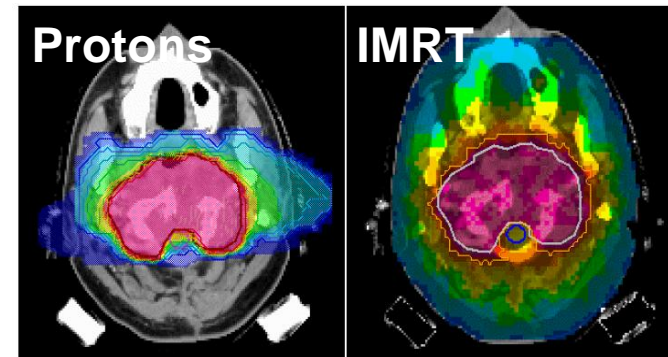
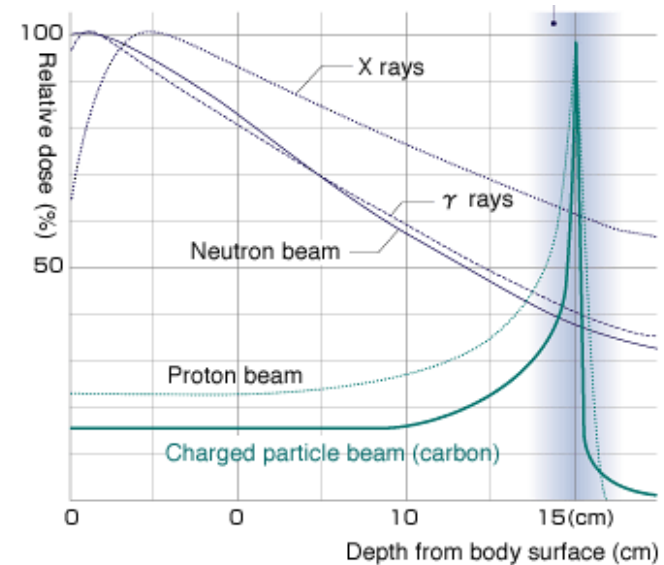
1. Conventional radiotherapy with electrons and photons up to 25 MeV

- ❑ the best choice for the treatment of the shallower tumors (electrons)
- ❑ high conformation with IMRT
- ❑ the most diffused option in radiotherapy treatments

2. Hadrontherapy

- ❑ more suitable for radioresistant tumors
- ❑ higher conformation (intrinsic)
- ❑ about 40 centers around the world

3. Others: BNCT, (Pion Therapy)



G. Kraft, GSI, Biophysik, Darmstadt and J. Debus, DKFZ, Heidelberg

Protontherapy with LINAC



Proton therapy accelerators produce beams with the following main features:

- energy high enough to reach the deepest tumors (up to 240 MeV)
- a beam current adequate to achieve treatment times comparable to those of conventional facilities
- the capability to provide uniform doses to the target volume

Hadrontherapy currently uses synchrotrons, cyclotrons or synchrocyclotrons

LINAC can be considered a valid option:

- There is no power loss from synchrotron radiation (simpler radioprotection)
- Injection and extraction are simpler than in circular accelerators
- LINAC can operate at any duty factor, working at high repetition rate and allowing pulse current modulation**
- Expected to be cheaper**

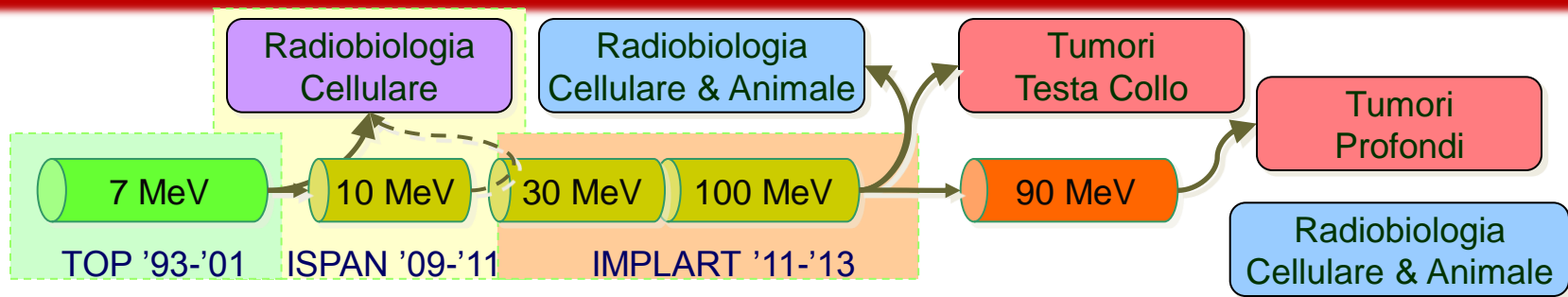
... but

- The technology is not fully proved for proton-therapy
- ions can not be accelerated in a proton LINAC

Protontherapy with LINAC: the TOP-IMPLART project

The TOP IMPLART (ENEA - ISS - IFO) project aims to realize an innovative proton therapy facility, based for the first time, on a linear accelerator.

Funding: ISS before 2002, Region after 2009



TOP-IMPLART LINAC features:

- ❑ The **active scanning (3+1D)** in
 - **Intensity** (instantaneous released dose)
 - **Energy** (depth)
 - **Transversal Position** (X/Y)

allows a highly conformational therapy ⇒ **need of accurate monitoring of the beam parameters on a pulse by pulse basis**

- ❑ The modular implementation allows a modular/progressive development (based on the financial flow)
- ❑ The use of widely diffused (3 GHz) radiofrequency technology reduces realization and maintenance costs

Development of the beam monitor system for the TOP_IMPLART LINAC with indirect information of dose delivery

- ✓ **Suitable for the monitoring of proton (or electron) beam in other facilities**

The monitoring system design must adhere to the following requirements:

- The beam parameters (position, intensity profile, direction/emittance) are continuously monitored independently from the beam controls
- Quick response (faster than beam pulse period)
- Provide feedback information to correct small deviation from the planned therapeutic treatment
- Automatic shutdown irradiation in case of large (not recoverable) deviation from planned parameters
- High reliability

Beam monitor system requirements for the TOP-IMLART LINAC



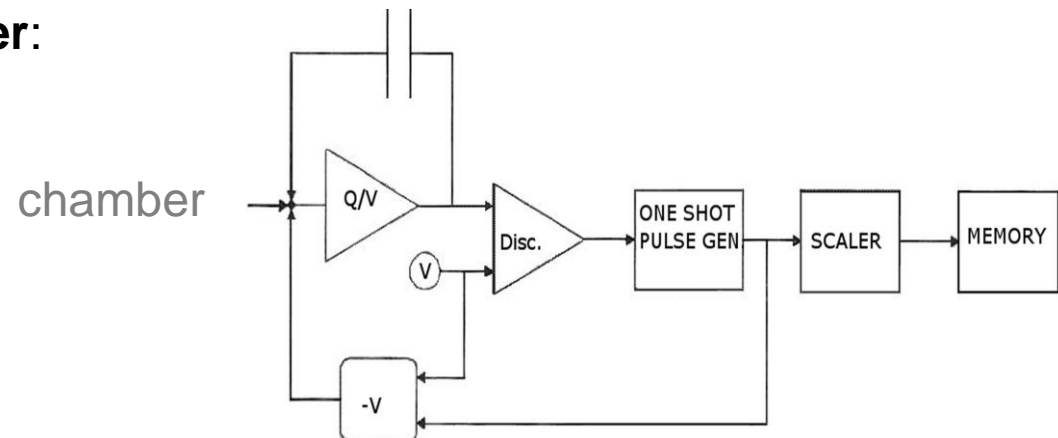
Pulsed beam characteristics		Beam monitor system specifications
■ Energy in the range	130-250 MeV	■ Light compact chamber (segmented)
■ Beam cross section	1-10 mm	■ Good spatial resolution ($\sim 1/10$ mm)
■ Beam current	0.1-10 μA	■ Wide dynamic range (10^4 at least) for each channel
■ Average current:	10 nA	■ Good sensitivity (~ 100 fC)
■ Pulse period	1-5 μs	■ Zero dead time (or near zero)
■ Pulse frequency	100-400 Hz	■ Rapid response (< 1 ms)
(it allows dose repainting without much time demanding)		■ Typical channels: few 100

Beam monitor in protontherapy

Beam monitoring systems in proton therapy are commonly based on **couples of ionization chambers**.

The chamber front-end electronics is generally performed by using traditional electronic schemes, e.g. **rate meter**:

*Works well on long pulses
(order of msec)*



- Sensitivity is related to the “quantum” voltage V
- Dynamic range is equal to the maximum number of pulses generated in the time duration of the beam pulse (high performance frequency/converter and scaler $\sim 100 \text{ MHz} \cdot 10 \mu\text{s}$, the dynamic range does not exceed 1000)

an alternative:

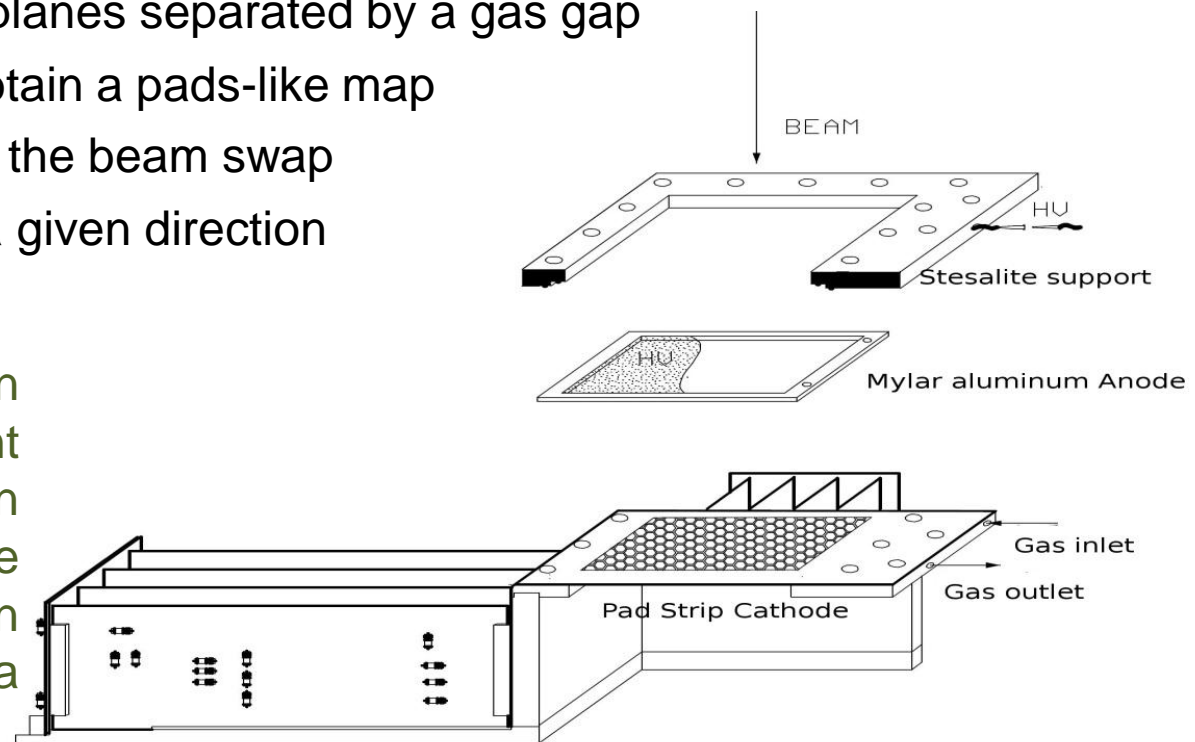
- Charge amp and good performance ADC converters (limited by the input stage saturation, the ADC bit number, achieving the dynamic range of ~ 1000)

The beam monitor developed for the TOP-IMPLART LINAC

The TOP-IMPLART monitor system is based on 2D segmented ionization chamber driven by a dedicated front end electronics designed to **OVERCOME** limitations of the traditional electronics schemes (ratemeter, charge amp and ADC converters):

- the prototype consists of 2 planes separated by a gas gap
- the anode is engraved to obtain a pads-like map
- active surface able to cover the beam spot
- pads are connected along a given direction
- dedicated electronics

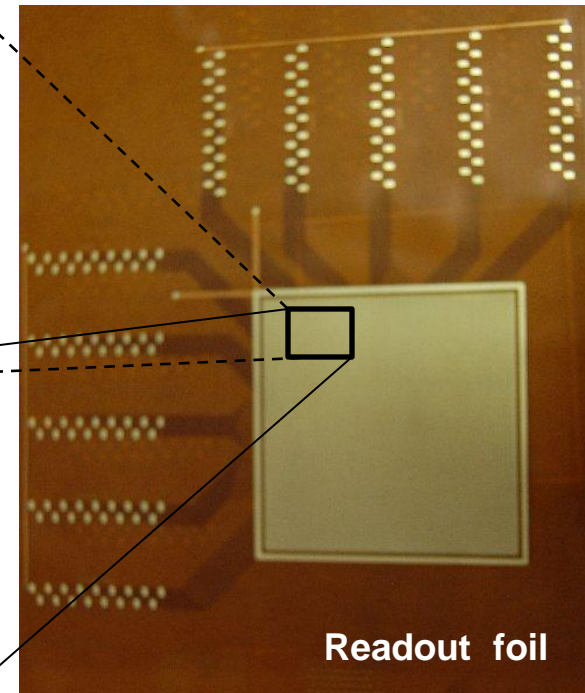
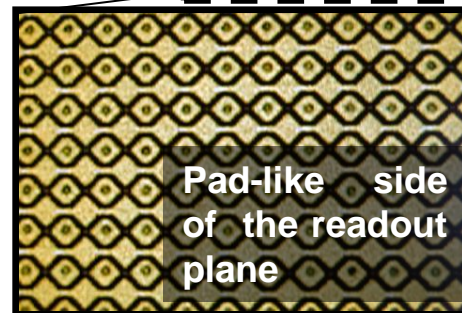
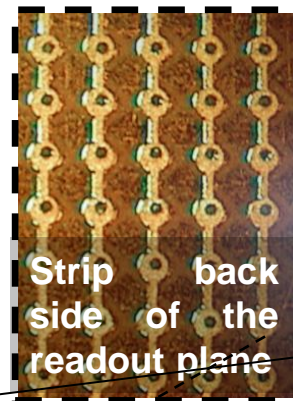
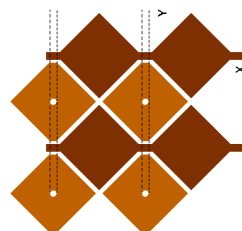
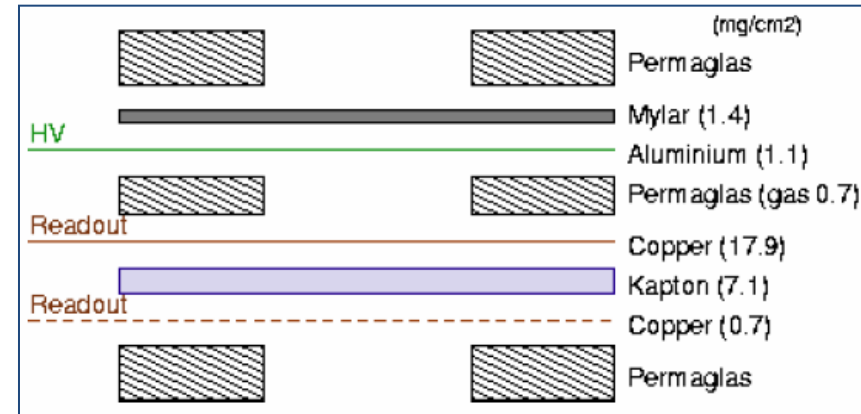
The chamber has been designed according to recent developments in micro pattern gaseous detectors and the readout foil has been produced by Rui De Oliveira at TS-DEM, CERN



The ionization chamber

The chamber operates in ionization region and has the following characteristics:

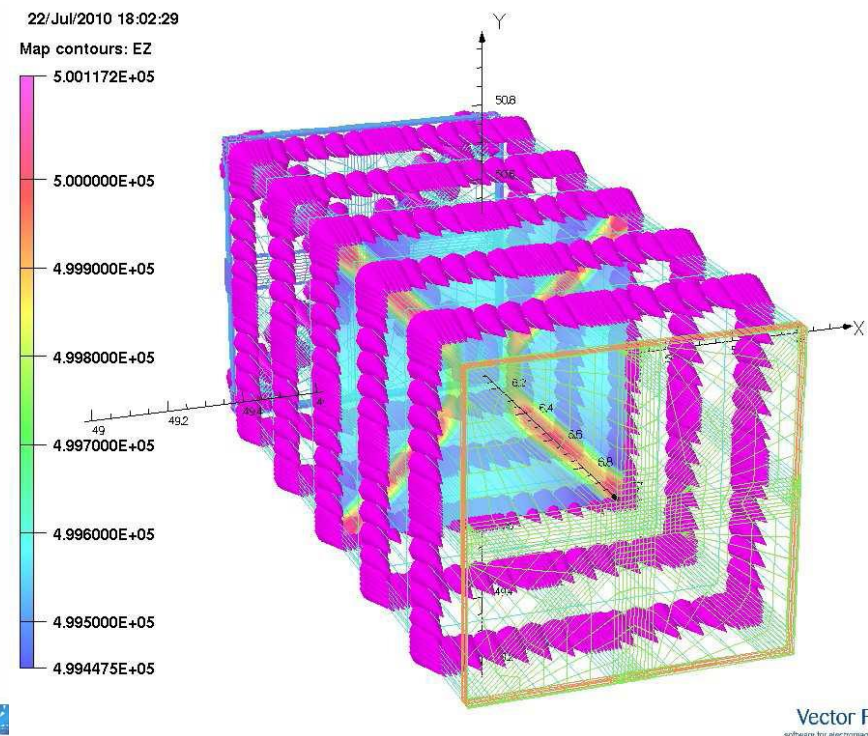
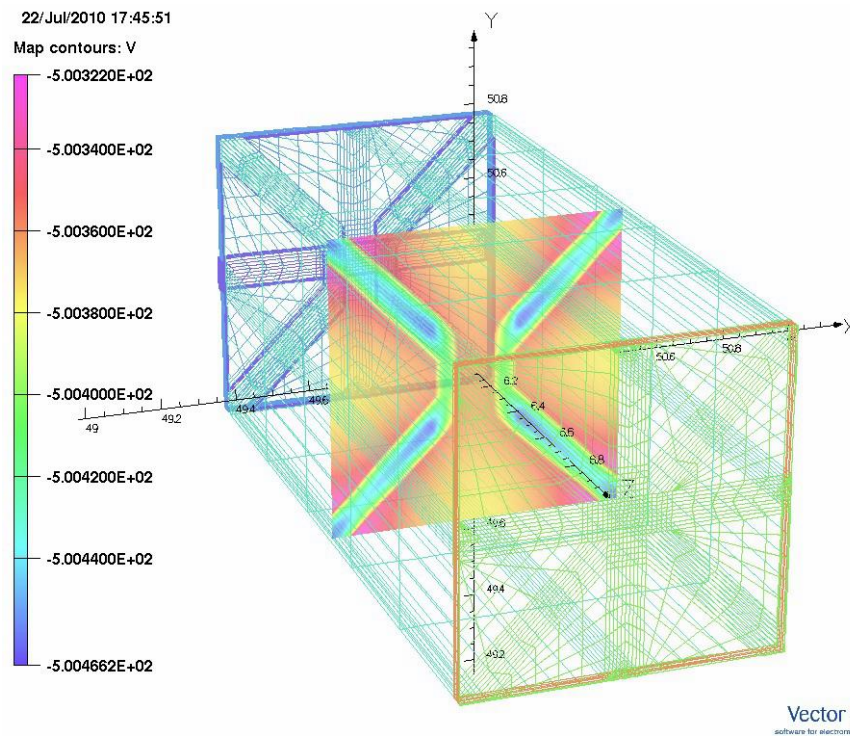
- **GAP** between anode and cathode: **2mm**
- Anode and cathode **ACTIVE AREA**: **7x7cm²**
- **ANODE**: Al (**5μm**)
- **CATHODE**: Kapton (**50 μm**) with **PADs** in **Cu** (**15 μm**) on the beam incidence side and **STRIPS** in **Cu** (**15 μm**) on the other side
 - ❖ **PITCH**: **875 μm**
 - ❖ **Gap between pad**: **120 μm**
- **CHANNELS**: **80 x 80**
- **BIAS**: **300 V**



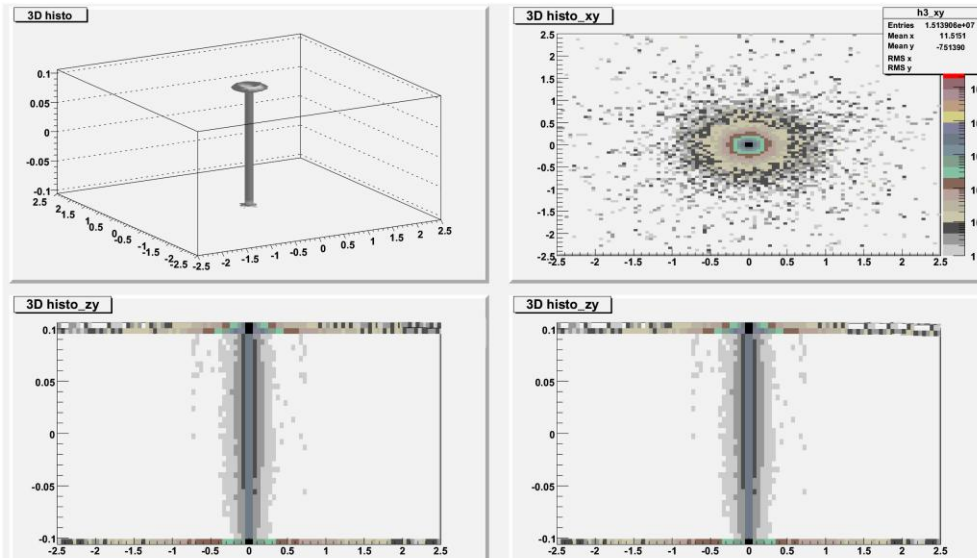
Simulation of the chamber Electrostatic Field

OPERA (OPerating environment for Electromagnetic Research and Analysis) simulation of the chamber field

- ❑ Relative variation of the potential in the middle of the gap less than **0,03%**
- ❑ Relative variation of the field in the middle of the gap about **0,13%**



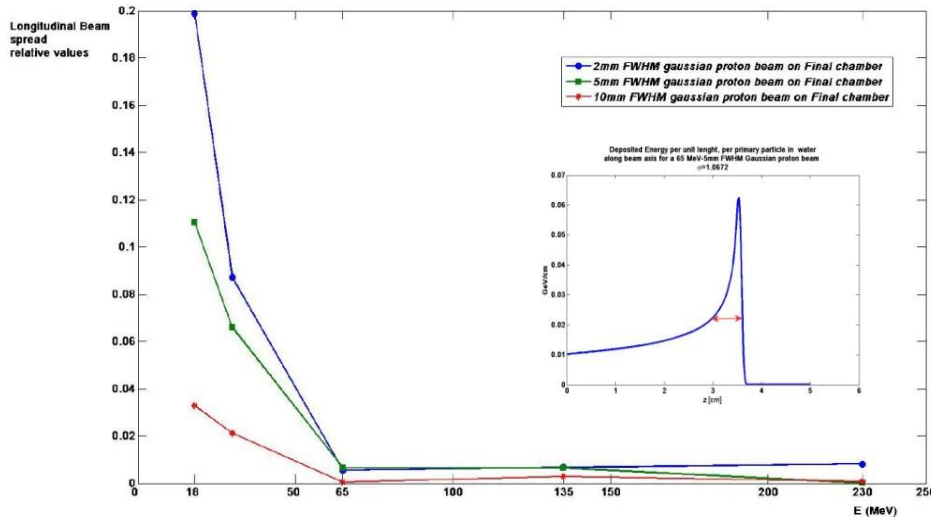
Simulation of the perturbation effect induced by the chamber on the dose delivery



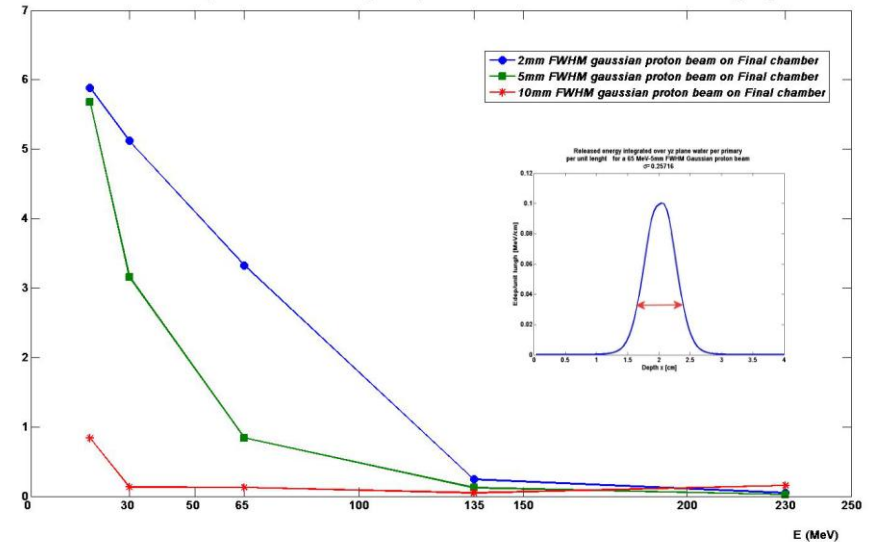
Fluka Simulation on water phantom.

- Longitudinal relative variation of the Bragg peak spread less than **1%** above 65 MeV
- Transversal relative variation of the Bragg peak spread less than **3%** above 135 MeV

Longitudinal spreads of 2-5-10mm FWHM proton beams on Final chamber in the 18-230 MeV energy range



Transverse spreads of 2-5-10mm FWHM gaussian proton beams on Final chamber in the 18-230 MeV energy range



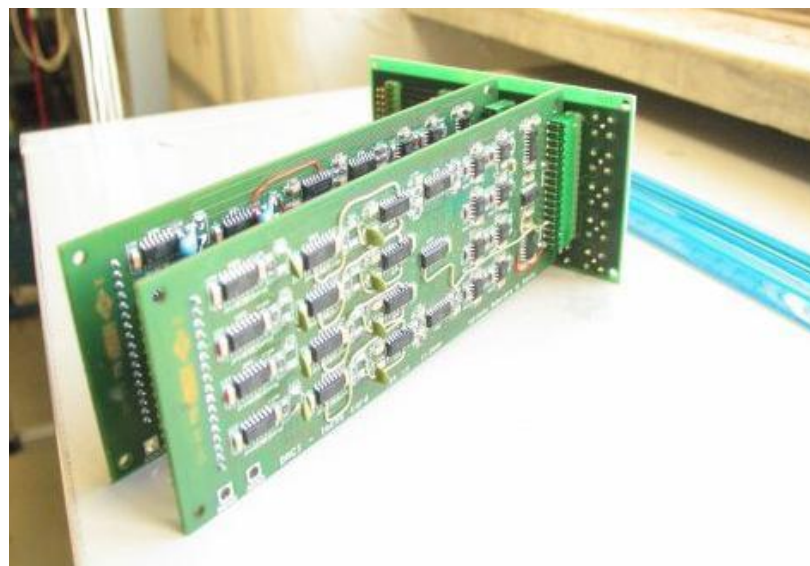
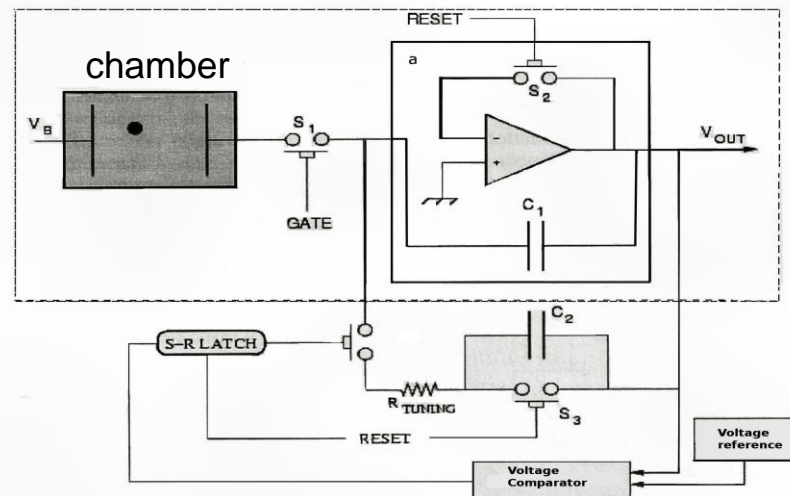
The readout electronics

Based on a “dual range” trans-impedance amplifier with “sample and hold” mechanism (able to ensure an adequate charge dynamic range and sensitivity).

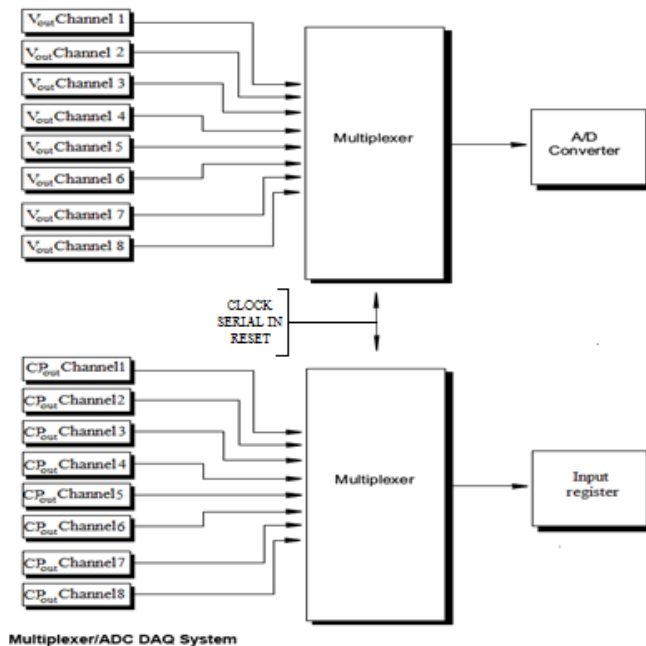
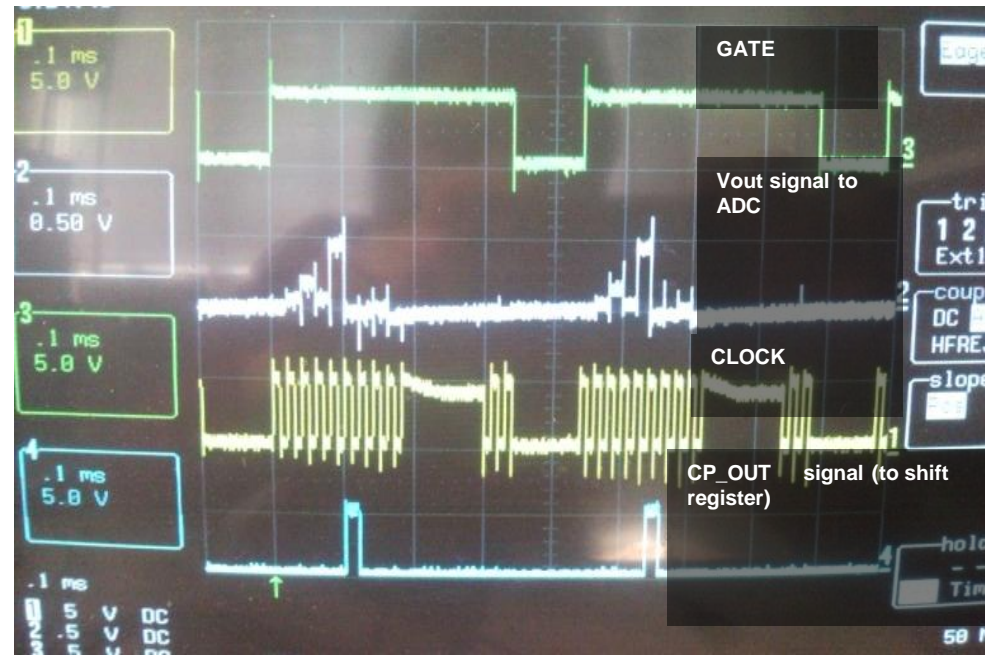
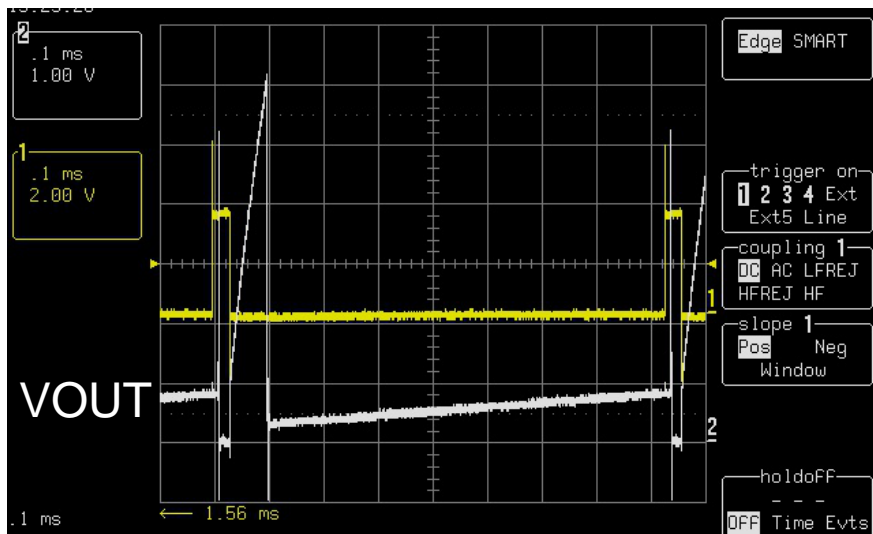
The **readout electronics** prototype controls 64 channels (but it is possible cascade several backplanes) and consists of:

- **4 front-end cards** (1 card/16 channels), made of 2 two main blocks:
 - the input stage with the trans-impedance amplifier and dual range logic
 - the multiplexing logic that route the collected charges into a single ADC
- a **passive backplane** which provides power supply and distributes the signals between front-end and controller

Dual Range logic

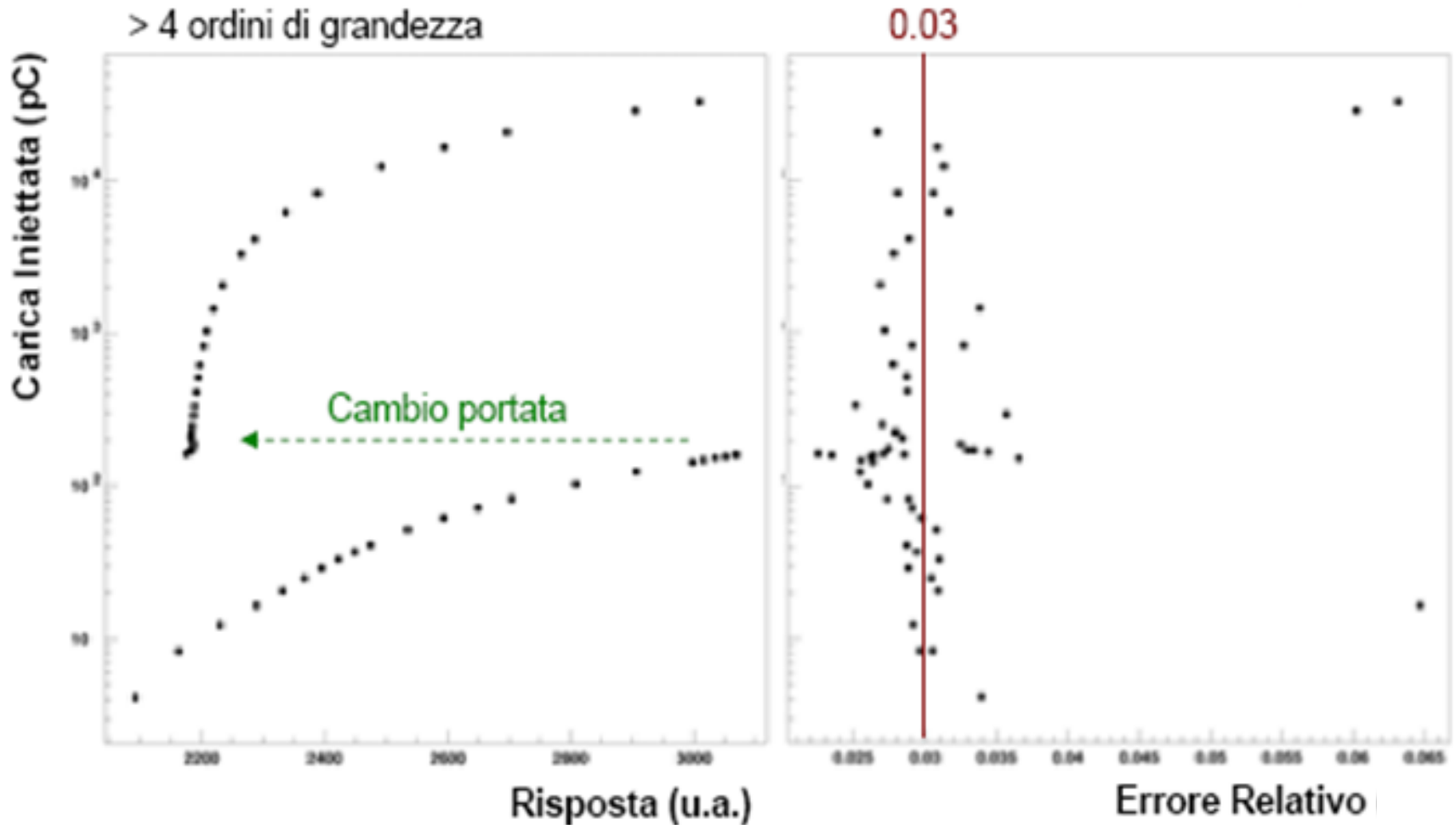


Dual Input Regime and MUX



- ❑ Single channel charge is stored on the trans-impedance capacitance (sampled and hold)
- ❑ Analog values (up to 64) are multiplexed on a single ADC

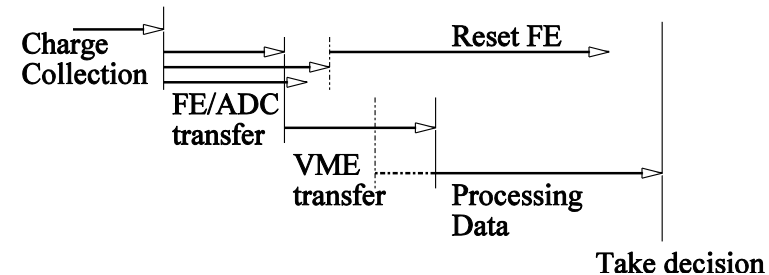
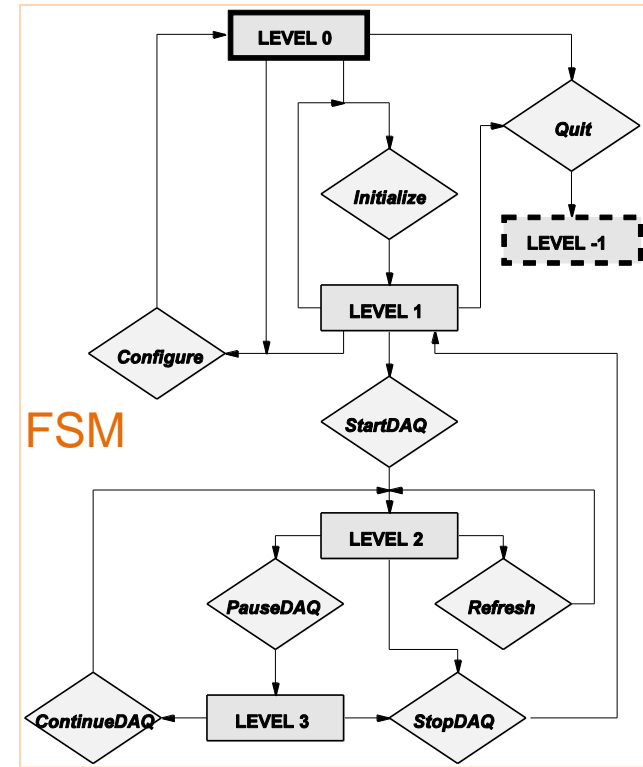
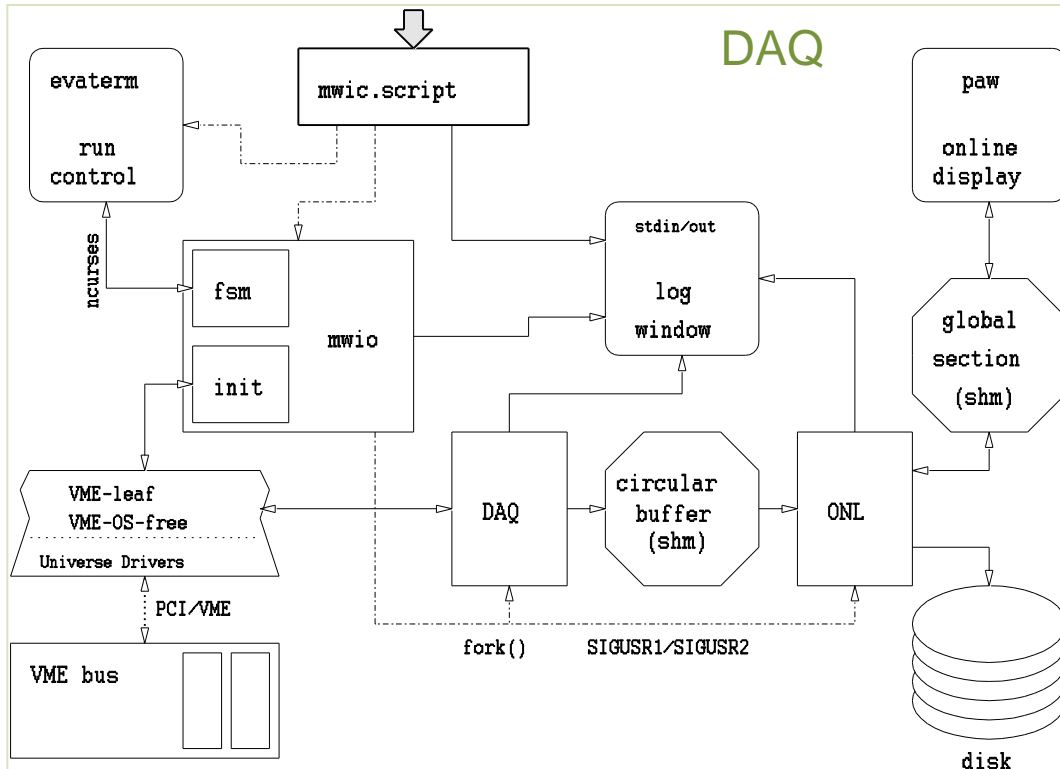
Dual Regime performance



- ❑ Input dynamic range larger than 10^4 (from about 2 pC to tens of nC)
- ❑ Relative sensitivity less than 3% (minimum absolute sensitivity of 70 fC)

The data acquisition and processing system

The DAQ system is based on VME standard components, managed by a modular software in C. Software use reliable FSM, multithreads and shared buffers used by the processing algorithms that produce the feedback to the beam control system within ms.



Current activity



- Lab test almost completed on electronics prototype
- DAQ software ready, processing to be optimized
- Chamber under construction

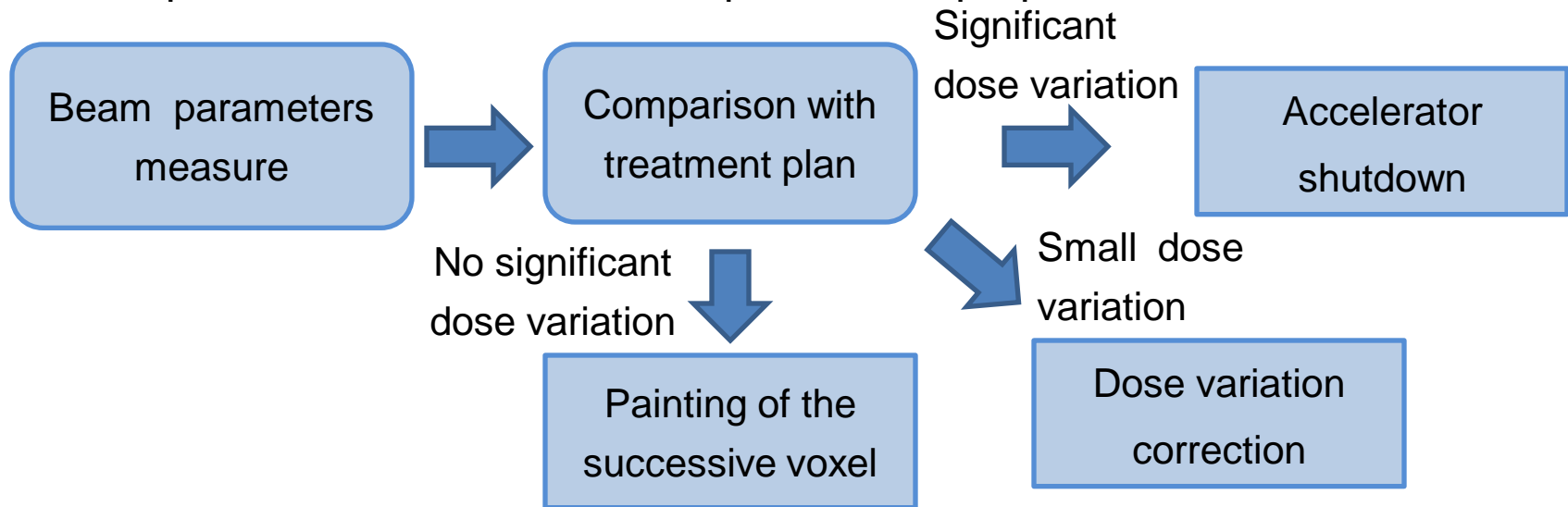
- Finalization of the chamber prototype
- Characterization with rad source and under test beams (X ray and charged beam)
- Tests and characterization under the TOP proton beam (up to 20 MeV)
- Realization of a chamber telescope (with 3 chambers, at least)

- Electronics control system miniaturization with the use of a microcontroller which will replace the VME modules
- Further development of the acquisition and processing software

Link with patient monitor and “analytical” TPS



- ❑ The monitor system must check the consistency of the assessed dose with the planned dose in real time to provide the proper feedback:



- ❑ A feedback system + patient monitor (e.g. movement) + a fast Treatment Plan System (using an analytical formulation of the dose distribution):
 - evaluate, in real-time, the actual delivered dose,
 - calculate in real time, the dose correction (if any) for the next pass

Considerazioni finali

- Tanto più localizzato è il rilascio di dose, tanto più precisi debbono essere gli strumenti per la sua pianificazione, controllo e verifica
- Un sistema di protonterapia in grado di competere con le tecniche più avanzate di radioterapia convenzionale deve integrare un **sistema dinamico** di rilascio del fascio

- L'utilizzo ottimale di un tale sistema richiede lo sviluppo e "fine tuning" di un gran numero di componenti fondamentali: **TPS, Radiobiologia, Dosimetria, Diagnostica, Sala Trattamento, Imaging ...**

